

Simultaneous Perception of Prosthetic and Natural Vision in AMD Patients

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Article

Keywords: age-related macular degeneration, photoreceptors, prosthetic and natural vision, simultaneous perception

Posted Date: March 26th, 2021

DOI: <https://doi.org/10.21203/rs.3.rs-141505/v1>

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Version of Record: A version of this preprint was published at Nature Communications on January 26th, 2022. See the published version at <https://doi.org/10.1038/s41467-022-28125-x>.

Abstract

Loss of photoreceptors in atrophic age-related macular degeneration (AMD) results in severe visual impairment. Since the low-resolution peripheral vision is retained in such conditions, restoration of central vision should not jeopardize the surrounding healthy retina and allow for simultaneous use of the natural and prosthetic sight. We report the first clinical results with a photovoltaic substitute of photoreceptors providing simultaneous use of the central prosthetic and peripheral natural vision in atrophic AMD. Four patients with geographic atrophy have been implanted subretinally with a wireless 2x2mm-wide 30 μm -thick device, having 378 pixels of 100 μm in size. They demonstrated Landolt acuity of 1.17 ± 0.13 pixels, corresponding to the Snellen range of 20/460–20/565. With electronic magnification of up to a factor of 8, patients demonstrated acuity in the range of 20/63 – 20/98. Under room lighting conditions, patients could simultaneously use prosthetic central vision and their remaining peripheral vision in the implanted eye and in the fellow eye.

Main Text

Age-related macular degeneration (AMD) is a leading cause of irreversible vision loss¹, and its prevalence dramatically increases with age: from 1.5% in the US population above 40 years to more than 15% in the subjects older than 80². The atrophic form of AMD (also known as geographic atrophy, GA) results in a gradual loss of photoreceptors in the central macula, which is responsible for high-resolution vision, and severely impairs reading and face recognition. Low-resolution peripheral vision is retained in this condition, enabling orientation and the use of eccentric fixation for visual discrimination at reduced acuity. Therefore, the goal of any treatment strategy should be to restore functional central vision without jeopardizing the surrounding retina and allowing for their simultaneous use.

While PRs gradually disappear in GA, the inner retinal cells survive to a large extent³. To restore sight in the scotoma, we replace the lost photoreceptors with photovoltaic pixels in the subretinal implant, which convert light into electric current to selectively stimulate the secondary neurons in the retina⁴. These electronic substitutes of photoreceptors replace the two main functions of the natural photoreceptors: (a) the light-to-current conversion, corresponding to the function of the outer segment, and (b) transfer of the visual information to secondary neurons by their polarization in extracellular electric field, substituting the function of the synapse.

To avoid irreversible electrochemical reactions at the electrode-electrolyte interface, stimulation current is pulsed and charge-balanced. On the other hand, to provide steady visual percepts under pulsatile illumination, repetition rate should exceed the frequency of flicker fusion. In preclinical studies, we demonstrated that selective stimulation of bipolar cells without direct activation of the downstream neurons results in preservation of multiple features of the natural retinal signal processing, including flicker fusion, adaptation to static images⁴, ON and OFF responses with antagonistic center-surround⁵, and non-linear summation of subunits in RGC receptive fields⁴. We have also shown that visual acuity matches the pixel pitch with 75 and 55 μm pixels^{4,6}.

The first generation of the human-grade photovoltaic subretinal prosthesis PRIMA (Pixium Vision SA, Paris, France) is 2 mm in width ($\sim 7^\circ$ of the visual angle in a human eye), 30 μm in thickness, containing 378 hexagonal pixels of 100 μm in width. Images captured by the camera are processed and projected onto the retina from video glasses using intensified light (Fig. 1). To avoid photophobic and phototoxic effects of bright illumination, we use near-infrared (NIR, 880 nm) wavelength⁷. Photovoltaic pixels in the implant directly convert the projected pulsed light into local electric current flowing through the retina between the active and return electrodes^{4,8}.

