

# Effect of Biomechanical Properties on Myopia: a Study of New Corneal Biomechanical Parameters

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## Research article

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# Abstract

**Background:** To assess the corneal stress-strain index (SSI), which is a marker for material stiffness and corneal biomechanical parameters, in myopic eyes.

**Methods:** A total of 1054 myopic patients were included in this study. Corneal visualisation Scheimpflug technology was used to measure the SSI. Corneal biomechanics were assessed using the first and second applanation times (A1-and A2-times); maximum deflection amplitude (DefAmax); deflection area (HCDefArea); the highest concavity peak distance (HC-PD), time (HC-time), and deflection amplitude (HC-DefA); integrated radius (IR); whole eye movement (WEM); stiffness parameter (SP-A1); biomechanically corrected intraocular pressure (BIOP); and Corvis biomechanical index (CBI). Scheimpflug tomography was used to obtain the mean keratometry (Km) and central corneal thickness (CCT). According to the spherical equivalent (SE) (low myopia:  $SE \geq -3.00D$  and high myopia:  $SE \leq -6.00D$ ), the suitable patients were divided into two groups

**Results:** The mean SSI value was  $0.854 \pm 0.004$ . The SSI had a positive correlation with A1-time ( $r=0.272$ ), HC-time ( $r=0.218$ ), WEM ( $r=0.288$ ), SP-A1 ( $r=0.316$ ), CBI ( $r=0.199$ ), CCT ( $r=0.125$ ), BIOP ( $r=0.230$ ), and SE ( $r=0.313$ ) (all  $p$ -values  $\leq 0.01$ ). The SSI had a negative correlation with HCDefA ( $r=-0.721$ ), HCDefArea ( $r=-0.665$ ), HC-PD ( $r=-0.597$ ), IR ( $r=-0.555$ ), DefAmax ( $r=-0.564$ ), and Km ( $r=-0.103$ ) (all  $p$ -values  $\leq 0.01$ ). There were significant differences in SSI ( $t=8.960$ ,  $p \leq 0.01$ ) and IR ( $t=-3.509$ ,  $p \leq 0.01$ ) between the low and high myopia groups.

**Conclusions:** In different grades of myopia, the SSI values were lower in eyes with higher SEs. It indicates that the mechanical strength of the cornea may be compromised in high myopia. The SSI was positively correlated with the spherical equivalent, and it may provide a new way to study the mechanism of myopia.

## 1 Background

Quantification of corneal biomechanics has helped us to understand the changes in corneal shape and structure after refractive surgery [1, 2]. The corneal stiffness is a recently described index with clinical significance for the detection in patients who are at risk of ectasia development [3, 4]. Previous studies have shown that the biomechanical properties of the cornea are correlated with many factors such as central corneal thickness (CCT) and intraocular pressure (IOP) [5, 6]. Eliasy et al. [7] used finite element models of human ocular globes with wide ranges of geometries. The models were subjected to different levels of IOP and the action of external air puff produced by a non-contact tonometer. The algorithm was assessed using clinical data obtained from two large datasets of healthy participants and produced a material stiffness parameter—stress-strain index—SSI—that showed no significant correlation with both CCT and IOP.

However, the distribution characteristics and influencing factors of SSI in myopic patients have not been reported. In this study, we aimed to determine the normative values in myopic patients and the effect of SSI on myopia and to assess its possible correlation with other corneal biomechanical parameters.

## 2 Methods

### 2.1 Subjects

This was a retrospective clinical study of 1054 myopic participants (464 women and 590 men) who were scheduled to undergo corneal refractive surgery at Tianjin Eye Hospital, Tianjin Medical University between March 2019 and November 2019. Data from a single representative eye per participant (right eye) were used for the analysis.

