What Is the Impact of Distraction Osteogenesis on the Upper Airway of Hemifacial Microsomia Patient With OSA: a Case Report

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Case report

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Abstract

Background: Current researches about hemifacial microsomia (HFM) patients after distraction osteogenesis (DO) most emphasize the morphologic changes. This case report shows the outcome of DO on the upper airway of a HFM patient with obstructive sleep apnea (OSA) based on the use of computational fluid dynamics (CFD).

Case presentation: A boy of 11-year-old was diagnosed as HFM with OSA, and underwent unilateral DO. Polysomnography and CT scans were performed before and six months after treatment. After DO, lowest blood oxygen saturation increased from 81% to 95% and apnea and hypopnea index decreased from 6.4 events/hour to 1.2 events/hour. The oropharynx and nasopharynx were obviously expanded. We observed apparently increased average pressure, decreased average velocity and pressure drop in all cross-sections, and largely decreased airflow resistance and maximum velocity entirely in the airway.

Conclusions: The results suggest that DO might be effective for the treatment of OSA by expanding the upper airway and reducing the resistance of inspiration.

Background

Hemifacial microsomia (HFM), also known as the first and second branchial arch syndrome or hemifacial hypoplasia, mainly characterized by unilateral mandibular maldevelopment [1]. Because of the impaired development of the affected side, the mandible progressively become shortening and narrowing, leading to concomitant reduction of the pharyngeal airway in HFM patients.

Distraction osteogenesis (DO), which has several advantages of reducing trauma, initiating adaptive changes of the soft tissues to enable greater bone movement and so on, has become a recognized curative treatment for children with HFM. Structural stenosis is one important pathogenesis for pediatric obstructive sleep apnea (OSA), so except considering the changes of the soft and hard tissues, the postoperative outcome of the upper airway should be taken into accounts too.

Computational fluid dynamics (CFD) has been verified as an effective technique to exactly calculate the airflow parameters [2], and has been applied to patients with OSA widely [3–5]. However, few researches have applied CFD to estimate the variation of upper airway after unilateral DO in HFM patients at present. This report was aimed to show the outcome of DO on the upper airway of a HFM patient with OSA based on the use of CFD, which may help to explore the therapeutic mechanism of DO for OSA.

Case Presentation

In accordance with Pruzansky-Kaban classification [6, 7], a diagnosed grade IIa male HFM patient, who was accompanied with OSA and underwent unilateral DO for mandibular advancement was selected. He performed in-hospital overnight polysomnography (PSG) monitoring before starting DO and 6 months later. He had no tonsillar and adenoid hypertrophy, no previous orthodontic and orthognathic treatments.

Personalized surgical scheme was made according to the preoperative cephalometric and CT datasets. Surgical procedures such as extraoral submandibular incision, were carried out with the patient under general anesthesia. Distraction was started 7 days after operation, the frequency was 0.25 mm four times a day, the distance was 20 mm and the consolidation phase was 5 months. Finally, once the repeated CT scan demonstrated well osteogenesis, the distractor was taken out along the initial approach.

Based on the CT scans which were obtained before (T0) and 6 months after (T1) DO, image segmentation and smoothing of the upper airway was performed in Mimics 19.0 based on the threshold from -1024 Hounsfield Units (HU) to -259 HU not accompanied by paranasal sinuses. Subsequently, the model was converted into non-uniform rational B-splines surfaces in Geomagic Wrap 2017. Then the optimized model, which was saved as stereolithography format, was imported to Ansys ICEM CFD (Ansys 19.1, Canonsburg, PA, USA) to create an unstructured tetrahedral mesh.

The transversal planes I, II, III, and IV, which traversed choana, PNS (posterior nasal spine), the superior border of the epiglottis and C4 (the most anterior superior edge of the fourth cervical vertebra) respectively, divided the upper airway into nasal cavity, nasopharynx, oropharynx, and hypopharynx, plane III was the minimum cross-sectional area plane (Fig. 1). Area of planes I-IV, length of nasopharynx (Lnp), oropharynx (Lop), and hypopharynx (Lhp), and volume of each part of the airway were measured to evaluate the morphological variation.

