Transplantation of neural stem cells encapsulated in hydrogels improve functional recovery in a cauda equina lesion model

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Abstract

Background This study explored the therapeutic effects of transplantation of neural stem cells (NSCs) encapsulated in hydrogels in a cauda equina lesion model. **Methods** NSCs were isolated from neonatal dorsal root ganglion (DRG) and cultured in three-dimensional porous hydrogel scaffolds. Immunohistochemistry, transmission electron microscopy, Luxol fast blue staining, TUNEL assay were performed to detect the differentiation capability, ultrastructural and pathological changes, and apoptosis of NSCs. Furthermore, the functional recovery of sensorimotor reflexes was determined using the tail-flick test. **Results** NSCs derived from DRG were able to proliferate to form neurospheres and mainly differentiate into oligodendrocytes in the three-dimensional hydrogel culture system. After transplantation of NSCs encapsulated in hydrogels, NSCs differentiated into oligodendrocytes, neurons or astrocytes *in vivo*. Moreover, NSCs engrafted on the hydrogels decreased apoptosis and alleviated the ultrastructural and pathological changes of injured cauda equina. Behavioral analysis showed that transplanted hydrogel-encapsulated NSCs decreased the tail-flick latency and showed a neuroprotective role on injured cauda equina. **Conclusions** Our results indicate transplantation of hydrogel-encapsulated NSCs promotes stem cell differentiation into oligodendrocytes, neurons or astrocytes and contributes to the functional recovery of injured cauda equina, suggesting that NSCs encapsulated in hydrogels may be applied for the treatment of cauda equina injury.

Background

Cauda equina syndrome (CES) is a neurological disease which is usually caused by central lumbar disc herniation. The consequences of CES, such as neuropathic pain, lower extremity dysfunction, and sexual dysfunction are extremely frustrating [1]. It greatly affects the patient's mental and physical condition and causes enormous economic impact to society. Although this disease has a low incidence in the population, ranging from 1:33,000 to 1:100,000 inhabitants, its sequelae still generate high public healthcare costs [2]. Current treatment strategies include application of corticosteroid, surgical stabilization and decompression, although effective but with unsatisfied therapeutic efficacy [3,4]. Because of the poor self-repair ability of nerve tissue, especially those in the central nervous system, the therapeutic effects of surgery and neurotrophic drugs on cauda equina injury-induced CES is limited.

Neural stem cells (NSCs) can make copies of themselves and generate different mature cell types. They are promising candidate cells for neural transplantation treatment of neurological disorders, such as brain trauma, spinal cord injury, peripheral nerve injury [5-7]. Many studies indicate that stem cells foster host axons to grow into the grafted spinal cord [8-10]. In addition, induced pluripotent stem cells differentiate into astrocytes, neurons and oligodendrocytes and further improve functional recovery after spinal cord injury [11]. Nevertheless, application of stem cell transplantation therapy is limited by the poor cell survival at the injury site. Thus, development of novel approaches to maintain neural stem cell viability is important to achieve ideal therapeutic outcomes.

Recently, tissue engineering has been developed that could provide solutions to the problem of stem cell deaths during transplantation [12]. Biopolymer hydrogels are designed to promote stem cell survival after cerebral transplantation, exhibiting promising therapeutic role in central nervous system damage [13]. As previously reported by Singh et al, neural stem cells derived from adult dorsal root ganglia not only retain the multi-differentiation potential, but also have a tendency to differentiate into sensory neurons after transplantation, supporting that dorsal root ganglion neural stem cells (DRG NSCs) may be useful for repair of damaged cauda equina [14]. In the present study, NSCs were isolated from neonatal dorsal root ganglion (DRG), encapsulated in three-dimensional porous hydrogel scaffolds, and used to repair damaged cauda equina in a rat model of CES.

Materials And Methods

Animals

Male Sprague-Dawley rats weighing 200-250 g and aged 6-8 weeks were purchased from the Animal Center of the Second Military Medical University. The surgical interventions for animal experiments were approved by the Ethical Committee of the Shanghai Jiao Tong University School of Medicine, and the animals were cared for in accordance with the Guide for the Care and Use of Laboratory Animals after the surgery.

