

Performance of The Decarboxylation Index To Predict CO₂ Removal And Mechanical Ventilation Reduction Under VV-ECMO Or High-Flow ECCO₂R

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Abstract

Background: Optimal decarboxylation dose under extracorporeal respiratory support to ensure sufficient reduction of mechanical ventilation stress remains unclear and understudied. The aim of this study was to assess the interdependence of blood flow (BF) and gas flow (GF) in predicting CO₂ removal and mechanical ventilation reduction (MVR) under extracorporeal respiratory support.

Methods: All patients who benefited from veno-venous ECMO (HLS-maquet 7.0, 1.8 m²) and high-flow ECCO₂R (HLS-maquet 5.0, 1.3 m²) in our intensive care unit over a period of 18 months were included. CO₂ removal was calculated from inlet/outlet blood gases performed in clinical practice during the first 7 days of oxygenator use. The relationship between the BF × GF product and CO₂ removal or MVR was studied using linear regression models.

Results: Eighteen patients were analysed, corresponding to 24 oxygenators and 261 datasets. CO₂ removal was 393 mL/min (IQR, 310–526 mL/min) for 1.8 m² oxygenators and 179 mL/min (IQR, 165–235 mL/min) for 1.3 m² oxygenators. The decarboxylation index was associated linearly with CO₂ removal ($R^2 = 0.62$ and $R^2 = 0.77$ for the two oxygenators, respectively) and MVR ($R^2 = 0.72$ and $R^2 = 0.62$, respectively). Values in the range 20–30 L²/min² were associated with an MVR ratio between 38% and 58% for 1.8 m² oxygenators, and between 37% and 55% for 1.3 m² oxygenators.

Conclusion: The decarboxylation index is a simple parameter to predict CO₂ removal and MVR under extracorporeal respiratory support. A BF of 2 L²/min² or more may be necessary to obtain a significant reduction of mechanical convection.

Trial Registration: Being a retrospective study, no trial registration was made.

Background

The use of veno-venous extracorporeal membrane oxygenation (vv-ECMO) as respiratory support for acute critical pulmonary alterations is increasing.¹ In this context, vv-ECMO allows the normalization of gas exchanges and might also reduce ventilator-induced lung injuries (VILI) and biotrauma by applying ultraprotective ventilation.^{2,3} Using this method of extracorporeal respiratory support, oxygen (O₂) and carbon dioxide (CO₂) are transferred following Fick's law through a semi-permeable polymethylpenthene membrane separating a pump-driven extracorporeal blood flow (BF) and a sweep gas flow (GF). Many parameters influence gas exchanges and affect blood oxygenation and decarboxylation differently. The main parameters of systemic oxygenation are the oxygen gas mix, BF/cardiac output ratio, extracorporeal blood flow recirculation and the importance of a pulmonary shunt.^{4,5} Thus, maintaining systemic oxygenation may be challenging in extreme cases despite a high BF in the case of significant recirculation, high cardiac output and/or massive intrapulmonary shunt. In contrast, extracorporeal blood decarboxylation is reputed to be simpler to achieve using a lower BF.⁶ Historically, vv-ECMO was

designed to treat refractory hypoxemia, and different extracorporeal devices using smaller BF_s were developed to allow CO₂ removal (extracorporeal CO₂ removal [ECCO₂R]).⁷⁻⁹ Thus, ECCO₂R strategies were proposed in the treatment of acute exacerbations of chronic obstructive pulmonary disease to avoid endotracheal intubation.¹⁰ Refractory hypercapnia or application of ultraprotective ventilation was another use in ventilated patients affected by acute respiratory distress syndrome (ARDS).^{11,12} Thus, both vv-ECMO and ECCO₂R are extracorporeal respiratory support systems that allow blood decarboxylation, but their importance is variable depending on the kind of device used.

Many determinants of extracorporeal blood decarboxylation have been described in previous works: the oxygenator surface and its intrinsic properties (i.e., shape, intra-oxygenator recirculation rate, and dead space), blood content of CO₂ in the drainage cannula, but especially the BF and GF.¹³⁻¹⁵ Using a low BF (<1 L/min), GF has a logarithmic association with CO₂ removal.^{16,17} In this setting, the main limiting parameter of blood decarboxylation is the low value of extracorporeal circulation flow. In contrast, using higher BF_s (i.e., vv-ECMO or high-flow ECCO₂R), the association between GF and CO₂ removal is linear.¹⁸ Based on this rationale, several authors have proposed using the GF/BF ratio to predict decarboxylation, which has also been reported to be linearly associated with CO₂ removal. However, the GF/BF ratio depends on the value of BF, leading to great variability in the value of CO₂ removal for a given GF/BF ratio. To understand the decarboxylation dose, it would seem more logical to consider the interdependence of the two variables, GF and BF, as previously proposed by Lehle *et al.*¹⁹; thus the product of BF and GF may be a more relevant variable to predict CO₂ removal. Surprisingly, to our knowledge, this simple parameter has never been studied directly. In the present study, we therefore hypothesized that BF × GF would be the central determinant of blood decarboxylation under extracorporeal respiratory support with vv-ECMO or high-flow ECCO₂R.

