

Quantifiable Breathing Pattern Components Can Predict Asthma Control: an Observational Cross-sectional Study

Panagiotis Sakkatos (✉ sakkatosp@yahoo.gr)

Smart Respiratory Products Ltd <https://orcid.org/0000-0001-5801-9765>

Anne Bruton

University of Southampton

Anna Barney

University of Southampton

Research

Keywords: Breathing patterns, within-subject variability, asthma control, Structured Light Plethysmography

Posted Date: January 25th, 2021

DOI: <https://doi.org/10.21203/rs.3.rs-152796/v1>

License:  This work is licensed under a Creative Commons Attribution 4.0 International License.

[Read Full License](#)

1 **Title:** Quantifiable breathing pattern components can predict asthma control: an observational
2 cross-sectional study

3 **Authors:** Panagiotis Sakkatos¹, Anne Bruton¹ and Anna Barney²

4 ¹School of Health Sciences, University of Southampton, UK

5 ²Institute for Sound and Vibration Research, University of Southampton, UK

6 **Corresponding author:** Dr Panagiotis Sakkatos; **Email:** sakkatosp@yahoo.gr

7

8

9

10

11

12

13

14

15

16

17

18

19

20

21 **Abstract**

22 **Background:** Breathing pattern disorders are frequently reported in uncontrolled asthma. At
23 present, this is primarily assessed by questionnaires, which are subjective. Objective measures of
24 breathing pattern components can provide additional useful information about asthma control. This
25 study examined whether respiratory timing parameters and thoracoabdominal (TA) motion
26 measures could predict and classify levels of asthma control. **Methods:** 122 asthma patients at STEP
27 2- STEP 5 GINA asthma medication were enrolled. Asthma control was determined by the Asthma
28 Control Questionnaire (ACQ7-item) and patients divided into 'well controlled' or 'uncontrolled'
29 groups. Breathing pattern components (respiratory rate (RR), ratio of inspiration duration to
30 expiration duration (Ti/Te), ratio of ribcage amplitude over abdominal amplitude during expiration
31 phase (RCampe/ABampe), were measured using Structured Light Plethysmography (SLP) in a sitting
32 position for 5-minutes. Breath-by-breath analysis was performed to extract mean values and within-
33 subject variability (measured by the Coefficient of Variance (CoV%). Binary multiple logistic
34 regression was used to test whether breathing pattern components are predictive of asthma
35 control. A post-hoc analysis determined the discriminant accuracy of any statistically significant
36 predictive model. **Results:** Fifty-nine out of 122 asthma patients had an ACQ7-item < 0.75 (well-
37 controlled asthma) with the rest being uncontrolled (n= 63). The absolute mean values of breathing
38 pattern components did not predict asthma control ($R^2 = 0.09$) with only mean RR being a significant
39 predictor ($p < 0.01$). The CoV% of the examined breathing components did predict asthma control
40 ($R^2 = 0.45$) with all predictors having significant odds ratios ($p < 0.01$). The ROC curve showed that
41 cut-off points > 7.40% for the COV% of the RR, > 21.66% for the CoV% of Ti/Te and > 18.78% for the
42 CoV% of RCampe/ABampe indicated uncontrolled asthma. **Conclusion:** The within-subject
43 variability of timing parameters and TA motion can be used to predict asthma control. Higher
44 breathing pattern variability was associated with uncontrolled asthma suggesting that irregular
45 resting breathing is an indicator of poor asthma control.

46 **Keywords:** Breathing patterns, within-subject variability, asthma control, Structured Light

47 Plethysmography

48

49

50

51

52

53

54

55

56

57

58

59

60

61

62

63

64

65

66 **Introduction**

67 Breathing pattern disorders (also known as dysfunctional breathing) are commonly reported in
68 patients with uncontrolled asthma, even though their relationship (causal or coincidental) has not
69 been clearly determined yet (1,2). Dysfunctional breathing has been characterised as a change in
70 the biomechanical and physiological components of breathing, resulting in intermittent or chronic
71 respiratory and non-respiratory symptoms, which worsens asthma patients' quality of life (3). The
72 most commonly reported respiratory symptoms of dysfunctional breathing are predominant upper
73 thoracic breathing, asynchrony between ribcage and abdominal motion, breathlessness, chest
74 tightness, wheezing and deep sighing (4). However, most of these have been described subjectively
75 through clinicians' observations or using symptom questionnaires, such as the Nijmegen
76 Questionnaire (NQ) (5). The use of the NQ in this way has been criticised due to its reliance on
77 patients' perceptions, and its subjectivity (6,7). Objective measures of quantifiable breathing pattern
78 components are needed to increase our understanding of the complex relationship between
79 breathing patterns, symptoms and asthma control.

