

Effects of Different Prosthetic Instrumentations on Tibial Bone Resection in Total Knee Arthroplasty

Yufeng Lu

Honghui Hospital, Xi'an Jiaotong University <https://orcid.org/0000-0003-4527-0760>

Xuechao Yuan

Shaanxi University of Chinese Medicine

Feng Qiao

Honghui Hospital, Xian Jiaotong University

Yangquan Hao (✉ haoyq2008@yahoo.com)

Osteonecrosis and Joint Reconstruction Ward, Department of Joint Surgery, Honghui Hospital, Xi'an Jiaotong University, Xi'an, Shaanxi 710054, P.R. China

Research article

Keywords: TKA, posterior tibial slope, measurement

Posted Date: November 19th, 2020

DOI: <https://doi.org/10.21203/rs.3.rs-107463/v1>

License:   This work is licensed under a Creative Commons Attribution 4.0 International License.

[Read Full License](#)

Abstract

Objective For total knee arthroplasty (TKA) tibial bone resection, various manufacturers provide cutting blocks with fixed angles. But the accuracy of these angles is uncertain. Our aim was to assess the accuracy of the obtained posterior tibial slope (PTS) with a fixed angle cutting block.

Methods 247 TKAs in 213 patients were reviewed. We included 104 Legion Prosthesis, 76 U2 Knee Prosthesis, 46 NexGen LPS-Flex Prosthesis, and 21 Vanguard Knee System products. Preoperative and postoperative PTS were measured via expanded lateral tibia radiographs. The tibial component coronal alignment angle (TCCA) was measured on postoperative standing full-length anteroposterior radiographs, and the tibia length was measured on preoperative standing full-length radiographs.

Results For postoperative PTS, the Legion group had significantly smaller slopes than the U2 Knee group and Vanguard group. However, there was no significant difference between the Legion and NexGen groups, and no significant difference among the NexGen, U2 Knee, and Vanguard groups. One sample t-test indicated that only the NexGen group showed no statistical difference from the 7° PTS and 90° TCCA it aimed to provide. Multiple linear regression showed that the different tibial lengths and preoperative PTS had statistically significant effect on postoperative PTS. However, there were weak correlations between the tibial length and PTS, and between preoperative and postoperative PTS.

Conclusion For TKA, using conventional tibial bone resection technology with different tibial cutting instrumentations provided by various manufacturers can obtain safe PTS. However, the PTS is not completely consistent with the angle of the cutting block.

Introduction

In total knee arthroplasty (TKA), the alignment of the sagittal plane of the prosthesis is as important as that of the coronal plane and axial position. Poor alignment can lead to early failure of the prosthesis [1,2]. The posterior tibial slope (PTS) relates to the postoperative range of motion [3] and function of the extensor mechanism [4]. PTS also impacts tibial insert wear [5] and loosening [6], as well as the stability of the TKA [7]. Previous studies [8,9,10] have suggested that the postoperative PTS should range from 0° to 10° to guarantee optimal prosthesis function. However, some authors [11,12,13] recently recommended the reconstruction of the native PTS, depending on the intraoperative mobility and stability of the knee joint.

For TKA tibial bone resection, various manufacturers provide cutting blocks with certain PTS. In our institution, the commonly used TKA instrumentations are provided by Smith & Nephew, United Orthopedic, Zimmer, and Biomet with angles of 3°, 5°, 7°, and 0° respectively.

In the current study, we aimed to assess the PTS after different tibial cutting instrumentations were employed for TKA. We hypothesized that the PTS achieved after osteotomy with different extramedullary guidance jigs are inconsistent with the fixed angle of the cutting blocks.

Patients And Methods

The protocols in this study were approved by the ethics reviewing council of Honghui Hospital, Xi'an Jiaotong University, which abides by the Declaration of Helsinki on Ethical principles for medical research involving human subjects (IRB Approval Number 202003058). Written informed consent was obtained from all participants.

This study retrospectively reviewed 320 TKAs using posterior-stabilizing prostheses between January 1, 2018, and December 31, 2019. The inclusion criteria were as follows: (1) preoperative diagnosis of knee osteoarthritis and (2) true knee lateral radiographs including at least 20 cm of the tibia. Exclusion criteria included (1) evidence of trauma, infection, tumor, or any congenital disorder; and (2) tibial plateau with severe bone defect(s).

Using these criteria, 247 knees of 213 patients (155 women and 58 men) were included. There were 122 left knees and 125 right knees. The mean patient age at the time of index operation was 62.5 years (range, 30–87 years). Mean follow-up was 15.3 months (range, 6–12 months). There were 104 Legion Prostheses (Smith & Nephew, Memphis, TN), 76 U2 Knee Prostheses (United Orthopedic, Taipei, Taiwan), 46 NexGen LPS-Flex Prostheses (Zimmer, Warsaw, IN), and 21 Vanguard Knee Systems (Biomet, Warsaw, IN) used.