The main goal of the present study was to assess the performance of BF × GF, named the decarboxylation index in our work, to predict extracorporeal CO₂ removal and minute ventilation reduction under vv-ECMO and high-flow ECCO₂R.

Materials And Methods

Study Design and Patients

After obtaining local ethics committee agreement (IRB number 202000662, Montpellier University Hospital), all patients who benefited from extracorporeal respiratory support by vv-ECMO or high-flow ECCO₂R (i.e., BF ≥ 2 L/min) in our critical care unit between January 2018 and July 2020 were assessed retrospectively for the present study. Exclusion criteria were minors, pregnancy, an ongoing juridic protection, and premature death within the first 24 h after the initiation of extracorporeal respiratory support.

Management of Patients

The pattern of extracorporeal respiratory support was chosen in our cohort according to the clinical context. Details of specific indications, devices used, cannulation procedures, specific management, monitoring, anticoagulation protocol and weaning of extracorporeal respiratory support are presented in Supplemental Digital Content 1. Briefly, patients who were hypoxemic, including cases of severe ARDS, benefited from vv-ECMO therapy using a femoro-jugular configuration as first line: 25–29 Fr (drainage)/20–22 Fr (reinfusion) cannulas and a 1.8 m² oxygenator (CardioHelp HLS 7.0 oxygenator; Maquet GmbH, Rastatt, Germany). For patients with acceptable oxygenation but under aggressive ventilation or with uncontrolled hypercapnia, high-flow ECCO₂R therapy was proposed using a jugulo-jugular ipsilateral configuration as first line: 19–21 Fr (drainage)/16 Fr (reinfusion) cannulas and a 1.3 m² oxygenator (CardioHelp HLS 5.0 oxygenator; Maquet GmbH). Minimal pump flow was established at 2 L/min in our protocol.

Data Collection

The following data were abstracted retrospectively from medical records and intensive care unit (ICU) monitoring records: demographics, medical history, occurrence of organ dysfunction (APACHE2 score; SOFA score), indications and characteristics of extracorporeal respiratory support as well as related complications. In addition, mechanical ventilatory parameters, vv-ECMO therapy parameters, and biology were extracted every 12 h. Blood gases were measured with an ABL90 Flex Plus blood gas analyser (Radiometer, Copenhagen, Denmark). Details of the duration of mechanical ventilation and extracorporeal respiratory support therapy, tracheotomy needs, length of ICU and hospital stay, survival on discharge and cause of death were collected.

Study Definitions

Baseline data were the values before initiation of extracorporeal respiratory support therapy. D1_A was considered as the first measure within 12 hours after extracorporeal respiratory support (initiation or oxygenator change), and D1_B as the consecutive measure 12 h later, and so on.

The decarboxylation index was defined as the product BF × GF and expressed in L²/min².

CO₂ removal through the membrane oxygenator expressed in mL/min was assessed using the standard formula: CO₂ removal = (c_tCO_{2-in} - c_tCO_{2-out}) × BF × 10/1000. Normalized CO₂ removal was calculated by normalizing the partial pressure of carbon dioxide before the lung membrane to 45 mmHg as described previously.²⁰

The mechanical ventilation reduction (MVR) ratio was defined as the percentage of reduction of expired minute ventilation compared with the value before initiation of extracorporeal respiratory support.

Statistical Analysis

The characteristics of the patients at baseline are reported as percentages for categorical variables and as medians (interquartile range [IQR]) for continuous variables. Categorical variables were compared with the chi-squared test, and continuous variables were compared with a Wilcoxon test. After presenting the cohort and extracorporeal therapies, each oxygenator was analysed independently from its rank of use to consider possible alterations in oxygenator gas exchanges. To minimize the risk of underestimating CO₂ removal or the performance of the decarboxylation index caused by extracorporeal respiratory support membrane alteration, the data analysis was focused on the 7 first days. Moreover, analysis of the decarboxylation index in the range 20–30 L²/min² was performed because this range of values corresponds to the maximum dose under high-flow ECCO₂R therapy (BF, 2–3 L/min; GF, 10 L/min).

Thereafter, the relationship between the decarboxylation index and CO₂ removal was studied as our primary endpoint. The association between these two variables was assessed through a linear regression model to highlight the direct potentiation of BF and GF under extracorporeal respiratory support. Homoscedasticity and the distribution of the residuals were assessed graphically to confirm the robustness of the regression analysis. Adjustment of the model was assessed using R² and the Bland-Altman approach; predicted and observed values were thus compared; the mean of differences was the mean bias and the standard deviation of these differences represented the dispersion. The relationship between the decarboxylation index and the MVR ratio was studied to highlight the direct clinical consequences of the decarboxylation index. Because visual analysis of the repartition showed two distinct phases separated by a threshold of the decarboxylation index (25 L²/min²), we chose to perform two linear regression models *a posteriori* to increase the accuracy of the modelling: one for decarboxylation index values <25 L²/min², another for values >25 L²/min². Statistical analysis was performed using XLSTAT Pro 5.7.2 (Addinsoft, New York, USA). A *P* value ≤0.05 indicated significance.