Five patients with GA were implanted in Paris during 2017–2018 (NCT03333954). In four of them, the implant was placed in the subretinal space, but in one it ended up inside the choroid due to patient's accidental movement during surgery. In one of the four patients, the implant accidentally shifted by about 2 mm from the central position after the fluid-air exchange since the patient did not keep the head in a prone position post implantation. Due to wireless nature of the implant, surgical procedure was relatively short – about 2 hours⁹. As shown in Table 1, residual natural acuity in the operated eye did not decrease in any of the subjects. Interestingly, in some patients, acuity improved compared to baseline, which could be attributed to either a neurotrophic benefit of subretinal surgery¹⁰ or of electrical stimulation¹¹ or just improvement with eccentric fixation after training.

In the first phase of the trial, reported earlier⁹, prosthetic vision was assessed independently from the remaining natural vision. For this purpose, opaque virtual reality glasses (VR, PRIMA-1) have been used. The projected images covered a horizontal field of 5.1 mm (17.5° on the retina), with approximate resolution of 10.5 μm . Maximum peak retinal irradiance was 3 mW/mm^2 , well within the thermal safety limits for chronic use of near-infrared light¹². Brightness of the percept was controlled by pulse duration, between 0.7 and 9.8 ms, in 0.7-ms increments.

The four patients with subretinal implant placement demonstrated monochromatic (white-yellowish “sun-color”) shaped vision, with flicker fusion above 30 Hz. In three patients with central location of the subretinal implant, acuity closely matched the pixel size: 20/460, 20/500 and 20/550 (1.1, 1.2 and 1.3 pixels). Patient with the off-center implant demonstrated lower acuity: 20/800 (1.9 pixels)⁹. Patient #1 with the intra-choroidal implant had blurry prosthetic vision, with no discernable acuity.

In the second phase of the study, starting at 18–24 months post-op, we introduced augmented reality glasses (AR, PRIMA-2), which allow unobstructed natural vision by the fellow eye and by the peripheral field of the operated eye, simultaneously with prosthetic central vision in the treated eye (Fig. 2a). The projected images covered a horizontal field of 5.3 mm (18.5°) on the retina, with a resolution of 6.7 μm , as illustrated in Fig. 2b. This design provided improved beam homogeneity and easier alignment, compared to VR glasses (PRIMA-1). The maximum retinal irradiance was increased to 3.5 mW/mm^2 , with the same range of pulse durations as in the VR glasses. This system allows the use of electronic magnification (x1, x2, x4 and x8) between the camera and the image projection onto the implant. As shown in Table 1, perceptual thresholds 18–24 months after the implantation, measured with PRIMA-2

glasses, were slightly lower than the thresholds measured during the first 6 months - in the first phase of the trial⁹. Patient #3 passed away due to unrelated cause before the second phase of the trial.

Prosthetic visual acuity with PRIMA-2 glasses was measured using Landolt C optotypes. To mimic the crowding effect of the letter charts, the Landolt rings were surrounded by a square frame (Fig. 3a). At each trial, subjects reported the font orientation (up, down, left or right), and its size was then adjusted, depending on the response. The visual acuity was determined using the Freiburg Visual Acuity Test (FrACT) software^{13,14}. For a stable perception under pulsatile illumination, 30 Hz repetition rate was applied. In the first set of the tests, computer-generated Landolt optotypes were projected into the eye directly from the AR glasses without using a camera. As shown in Table 1, patients #2 and #5 demonstrated prosthetic acuity at the level similar to that observed with VR glasses in the first phase of the trial (20/500, 20/460), but patient #4 significantly improved compared to the earlier result - from 20/800 to 20/438. This is potentially due to easier alignment of the display to the off-center location of the implant with improved glasses. The average acuity in the four patients with the subretinal implant placement was 1.17 ± 0.13 pixels at the latest measurement, corresponding to logMAR 1.39, or 20/500 on a Snellen scale.

In the second set of the acuity tests, letters were displayed at 40 cm distance from the subject, so patients used camera and were allowed to apply their preferred electronic magnification (1, 2, 4 or 8). To ensure that prosthetic acuity is measured rather than the residual natural vision, in these tests the fellow eye was covered. In addition, contrast of the electronic image was inverted from the original black letter on white background to white letters on black background (white patterns stimulate the retina), and patients were asked about the color of the percept. With magnification, all three participants of the second trial demonstrated significant improvement in prosthetic acuity: to the level of 20/98, 20/71 and 20/63, respectively. As shown in Table 1, these values significantly exceeded their residual natural acuity in the treated eye, and for patients 4 and 5, even in the (better) fellow eye.