Surgical technique

All TKAs were performed by the senior surgeon using a midline skin incision and medial parapatellar arthrotomy. The tibia cuts were made with the use of an extramedullary guidance jig. After resection of the distal femur, the tibia was anteriorly subluxated, and the tibial alignment guide and cutting block were assembled. The guide spike was anchored to the ACL attachment of the tibia. In the coronal plane, the alignment guide pointed to the second metatarsal, and the proximal tibia was cut perpendicular to the guide in the coronal plane. In the sagittal plane, the surgeon used his fingers to determine the PTS osteotomy. At the lower edge of the tibial tuberosity, the anterior side of the tibia was two fingers' width from the guide, and, at the upper side of the ankle joint clamp, the anterior tibial skin was three fingers' width from the guide rod. Each tibial cutting block provided by the manufacturers had an angle of posterior inclination, which was 3° for the Legion system, 5° for the U2 Knee system, 7° for the NexGen system, and 0° for the Vanguard system.

All measurements were carried out with a picture archiving and communication system (PACS, Synapse, Fujifilm Inc., Tokyo, Japan). (1) PTS was measured according to Faschingbauer's method [14] using the true knee lateral radiographs. The anatomic axis of the tibia was taken as the line connecting the midline of the anterior and posterior (AP) cortical edges 6 cm and 16 cm distal from the tibial plateau. The AP axis of the tibial plateau was the line connecting the AP edges of the tibial plateau. If there was an obvious osteophyte on the AP edge of the tibial plateau, the medial plateau was used as the AP axis. The preoperative PTS was 90° minus the angle between the two axes (Fig. 1). The postoperative PTS was 90° minus the angle between the anatomic axis of the tibia and the AP axis of the tibial component (Fig. 2).

(2) The tibial component coronal alignment angle (TCCA) was defined as the angle between the mechanical axis of the tibia and transverse axis of the tibial component on postoperative standing full-length AP radiographs (Fig. 3). (3) The tibia length was defined as the distance between the midpoint of the proximal tibial articular surface and the midpoint of the distal tibial articular surface on preoperative standing full-length radiographs (Fig. 4).

The measurement data were divided into four groups according to prosthesis type: Legion group, U2 Knee group, NexGen group, and Vanguard group. All measurements were performed by two blinded observers using radiographs. After 3 weeks, 20 randomly selected patients were measured again for the determination of intra-rater and inter-rater reliability.

Clinical outcome assessment used the knee social score (KSS) pre-operatively and at final follow-up. The KSS comprises two parts: a knee score, which include pain, stability and range of motion (ROM), and a function score, which include the ability of the patient to walk, climb stairs and the use of ambulatory aids.

Quantitative data were expressed as means \pm standard deviation (SD). Statistical analyses were performed using the PASW statistics 18 (SPSS Inc., Chicago, IL, USA).

The normality assumption of our data was validated by the Kolmogorov-Smirnov test. A one-way ANOVA test and Kruskal-Wallis non-parametric tests were used to compare the data for the four groups. Intra- and inter-rater reliability [15] were determined using the intraclass correlation coefficient (ICC). Multiple linear regression analysis was used to investigate the possibility of association of age, sex, body side, TCCA, and tibial length with PTS. $P < 0.05$ was considered to be statistically significant.

Results

The Kolmogorov–Smirnov test revealed that all data followed a normal distribution pattern. ICC and interclass correlation coefficients for the reproducibility of all parameters were $>80\%$ (Table 1).

There were no statistically significant differences among the groups with regards to the demographic characteristics of patients before surgery, except that the age of the U2 Knee group was greater than the other groups (Table 2). The homogeneity of variance test indicated that there was no statistically significant difference among the corresponding data of each group (all P -values >0.05) (Table 3).

For the preoperative PTS and the tibia length, there were no significant differences among the four groups (all P -values >0.05). For postoperative PTS, the Legion group had a significantly smaller slope than the U2 Knee and Vanguard groups ($P = 0.001$) (Fig. 5). However, there was no significant difference in postoperative PTS between the Legion and NexGen groups ($P = 0.08$), and no significant differences were found among the NexGen, U2 Knee, and Vanguard groups (all P -values >0.05).

There was no significant difference in TCCA among the four groups (all P -values >0.05). However, a one sample t-test was performed for the TCCAs of each group and 90° , and only the NexGen group showed

no significant difference from 90° ($t = -1.421$, $P = 0.162$). Furthermore, the other prosthetic instruments and their PTS showed significant differences (all $P < 0.05$) (Table 4). A one sample t-test was performed for the postoperative PTS of each group and the fixed angle provided by the prosthetic instrumentations, and the results indicated that only the NexGen group showed no statistical difference from the 7° provided by the product ($t = 0.429$, $P = 0.670$), whereas the PTS of the other prosthetic instrumentations and were significantly different their specific fixed angles (all $P < 0.05$) (Table 4).