Results

Patient Characteristics and Management

Among the 24 patients who benefited from extracorporeal respiratory support during the study period, 6 were excluded: 3 patients due to premature death and 3 due to missing data. Eighteen patients were included in the final analysis (APACHE2 = 57 [IQR, 40–70], SOFA at vv-ECMO initiation = 11.6 [IQR, 9–13.8]). Reasons for hospitalization were bacterial pneumonia (8 of 18, 44%), severe trauma (8 of 18, 44%), pulmonary embolism (1 of 18, 5%), others (1 of 18, 5%). The main characteristics and demographics of the patients, as well as ventilatory parameters and blood gases before initiation of extracorporeal respiratory support are presented in Table 1.

Thirteen patients (72%) were treated initially with vv-ECMO, and 5 (28%) were treated with high-flow ECCO₂R. Duration of mechanical ventilation, ICU stay and total hospital stay were 25 days (IQR, 11–34

days), 36 days (IQR, 11–46 days), 48 days (IQR, 13–69 days), respectively for 1.8 m² oxygenators. Corresponding values for 1.3 m² oxygenators were 14 days (IQR, 6–35 days), 24 days (IQR, 15–46 days), and 58 days (IQR, 56–65 days), respectively. Outcomes, complications, total duration of extracorporeal respiratory support, details of configurations used and changeout procedures are presented in Supplemental Digital Content 1.

Extracorporeal Respiratory Support and Mechanical Ventilation Changes

For 1.8 m² oxygenators, extracorporeal parameters at D1_A were BF 4.3 L/min (IQR, 3.5–5.0 L/min), GF 4 L/min (IQR, 5–6 L/min), resulting in a median decarboxylation index of 23.4 L²/min² (IQR, 12.0–30.8 L²/min²). Extracorporeal therapy allowed a clinically significant reduction of mechanical ventilation from baseline to D1_A: V_T -3.3 mL/kg (IQR, 0.3–4 mL/kg); respiratory rate (RR) -15 cycles/min (IQR, 4.5–16.5 cycles/min); P_{PLAT} -7 cmH₂O (IQR, 0.7–14.5 cmH₂O); driving pressure -5.5 cmH₂O (IQR, 0–12.7 cmH₂O); VM_E -7.2 L/min (IQR, 2.4–10.1 L/min) leading to an MVR of 88%; values for crude and normalized CO₂ removal were 393 mL/min (IQR, 310–526 mL/min) and 385 mL/min (IQR, 203–524 mL/min), respectively. During the first week, these parameters were stable globally (**Figure 1**). Paired BF and GF are presented in (**Figure 2**). PaCO₂ during the first week of extracorporeal therapy was <35 mmHg for 11% of samples (27 of 251) and >45 mmHg for 26% of samples (67 of 251).

For 1.3 m² oxygenators, the extracorporeal parameters at D1_A were BF 2 L/min (IQR, 1.8–2.5 L/min), GF 8 L/min (IQR, 6.5–9 L/min), resulting in a median decarboxylation index of 15 L²/min² (IQR, 14.5–19.9 L²/min²). Extracorporeal therapy allowed a clinically significant reduction of mechanical ventilation from baseline to D1_A: V_T -2.1 mL/kg (IQR, 1.4–2.2 mL/kg); RR -10 cycles/min (IQR, 8–10 cycles/min); P_{PLAT} -4 cmH₂O (IQR, 2–13 cmH₂O); driving pressure -8 cmH₂O (IQR, 5–14 cmH₂O); VM_E -6.5 L/min (IQR, 6.2–8 L/min) leading to an MVR of 76%; values for crude and normalized CO₂ removal were 179 mL/min (IQR, 165–235 mL/min) and 171 mL/min (IQR, 157–235 mL/min), respectively. During the first week, these parameters were stable globally (**Figure 1**). PaCO₂ during the first week of extracorporeal therapy was <35 mmHg in 7% of samples (4 of 59) and >45 mmHg in 32% of samples ((19 of 59).

Specific Thresholds for a Decarboxylation Index of 20–30 L²/min²

A decarboxylation index of 20 L²/min² was associated with an MVR ratio between 38% and 60% for 1.8 m² oxygenators and between 37% and 71% for 1.3 m² oxygenators, while maintaining physiological PaCO₂ values (**Figure 1**). Corresponding values for a decarboxylation index of 30 L²/min² were 58%–82% and 55%–73%, respectively.

Decarboxylation Index and Prediction of CO₂ Removal

The decarboxylation index had a linear association with CO₂ removal, with the 1.8 m² oxygenator ($R^2 = 0.62$, $P < 0.001$) and the 1.3 m² oxygenator ($R^2 = 0.77$, $P < 0.001$) (**Figure 3**); for each supplementary unit of the decarboxylation index, the CO₂ removal value increased 7 and 8 ml/min, respectively.

Comparing the observed and predicted values provided by linear regression models, mean bias were -3 mL/min and -2 mL/min; dispersions were 85 mL/min and 27 mL/min, respectively (**Figure 3**).