80 Breathing pattern comprises components of volume, timing and thoracoabdominal (TA) movements
81 (8). Breathing pattern components, such as tidal volume (V_t), timing parameters (inspiration and
82 expiration duration or their ratio, respiratory rate (RR)) and TA motion, can now be measured non-
83 invasively without requiring patients' cooperation as traditional lung function tests do (9,10).
84 Although changes in some of these quantifiable breathing pattern components among asthma
85 patients have been previously reported (11), any relationship of them with different levels of asthma
86 control have not been examined thoroughly. This may lead to a current lack of use of quantifiable
87 breathing pattern components in the evaluation process of asthma control. A positive weak
88 correlation ($r=0.33$) has been previously reported between TA asynchrony, as measured using
89 Respiratory Inductive Plethysmography (RIP), and Asthma Control Questionnaire (ACQ7-item) (12).
90 In addition, Raoufy et al. (2016) has previously reported that within-subject variability of V_t and

91 breath cycle duration as measured by the RIP, could differentiate uncontrolled asthma patients
92 (n=10) from patients with well-controlled asthma (n=10) as determined by the presence of asthma
93 symptoms. However, there is still a lack of information about the use of other quantifiable breathing
94 pattern components to indicate levels of asthma control.

95 To date, traditional lung function tests primarily provide information about airway calibre and lung
96 volume during single forced expiratory maneuvers. Dynamic breathing pattern measures during
97 resting breathing over time may provide additional information to increase our understanding of
98 their physiological role in the evaluation process of asthma control. Thus, the aim of this study was
99 to establish whether respiratory timing parameters and/ or respiratory TA movements measured
100 using Structured Light Plethysmography (SLP) during resting breathing, could predict asthma control.

101 **Methods**

102 This observational cross-sectional study recruited 122 adult asthma patients with a range of asthma
103 severity from a difficult-to-treat outpatient clinic at the University Hospital Southampton and from
104 staff and students at the University of Southampton. Individuals with a medical diagnosis of asthma
105 without any other chronic respiratory disease or any upper respiratory tract infection on the day of
106 data collection were eligible for this study. Levels of asthma control were determined by the ACQ7-
107 item, and cut-off points < 0.75 and > 1.50 were used to define well-controlled and uncontrolled
108 asthma respectively. Asthma patients with partially-controlled asthma (ACQ7-item scores between
109 0.75 and 1.50) were not included in this study. All participants were between STEP 2 and STEP 5
110 asthma medication according to GINA guidelines (14).

111 After obtaining informed consent, participants' demographic data and medication history were
112 collected. Asthma medication data was used to determine asthma severity. Participants' breathing
113 pattern components were recorded during resting breathing in a seated position and then
114 spirometry (Vitalograph) was performed to evaluate lung function.

115 Breathing pattern components were recorded using the SLP (Thora-3Di™, Pneumacare Ltd)
116 according to manufacturers' guidelines (15). This is a non-invasive motion-analysis recording
117 system. It comprises a contactless device which projects a grid pattern of light onto an individual's
118 chest wall covering the area between the clavicles and the umbilicus. The distortion of the grid
119 pattern intersection points caused by the displacement of the anterior surface of the chest wall is
120 recorded by two digital cameras. The two digital cameras are attached on the SLP which generates a
121 time-varying output trace. The manufacturer's own software did not allow direct breath-by-breath
122 estimations of ribcage and abdominal amplitudes (RCampe and ABampe). Thus, an automatic peak
123 detection algorithm written in Matlab code and used in our previous research (16) was used to
124 obtain values of breathing pattern components during a breath by breath analysis of SLP's output
125 trace.

126 The automatic algorithm identified local minima and maxima of the inspiration phase for each
127 breath cycle. The RR was defined as the number of complete breath cycles in one minute and the
128 inspiratory/ expiratory phase ratio (T_i/T_e) was defined as the proportionality between inspiratory
129 and expiratory phases. The inspiratory time (T_i) was calculated as the time between a minimum in
130 the sum SLP output trace and the next peak. The expiratory time (T_e) was calculated as the time
131 between a peak and the next minimum. The ribcage and abdominal amplitudes (RCampe and
132 ABampe) were defined as the vertical distances between a trough and the next peak on the SLP's
133 output as derived from the different SLP's traces used to record the motion of the ribcage and
134 abdomen separately. The within-subject variability of the breathing pattern components was
135 calculated as the Coefficient of Variance expressed as a percentage (CoV%).