There were no statistically significant differences among the four groups with regards to preoperative and postoperative KSS and ROM (Table 2). Multiple linear regression showed that the tibial length and preoperative PTS had statistically significant effect on postoperative PTS ($b = -0.023$ and 0.093 , $t = -3.474$ and 2.679 , $P = 0.001$ and 0.008 , respectively) (Table 5); although, there were weak correlations between the tibial length and postoperative PTS ($R = 0.255$, $P < 0.001$), and between preoperative PTS and postoperative PTS ($R = 0.210$, $P = 0.001$). The different ages, TCCAs, BMI, postoperative KSS and ROM had no significant effect on PTS (Table 5).

Discussion

The PTS is defined as the angle between the tangent of the medial and lateral plateaus and the line perpendicular to the longitudinal mechanical axis [14]. This angle is very different between individuals and ranges in studies from -9° to 16° with an average of approx. $3-10^\circ$ [16,17,18].

Currently, the most commonly used method for measuring the PTS is the true lateral radiograph of the tibia. For optimal determination, a strictly lateral radiograph of the entire length of the tibia, including the ankle and knee joint, is required [14]. The mechanical axis is constructed from a line between the center of the tibial plateau and that of the lateral ankle joint. A tangent is placed over the tibial plateau, and the angle between the mechanical axis and the tangent determines the PTS. However, in clinical practice, before and after TKA, full-length lateral radiographs of the tibia are not routinely available, so there are many alternatives for the tibial mechanical axis, such as the tibial proximal anatomical axis [18-22], tibial shaft anatomical axis [18,23], posterior tibial cortex [18, 20, 22], anterior tibial cortex [18-20, 22], and fibular shaft axis [18,23]. Compared with the tibial mechanical axis, the accuracy of the PTS measurements vary. Current studies show there is good correlation between the tibial proximal anatomical axis, constructed by measuring points 5–15 cm or 6–16 cm below the joint surface, and the mechanical axis. In this way, deviations can be reduced to up to 1.5° [14,18]. The shorter the radiograph that includes the tibia, the worse the PTS measurement accuracy tends to be in these studies. Therefore, based on the results of these studies, we used an expanded lateral radiograph of a 20-cm long section of the tibia to measure PTS in this study. Obviously, the accuracy of this measurement is lower than that obtained when using the full-length lateral tibia, which is a limitation of this study. Another limitation of this study is that the sample size of Vanguard prosthesis is too small.

Appropriate PTS for TKA is very important. Previous studies suggested that postoperative PTS should range from 0° to 10° to guarantee optimal prosthetic function. Excessive PTS after TKA may cause

anterior and posterior instability, leading to anterior subluxation of the tibia, thus increasing the shear stress of the posterior tibia polyethylene and resulting in aseptic loosening [22]. Conversely, a reduction in the PTS leads to increased stress in the anterior part of the subchondral bone, thereby increasing the risk of component subsidence [24]. Decreased PTS also leads to limited flexion because of the tight flexion gap [25].

The method used for tibial bone resection primarily depends on the implant instrumentation provided by the manufacturer. In the coronal plane, the tibial bone resection needs to be perpendicular to the tibial mechanical axis. In addition to navigation and patient-specific instrumentation, the traditional method of aligning the tibial mechanical axis is to use the proximal spike of the cutting guide to anchor the ACL attachment to the tibia [26], the anterior middle third of the anterior and posterior axis of the tibial plateau [27], and the intercondylar eminentia [28], as well as the point on the tibia plateau, resulting in the extramedullary rod being parallel to the palpable fibula [27]. In the distal tibia, because the ankle joint center is difficult to locate, the second metatarsal [29], first and second metatarsal spaces [30], tibialis anterior tendon, or anterior tibial crest [31,32] are often used as markers, and through these, generally good coronal alignment can be obtained. The sagittal mechanical axis of the tibia is more difficult to mark than the coronal mechanical axis. Therefore, the specific method of bone resection of the PTS is still controversial, and there is no unified standard. The traditional method is to adjust the PTS using the distance between the tibial cutting guide rod and the anterior skin surface of the tibia as a reference [33]. The accuracy of the cutting block with a fixed angle posterior slope provided by the manufacturer was uncertain. Therefore, the present study used conventional tibial bone resection techniques to compare the actual PTS obtained by various makes of cutting blocks with fixed angles to test their accuracy. We found that when we used a 3° cutting block (Legion), the angle after bone resection was $6.3 \pm 2.6^\circ$. For a 5° cutting block (U2 Knee), the angle after osteotomy was $7.6 \pm 2.6^\circ$. With the 7° cutting block, the angle after osteotomy was $7.1 \pm 2.7^\circ$ (NexGen). Surprisingly, for Vanguard's 0° cutting block, the angle after resection were $8.6 \pm 3.3^\circ$. We performed multiple linear regression analysis of the PTS with the parameters of age, TCCA, BMI, preoperative PTS, postoperative KSS, ROM and tibial length, and found that only the tibial length and preoperative PTS affected the PTS, although, the effect was very small ($R = 0.255$ and 0.210 , respectively). However, considering that we used the expanded lateral radiograph with a 20-cm section of the tibia instead of the full-length lateral tibial radiograph, the actual PTS may be 1–1.5° less than the above value. In addition, in the coronal plane, we used the second metatarsal bone to align the cutting guide rod, and the TCCAs obtained with these four prosthetic instrumentations were 89.5–89.6°; only the NexGen group had no statistical difference from 90°, while the other three groups all showed statistical difference from 90°. This suggests that the second metatarsal bone is not a reliable reference marker for coronal tibial bone resection with some instrumentations, as it is more easily affected by the position of the ankle joint.