Standard κ - ω turbulence model was used to imitate the airflow in a complete respiratory cycle with the nostrils as the inlet (impose a transient incompressible flow rate $Q = 500$ ml/s) and the bottom of hypopharynx as the outlet, the viscosity coefficient (1.789×10^{-5} kg/m/s) and density coefficient (1.225 kg/m³) were applied in the present research. Meanwhile, a non-slip boundary condition was adopted on the wall. The patient's respiratory rate was 20 breaths per minute, so the respiratory cycle was 3 s. The second-order discrete scheme and SIMPLE scheme were applied to solve the pressure-velocity coupling. The average pressure, average velocity, the airflow pressure drop (ΔP) of cross-sections I-IV, the maximum velocity ($v_{\max}$) and ΔP of the nasal cavity, nasopharynx, oropharynx, and hypopharynx were computed at peak inspiration. The effective resistance (R) was computed by $R = \Delta P/Q$.

Follow up

The patient's clinical symptoms of OSA were significantly alleviated 6 months after unilateral distraction. The results of PSG examination before and 6 months after operation are shown in Table 1. The apnea-hypopnea index (AHI) was decreased and the lowest blood oxygen saturation (LSR) was increased. Morphological variations of the upper airway between pre-distraction and post-distraction are detailed in Table 2. Figure 2 displays the comparison of the average velocity, the average pressure and ΔP at the selected cross-sectional planes. Comparison of resistance and $v_{\max}$ of the nasal cavity, nasopharynx, oropharynx, and hypopharynx are showed in Fig. 3.

Table 1
Comparison of the PSG tests before and after distraction osteogenesis.

Variables	T0	T1
Age	11 years and 7 months	12 years and 1 month
BMI (kg/m ²)	21.0	20.4
AHI (events/hour)	6.4	1.2
LSR (%)	81	95
T0: before distraction osteogenesis; T1: after distraction osteogenesis.		
BMI: body mass index; AHI: apnea-hypopnea index; LSR: lowest blood oxygen saturation.		

Table 2
Comparison of the morphological variables before and after distraction osteogenesis.

variables	T0	T1	T1-T0	change
Area (cm ²)				
plane I	2.77	3.04	0.27	9.75
plane II	1.85	4.46	2.61	141.08
plane III	1.38	1.95	0.57	41.30
plane IV	2.49	2.17	-0.32	-12.85
plane V	1.94	2.26	0.32	16.49
Length (cm)				
Lnp	1.36	1.38	0.02	1.47
Lop	3.55	4.01	0.46	12.96
Lhp	1.48	1.53	0.05	3.38
Volume (cm ³)				
nasal cavity	18.74	20.57	1.83	9.77
nasopharynx	4.48	5.85	1.37	30.58
oropharynx	6.13	9.13	3.00	48.94
hypopharynx	3.70	3.57	-0.13	-3.51
T0: before distraction osteogenesis; T1: after distraction osteogenesis.				
change: [(T1-T0)/T0] ×100%.				

Discussion

Establishment of CFD models of the upper airway based on HFM patient with OSA to quantitatively estimate the changes of the airway after unilateral DO, might be helpful to explain the relationship between the airway morphology and function and improve the understanding of pathogenesis and treatment strategy of OSA. PSG tests were used to verify the effectiveness of CFD.

OSA is a disease characterized by recurrent collapse of the pharyngeal soft tissues during sleep [8], which can lead to hypoxemia and sleep-disordered breathing, and cause functional damage of multiple systems. The researches on the relationship between OSA and the complications of various systems have also attracted the attention of many scholars. Effective researches and treatments of this disease require quantitative analysis of the airway morphology and function. With the development of the

biomechanical technique and on the basis of studies on the airflow characteristics in normal airway, there are more and more researches on the internal flow field of upper airway in OSA patients. In order to meet the needs of clinical diagnosis and treatment, scholars have carried out a lot of CFD studies on the biomechanical model of upper airway in OSA patients, from simulating various virtual surgeries [9] to evaluating the real surgical effects [10–12]. Based on the previous studies, CFD has been considered to have high reliability and accuracy, can be used to evaluate the changes of airflow in the upper airway caused by stenosis in OSA patients, also can be used to quantitatively analyze the influence of the changes caused by surgical treatments on airflow characteristics, which are helpful to objectively evaluate the curative effects after surgical treatment.