136 The patients' breathing pattern components were recorded for 5 minutes at the sitting position. The
137 participants were requested to stay still and quiet during the whole recording procedure. This was to
138 minimise external body movement artefacts on the SLP's output trace as this could bias values of
139 breathing pattern components during data extraction. When patients were ready to be recorded,

140 they were falsely informed about the start of breathing pattern recording. The actual recording time
141 started one minute after the initial notification. This was to eliminate any impact of the patients'
142 awareness on breathing pattern measurements whilst recording natural behavior of their breathing.
143 Descriptive statistics were used to summarise demographic data and lung function measurements
144 Comparisons of the breathing pattern components between well-controlled and uncontrolled
145 asthma groups were made using the Mann-Whitney U test (significance level $p < 0.01$) as normal
146 distribution of the data was not found. Multiple binary logistic regression, using the forced method,
147 was performed to predict uncontrolled asthma (ACQ7-item > 1.50). Two regression models were
148 applied, one using absolute mean values of RR, Ti/Te and RCampe/ABampe as predictors. The other
149 one involved the within-subject variability measures (Cov%). Both regression models met the
150 assumption of multicollinearity (Variance Inflation Factor < 10). When all predictors of a regression
151 model significantly predicted uncontrolled asthma, a post-hoc analysis using a Receiver Operating
152 Characteristic curve (ROC) was used to identify cut-off points for changes in breathing pattern
153 components distinguishing well-controlled and uncontrolled asthma.

154 **Results**

155 One hundred twenty two adult asthma patients (75 females) were recruited and completed the
156 study (mean age (sd) 44.75 years (15.98 years). Sixty-three participants had an ACQ score of > 1.5
157 (uncontrolled asthma), whereas 59 participants scored < 0.75 (well-controlled asthma). Thirty-three
158 participants had mild asthma (STEP 2 on GINA asthma medication), with 29 of these being in the
159 well-controlled group while the rest of them had moderate-to-severe asthma (STEP 3, 4 and 5 on
160 GINA asthma medication). There were similar numbers of males and females in both groups (Table
161 1). Both groups also had similar average body mass index (BMI). Those in the uncontrolled asthma
162 group had reduced average lung function compared to the well-controlled asthma group (Table 1).
163 Although those in the uncontrolled asthma group had significantly higher median RR than those in
164 the well-controlled group, no significant differences were found for the other absolute mean values

165 of breathing pattern components (Ti/Te and RCampe/ABampe) (Table 2). On the other hand, the
166 within-subject variability measures (CoV%) of all the breathing pattern components were found to
167 be significantly increased in the uncontrolled asthma group compared to the well-controlled group
168 (Table 2).

169 When mean values of RR, Ti/Te and RCampe/ABampe were entered into the regression model
170 asthma control was not predictable with only the beta coefficient of RR being significantly greater
171 than zero (Table 3). When within subject variability measures (CoV%) of breathing pattern
172 components were entered into the model, a good fit was found (Table 4). This accounted for 45% of
173 the variance in the ACQ7-item scores. The beta coefficients of the CoV% of all breathing pattern
174 components were found to be significantly greater than zero suggesting that increased within-
175 subject variability of RR, Ti/Te and RCampe/ABampe predicts uncontrolled asthma. A linear
176 relationship was found between the CoV% of all breathing pattern components and the log of the
177 ACQ7-item score with no more than 5% of the total cases being considered as influential cases
178 (standardised residuals > 2) in the specific regression model.

179 A post-hoc analysis showed that a regression model including the CoV% of breathing pattern
180 components correctly classified 53 out of 59 patients with ACQ7-item < 0.75. It also correctly
181 classified 48 out of 63 patients with ACQ7-item > 1.50. The sensitivity and specificity of the
182 regression model were estimated to be 77.94% and 88.88% respectively with the area under the
183 ROC being 0.895 (95% C I [0.84, 0.95], sig 0.000, $p < 0.01$) (Figure 1). Based on individual ROCs for the
184 CoV% of individual breathing pattern components (Figure 2), a cut-off point > 7.40% for the CoV% of
185 the RR discriminated well-controlled from uncontrolled asthma. Optimal cut-off points for the CoV%
186 of Ti/Te and RCampe/ABampe were estimated to be > 21.66% and > 18.96% respectively (Table 5).