In conclusion, using conventional tibial bone resection technology with different tibial cutting instrumentations provided by various manufacturers in TKA can obtain safe PTS. However, the PTS is not completely consistent with the angle of the cutting block.

Abbreviations

TKA: total knee arthroplasty; PACS: Picture Archiving and Communications Systems; PTS: posterior tibial slope; TCCA: Tibial component coronal alignment angle; BMI: body mass index; KSS: Knee Society score; ROM: Range of motion

Declarations

Ethics approval and consent to participation

The ethical approval was obtained from the Institutional Review Board (IRB) (IRB-2020-03-058) of the Honghui Hospital, Xi'an Jiaotong University. The participants provided their written informed consent for participation in the study and for the use of their data in the study.

Consent for publication

The study participants provided written informed consents for their participation and for the use of their data in this study.

Availability of data and materials

The datasets used and/or analyzed in the current study are available from the corresponding authors on request.

Competing interests

The authors declare no competing interests.

Funding

This study was supported by a grant from the Shaanxi Provincial Key Research and Development Project (CN) (grant no. 2019SF-214) and the Xi'an Health Scientific Research Talent Project (CN) (grant no. J201903058).

Authors' Contributions

YL processed data, participated in the study design, and drafted the manuscript. XY and FQ collected the data. FQ performed the statistical analysis. YH designed the study, supervised the whole study process, and helped to review the manuscript. All authors read and approved the final manuscript.

Acknowledgments

The researchers acknowledge the support of the Imaging Center of Honghui Hospital, Xian Jiaotong University.

References

1. Johnston H, Abdelgaied A, Pandit H, Fisher J, Jennings LM. The effect of surgical alignment and soft tissue conditions on the kinematics and wear of a fixed bearing total knee replacement. *J Mech Behav Biomed Mater* 2019; 100:103386
2. Klatt BA, Goyal N, Austin MS, Hozack WJ. Custom-fit total knee arthroplasty (OtisKnee) results in malalignment. *J Arthroplasty* 2008; 23:26-29.
3. Fujito T, Tomita T, Yamazaki T, Oda K, Yoshikawa H, Sugamoto K. Influence of Posterior Tibial Slope on Kinematics After Cruciate-Retaining Total Knee Arthroplasty. *J Arthroplasty* 2018; 33:3778-3782.
4. Kang KT, Koh YG, Son J, Kwon OR, Lee JS, Kwon SK. Biomechanical Effects of Posterior Condylar Offset and Posterior Tibial Slope on Quadriceps Force and Joint Contact Forces in Posterior-Stabilized Total Knee Arthroplasty. *Biomed Res Int* 2017:4908639.
5. O'Rourke MR, Callaghan JJ, Goetz DD, Sullivan PM, Johnston RC. Osteolysis associated with a cemented modular posterior-cruciate-substituting total knee design : five to eight-year follow-up. *J Bone Joint Surg Am* 2002; 84:1362-1371.
6. Karas V, Calkins TE, Bryan AJ, Culvern C, Nam D, Berger RA, Rosenberg AG, Valle CJD. Total Knee Arthroplasty in Patients Less Than 50 Years of Age: Results at a Mean of 13 Years. *J Arthroplasty* 2019; 34:2392-2397.
7. Okamoto S, Mizu-uchi H, Okazaki K, Hamai S, Nakahara H, Iwamoto Y. Effect of Tibial Posterior Slope on Knee Kinematics, Quadriceps Force, and Patellofemoral Contact Force After Posterior-Stabilized Total Knee Arthroplasty. *J Arthroplasty* 2015; 30:1439-1443.
8. Bai B, Baez J, Testa N, Kummer FJ. Effect of posterior cut angle on tibial component loading. *J Arthroplasty* 2000; 15:916-920.
9. Dorr LD, Boiardo RA. Technical considerations in total knee arthroplasty. *Clin Orthop Relat Res* 1986; 205:5-11.
10. Ewald FC, Jacobs MA, Miegel RE, Walker PS, Poss R, Sledge CB. Kinematic total knee replacement. *J Bone Joint Surg Am* 1984; 66:1032-1040.
11. Chambers AW, Wood AR, Kosmopoulos V, Sanchez HB, Wagner RA. Effect of Posterior Tibial Slope on Flexion and Anterior-Posterior Tibial Translation in Posterior Cruciate-Retaining Total Knee Arthroplasty. *J Arthroplasty* 2016; 31: 103-106.
12. Kang KT, Kwon SK, Son J, Kwon OR, Lee JS, Koh YG. The increase in posterior tibial slope provides a positive biomechanical effect in posterior-stabilized total knee arthroplasty. *Knee Surg Sports Traumatol Arthrosc* 2018; 26:3188-3195.
13. Singh G, Tan JH, Sng BY, Awiszus F, Lohmann CH, Nathan SS. Restoring the anatomical tibial slope and limb axis may maximise post-operative flexion in posterior-stabilised total knee replacements. *Bone Joint J* 2013; 95-B:1354-1358.
14. Faschingbauer M, Sgroi M, Juchems M, Reichel H, Kappe T. Can the tibial slope be measured on lateral knee radiographs? *Knee Surg Sports Traumatol Arthrosc* 2014; 22:3163-3167.