Video S1 illustrates a test of prosthetic vision using an ETDRS chart, with 4x magnification and a contrast reversal. Video S2 illustrates a reading test with 4x magnification and a control experiment (Video S3) where patient is attempting to read the same word without the PRIMA glasses.

To evaluate the effect of background light on prosthetic vision when the transparent AR glasses are used, Landolt C optotypes have been presented on the glasses display directly, without using the camera, while intensity of the background visible light was varied. In this experiment, subjects with both eyes open were placed 40 cm in front of a wide LCD screen, where a homogeneous white illumination at 16 levels (ranging from 1.4 to 256 cd/m²) was presented. Prosthetic patterns were presented at maximum brightness: 3.5 mW/mm² of NIR irradiance with 9.8 ms pulse duration. As shown in Table 1, subjects 2 and 4 did not have a problem seeing the Landolt C in front of the screen even with the highest background luminance (256 cd/m²). Subject 5 had difficulties with luminance above 64 cd/m², and therefore was provided later with a shaded lens (65% attenuation of white light) to allow using the device in a bright office environment.

It is important to note that patients could simultaneously use prosthetic and residual natural vision from both, the study eye, and the fellow eye. For example, in a setup shown in Fig. 3b, green bars of various orientations were presented on a large screen for natural vision and another set of bars was simultaneously presented just on the NIR display inside the glasses. The patient was asked about both orientations and colors, as illustrated in the video S4 for binocular vision and in S5 for monocular vision. In both cases, bars were perceived simultaneously and orientations detected correctly.

In summary, this trial confirmed the safety and stability of the PRIMA implant over 24–30 months follow-up in four patients with geographic atrophy. Prosthetic central vision in the former scotoma represents shaped monochromatic perception matching the presented patterns and, most importantly, is perceived in conjunction with the residual peripheral vision, thus enabling natural orientation and central discrimination. Spatial resolution was, on average, 1.2 pixels of the implant, corresponding to letter acuity of about 20/500, and using electronic magnification, all patients with subretinal implant demonstrated acuity exceeding 20/100. Further advancements in the photovoltaic pixel design¹⁵, video glasses and image processing promise even more functional restoration of sight for numerous patients suffering from atrophic macular degeneration.

Methods

Patients

The aim of this study (NCT03333954) was to test functionality of the PRIMA system in 5 patients with atrophic AMD. The study adhered to the Declaration of Helsinki and received the ethics committee approval from the Comité de Protection des Personnes Ile de France II and approval by the Agence Nationale de Sécurité du Médicament et des Produits de Santé in France. Study participants were above 60 years of age and had advanced atrophic AMD with an atrophic zone of at least 3 optic disc diameters and best corrected visual acuity of $\leq 20/400$ in the worse-seeing study eye; no foveal light perception (absolute scotoma) but visual perception in the periphery, with preferred retinal locus determined by micro-perimetry; absence of photoreceptors and presence of the inner retina in the atrophic area as confirmed by optical coherence tomography (OCT); absence of choroidal neovascularization verified by retinal angiography. All other ocular and general pathologies that could contribute to the low visual acuity were excluded. Patients provided written informed consent to participate in the study. Implantation took place at the Foundation A Rothschild Hospital (Paris, France). The patients' rehabilitation and visual function assessment were carried out at the Clinical Investigation Center of Quinze-Vingts National Eye Hospital (Paris, France).

Assessment of prosthetic vision

Visual acuity was assessed using a computer-generated Landolt C in 4 different orientations (gap at the top, bottom, right or left), so that a random response corresponds to 25% accuracy. The threshold optotype size was defined as the proper symbol recognition with at least 62.5% accuracy. To minimize

the number of presentations, the study was conducted using the method of the Freiburg Acuity and Contrast Test (FrACT) test¹⁴. In this protocol, a single Landolt C is presented in a fixed central position on a display, and the best Parameter Estimation by Sequential Testing (best PEST) procedure¹⁶ was used to estimate the VA. Since it is an adaptive test, the number of times that each optotype is presented varies depending on the patient responses. The test was performed three times on three different days. At each day, 24 trials were performed twice, and the mean of these two runs was considered the daily result. The final result was defined as the median of the three daily measurements. To mimic the crowding effect of the letters in vision charts, Landolt C was presented with a frame around it (Figure 3a).