187 **Discussion**

188 The study aimed to examine whether respiratory timing parameters and/ or respiratory TA
189 movements could predict and classify levels of asthma control. The within-subject variability of

190 breathing pattern components, such as RR, Ti/Te and RCampe/ABampe, was found to predict
191 asthma control, but their absolute mean values did not. Based on these findings, the within-subject
192 variability of breathing pattern components is likely to be a better indicator of asthma control than
193 their mean values when measured in a single occasion. This may be because the within-subject
194 variability can efficiently reflect the natural behaviour of tidal breathing over time compared to the
195 absolute mean values of the same respiratory parameters. Therefore, the study's findings suggest
196 that the regularity of resting breathing can be considered as another physiological marker which
197 reflects levels of asthma control. The importance of measuring the natural behaviour of breathing
198 patterns has been previously highlighted as this may reflect better the adaptability of the respiratory
199 system occurred during symptomatic periods of asthma (17).

200 On the other hand, the limited variance we found in the absolute mean values of Ti/Te and
201 RCampe/ABampe may have biased the asthma control prediction. Although the RR was found to be
202 a significant predictor of asthma control, there was a lack of a linear relationship between mean RR
203 and asthma control. All these may be attributed to the presence of confounders previously reported
204 in cross-sectional observational study designs (18, 19). Authors' expect that examples of such
205 confounders could be a postural effect, the patients' asthma complexity, the underlying patients'
206 anxiety levels, and an effect of rescue medication usage prior to breathing pattern measurements.
207 Some of these, such as posture and emotions, have been clearly suggested to affect absolute mean
208 values of breathing pattern measurements (18,19, 20), but the impact of asthma complexity and
209 medication usage on breathing patterns is not clear yet.

210 Respiratory rate is affected by many factors, and so there was no clear separation between the well-
211 controlled and controlled groups for this parameter. Asthma patients frequently have co-existing
212 anxiety which can have an impact on RR (21). There is also a relationship between asthma and
213 obesity (22), and it is well known that BMI can have an impact not only on patients' asthma control
214 but also on timing components of breathing patterns (23). Although levels of anxiety were not

215 assessed in our study, our study's individuals with raised RR and well-controlled asthma were obese
216 (BMI >30 kg/m²). The normal RR found in some individuals of the uncontrolled asthma group is
217 unexplained, but this may have been caused by the use of rescue medication prior to breathing
218 pattern recordings during this study.

219 Raoufy et al. (2016) have previously reported that the within-subject variability of Vt and breath
220 cycle duration can differentiate patients with well-controlled asthma from those with uncontrolled
221 asthma. Our findings are in agreement with Raoufy et al.'s work despite methodological differences,
222 such as the method used to determine asthma control (National Asthma Education and Prevention
223 program vs ACQ7-item), the breathing pattern recording time (60 minute vs 5 minutes), the
224 recording posture (supine vs sitting) and the equipment used to monitor breathing patterns (SLP vs
225 RIP) at rest.

226 The optimal time for recording variability within breathing pattern parameters is not known in the
227 literature. We measured within-subject variability over 5 minutes and found this was sufficient for
228 making significant predictions of asthma control using respiratory rate, proportionality of respiratory
229 phases, and TH motion. To the best of authors' knowledge, the study presented here also provides
230 for a first time specific cut-off points for the within-subject variability of the breathing pattern
231 components, which can be used to differentiate well-controlled from uncontrolled asthma.
232 However, more research is required to confirm the accuracy of our results in the future.

233 In addition, the different posture selected in our study compared to Raoufy et al. (2016) did not
234 seem to have an impact on the ability of within-subject variability of the breathing pattern
235 components to predict asthma control. However, more research involving different postures, such
236 as supine or standing, is required to check maintenance of the identified association between
237 asthma control and within-subject variability of breathing pattern components.

238 Some limitations underlie this research. We did not include patients with partially controlled asthma
239 (ACQ7-item score between 0.75 and 1.50) so that ACQ7-item score could be used as a binary

240 outcome within the recruited sample. A causal or coincidental relationship between within-subject
241 variability and asthma control could not be determined from our findings due to the selected study
242 design. It is not known whether uncontrolled asthma preceded the increased within-subject
243 variability of the breathing pattern components, or vice versa. However, it is assumed that increased
244 within-subject variability in the presence of uncontrolled asthma might be due to physiological,
245 psychological or biomechanical factors as previously observed in the literature (3). In any way, a
246 future prospective cohort study is required to examine the exact nature of the relationship between
247 the changes in quantifiable breathing pattern components and asthma control.

248 **Conclusion**

249 The study showed that within-subject variability of timing parameters and THA motion predicts and
250 classifies levels of asthma control, but same results were not found for mean values of them. It is
251 concluded that increased within-subject variability of RR, Ti/Te and RCampe/ABampe is associated
252 with uncontrolled asthma. This sheds a light on the use of stable resting breathing as another
253 important marker of asthma control.