15. Landis JR, Koch GG. The measurement of observer agreement for categorical data. *Biometrics* 1977; 33:159-174.
16. Lombardi AV Jr, Berend KR, Aziz-Jacobo J, Davis MB. Balancing the flexion gap: relationship between tibial slope and posterior cruciate ligament release and correlation with range of motion. *J Bone Joint Surg Am* 2008; 90 Suppl 4:121-132.
17. Nunley RM, Nam D, Johnson SR, Barnes CL. Extreme variability in posterior slope of the proximal tibia: measurements on 2395 CT scans of patients undergoing UKA? *J Arthroplasty* 2014; 29:1677-1680.
18. Yoo JH, Chang CB, Shin KS, Seong SC, Kim TK. Anatomical references to assess the posterior tibial slope in total knee arthroplasty: a comparison of 5 anatomical axes. *J Arthroplasty* 2008; 23:586-592.
19. Bae DK, Song SJ, Yoon KH, Noh JH, Moon SC. Comparative study of tibial posterior slope angle following cruciate-retaining total knee arthroplasty using one of three implants. *Int Orthop* 2012; 36:755-760.
20. Pan XQ, Peng AQ, Wang F, Li F, Nie XZ, Yang X, Ji G, Wang MX. Effect of tibial slope changes on femorotibial contact kinematics after cruciate-retaining total knee arthroplasty. *Knee Surg Sports Traumatol Arthrosc* 2017; 25: 3549-3555.
21. Utzschneider S, Goettinger M, Weber P, Horng A, Glaser C, Jansson V, Müller P E. Development and validation of a new method for the radiologic measurement of the tibial slope. *Knee Surg Sports Traumatol Arthrosc* 2011; 19:1643-1648.
22. Zhang Y, Wang J, Xiao J, Zhao L, Li ZH, Yan G, Shi ZJ. Measurement and comparison of tibial posterior slope angle in different methods based on three-dimensional reconstruction. *Knee* 2014; 21:694-698.
23. Han HS, Chang CB, Seong SC, Lee S, Lee MC. Evaluation of anatomic references for tibial sagittal alignment in total knee arthroplasty. *Knee Surg Sports Traumatol Arthrosc* 2008; 16:373-377.
24. Hofmann AA, Bachus KN, Wyatt RW. Effect of the tibial cut on subsidence following total knee arthroplasty. *Clin Orthop Relat Res* 1991; 269:63-69.
25. Jojima H, Whiteside LA, Ogata K. Effect of tibial slope or posterior cruciate ligament release on knee kinematics. *Clin Orthop Relat Res* 2004; 426:194-198.
26. Reed MR, Bliss W, Sher JL, Emmerson KP, Jones SM, Partington PF. Extramedullary or intramedullary tibial alignment guides: a randomised, prospective trial of radiological alignment. *J Bone Joint Surg Br.*2002; 84:858-860.
27. Laskin RS. Instrumentation pitfalls: you just can't go on autopilot!. *J Arthroplasty* 2003; 18:18-22.
28. Bek D, Ege T, Yıldız C, Tunay S, Başbozkurt M. The accuracy of two different extra-medullary tibial cutting guides for posterior tibial slope in total knee arthroplasty. *Eklemler Hastalıkları Cerrahisi* 2014; 25:75-79.
29. Tsukeoka T, Tsuneizumi Y, Lee TH. Accuracy of the second metatarsal as a landmark for the extramedullary tibial cutting guide in total knee arthroplasty. *Knee Surg Sports Traumatol Arthrosc*

2014; 22:2969-2974.