Background illumination

To provide a uniform and controllable background illumination, a 71 cm-wide Samsung U28E590D LCD screen has been used. Subjects were placed 40 cm in front of a screen, where a homogeneous white illumination at 16 levels was presented: 256, 181, 128, 90.5, 64, 45.3, 32, 22.6, 16, 11.3, 8, 5.7, 4, 2.8, 2, 1.4 cd/m², while room lights were turned off.

The best-PEST (Parameter Estimation by Sequential Testing) method¹⁶ was used to determine the maximum luminance which still allowed identifying the prosthetic patterns (Landolt C optotypes with four different orientations) with accuracy exceeding 62.5% using the following parameters: 20 iterations, 0.25 false positive rate, 0 false negative rate, and sigmoid slope of 0.5. The last value of the best-PEST was used as the resulting threshold luminance. Data for the three patients with a subretinal implant are presented, but not for subject #1 since this subject with intra-choroidal chip placement could not recognize Landolt C. Prosthetic patterns were presented at maximum brightness: 3.5 mW/mm² of NIR irradiance with 9.8 ms pulse duration and 30 Hz repetition rate. The patterns were presented for up to 30 seconds, with 10 seconds break between the stimuli.

Simultaneous perception of prosthetic and natural vision

A green bar is displayed on an LCD screen placed at 40 cm in front of the subject in one of the four possible orientations (vertical, horizontal, 45° diagonal from the upper left, 45° diagonal from the lower left). Simultaneously a bar is also projected in Artificial Pattern Mode (APM) on the PRIMA Glasses in one of the four orientations (Figure 3b). The width of the bars corresponds to 0.4 mm on the retina (4 implant pixels). The bar orientation on LCD screen is random, but 50% of the times orientation of the bar displayed on the glasses matches the bar orientation on LCD. The subject is expected to see the bar displayed on the LCD screen with the natural peripheral vision and report it as green, and the bar projected by the PRIMA Glasses with prosthetic vision, perceived as white. At each repetition, the subject is asked about orientation of each bar individually.

A total of 48 bar pairs were presented (24 presentations with the fellow eye open and 24 presentation with the fellow eye closed), each for a duration of up to 20 seconds. The subjects were not allowed to move their head – only the eyes.

Declarations

Consent: A healthy volunteer demonstrating the augmented reality glasses in Figure 3 consented to publication of her picture.

Acknowledgements

The authors thank the patients who participated in the study; the Pixium Vision team who designed, fabricated, and tested the PRIMA system; the Scientific and Medical Advisory Board of Pixium Vision for its guidance on the clinical trial design; and all the scientific, research and development, medical, and clinical research staff who continue the patient care, rehabilitation, and evaluation.

Financial disclosures: DP: Consultant, Patents and Royalties with Pixium Vision, YL: Consultant with Pixium Vision. JS: Equity owner at Pixium Vision.

Studies are supported by: Pixium Vision SA; the Sight Again project (via Structural R&D Projects for Competitiveness and Investment for the Future funding managed by BpiFrance) and the Clinical Investigation Center at the Quinze-Vingts National Hospital, which is supported in part by the Inserm-DHOS, France. DP is supported in part by the National Institutes of Health (R01-EY027786, P30-EY-026877) and by Research to Prevent Blindness.

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Table

Table 1. Residual natural vision, anatomical and functional outcomes with the implant.

* Patient 3 passed away before the second phase of the trial. ** Patient 5 was not available for this measurement because of the COVID restrictions.