254 **List of abbreviations**

255 TA: thoracoabdominal; ACQ7-item: Asthma Control Questionnaire ; RIP: Respiratory Inductive
256 Plethysmography; RR : Respiratory Rate ; Ti/Te : ratio of inspiration phase over expiration phase;
257 RCampe/ABampe: ratio of ribcage amplitude over abdominal amplitude during the expiration phase;
258 SLP: Structured Light Plethysmography; CoV%: Coefficient of Variance expressed in a percentage;
259 DB: Dysfunctional breathing; NQ: Nijmegen Questionnaire; sd: standard deviation; ROC: Receiver
260 Operating Characteristics curve

261 **Declarations**

262 **Ethics approval and consent to participate**

263 The study has been approved by the London-Queen Square Ethics Committee (Rec no: 17/LO/1640;
264 IRAS ID: 230295). All participants provided a written consent form prior to their participation in the
265 study.

266 **Consent for publication**

267 Patients' anonymous data were agreed to be published for maintaining anonymity and protecting
268 individuals' health data.

269 **Availability of data and materials**

270 The datasets used and analysed during the current study are available from the corresponding
271 author on reasonable request.

272 **Competing interests**

273 The authors declare that they have no competing interests

274 **Funding**

275 This research study was funded by British Lung Foundation and Wessex Medical Trust. This study
276 was part of the first author's PhD work which would not be possible to be completed without the
277 funders' financial support.

278 **Authors' contributions:**

279 All authors participated in the developmental phase of this research and the preparation of this
280 paper. The first author was also responsible for collecting and analysing study's data with the other
281 authors providing their valuable supervision.

282 **Acknowledgements**

283 The authors thank the funders for their financial support of this study through a fellowship. The
284 authors also thank all the participants for their input in this study. Finally, the authors thank Dr Hans

285 Michael and Dr Ramesh Kurukullaaratchy for facilitating access to their outpatient clinic at University
286 Hospital Southampton where participants' recruitment and data collection occur.

287 **Authors' information:**

288 Panagiotis Sakkatos, PhD, MSc, BSc respiratory physiotherapist; Anne Bruton, Emeritus Professor of
289 Respiratory Rehabilitation, PhD MA (Cantab), MCSP; Anna Barney, Professor of Biomedical Acoustic
290 Engineering PhD, MSc, BSc.

291 **References**

- 292 1. Agache I, Ciobanu C, Paul G, Rogozea L. Dysfunctional breathing phenotype in adults with
293 asthma-incidence and risk factors. *Clin Transl Allergy*. 2012;2:8
- 294 2. Veidal JM, Jeppegaard M, Sverrild A, Backer V, Porsbjerg C. The impact of dysfunctional
295 breathing on the assessment of asthma control. *Respiratory Medicine*. 2017;123:3
- 296 3. Courtney R. Breathing retraining for dysfunctional breathing in asthma: taking a
297 multidimensional approach. *European Respiratory Journals Open Research*. 2017; 3:4
- 298 4. Baker N, Everard ML. Getting to grips with "dysfunctional breathing". *Paediatric Respiratory*
299 *Reviews*. 2015;16:1
- 300 5. Boulding R, Stacey R, Niven Rand Fowler SJ. Dysfunctional breathing: a review of the
301 literature and proposal for classification. *European Respiratory Reviews*. 2016; 25:141
- 302 6. Van Dixhoorn J, Folgering H. The Nijmegen Questionnaire and dysfunctional breathing.
303 *European Respiratory Journal Open Research*. 2015;1:1
- 304 7. Vidotto LS, Carvalho CRF, Harvey A, Jones M. Dysfunctional breathing: what do we know?
305 *Jornal Brasileiro de Pneumologia*. 2019;45:1
- 306 8. Tobin MJ. Breathing pattern analysis. *Intensive Care Medicine*. 1992;18:4
- 307 9. Folke M, Cernerud L, Ekstrom M, Hok B. Critical review of non-invasive respiratory
308 monitoring in medical care. *Medical and Biological Engineering and Computing*. 2003;41:4
- 309 10. Motamedi-Fakhr S, Wilson RC and Iles R. Tidal breathing patterns derived from Structured
310 Light Plethysmography in COPD patients compared with healthy subjects. *Medical devices*.
311 2017;10:1
- 312 11. Lavorini F, Magni C, Chellini E, Camiciottoli MP, Fontana GA. Different respiratory behaviours
313 disclosed by induced bronchoconstriction in mild asthma patients. *Respiratory Physiology &*
314 *Neurobiology*. 2013;189:3
- 315 12. Upton J, Brodie D, Beales D, Richardson J, Jack S, Warburton C. Correlation between
316 perceived asthma control and thoraco-abdominal asynchrony in primary care patients diagnosed
317 with asthma. *Journal of Asthma*. 2012;49:8