According to the spherical equivalent (SE; low myopia:  $SE \geq -3.00 D$  and high myopia:  $SE \leq -6.00 D$ ), suitable patients were divided into two groups. The study protocol followed the tenets of the Declaration of Helsinki and was approved by the ethics committee of Tianjin Eye Hospital. Written informed consent was obtained from all participants before enrolment. Inclusion criteria included: stable refraction for at least 2 years and the absence of ocular inflammation. Patients were asked to refrain from using soft contact lenses for at least 2 weeks and rigid contact lenses for at least 4 weeks. Exclusion criteria included: history of ophthalmic surgery, ocular trauma, keratoconus, glaucoma, diabetes, systemic connective tissue disease and abnormal immune function.

### 2.2 Methods

All the participants underwent comprehensive eye examinations, including uncorrected visual acuity and best corrected visual acuity measurements, subjective refraction, non-contact tonometry, and slit lamp examinations. Corneal thicknesses and mean curvatures were obtained using Scheimpflug imaging (Pentacam, Oculus, Germany). Corneal biomechanical parameters were obtained using the corneal visualisation Scheimpflug technology (Corvis ST) analyser (Oculus, Germany).

## 2.3 Corvis ST and SSI

The Corvis ST (software version 1.6r2015) is a non-contact tonometer that enables quantitative and qualitative (visual) assessments of corneal dynamic response to an air pulse using an ultra-high speed Scheimpflug camera that captures 4330 images and covers 8 mm of the central cornea in a single horizontal meridian (Figure 1). The new software used in the current study measures dynamic corneal response (DCR) parameters including first applanation (A1) parameters (A1-time, A1-length and A1-velocity), second applanation (A2) parameters (A2-time, A2-length and A2-velocity), highest concavity (HC) parameters (HC-time, HC-radius, HC deformation amplitude [DA], and HC peak distance [PD]), maximum deflection amplitude (DefAmax), deflection area (HCDefArea), uncorrected IOP, corneal stiffness parameter (SP-A1), biomechanically corrected intraocular pressure (bIOP), Corvis biomechanical index (CBI), and SSI.

An in-built software using the least squares method was used to estimate the value of SSI according to numerical modelling using CCT, bIOP, and SP-HC as input and output parameters [7]. It fits data via a regression equation to prior numerical analysis results.

$$SSI=f(a_1+a_2C_1+a_3C_2+a_4+a_5C_1C_2+a_6+a_7+a_8C_2+a_9C_1++\ln(SP-HC))$$

where  $C_1=CCT/545$  and  $C_2=bIOP/20$ .  $\ln(SP-HC)$  the natural logarithm of the SP at HC, and  $a_1$ - $a_9$  constants are determined by fitting the equation to the numerical input and output values. The ssi was considered as 1.0 for the average experimental behaviour obtained for corneal tissue with age=50 years[8]. Higher values of SSI are indicative of higher tissue stiffness and vice versa.

## 2.4 Statistical analyses

The statistical analyses were performed using SPSS version 26.0 software (IBM, Corp, Armonk, NY, USA). Descriptive statistical results included means, standard deviations, and minimum and maximum values of parameters. The 95% confidence interval (CI) of the overall mean of the parameters was calculated. Normality of all data samples was checked using the Kolmogorov-Smirnov test. Pearson bivariate correlation statistical analysis was used to obtain the linear fit of the correlation among variables. Stepwise multivariate linear regression analysis was applied to assess the correlation between SSI and other corneal properties;  $p \leq 0.05$  was considered to be statistically significant.

# 3 Results

## 3.1 Baseline characteristics

Data were collected from 1054 patients. The right eyes were used for the analysis. The characteristics of the participants are summarised in Table 1. The mean age and SE of the participants were  $23.9 \pm 5.96$  years and  $-5.03 \pm 2.03D$ , respectively.