Decarboxylation Index and Prediction of MVR Ratio

Similarly, the decarboxylation index was found to be linearly associated with the MVR ratio using the 1.8 m² and 1.3 m² oxygenators. For 1.8 m² oxygenators, two linear regression models were built according to the decarboxylation index value. For values $<25 \text{ L}^2/\text{min}^2$, each supplementary unit of decarboxylation index was associated with a supplementary MVR ratio of 2% ($Y = 2 \times \text{decarboxylation index} + 20\%$; $P < 0.001$), whereas for values $>25 \text{ L}^2/\text{min}^2$, this increase was only of 0.5% ($Y = 0.5 \times \text{decarboxylation index} + 50\%$; $P < 0.001$) (**Figure 4**). The R^2 value for each model was 0.72 and 0.63, the mean bias was 1% and 3%, and the dispersion was 6% and 3%, respectively. For 1.3 m² oxygenators, only one linear regression was considered. Each supplementary unit of the decarboxylation index was associated with a supplementary MVR ratio of 1.5% ($Y = 1.5 \times \text{decarboxylation index} + 20\%$; $P < 0.001$) with an R^2 value of 0.62, a mean bias of 3% and a dispersion of 9% (**Figure 4**).

Discussion

The present series focused specifically on the determinant of blood decarboxylation under vv-ECMO (1.8 m² oxygenators) and high-flow ECCO₂R (1.3 m² oxygenators). Our study aimed to characterize the relationship between the BF \times GF product, named decarboxylation index, and CO₂ removal under extracorporeal respiratory support, as well as the reduction of minute ventilation. The primary finding is that the decarboxylation index is linearly associated with extracorporeal CO₂ removal with 1.8 m² oxygenators, as well as 1.3 m² oxygenators, in the BF range of 1.5–6.8 L/min; our linear regression models demonstrated a good adjustment ($R^2=0.62$ for 1.8 m² oxygenators, $R^2=0.77$ for 1.3 m² oxygenators) with low mean bias, suggesting a strong association between these two variables. The direct clinical consequence is that the decarboxylation index can predict minute ventilation reduction while maintaining PaCO₂ at physiological values. The linear regression models also showed good adjustment for 1.8 m² oxygenators ($R^2 = 0.72$ and 0.63), as well as 1.3 m² oxygenators ($R^2 = 0.62$) with significance. Our work therefore highlights that the decarboxylation index is a simple and reliable indicator for predicting the amount of blood decarboxylation under extracorporeal respiratory support and the potential of MVR. Moreover, based on these observations, the present analysis also supports that significant BF values must be used by clinicians to obtain an effective decarboxylation index, and

therefore clinically relevant CO₂ removal. Values in the range 20–30 L²/min² were associated with an MVR ratio between 38% and 58% for 1.8 m² oxygenators and between 37% and 55% for 1.3 m² oxygenators.

Blood decarboxylation by extracorporeal respiratory support is used increasingly as a therapeutic option in many clinical situations, either to avoid invasive mechanical ventilation or to reduce its well-known harmful effects.²¹ It has been demonstrated in the case of ARDS that decreasing V_T, airway pressures (driving pressure, P_{PLAT}) or RR while controlling PaCO₂ under mechanical ventilation is associated with a better outcome.^{22–25} Development of these concepts led to a strategy of ultrprotective mechanical ventilation associated with extracorporeal respiratory support for patients with severe ARDS to reduce VILI.^{11,26,27} Different devices may thus be used for this specific purpose, with various membrane surfaces and diverse ranges of extracorporeal BF, two main determinants of extracorporeal CO₂ removal. Although ECCO₂R has shown its efficacy for blood decarboxylation in different clinical settings, some studies revealed the modest potential of MVR when low BFs (<1 L/min) are used; V_T values were modestly decreased in these works, requiring maintenance of a high RR (25–30 cycles per minute) to control PaCO₂.^{28,29} Moreover, a non-negligible number of these patients experienced significant hypercapnia. The use of low BF appears to be a main cause of these failures. Accordingly, a recent secondary analysis has highlighted that the use of higher BFs (around 1 L/min) combined with larger oxygenator surfaces (1.3 m²) is more effective to apply ultrprotective ventilator settings.³⁰ These observations were also confirmed by Hermann *et al.*¹⁸ who demonstrated that CO₂ removal increased when the BF increased from 0.5 to 2 L/min. Therefore, the optimal value of BF required under ECCO₂R therapy has still to be determined. The answer depends probably on the patient's characteristics (pulmonary dead space, intrinsic CO₂ production, etc.) and the objectives of MVR.³¹