318 13. Raoufy MR, Ghafari T, Darooei R, Nazari M, Mahdavian SA, Eslaminejad AR, Almasnia M,
319 Gharibzadeh S, Mani AR, Hajizadeh S. Classification of asthma based on nonlinear analysis of
320 breathing pattern. PLoS One. 2016;11:1

321 14. Global Initiative for Asthma Global Strategy for Asthma Management and Prevention. GINA
322 guidelines. 2018. <https://ginasthma.org/gina-reports/>. Accessed 16 April 2018

323 15. Motamedi-Fakhr S, Iles R, Barney A, De Boer W, Conlon J, Khalid A, Wilson RC. Evaluation of
324 the agreement of tidal breathing parameters measured simultaneously using pneumotachography
325 and structured light plethysmography. *Physiological Reports*. 2017;5:3

326 16. Tehrany R. Speech breathing patterns in health and chronic respiratory disease.

327 17. Frey U, Maksym G, Suki B. Temporal complexity in clinical manifestations of lung disease.
328 *Journal of Applied Physiology*. 2011;110:6

329 18. Homma I, Masaoka Y. Breathing rhythms and emotions. *Experimental Physiology*. 2008;93:9

330 19. Romei M, Lo Mauro A, D'Angelo MG, Turconi AC, Bresolin N, Pedotti A, Aliverti A. Effects of
331 gender and posture on thoracoabdominal kinematics during quiet breathing in healthy adults.
332 *Respiratory Physiology & Neurobiology*. 2010;172:3

333 20. Kaneko H, Horie J. Breathing movements of the chest and abdominal wall in healthy
334 subjects. *Respiratory Care*. 2012;57:9

335 21. Ritz T, Meuret AE, Trueba AF, Fritzsche A, Von Leupoldt A. Psychosocial factors and behavioural
336 medicine interventions in asthma. *Journal of Consulting and Clinical Psychology*. 2013;81:2

337 22. Boulet LP. Asthma and obesity. *Clinical & Experimental Allergy*. 2012;43:1

338 23. Chlif M, Keochkerian D, Choquet D, Vaidie A, Ahmaidi S. Effects of obesity on breathing pattern,
339 ventilatory neural drive and mechanics. *Respiratory Physiology & Neurobiology*. 2009;168:3

340

341 **Tables and Figures**

342 Table 1: Demographic data and lung function measurements of asthma control groups

Variable	Well controlled asthma group (n=59)			Uncontrolled asthma group (n=63)		
	μ	sd	95%CI	μ	sd	95%CI
Gender	23 males; 36 females			24 males; 39 females		
Asthma severity	29 mild; 30 moderate-to-severe			4 mild; 59 moderate-to-severe		
Age (years)	41.20	17.78	36.83-45.58	48.06	14.56	44.40-51.73
BMI (kg/m ²)	24.95	3.75	23.97-25.93	26.49	4.01	25.48-27.50
FEV ₁ predicted (%)	100.90	18.81	96.00-105.81	76.06	24.93	69.79-82.34
FEV ₁ /FVC	81.91	9.44	79.45-84.37	74.49	15.28	70.64-78.34

PEF(l/min)	5.27	1.42	4.90-5.65	4.06	1.56	3.67-4.45
------------	------	------	-----------	------	------	-----------

μ : Mean value; sd : standard deviation; **95%CI**: 95% Confidence intervals; asthma control groups were determined by the ACQ7-item with scores <0.75 and >1.50 showing well-controlled and uncontrolled asthma respectively

343

344 Table 2: The differences in the breathing pattern components between asthma control
345 groups

Breathing component	Well-controlled group (n =5 9)		Uncontrolled group (n = 63)		Mann-Whitney U	p (1-tailed)
	M***	Min-Max**	M	Min-Max		
RR(bpm)	14.92	7.09-21.05	17.16	7.40-32.02	1175	0.000*
Ti/Te	0.66	0.40-0.90	0.68	0.40-0.96	1689	0.385
RC _{ampe} /AB _{ampe} [^]	1.29	0.43-4.20	1.33	0.37-5.31	1798	0.729
CoV _{RR} (%)	4.79	0.00-23.02	11.73	0.00-29.71	655	0.000*
CoV _{Ti/Te} (%)	19.05	10.49-46.11	33.22	14.28-57.39	606	0.000*
CoV _{RC_{ampe}/AB_{ampe}^{^^}} (%)	14.82	6.05-24.82	26.45	7.74-57.62	844	0.000*