Katz et al. [13] used PSG results to show that the duration of apnea-hypopnea > 2 breathing cycles, AHI $\geq$ 5 times/h, and LSR < 92% were the diagnostic criteria for children with OSA. OSA is a disease with high incidence rate, many etiologies and complicated pathogenesis. Because of its characteristic repeated or incomplete obstruction of upper airway and intermittent hypoxemia that occur during sleep, OSA is considered as one of the important risk factors for hypertension, angina pectoris and cerebral vascular embolism [14]. At present, it is considered that the stenosis and dysfunction of the upper airway are the most important causes of OSA [15]. In terms of treatment, OSA is a sleep disorder characterized by obstruction of the upper airway, and surgical removal of its anatomical stenosis is an important principle for the treatment of OSA [16]. Among the surgical treatments, tracheotomy is the earliest, but it is only used in palliative or emergency situations. Uvulopalatopharyngoplasty only relieves the problem of soft tissue obstruction around the upper airway, and has no obvious effect on posterior lingual stenosis caused by mandibular retrusion, and the total effective rate is less than 50% [17]. Because of the traction of the surrounding soft tissues, the potential risk of bone recurrence and neurosensory impairment would be increased along with larger mandibular advancement. In patients with severe retrusive and narrow mandible, the pharyngeal cavity behind the tongue may collapse and lead to OSA. Mandibular DO can make the mandible move forward and increase the tension of soft tissues such as mandible hyoid muscle, genioglossus muscle, and genioglossus muscle, so as to make the tongue root move forward, which can expand the upper airway, and fundamentally relieve the stenosis of the upper airway. The accompanying insufficient lower 1/3 facial height in patients with micrognathia can also be improved.

At present, many studies have shown that pediatric OSA involves multiple occlusive planes of upper airway. Therefore, acquisition of more accurate morphological data of the upper airway is necessary to locate the stenosis sites. Major et al. [18] pointed out that the upper airway had complex 3D geometric structures. Due to the influence of OSA, the shape of the upper airway would generally have a certain degree of variation, and some information would be lost when it was transformed into two-dimensional images. In this study, the 3D reconstruction could obtain more accurate morphology of the upper airway. In addition, the pathophysiological process of OSA is greatly affected by the flow field inner the airway. The investigation and analysis of the airflow is helpful for us to further understand the connection between the anatomical structure and function of the upper airway, and facilitate to explore the pathogenesis of OSA and the implementation of clinical diagnosis and treatment measures. However, due to the lack of direct examination methods and uniform standards, the researches on OSA and the

related problems are greatly limited. With the development of medical imaging and 3D reconstruction technology, we can obtain more information about the anatomical structure of the upper airway more easily and intuitively. The interdisciplinary development has prompted many scholars to establish biomechanical models of the upper airway in order to analyze the connection between the morphological changes and function by CFD, which bring a new way for clinical researches on OSA. The establishment of biomechanical models of the upper airway and analysis of the internal airflow characteristics have become a research hotspot, aiming to provide theoretical basis for the pathogenesis research, clinical diagnosis, and treatment strategy of OSA.

In this case, the area of planes II and III, and the volume of oropharynx and nasopharynx showed obvious increase after distraction. As shown in Fig. 1, we can see that the upper airway before treatment was narrowed in the sagittal and coronal directions, especially in oropharynx. After treatment, with the mandible moving forward, the nasopharynx and oropharynx were expanded in the sagittal direction; in the coronal direction, the narrowing area of the affected side was expanded, and from the back view, the shape of the upper airway was more symmetrical. The average velocity achieved the peak at the narrowest part of the oropharynx before DO. The airflow velocity would decrease while the diameter of the airway would increase because of their proportional relationship [19]. Therefore, the average velocity of planes II and III was apparently reduced and $v_{\max}$ in oropharynx appeared maximum decrease after distraction.