In addition to the BF, GF is also strongly correlated with CO₂ removal.¹⁴ Its value is usually between 0.5 and 12 L/min in most extracorporeal respiratory support devices. The influence of GF on blood decarboxylation potential is well known to strongly depend on the BF value; with a low BF, the relationship rapidly reaches a plateau, whereas with a BF higher than 1 L/min, the association GF–CO₂ removal seems to be more linear.¹⁸ Thus, the interdependency between BF and GF to predict blood decarboxylation has been highlighted in the literature, however no work has directly studied the product of these two variables. The present study was done to demonstrate that the decarboxylation index (BF × GF) is the cornerstone of blood decarboxylation achieved under extracorporeal respiratory support. One of the main strengths of our work is disposal of most of the inlet and outlet blood gases (sampled every 12 h), especially in a high BF under ECMO therapies where data on CO₂ removal are scarce. Thus, a linear association has been demonstrated in our work to predict CO₂ removal, as well as the MVR ratio. However, these findings are applicable for BF ranging from 2 to 6.8 L/min in vv-ECMO and from 1.7 to 3.2 L/min in ECCO₂R, resulting in a decarboxylation index ranging from 2 to 68 L²/min². More than a physiological reflection about CO₂ elimination, our analysis provides a clinical translation in terms of

mechanical ventilation to reduce dynamic stress induced by aggressive mechanical ventilation, which is probably one of the major challenges in patients with ARDS for the next decade. Furthermore, maintaining physiological PaCO₂ may also be crucial in many other pathologies such as massive airway leaks or total major bronchospasm where mechanical ventilation will fail. Our series demonstrates that vv-ECMO and ECCO₂R should not be thought of in opposition but as a continuum in terms of the amount of extracorporeal blood decarboxylation. Differences in the membrane surface influence CO₂ removal, but this was not considerable in our work (**Figure 3**). Note that when V_T decreased to very low values (near-apnoeic ventilatory strategy), the influence of an anatomical dead space component becomes dominant in the alveolar dead space fraction, explaining the lower ability to decrease mechanical ventilation with a given decarboxylation index. This justified performing two linear regressions to predict CO₂ removal under ECMO therapy.

To highlight the boundary between high-flow ECCO₂R and vv-ECMO, we specifically assessed the 20–30 L²/min² range. These values of the decarboxylation index, corresponding to a BF of 2–3 L/min and a GF of 10 L/min, allowed an MVR ratio of 38% to 58% for 1.8 m² oxygenators and 37% to 55% for 1.3 m² oxygenators. However, despite the use of a consistent level of blood decarboxylation, our results reveal that ultraprotective ventilation may be not reached for a non-negligible number of patients. Based on this observation, we assume that jugulo-jugular high-flow ECCO₂R with a set BF around 2–3 L/min is an acceptable compromise in the absence of hypoxaemia, allowing a sufficient amount of extracorporeal blood decarboxylation. This double cannulation configuration offers sufficient diameter and a low impedance allowing a stable extracorporeal BF, limited recirculation phenomena and low haemolysis. In our opinion, this percutaneous approach has an acceptable benefits/risks ratio for these severe critically ill patients while providing an optimal BF. Furthermore, jugulo-jugular high-flow ECCO₂R may be simply converted to a femoro-jugular V-VV ECMO configuration in the case of delayed refractory hypoxaemia. Future studies will be needed to assess the real benefits of this particular configuration in patients with ARDS, as well as the superiority of ultraprotective ventilation strategies under extracorporeal respiratory support.

Our study has several limitations. First, it is a single-centre retrospective design, with limited extrapolation and missing data. Second, data on the estimated pulmonary dead space fraction before extracorporeal respiratory support initiation, an important determinant of CO₂ removal, were not available. Third, the performance of membrane gas exchange of the extracorporeal respiratory support was considered stable during extracorporeal therapy and might influence the results. This justified data collection only during the first week.³² Finally, the present series included different clinical situations and different configurations of extracorporeal respiratory support. However, we assume that our analysis provides a global tool to understand the level of extracorporeal decarboxylation.

Conclusions

Our findings support that the decarboxylation index is a simple and reliable indicator to estimate CO₂ removal under extracorporeal respiratory support. The decarboxylation index may also predict the potential of MVR and should be considered more in clinical practice. Our study highlights that a decarboxylation index >20 L²/min² could be insufficient to achieve an ultraprotective ventilation, suggesting that a BF <2 L/min does not lead to the necessary level of extracorporeal blood decarboxylation in several patients. Further studies on extracorporeal respiratory support are necessary to confirm our assumptions and to understand the precise targets of BF necessary in clinical practice.

Declarations

Support was provided only from institutional sources.

No conflict of interest is declared.

Ethical Approval And Consent to participate

Local ethics committee agreement (IRB number 202000662, Montpellier University Hospital) was obtained. Consent to participate was no requested in agreement with the French health research laws in retrospective design studies.

Consent for publication

Consent for publication is given by all authors.

Availability of supporting data

Supporting data are fully available on request.

Competing interests

The authors declare that there is no conflict of interest.

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Author's contributions

PD, MG, OM, CM, HW retrieved the data. TL and JC performed the study draft and statistical analysis of the data. TL and JC wrote the manuscript, which was reviewed by EC, GD and XC. All authors contributed to critical reading of the text and its revision. All authors read and approved the final manuscript.