30. Tew M, Waugh W. Tibiofemoral alignment and the results of knee replacement. *J Bone Joint Surg Br* 1985; 67:551-556.
31. Sasanuma H, Sekiya H, Takatoku K, Ajiki T, Hagiwara H. Accuracy of a proximal tibial cutting method using the anterior tibial border in TKA. *Eur J Orthop Surg Traumatol* 2014; 24:1525-1530.
32. Tsukeoka T, Lee TH, Tsuneizumi Y, Suzuki M. The tibial crest as a practical useful landmark in total knee arthroplasty. *Knee* 2014; 21:283-289.
33. Tsukeoka T, Tsuneizumi Y. The distance from the extramedullary cutting guide rod to the skin surface as a reference guide for the tibial slope in total knee arthroplasty. *Knee* 2016; 23:314-317.

Tables

Table 1. Summary of patient and clinical results

Measurement	Intra-observer I reliability	Intra-observer II reliability	Inter-observer reliability
Post-op. PTS	0.93	0.90	0.91
Pre-op. PTS	0.88	0.90	0.82
TCCA (°)	0.87	0.94	0.89
Tibia length	0.99	0.99	0.99

PTS: posterior tibial slope

TCCA: Tibial component coronal alignment angle

Table 2. The intraclass correlation coefficient analysis of the measured data.

	Legion	U2 Knee	NexGen	Vanguard	
Age(years)	66.0±7.8	70.9±6.1	64.7±7.3	63.7±7.7	<0.001*
Gender (m/f)	24/65	19/49	11/29	4/12	0.996
Side(l/f)	45/59	39/37	24/22	14/7	0.230
Height(cm)	157.9±10.5	157.2±9.4	159.5±9.2	158.3±9.0	0.670
Weight(kg)	64.1±11.1	62.9±9.7	65.7±10.1	63.6±9.4	0.555
BMI (kg/m ²)	25.5±2.3	25.3±2.5	25.2±4.1	25.2±2.1	0.962
Pre-op. KSS					
Knee score	37.4±11.4	35.5±11.9	38.1±11.1	37.1±12.0	0.619
function Score	41.3±9.4	39.1±10.3	40.1±11.2	37.3±12.4	0.300
Post-op. KSS					
Knee score	90.2±4.1	90.1±5.4	89.9±5.3	90.8±5.4	0.899
function score	85.0±8.3	85.1±8.4	87.3±8.8	85.2±9.8	0.456
Pre-op. ROM	74.2±18.2	75.3±15.9	73.4±16.4	74.2±16.6	0.938
Post-op. ROM	112.4±12.5	111.9±12.2	113.1±15.5	111.5±14.7	0.959

* U2 Knee was significantly different from other groups

BMI: body mass index, KSS: Knee Society score, ROM: Range of motion

Table 3. Measurement data and homogeneity of variance test of four kinds of prosthesis instrumentation.

Group	n	Pre-op. PTS (°)	Post-op. PTS (°)	TCCA (°)	Tibia length [cm]
Legion	104	11.6±4.7	6.3±2.6	89.5±1.8	34.2±2.5
U2 Knee	76	10.8±4.9	7.6±2.6	89.5±1.9	34.0±2.6
NexGen	46	10.0±5.8	7.1±2.7	89.6±1.8	35.0±2.3
Vanguard	21	11.0±4.4	8.6±3.3	88.5±2.6	34.8±2.6
P		0.628	0.768	0.088	0.742

PTS: posterior tibial slope, TCCA [Tibial component coronal alignment angle]

Table 4. One-sample t-test results for the postoperative PTS compared with the fixed angle provided by the cutting block and between the TCCAs and 90°

Group	Post-op. PTS (°)	Fixed angle (°)	t	P	TCCA°	90°	t	P
Legion	6.3±2.6	3	12.532	<0.001	89.5±1.8	90	-2.337	0.021
U2 Knee	7.6±2.6	5	8.896	<0.001	89.5±1.9	90	-2.213	0.030
NexGen	7.1±2.7	7	0.429	0.670*	89.6±1.8	90	-1.421	0.162*
Vanguard	8.6±3.3	0	11.725	<0.001	88.5±2.6	90	-2.464	0.023

PTS: posterior tibial slope, TCCA°Tibial component coronal alignment angle

*P > 0.05

Table 5. Multiple linear regression of influencing factors on postoperative PTS

Independent variable	Unstandardized coefficient b	Standard error	Standardized coefficient b	t Value	P Value
Constant	19.466	9.095	—	2.140	0.033
Pre-op. PTS	0.093	0.035	0.165	2.679	0.008*
TCCA	-0.129	0.087	-0.089	-1.484	0.139
Tibia length	-0.023	0.007	-0.212	-3.474	0.001*
BMI	-0.076	0.062	-0.074	-1.230	0.220
Post-op. KSS (knee score)	0.046	0.070	0.080	0.664	0.507
Post-op. KSS °function score°	-0.008	0.037	-0.023	-0.204	0.839
Post-op. ROM	0.041	0.022	0.191	1.848	0.066

Dependent variable: post-op. PTS

* p<0.05

PTS: posterior tibial slope, TCCA°Tibial component coronal alignment angle, BMI: body mass index, KSS: Knee Society score, ROM: Range of motion

Figures



Figure 1

Preoperative PTS was defined as 90° minus the angle between the anatomic axis of the tibia and the AP axis of the tibial plateau.