Test \ Patient	1	2	3	4	5
<i>Residual peripheral vision</i>					
Pre-op eccentric natural letter acuity in the study eye	20/400	20/800	20/1000	20/500	20/500
Postop natural letter acuity in the study eye (12 months)	20/320	20/800	20/800	20/400	20/400
(24 months)	20/160	20/200	*	20/500	20/250
Pre-op letter acuity in the fellow eye	20/100	20/50	20/125	20/400	20/100
Postop letter acuity in the fellow eye (12 months)	20/160	20/50	20/200	20/400	20/125
(24 months)	20/160	20/50	*	20/640	20/125
<i>Implant location</i>					
Implant location in the macula	Intra-choroidal	Central subretinal	Central subretinal	Off-center subretinal	Central subretinal
<i>Stimulation threshold</i>					
Perceptual threshold with PRIMA 1 glasses, ms	2.1	0.8	0.7	1.0	0.8
Perceptual threshold with PRIMA-2 glasses, ms	1.28±0.84	0.75±0.19	*	0.82±0.29	0.70±0.00
<i>Prosthetic visual acuity</i>					
PRIMA-1 (VR), 12 months No magnification Min. Landolt C gap, pix	Light perception	20/550 logMAR 1.44 1.3 pix	20/500 logMAR 1.4 1.2 pix	20/800 logMAR 1.6 1.9 pix	20/460 logMAR 1.37 1.1 pix
PRIMA-2 (AR), 18-24 months No magnification Min. Landolt C gap, pix	Light perception	20/564 logMAR 1.45 1.34 pix	*	20/438 logMAR 1.34 1.04 pix	**
PRIMA-2 (AR), Landolt VA with preferred magnification, 18-24 months	Light perception	20/98 logMAR 0.69	*	20/71 logMAR 0.55	20/63 logMAR 0.5
Natural Landolt VA in the study eye, 18-24 months	20/182 0.96	20/246 logMAR 1.09	*	20/428 logMAR 1.33	20/332 logMAR 1.22
LogMAR gain due to PRIMA 18-24 months	0	0.4	*	0.78	0.72
<i>Background lighting</i>					
Background light threshold [cd/m ²]	NA, No shape perception	>256	*	>256	64
Attenuation for bright room lighting	NA	clear	*	clear	65%