Culture of DRG-NSCs

DRG were dissected from postnatal day 2 rats, mechanically dissociated in Hank's balanced saline solution, pH 7.4, and seeded in Dulbecco's modified Eagle's medium (DMEM)/F12 (Invitrogen) supplemented with 2% B27, 10 ng/mL epidermal growth factor (EGF), and 10 ng/mL basic fibroblast growth factor (bFGF). NSCs were cultured in a 6-well culture plate at a density of 50-100 cells/ μ L with 5% CO₂ at 37°C. The medium was changed 2-3 times a week. The dissociated DRG cells formed clusters or neurospheres within 72 hours. During the passage of neurospheres, the contaminated neurosphere should be removed from each culture hole. The neurospheres and culture medium in the whole culture plate should be transferred to a 15mL centrifuge tube, centrifuged for 200g 5 minutes, and the supernatant should be discarded. 2mL trypsin was added to the cells precipitation. Use Pasteur pipette to gently blow the neurospheres, place it at 37°C for 20 minutes, centrifugation, and discard the supernatant. The precipitation was suspended in a small amount of medium, gently beaten and mixed, counted, and then laid in a 6-well plate, each hole about 200-300 neurospheres [15].

After 3 generations of subcloning, the NSCs derived from the neurospheres. Some of them were subjected to lentivirus transfection for carrying green fluorescent protein (GFP) .

Hydrogel preparation

Hydrogels were purchased from Beaver Nano-Technologies Co., Ltd, China. Hydrogel products are made from polypeptide nanomaterials. After entering the body, the gelation process can be initiated quickly in

the damaged part, and then half liquid or solid hydrogel can be formed in about 30 seconds.

Hydrogel pretreatment: The original solution of the hydrogel was treated with ultrasonic water bath for 30 minutes at room temperature to reduce the viscosity of the original solution.

Preparation of cells working solution: the NSCs suspension was centrifuged at low speed to remove the supernatant. 5mL of 10% sterile sucrose solution was added to the collected cells to resuspend the cells. The cells suspension was centrifuged again, and the supernatant was discarded to remove the remaining ionic components in the protocell precipitation. Then, the cells were resuspended with 50 μ L 10% sterile sucrose solution to prepare salt ion free isotonic cells suspension.

Preparation of hydrogel cells mixture: The 50 μ L pretreatment hydrogel solution was mixed lightly with 50 μ L NSCs suspension. Slightly 100 μ L Phosphate buffer saline was added to the upper layer of the above mixture. Then, the PBS layer and the hydrogel layer were mixed evenly with the pipette, and finally 200 μ L hydrogel cell mixture was obtained. The final concentration of the hydrogel is 0.25%.

Model establishment and NSC transplantation

Forty-eight SD rats were randomly divided into sham, CES model and NSCs transplantation groups. After anesthesia with chloral hydrate, laminectomy was performed at the lumbar 4 and a silicone band (10 mm long, 1 mm wide, and 1 mm thick) was placed under the laminae of the L5-6 vertebra to produce the CES animal model [15,16]. Sixteen rats were subjected to NSC transplantation, and another 16 rats were used as control. A sham operation was performed with a simple laminectomy but without contusion injury (n = 16).

For transplantation of NSCs, we removed the silicone 7 days after the compression injury and then intrathecally injected 12 μ L 0.25% hydrogels containing approximately 1000,000 NSCs (transfected with lentivirus vectors carrying GFP) using a micropulled pipette connected to a Hamilton syringe. As control, 12 μ L 0.25% hydrogels containing no NSCs was injected into the subarachnoid space.

Immunohistochemistry assay

The rats were perfused with 4% paraformaldehyde as the fixative. The cauda equina was then extracted, placed in EDTA solution, and heated in an oven for antigen retrieval. Then, 15- μ m thick sections of the cauda equina around the lesion site were prepared longitudinally. The tissue sections were permeabilized with 0.2% Triton X-100 and blocked in blocking solution for 1 hour at room temperature. After rinsing with PBS, the sections were incubated with primary antibodies against O4, β III-tubulin, glial fibrillary acidic protein (GFAP) and S100 overnight at 4°C followed by incubation with secondary antibodies for 1 hour at 37°C. The slices were stained with Hoechst for 10 minutes and images were photographed by inverted fluorescence microscopy. The staining of NSCs in vitro was the same as the above methods.

Ultrastructural imaging

For transmission electron microscopic (TEM) studies, the sections were fractured with liquid nitrogen and quenched in hydrogen peroxide solution. After rinsing in PBS, the sections were prepared for ultra-thin sectioning. Tissue sections were fixed in osmium tetroxide, dehydrated in ethanol, and embedded in resin. All samples were observed under TEM.