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Table

Table 1. Characteristics of the Patients

	Overall (<i>n</i> =18)	vv-ECMO (<i>n</i> =13)	High-flow ECCO ₂ R (<i>n</i> =5)	<i>P</i> value
Demographics	-	-	-	-
Age (years)	44 (32–62)	46 (31–65)	42 (41–43)	0.62
Male, <i>n</i> (%)	14 (77)	11 (84)	3 (60)	0.26
BMI (kg/m ²)	27.3 (25.3–30.5)	28.3 (27–30.9)	25.7 (23.5–26.6)	0.15
IBW (kg)	72 (66–75)	75 (66–75)	66 (60–73)	0.42
RESP score	-1.5 (-3.8 to 3.8)	-1 (-4 to 3)	-2 (-2.5 to 0)	0.51
IGS II score	56 (40.3–70)	57 (50–67)	38 (26–73)	0.45
SOFA score at treatment initiation	11 (9–13.8)	12 (10–14)	9 (8–9)	0.032
Cause of ICU admission, <i>n</i> (%)				
Pneumonia	8 (44)	5 (38)	3 (60)	0.41
Severe trauma	8 (44)	6 (46)	2 (40)	0.81
Pulmonary embolism	1 (5)	1 (13)	0 (0)	0.52
Allergic bronchospasm	1 (5)	1 (13)	0 (0)	0.52
Ventilatory parameters				
V _{Te} (mL/kg IBW)	6.4 (5.8–6.9)	6.3 (5.4–6.5)	6.6 (6.0–8.0)	0.26
Respiratory rate (cycles/min)	26 (24–28)	27 (25–28)	25 (22–28)	0.86
VMe (L/min)	12.0 (8.7–13.9)	11.8 (9.3–13.1)	13.4 (8.8–14.2)	0.66
P _{PLAT} (cmH ₂ O)	32 (28–36)	34 (28–38)	31 (31–34)	1
PEEP (cmH ₂ O)	12 (10–14)	12 (8–15)	12 (12–12)	0.93
Driving pressure (cmH ₂ O)	20 (17–22)	20 (15–21)	19 (19–22)	0.92
FiO ₂ (%)	100 (76–100)	100 (100–100)	50 (50–100)	0.06
Admission-to-MV time (h)	0.3 (0–0.3)	0 (0–0.3)	0.3 (0.3–4)	0.17
MV-to-treatment initiation time (h)	50 (5–128)	29 (5–156)	71 (28–77)	0.69

Prior prone positioning, <i>n</i> (%)	6 (33)	5 (38)	1 (20)	0.45
Blood gases				
PaO ₂ (mmHg)	65 (54–78)	57 (53–71)	83 (77–140)	0.01
PaO ₂ :FiO ₂ ratio	71 (63–90)	65 (54–74)	173 (166–253)	0.01
SaO ₂ (%)	90 (88–97)	88 (87–90)	98 (96–99)	0.02
PaCO ₂ (mmHg)	54 (46–60)	57 (44–60)	47 (47–60)	1
pH	7.34 (7.20–7.36)	7.35 (7.19–7.41)	7.32 (7.31–7.35)	0.31
HCO ₃ ⁻ (mEq)	26.9 (20.1–32.3)	27.9 (17.5–32.7)	25.8 (24–31.2)	0.80
Hb (g/L)	10.0 (9.1–12.3)	10.1 (9.2–12.3)	9.4 (8.7–12.1)	0.50

Mann-Whitney or chi² test was used as appropriate. Data are presented as median (IQR) except where indicated otherwise. BMI, body mass index; ECCO₂R, extracorporeal carbon dioxide removal; IBW, ideal body weight; ICU, intensive care unit; MV, mechanical ventilation; RESP, Respiratory Extracorporeal Membrane Oxygenation Survival Prediction; vv-ECMO, veno-venous extracorporeal membrane oxygenation.