Figures

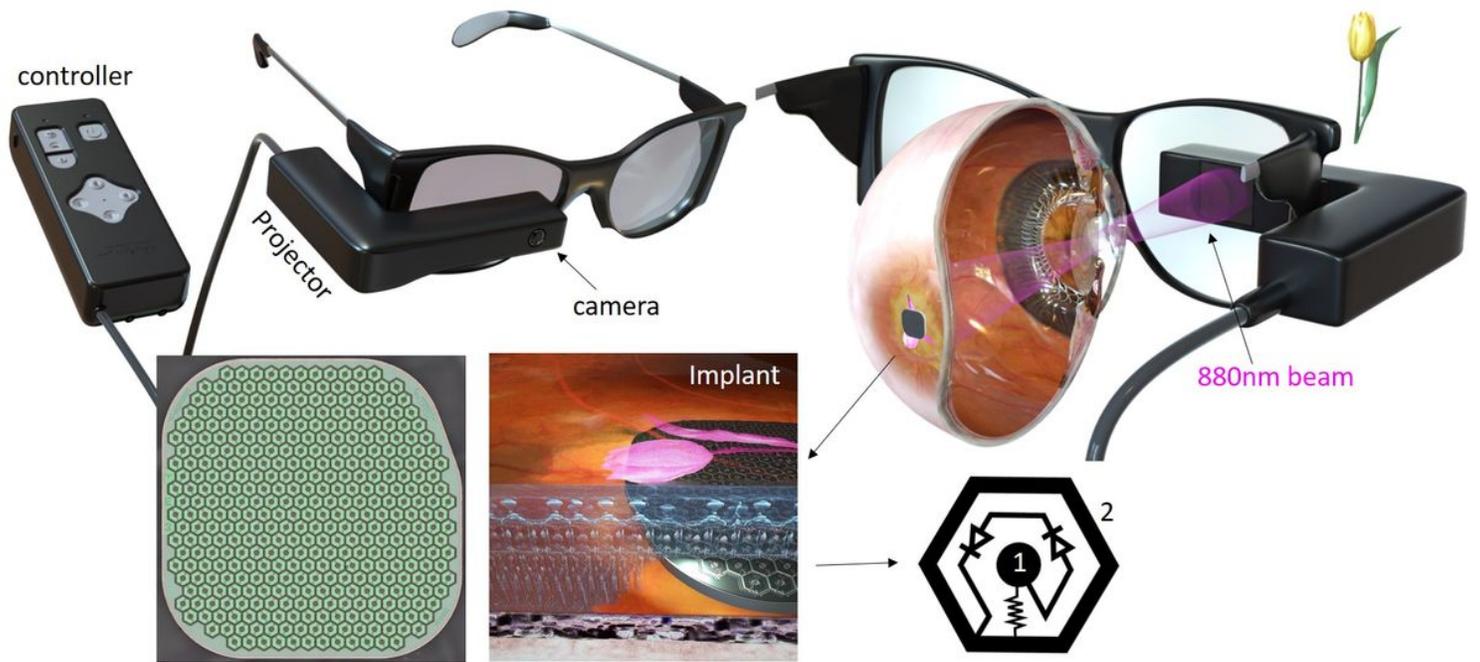


Figure 1

top row: Artistic rendering of the augmented reality glasses with a projector and a camera. The 880nm beam projects the video stream onto the retina. Bottom row: PRIMA implant with a hexagonal array of 100µm pixels. Implant is placed under the degenerate retina without damaging the peripheral healthy retina. Pixels are composed of two photodiodes connected in series between the active (1) and a circumferential return (2) electrode.