Luxol fast blue staining

Tissue sections were stained with Luxol fast blue (LFB) to detect myelin damage as previously described [17]. Briefly, the cauda equina sections were immersed in Luxol fast blue solution in an oven overnight. After rinsing in 95% ethanol and distilled water, the pathological changes of nerve fibers were observed under a light microscope.

TdT-mediated dUTP-biotin nick end labeling (TUNEL) staining

Apoptosis of cauda equina were measured by using a TUNEL detection kit according to the manufacturer's instructions (Sigma, USA). In brief, paraffin-embedded tissue sections (4-mm-thick) were dewaxed, rehydrated, and incubated with reaction mixture of terminal deoxynucleotidyl transferase for 1 h. After rinsing in PBS, the sections were incubated with biotinylated antibody and ABC complex, and photographed in a light microscope (Zeiss) equipped with a digital camera.

Behavioral analysis

For the tail-flick test, the rats were immobilized 20 min before the test, and the tail was placed over a slit. A beam of light from a projection lamp (voltage of 18.5 V) was focused on the tail skin at the junction between the middle and distal 1/3 of the tail. The latency to respond was recorded with a maximal 15s radiant heat stimulus [15].

Statistical analysis

Experimental data are presented as mean $\pm$ SD. One-Way ANOVA was used for comparison of different groups. Results were considered statistically significant when the *P* value was less than 0.05.

Results

Characterization of NSCs in hydrogel scaffolds

NSCs were isolated from the neonatal rat DRG and cultured in proliferation culture medium for different days. We observed that many cells were floated in the medium and formed neurospheres (Figure 1A). Then, NSCs were successfully grown in 0.25% and 0.5% hydrogels (Figure 1A). Immunohistochemical staining showed that cells were positive for nestin and P75R, two markers of NSCs (Figure 1B).

Differentiation of NSCs in hydrogel scaffolds

After 7 days of differentiation in vitro, the neural progenitors (without GFP) in the spheres attached to the hydrogel scaffolds and differentiated into different types of cells. Immunohistochemical staining showed that most of the NSCs differentiated into O4+ oligodendrocytes, and only a very few cells differentiated into S100+ Schwann cells, β III-tubulin+ neurons and GFAP+ astrocytes (Figure 2B).

Differentiation of NSCs following transplantation in the injured cauda equina

To more easily track cells, NSCs were transfected with lentivirus vectors carrying GFP before transplantation in rats (Figure 2A). Next, we successfully established the rat model of cauda equina injury and transplanted hydrogel-encapsulated NSCs (Figure 3A). To detect the viability of the transplanted NSCs in the cauda equina, the frozen sections were imaged by confocal microscopy after 7 days of transplantation. As expected, GFP-positive grafted NSCs were present in the injured cauda equina (Figure 3B). Furthermore, immunostaining of the sagittal sections of the cauda equina showed that GFP-positive cells were co-stained with O4, β III-tubulin or GFAP, but not with S100, suggesting that NSCs differentiated into oligodendrocytes, neurons or astrocytes in vivo (Figure 4).

Functional recovery following NSC transplantation encapsulated in three-dimensional hydrogels

To explore the regenerative effect of the transplanted NSCs, the functional recovery of sensorimotor reflexes was determined using the tail-flick test. Fourteen days after transplantation, rat bilateral L5-6 DRG tissues were isolated and subject to TUNEL staining. Results showed that CES model group led to a significant increase in apoptotic cells compared to sham group ($21.63\% \pm 2.08$ vs. $1.41\% \pm 0.56$, $P < 0.01$). By contrast, NSCs transplantation with three-dimensional hydrogels obviously decreased the apoptosis rate compared to CES model group ($13.92\% \pm 3.67$ vs. $21.63\% \pm 2.08$, $P < 0.05$) (Figure 5A). Two weeks after surgery, LFB staining and TEM analysis showed cauda equina nerve fibers in an organized state, normal axons, and intact myelin sheath. However, compression of cauda equina resulted in disorganized nerve fibers, swollen axons and myelin sheaths, and demyelination. These observations were alleviated after transplantation of NSCs encapsulated in hydrogels (Figure 5A). Additionally, G-ratio (inner diameter/outer diameter of myelinated axons) was significantly higher in model group than sham group, and then decreased in the grafted NSCs animals (Figure 5B).