After DO, the pharyngeal stenosis was greatly improved by skeletal expansion. Nevertheless, the area of plane I and the volume of hypopharynx were slightly reduced unexpectedly. This probably on account of the posterior shift of the tongue root, which might be resulted from the premature contact of the left second primary molar after DO and hypotonia of tongue muscles in the supine position during CT scanning (Fig. 4). However, we observed increased average pressure and decreased average velocity in plane I, greatly decreased resistance and $v_{\max}$ in hypopharynx, which were consistent with the performance of the expanded regions.

According to Bernoulli's principle, the pressure would increase when the airflow slowed down, which is consistent with our results of the CFD analysis. We observed greatly increased negative pressure and decreased ΔP in all selected planes and each part of the upper airway after distraction. Upon dilation of the stenosis by surgeries, airflow resistance usually decreases with reduction of the required pressure during inspiration. Similarly, the present case indicated that unilateral DO improved OSA by reducing resistance of the whole upper airway. The markedly improved AHI and LSR after distraction confirm the efficacy of unilateral DO on expanding the upper airway.

The establishment of the biomechanical upper airway models in OSA children can help us better understanding the pathogenesis and evaluating the therapeutic effect of DO on OSA. In the past, the clinical diagnosis of OSA mainly depended on their clinical symptoms and PSG examination, but there was no better method to predict the actual stenosis site. The assessment of the morphology and internal flow field of the whole upper airway by computational modeling is helpful to make a more objective

diagnosis of pediatric OSA. The 3D computer numerical simulation of this study was based on the established 3D accurate models of the upper airway according to the individualized CT datasets, and obtained the aerodynamic parameters by non-invasive CFD technology, and provided a theoretical basis for the evaluation of curative effects after DO.

Conclusions

Through the establishment of the CFD models of the upper airway in the HFM patient with OSA before and after unilateral DO, the numerical simulation of the airflow inner the upper airway, the morphological and aerodynamical changes were quantitatively evaluated, and the effectiveness of DO was verified by the results of preoperative and postoperative PSG monitoring. The results suggest that DO might be effective for the treatment of OSA by expanding the upper airway and reducing the resistance of inspiration.

Abbreviations

HFM: Hemifacial microsomia; DO: Distraction osteogenesis; OSA: Obstructive sleep apnea; CFD: Computational fluid dynamics; CT: Computed tomography; PSG: Polysomnography; AHI: Apnea-hypopnea index; LSR: Lowest blood oxygen saturation.

Declarations

- **Ethics approval and consent to participate**

Ethical approval is not applicable. Written informed consent was acquired from the patient and his parents to allow his datasets being used for scientific purposes.

- **Consent for publication**

Not applicable.

- **Availability of data and materials**

Not applicable.

- **Competing interests**

The authors declare that they have no competing interests.

- **Funding**

Not applicable.

- **Authors' contributions**

RW analyzed and interpreted the patient's datasets, and was the major contributor in writing the manuscript. SX contributed to planning of the treatment and performing the surgeries. RY was responsible manuscript checking. All authors read and approved the final manuscript.