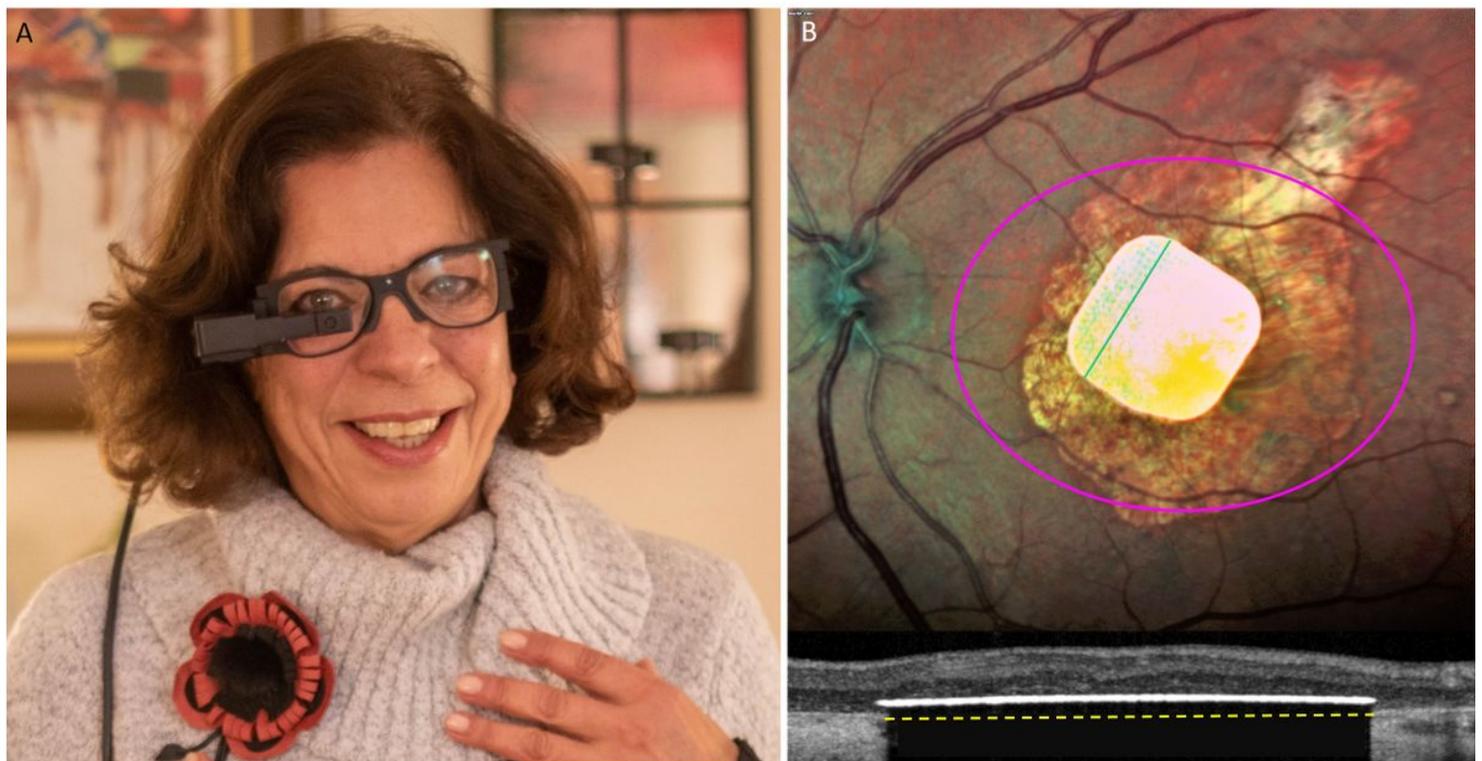


Figure 2

A. PRIMA-2 glasses on a person. B. Fundus photo of a patient with the PRIMA implant inside the geographic atrophy area. Magenta oval illustrates the size of the beam (5.3x4.3 mm) projected onto the retina. OCT image demonstrates the implant in subretinal space 6 months post-op. Yellow dash line depicts the approximate position of the back side of the implant resting on the Bruch's membrane.

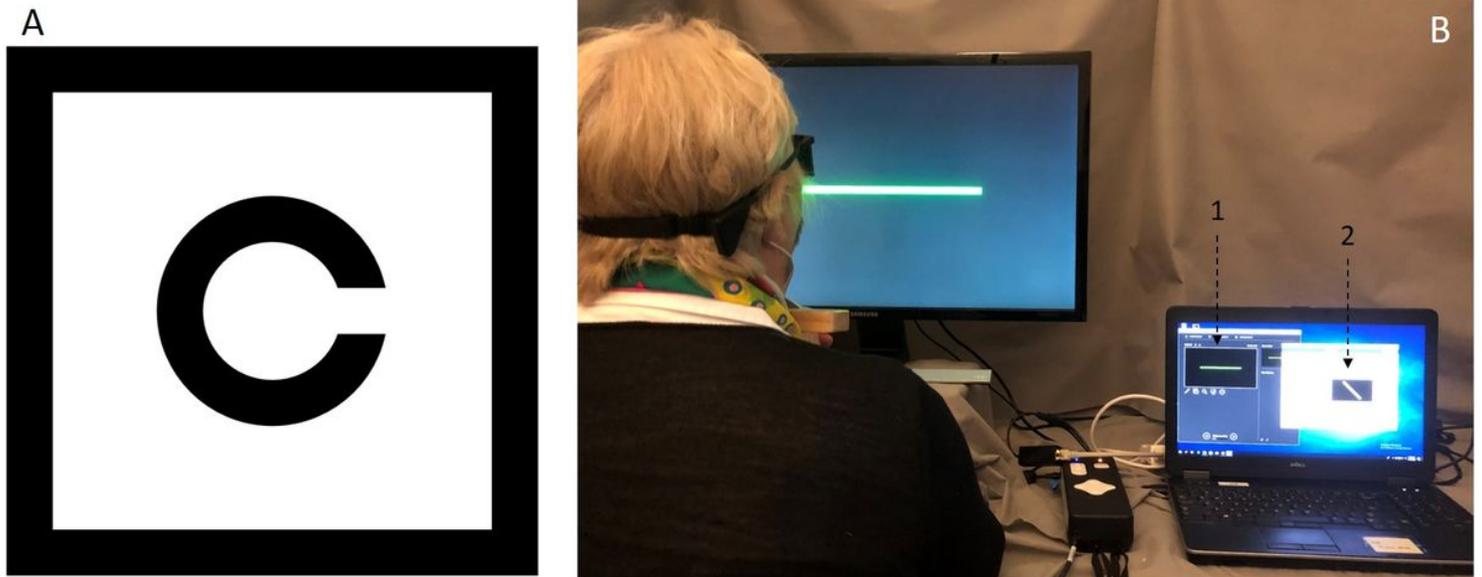


Figure 3

A. Landolt C in the frame mimicking the crowding effect. B. Testing setup with a patient sitting 40 cm from the screen. Horizontal green bar shown on a large display (1) can be seen with the remaining natural vision, while the diagonal bar (2) is presented only on the NIR display inside the glasses.

Supplementary Files

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- [VideoS1ETDRSanonym.mp4](#)
- [VideoS2Readingshortanonym.mp4](#)
- [VideoS3Readingnaturalcontrolanonym.mp4](#)
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- [VideoS5simultaneousmonocularanonym.mp4](#)
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