Figure 1

Preoperative PTS was defined as 90° minus the angle between the anatomic axis of the tibia and the AP axis of the tibial plateau.



Figure 2

Postoperative PTS was defined as 90° minus the angle between the anatomic axis of the tibia and the AP axis of the tibial component.



Figure 2

Postoperative PTS was defined as 90° minus the angle between the anatomic axis of the tibia and the AP axis of the tibial component.



Figure 3

Tibial component coronal alignment angle (TCCA) was defined as the angle between the mechanical axis of tibia and transverse axis of tibial component.



Figure 3

Tibial component coronal alignment angle (TCCA) was defined as the angle between the mechanical axis of tibia and transverse axis of tibial component.



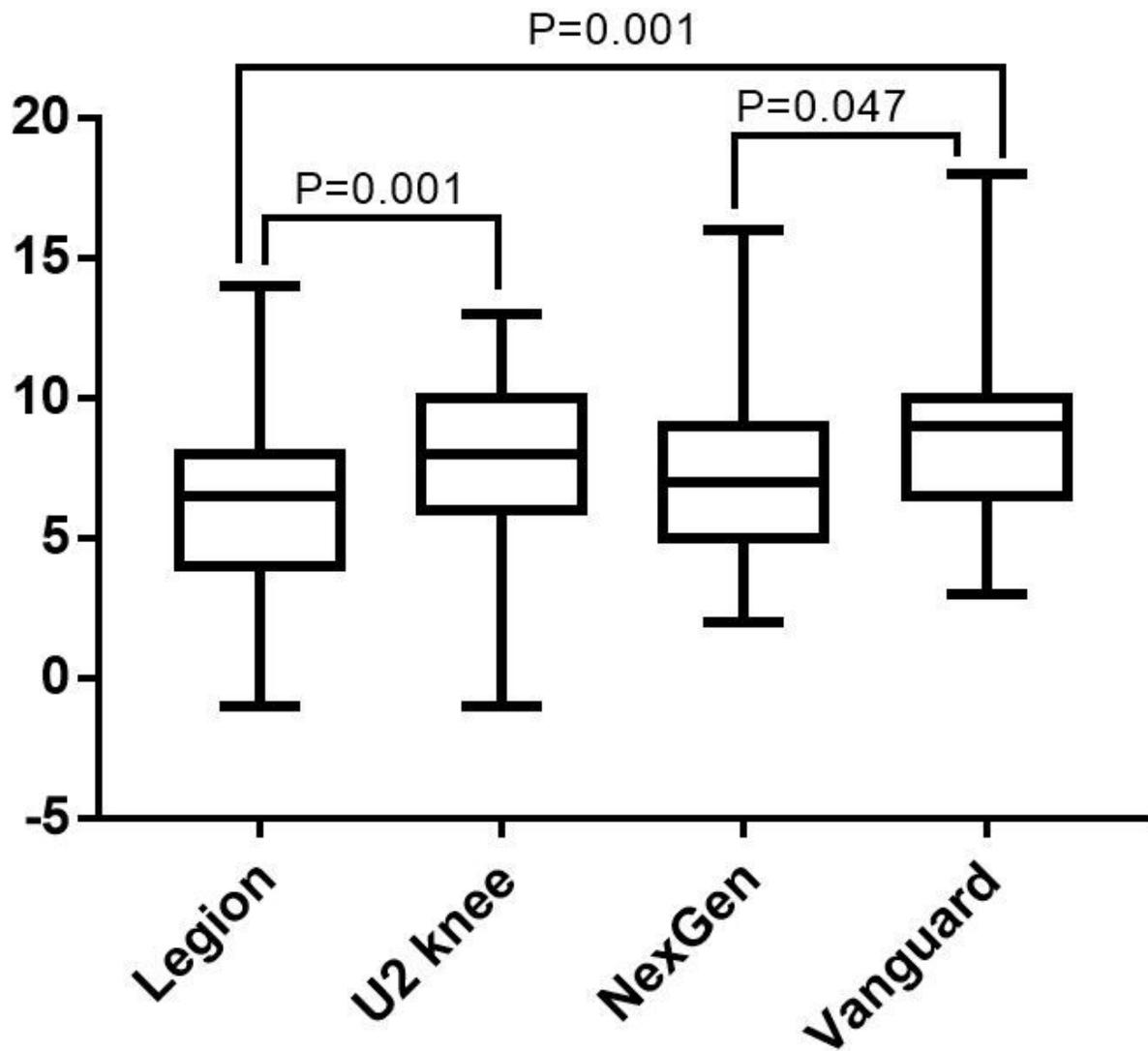
Figure 4

Tibia length was defined as the distance between the midpoint of the proximal tibial articular surface and the midpoint of the distal tibial articular surface.