The rat model procedure was described and modified by our research team, which has been successfully used in many studies. When we established the model, we proved that: at day 1, 3, and 7 post compression of cauda equina, we observed higher the tail flick latency (TFL) of the compression group than that of the sham group. The compression group was significantly prolonged. After 7 days, immunofluorescence staining showed dense and organized cauda equina nerve fibers, no swollen axons, and intact myelin in the sham group. However, in the compression group, we observed disorganized cauda equina nerve fibers, swollen axons and demyelinated myelin.

Three weeks after transplantation, animals with cauda equina injury exhibited a significant increase in tail-flick latency compared with those in the sham group. However, transplantation of hydrogel-

encapsulated NSCs partly decreased the tail-flick latency, exhibiting a neuroprotective activity on injured cauda equina (Figure 6).

Discussion

CES is a rare neurological disorder characterized low back pain, muscle weakness, and sensory disturbance [1]. At the cellular level, DRG cells appear disorganized with some apoptotic bodies. In addition, CES will cause demyelination and swelling of myelin. Because of the poor self-repair ability of nerve tissue, especially those in the central nervous system, the therapeutic effects of surgery and neurotrophic drugs on cauda equina injury-induced CES is limited. Patients often have residual bladder and sexual dysfunction, and skin sensory disorder in the sella area. Although this disease has a low incidence in the population, ranging from 1:33,000 to 1:100,000 inhabitants, its sequelae still generate high public healthcare costs [2]. Thus, development of novel approaches to maintain neural stem cell viability is important to achieve ideal therapeutic outcomes. The functional recovery of CES is not satisfied because of the failure of axon regeneration and the nerve damage.

Because the cauda equina is different from the spinal cord, it is impossible to transplant the neural stem cells into the solid tissues. Our previous study showed that GFP-NSCs survived in the cerebrospinal fluid around the damaged cauda equina after intrathecal transplantation, but the surviving time was very short, i.e., only one week [15]. Based on the previous study, hydrogels were used to localize neural stem cells to the injured cauda equina to promote the axon regeneration and remyelination of damaged cauda equina, eventually achieving the goal of neuron preservation and functional repair.

In the present study, we applied tissue engineering technology combined with NSCs transplantation, and explored the potential therapeutic effects on cauda equina injury. Consequently, our study demonstrated that transplantation of hydrogel-encapsulated NSCs can limitedly promoted the differentiation of stem cells and improved the functional recovery of injured cauda equina.

NSCs have shown promising and beneficial effects in the therapy of neurological disorders, such as spinal cord injury, brain trauma, and cauda equina lesion [18]. Accumulating evidence demonstrates that transplanted NSCs successfully survive in the injured tissues and integrate into the host brain to achieve the functional recovery [19]. Moreover, the pluripotency of DRG has been reported by several research groups, including our group [15,20,21]. The sensory branch in the cauda equina is composed of the central processes of DRG neurons. Thus, DRG-NSCs were used to repair the damaged cauda equina because the homology of DRG-NSCs with cauda equina. The mechanisms by which NSCs exert their neuroprotective effects have begun to be elucidated. Increasing studies have shown that NSCs may synthesize a variety of neurotrophic cytokines stimulating nerve growth, such as vascular endothelial growth factor (VEGF), brain derived neurotrophic factor (BDNF), and nerve growth factor (NGF) [22,23]. Previous studies showed that deficiency of endogenous neurotrophins is associated with poor neuronal survival and cell death [24]. BDNF has very extensive neurotrophs and can maintain the survival of various kinds of neurons and directly promote their axon growth [25]. Following a cervical spinal cord

injury, administration of BDNF into the site of spinal cord injury promoted axonal regeneration and prevented axotomy-induced atrophy and/or death of rubrospinal neurons [26,27]. Furthermore, cell transplantation may also enhance endogenous repair processes including neurogenesis, axonal sprouting, and angiogenesis [28,29]. However, NSCs application is limited due to the poor cell survival in host tissues. In our study, NSCs were successfully isolated and cultured in hydrogels. Moreover, we found the possibility of NSCs differentiating into oligodendrocytes, Schwann cells, neurons and astrocytes.