Figures

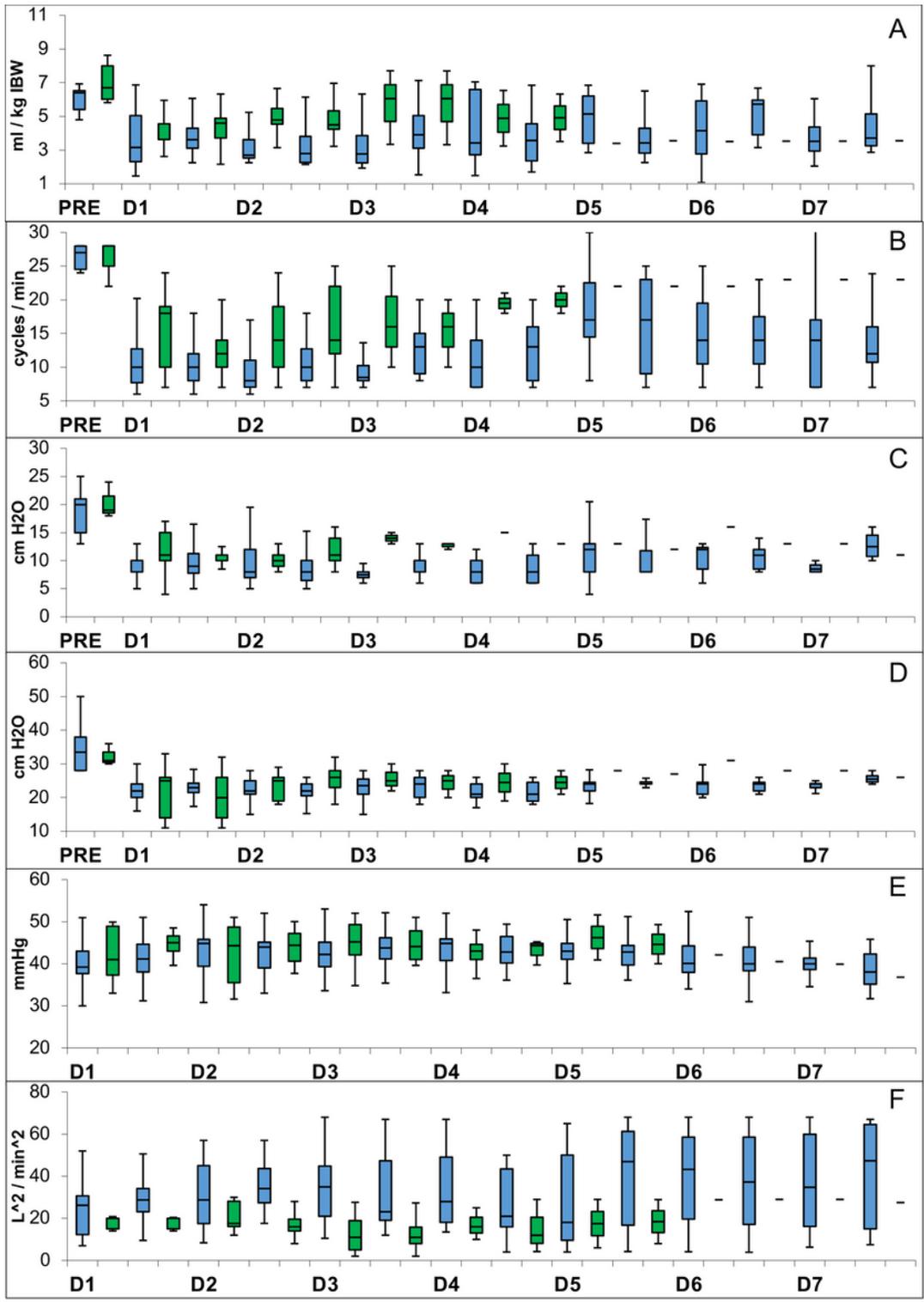


Figure 1

Evolution of VT_e (A), respiratory rate (B), plateau pressure (C), driving pressure (D), PaCO₂ (E), decarboxylation index (F) over the first 7 days of treatment (D1 to D7) for 1.8 m² oxygenators (blue) and 1.3 m² oxygenators (green) measured every 12 h. D1, day 1 of treatment; IBW, ideal body weight; PRE, pre-treatment parameters.

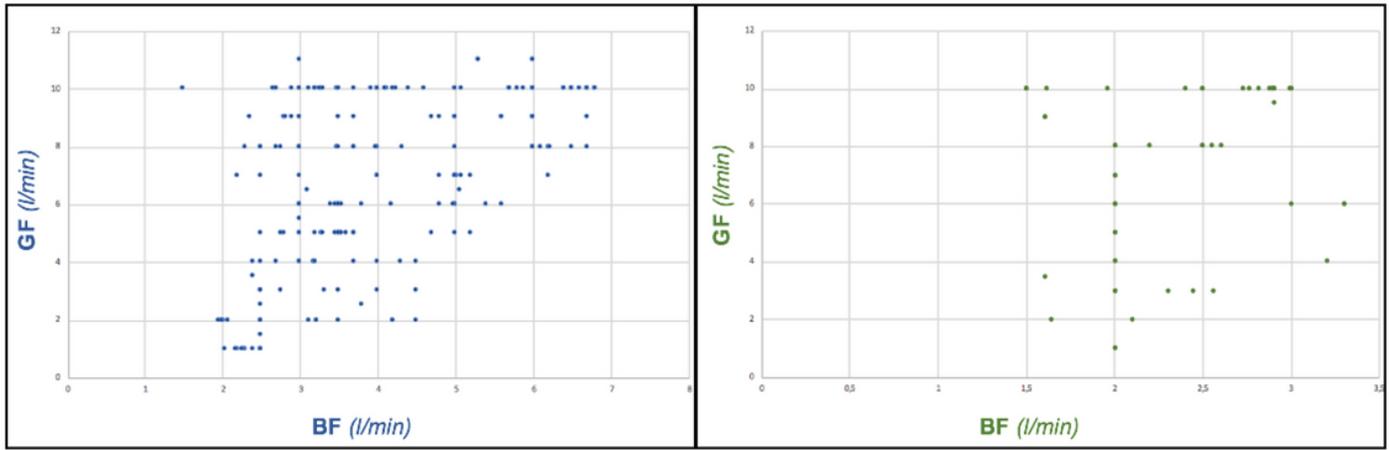


Figure 2

Dispersion for observed BF/GF couples for 1.8 m² (left, blue) and 1.3 m² (right, green) oxygenators.