Figure 4

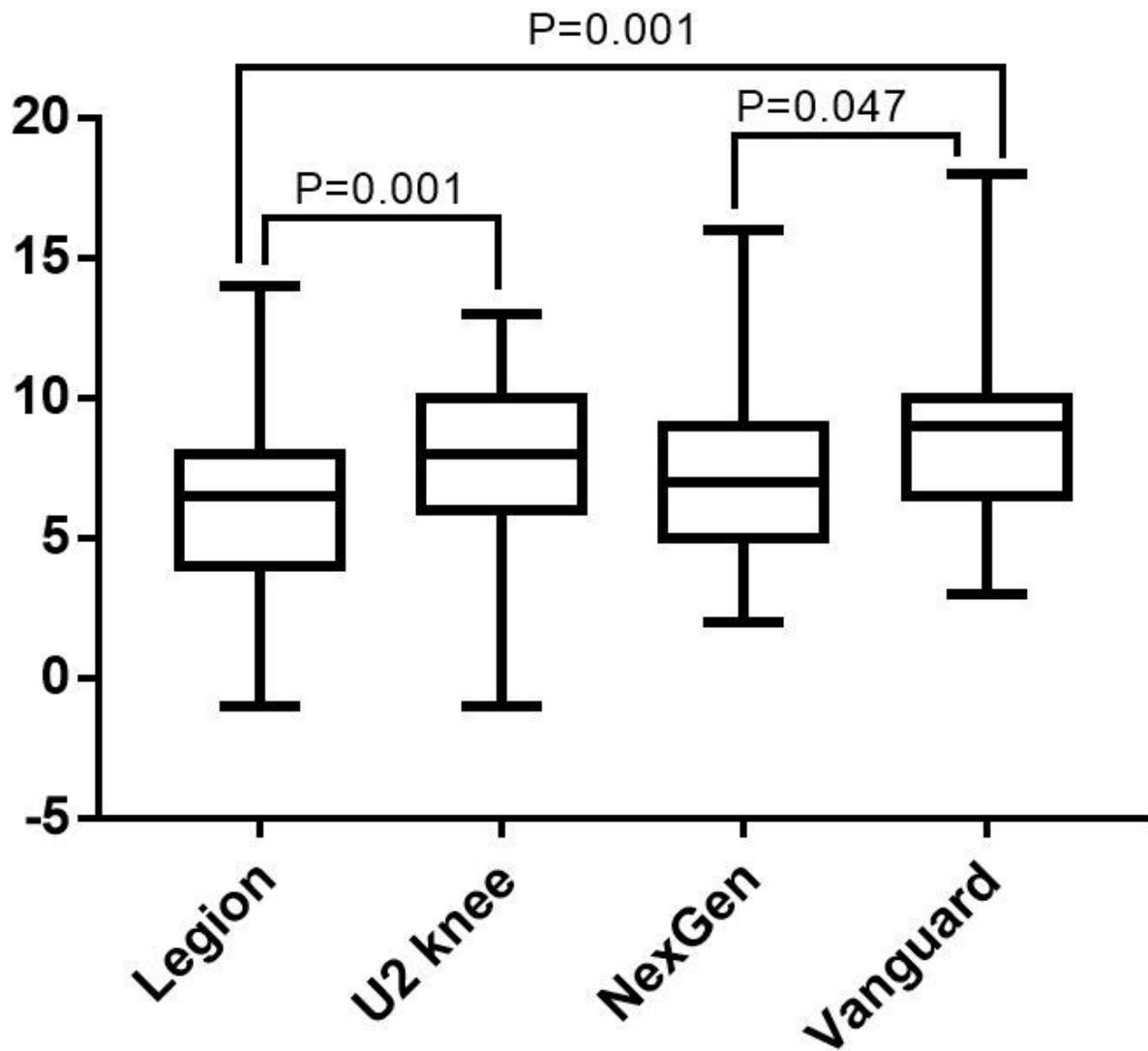
Tibia length was defined as the distance between the midpoint of the proximal tibial articular surface and the midpoint of the distal tibial articular surface.



postoperative PTS with different instrumentation

Figure 5

A boxplot illustrating the distributions of the four postoperative PTS.



postoperative PTS with different instrumentation

Figure 5

A boxplot illustrating the distributions of the four postoperative PTS.