Tissue engineering may provide solutions to the challenges of stem cell death and damage associated with transplantation [30]. Biopolymer hydrogels can promote stem cell survival, enhance stem cell engraftment, and minimize wound scar formation [13]. Published studies have shown that hydrogels alter the survival and differentiation of stem cells both in vitro and in vivo [31,32]. In the present study, we isolated NSCs from neonatal DRG to repair damaged cauda equina in a rat model of lumbar spinal canal stenosis. As a result, hydrogel-encapsulated NSCs presented high viability in the injured cauda equina and mainly differentiated to oligodendrocytes. Oligodendrocytes are known to be susceptible to spinal cord contusion and loss of oligodendrocytes may induce demyelination, disturb the functional recovery of damaged nerve tissues, and damage the conductive capacity of sensory nerves [33]. Therefore, stem cell transplantation is helpful to improve myelination and enhance functional recovery after CNS injury [34]. To evaluate the neuroprotective role of the hydrogel encapsulated NSCs, the tail-flick test was performed to measure the functional recovery of sensorimotor reflexes. As expected, NSCs engrafted on the hydrogels obviously decreased apoptosis of injured cauda equina tissue. Moreover, cauda equina nerve fibers presented an organized state, normal axons, and intact myelin sheath. Additionally, transplanted hydrogel-encapsulated NSCs decreased the tail-flick latency and showed a neuroprotective role on injured cauda equina.

In summary, our study demonstrates that transplantation of hydrogel-encapsulated NSCs enhances the viability of transplanted cells, promotes stem cell differentiation into oligodendrocytes, thereby contributing to the functional recovery of injured cauda equina. These results implied that NSCs encapsulated in three-dimensional hydrogels may be used for the treatment of cauda equina disorder.

Conclusions

Our results indicate transplantation of hydrogel-encapsulated NSCs promotes stem cell differentiation into oligodendrocytes, neurons or astrocytes and contributes to the functional recovery of injured cauda equina, suggesting that NSCs encapsulated in hydrogels may be applied for the treatment of cauda equina injury.

Abbreviations

CESI

Cauda equina syndrome

NSCs:

neural stem cells

DRG:

dorsal root ganglion

GFAP:

glial fibrillary acidic protein

TEM:

transmission electron microscopic

GFP:

green fluorescent protein

LFB:

Luxol fast blue

Declarations

Availability of data and materials

All data generated or analyzed during this study are included in this published article..

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Ethics declarations

Ethics approval and consent to participate

The study protocol was approved by by the Ethical Committee of the Shanghai Jiao Tong University School of Medicine. Informed consent was provided by all participating individuals.

Consent for publication

Not applicable.

Competing interests Statement

No competing interests.

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Figures

Figure 1

Characterization of NSCs in hydrogel scaffolds NSCs were isolated from the neonatal rat DRG and cultured in proliferation culture medium for different time points at 0, 3, 6, and 10 days (A). Then, NSCs were successfully grown in 0.25% and 0.5% hydrogels (A). For identification of NSCs, stem cells were immunohistochemically stained with antibodies against nestin and P75R, and nucleus was stained with Hoechst (B).

Figure 2

Differentiation of NSCs in vitro NSCs were transfected with lentivirus vectors carrying green fluorescent protein (GFP) and cultured in differentiation medium (A). After 7 days of differentiation, stem cells were immunohistochemically stained with antibodies against O4, S100, β III-tubulin, and GFAP, and nucleus was stained with Hoechst (B). Scale bar=100 μ m.

A **B****Hydrogel** **GFP**

Figure 3

Transplantation of NSCs in the injured cauda equina A rat model of cauda equina injury were established and then transplanted with hydrogel-encapsulated NSCs (A). After 7 days of transplantation, the frozen sections were imaged and GFP-positive grafted NSCs were observed in the injured cauda equina (B).

Figure 4

Differentiation of NSCs in vivo After 7 days of transplantation, the frozen sections were immunohistochemically stained with antibodies against O4, S100, β III-tubulin, and GFAP, and imaged by confocal microscopy. Scale bar=100 μ m.

Figure 5

Ultrastructural and pathological changes of DRG after NSC transplantation The rat DRG tissues were subject to TUNEL and LFB staining, and TEM (A). Then, G-ratio (inner diameter/outer diameter of myelinated axons) was calculated (B). * $P < 0.05$, compared to sham group; # $P < 0.05$, compared to CES model group. Data are reported as means $\pm$ SD. Scale bar=100 μ m.

Figure 6

Functional recovery following transplantation of NSCs encapsulated in hydrogels The functional recovery of sensorimotor reflexes in sham, CES model and NSCs groups was determined using the tail-flick test. ** $P < 0.01$, compared to sham group; # $P < 0.05$, compared to CES model group. Data are reported as means $\pm$ SD.