*****M**: median value; ****Min-Max**: minimum and maximum values; * significant result at $p < 0.01$;

[^]RC_{ampe}/AB_{ampe}: Ribcage over abdominal amplitude during expiration phase; ^{^^} CoV_{RC_{ampe}/AB_{ampe}}: The within-individual variability of ribcage over abdominal amplitude during expiration phase

346

347 Table 3: The regression model including mean values of breathing pattern components used
348 to predict uncontrolled asthma

Predictors	B (SE)	95% CI for Odds Ratio			p
		Lower	Odds Ratio	Upper	
RR (bpm)	0.16 (0.05)	1.06	1.17	1.30	0.002*
Ti/Te	0.10 (1.79)	0.03	1.10	37.36	0.954
RC _{ampexp} /AB _{ampexp} [^]	0.07 (0.29)	0.61	1.07	1.88	0.812

B₀ 0.07; R² 0.09; R 0.12; -2LL 157.38; * starred sig. value was found to be significant at $p < 0.01$

349

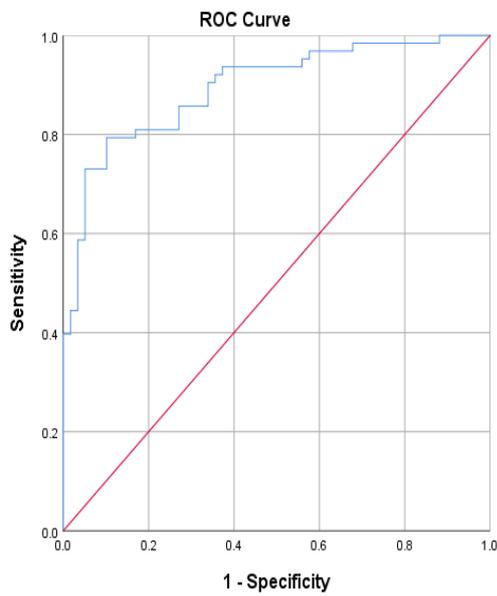
350

351 Table 4: The regression model including the CoV% of breathing pattern components used to
 352 predict uncontrolled asthma

Predictors	B (SE)	95% CI for Odds Ratio			p
		Lower	Odds Ratio	Upper	
CoV _{RR} (%)	0.15 (0.05)	1.05	1.16	1.29	0.000*
CoV _{Ti/Te} (%)	0.10 (0.03)	1.04	1.11	1.18	0.001*
CoV _{RCampexp/ABampexp} (%)	0.09 (0.05)	1.05	1.11	1.17	0.005*

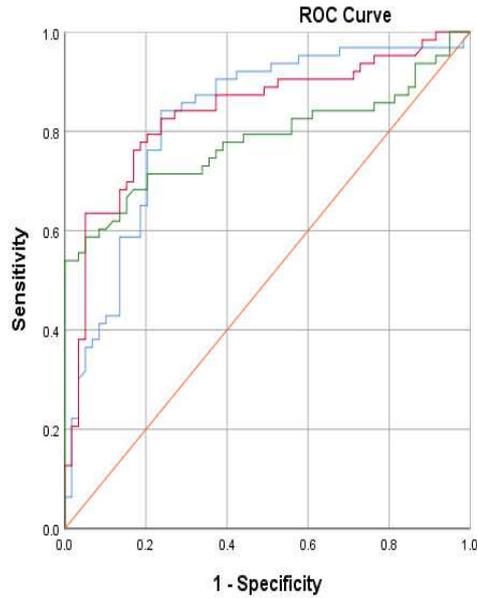
B₀ 0.07; R² 0.45; R 0.59; -2LL: 96.87; * starred values were significant results at p < 0.01;

353



354

355 **Figure 1:**The ROC curve of the regression model including the CoV% of the examined breathing
 356 pattern components



357

358 Figure 2: The different ROC curves for the CoV% of RR (blue line), Ti/Te (red line) and
 359 RCampe/ABampe (green line)

360

361 **Table 5:** Optimal cut-off points for the CoV% of each breathing pattern component and estimates of
 362 the area under the curve (AUC)

Breathing component	Optimal cut-off point [^]	AUC	Std error	95% CI	p
CoV _{RR} (%)	>7.40	0.824	0.039	0.747-0.900	0.000*
CoV _{Ti/Te} (%)	>21.66	0.837	0.038	0.763-0.911	0.000*
CoV _{RCampe/ABampe} (%)	>18.78	0.773	0.044	0.686-0.859	0.000*

[^]Optimal cut-off points were selected as the closest points from the left corner of the individual ROC curves for the CoV% of each breathing parameter; * significant result was defined at p < 0.01