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References

1. Monahan R, Seder K, Patel P, Alder M, Grud S, O'Gara M. Hemifacial microsomia. Etiology, diagnosis and treatment. *J Am Dent Assoc.* 2001;132(10):1402-8.
2. Shang Y, Dong J, Tian L, Inthavong K, Tu J. Detailed computational analysis of flow dynamics in an extended respiratory airway model. *Clin Biomech.* 2019;61:105-11.
3. Yu CC, Hsiao HD, Tseng TI, Lee LC, Yao CM, Chen NH, et al. Computational fluid dynamics study of the inspiratory upper airway and clinical severity of obstructive sleep apnea. *J Craniofac Surg.* 2012;23(2):401-5.
4. Taherian S, Rahai H, Lopez S, Shin J, Jafari B. Evaluation of human obstructive sleep apnea using computational fluid dynamics. *Commun Biol.* 2019;2:423.
5. Suga H, Iwasaki T, Mishima K, Nakano H, Ueyama Y, Yamasaki Y. Evaluation of the effect of oral appliance treatment on upper-airway ventilation conditions in obstructive sleep apnea using computational fluid dynamics. *Cranio.* 2019;31:1-9.
6. Pruzansky S. Not all dwarfed mandibles are alike. *Birth Defects.* 1969;2:120-9.
7. Kaban LB, Padwa BL, Mulliken JB. Surgical correction of mandibular hypoplasia in hemifacial microsomia: the case for treatment in early childhood. *J Oral Maxillofac Surg.* 1998;56(5):628-38.
8. Lin J, Suurna M. Sleep apnea and sleep-disordered breathing. *Otolaryngol Clin North Am.* 2018;51(4):827-33.
9. Hu C, Han D, Zhou B, Zhang L, Li Y, Zang H, et al. Investigation of resectability degree for adenoidal surgery in OSA children with the method of computational fluid dynamics. *Acta Otolaryngol.* 2017;137(1):82-5.
10. Luo H, Sin S, McDonough JM, Isasi CR, Arens R, Wootton DM. Computational fluid dynamics endpoints for assessment of adenotonsillectomy outcome in obese children with obstructive sleep apnea syndrome. *J Biomech.* 2014;47(10):2498-503.
11. Liu SY, Huon LK, Iwasaki T, Yoon A, Riley R, Powell N, et al. Efficacy of maxillomandibular advancement examined with drug-induced sleep endoscopy and computational fluid dynamics airflow modeling. *Otolaryngol Head Neck Surg.* 2016;154(1):189-95.
12. Zhu L, Liu H, Fu Z, Yin J. Computational fluid dynamics analysis of H-uvulopalatopharyngoplasty in obstructive sleep apnea syndrome. *Am J Otolaryngol.* 2019;40(2):197-204.

13. Katz ES, Marcus CL. Diagnosis of obstructive sleep apnea syndrome in infants and children. In: Sheldon SH, Ferber R, Kryger MH, editors. Principles and practice of pediatric sleep medicine. Holland: Elsevier Science Health Science div; 2005. p. 207.
14. Olaithe M, Bucks RS, Hillman DR, Eastwood PR. Cognitive deficits in obstructive sleep apnea: Insights from a meta-review and comparison with deficits observed in COPD, insomnia, and sleep deprivation. *Sleep Med Rev.* 2018;38:39-49.
15. Slaats MA, Van Hoorenbeeck K, Van Eyck A, Vos WG, De Backer JW, Boudewyns A, et al. Upper airway imaging in pediatric obstructive sleep apnea syndrome. *Sleep Med Rev.* 2015;21:59-71.
16. Hardy Tabet C, Lopez-Bushnell K. Sleep, snoring, and surgery: OSA screening matters. *J Perianesth Nurs.* 2018;33(6):790-800.
17. Awad MI, Kacker A. Nasal obstruction considerations in sleep apnea. *Otolaryngol Clin North Am.* 2018;51(5):1003-9.
18. Major MP, Flores-Mir C, Major PW. Assessment of lateral cephalometric diagnosis of adenoid hypertrophy and posterior upper airway obstruction: a systematic review. *Am J Orthod Dentofac Orthop.* 2006;130(6):700-8.
19. Yang C, Woodson BT. Upper airway physiology and obstructive sleep-disordered breathing. *Otolaryngol Clin North Am.* 2003;36(3):409-21.

Figures

Figure 1

The reconstructed upper airway. a pre-distraction: I- the choana plane, II- the plane parallel to Frankfort horizontal plane through PNS (posterior nasal spine), III- the minimum cross-sectional area plane, IV- the plane parallel to Frankfort horizontal plane through the superior border of the epiglottis, V- the plane parallel to Frankfort horizontal plane through the most anterior superior edge of the fourth cervical vertebra. b post-distraction: Lnp- length of the nasopharynx, Lop- length of the oropharynx, Lhp- length of the hypopharynx.

Figure 2

Comparison of the aerodynamic variables at the selected cross-sections (I - V). a average velocity. b average pressure. c pressure drop (ΔP).

Figure 3

Comparison of R and v_{max} in each part of the upper airway. a R: resistance. b v_{max} : maximum velocity.

Figure 4

Comparison between the cross-sections at the superior border of epiglottis. a post-distraction maxillofacial model indicating the premature contact of the left second primary molar. b pre-distraction. c

post-distraction.

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