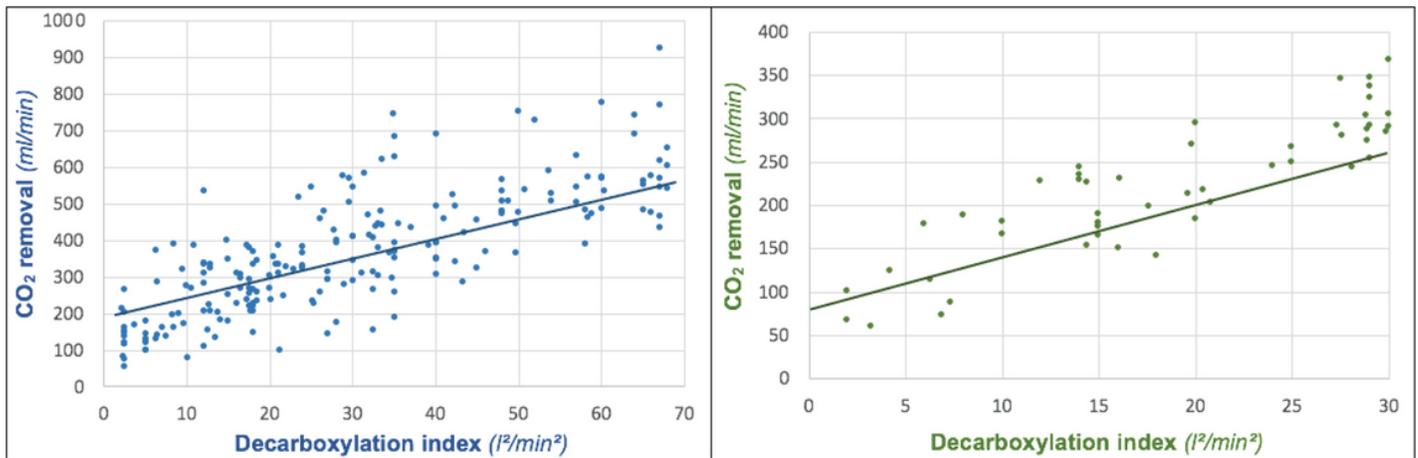


Figure 3

Linear regression of CO₂ removal according to the decarboxylation index for 1.8 m² oxygenators (left, blue) and 1.3 m² oxygenators (right, green). The respective equations are as follows: CO₂ removal = 7 × decarboxylation index + 160 (R² = 0.62, P < 0.001); CO₂ removal = 8 × decarboxylation index + 80 (R² = 0.77, P < 0.001).

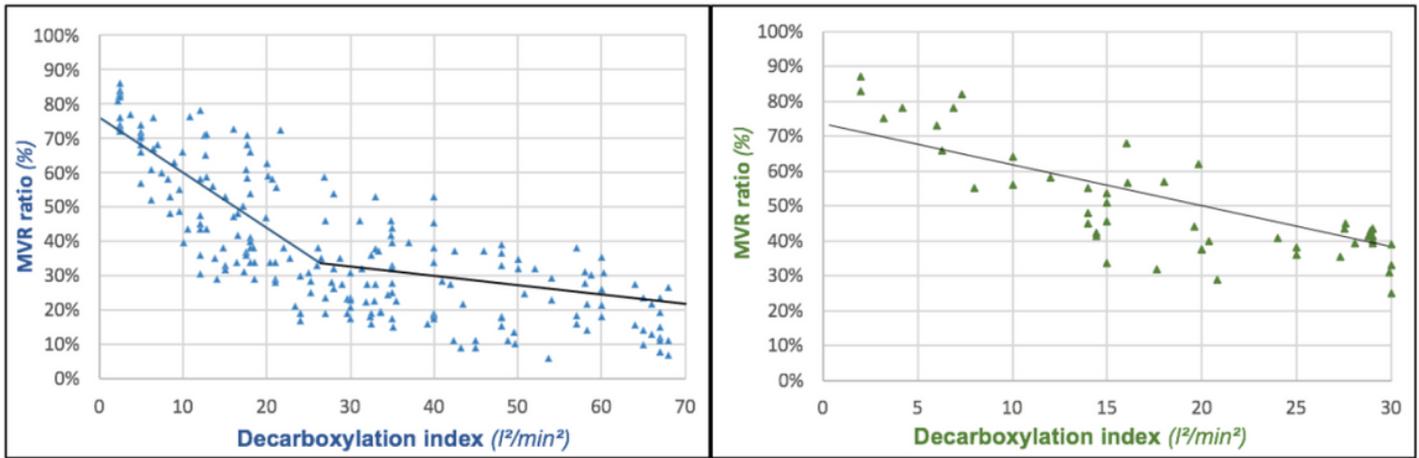


Figure 4

Linear regression of the mechanical ventilation reduction (MVR) ratio according to the decarboxylation index for 1.8 m² oxygenators (left, blue) and 1.3 m² oxygenators (right, green). The respective equations are as follows: MVR ratio = 80% - 2 × decarboxylation index <25 L²/min² (R² = 0.72, P < 0.001), MVR ratio = 50% - 0.5 × decarboxylation index >25 L²/min² (R² = 0.63, P < 0.001); MVR ratio = 80% - 1.5 × decarboxylation index (R² = 0.62, P < 0.001).

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