363

Figures

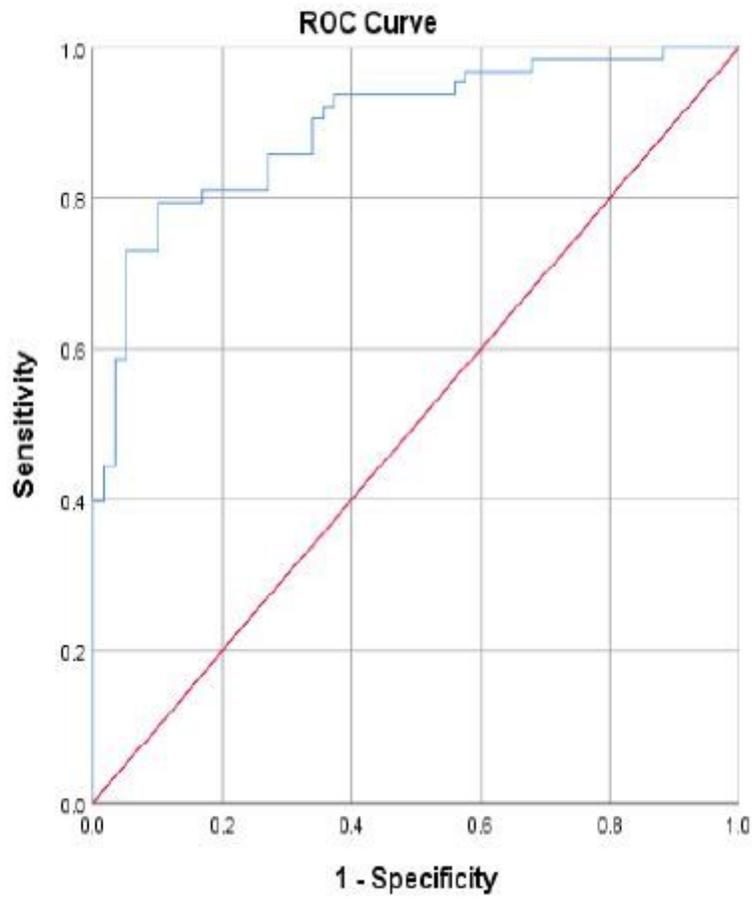


Figure 1

The ROC curve of the regression model including the CoV% of the examined breathing pattern components

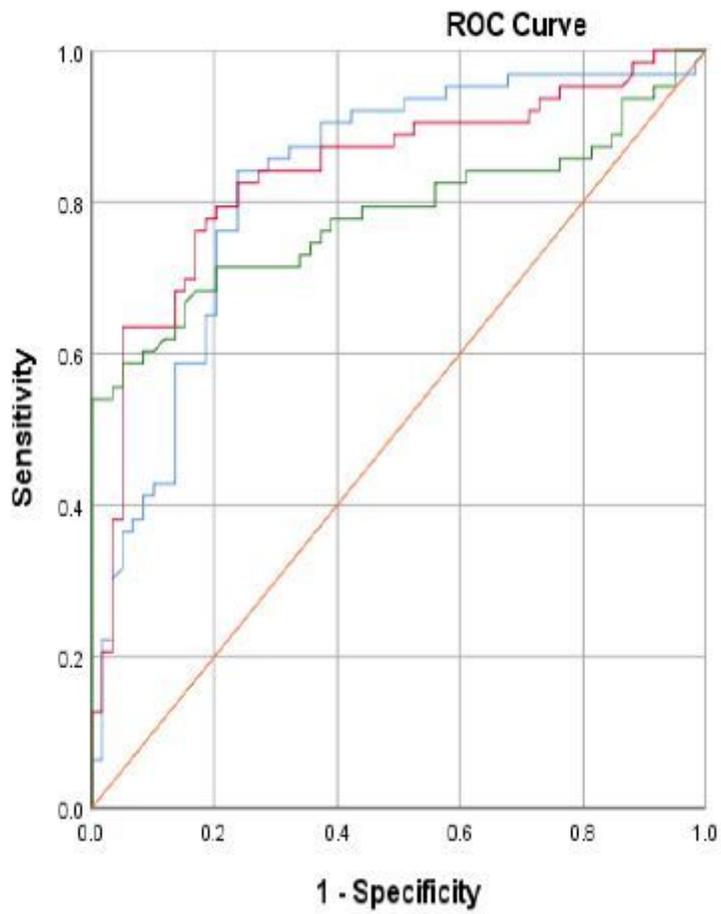


Figure 2

The different ROC curves for the CoV% of RR (blue line), Ti/Te (red line) and RCampe/ABampe (green line)