Table 1. Characteristics of the participants included in the study

Parameters	Mean $\pm$ SD	Range
Age (years)	$23.9 \pm 5.96$	17-45
MRSE (D)	$-5.36 \pm 2.07$	-0.5- -14.25
Spherical (D)	$-5.03 \pm 2.03$	-0.5- -13.50
Cylinder (D)	$-0.66 \pm 0.48$	0- -1.75
CCT (microns)	$553.4 \pm 29.9$	482-654
Km (D)	$43.14 \pm 1.35$	39.0-46.75
IOPnct (mmHg)	$16.39 \pm 2.37$	9.5-27.5

CCT, central corneal thickness; Km, mean keratometry; MRSE, manifest refraction spherical equivalent; IOPnct, intraocular pressure with non-contact tonometry; SD: standard deviation

Values are presented as means (standard deviations) or as ranges.

## 3.2 Biomechanical parameters

The mean values of DCR parameters in eyes with corresponding standard deviations and 95% CIs are shown in Table 2.

Table 2: Distribution of normative values of Corvis ST parameters

Parameters	Mean±SD	95% CI
A1-time (ms)	7.208±0.289	7.194,7.223
A2-time (ms)	21.968±0.373	21.949,21.987
HC-time (ms)	17.032±0.401	17.011,17.052
A1DefA (mm)	0.097±0.006	0.096,0.097
A2DefA (mm)	0.109±0.011	0.108,0.109
HCDefA (mm)	0.941±0.096	0.936,0.946
HCDefArea (mm <sup>2</sup> )	3.521±0.501	3.495,3.547
DefAmax (mm)	0.953±0.095	0.948,0.957
DAmax (mm)	4.349±0.424	4.328,4.372
PD (mm)	5.181±0.251	5.169,5.194
WEM (mm)	0.201±0.065	0.258,0.265
SP-A1	107.866±14.927	107.091,108.640
ARTh	581.715±112.10	575.918,587.512
IR	7.902±0.977	7.852,7.951
CBI	0.221±0.187	0.212,0.230
SSI	0.854±0.133	0.847,0.860
CCT (µm)	554±32.75	576,587
blOP (mmHg)	16±2.06	15.9,16.1

Corvis ST: corneal visualisation Scheimpflug technology; SD: standard deviation; CI: confidence interval; A1-and A2-times: time reaching the first and second applanation; HC-time: highest concavity-time; A1 and A2DefA: displacement of corneal apex at the first or second applanation or at the moment of highest concavity after whole eye motion is removed; HCDefA: amplitude at the highest concavity; HCDefArea: deflection area at the highest concavity; DefAmax: maximum deflection amplitude; DAmax: maximum deformation amplitude; PD: peak distance; WEM: whole eye movement; SP-A1: stiffness parameter; IR: integrated radius; ARTh: ambrosio relational thickness horizontal; CBI: Corvis biomechanical index; SSI: stress-strain index; CCT: central corneal thickness; blOP: biomechanically corrected intraocular pressure

Values are presented as means (standard deviations) with 95% confidence intervals.

### 3.3 Correlations of SSI with other biomechanical parameters

#### 3.3.1 Correlation between baseline characteristics and SSI

No statistically significant correlations were observed between SSI and sex ( $p \geq 0.05$ ). The SSI was negatively correlated with mean keratometry (Km) ( $r = -0.103$ ,  $p \geq 0.01$ ) and positively correlated with SE ( $r = 0.313$ ,  $p \geq 0.01$ ) (Figure 2), CCT ( $r = 0.125$ ,  $p \geq 0.01$ ), age ( $r = 0.198$ ,  $p \geq 0.01$ ), and blOP ( $r = 0.23$ ,  $p \geq 0.01$ ) (Table 3).

Table 3: Correlations between SSI and characteristics of the participants

Parameters	SSI	
	r	p
Age (years)	0.198	0.01
MRSE (D)	0.313	0.01
CCT (microns)	0.125	0.01
Km (D)	-0.103	0.01
biOP (mmHg)	0.230	0.01

SSI: stress-strain index; MRSE: manifest refraction spherical equivalent; CCT: central corneal thickness; Km: mean keratometry; BIOP: biomechanically corrected intraocular pressure

Statistical significance has been defined as  $p < 0.05$ .

### 3.3.2 Comparison of parameters in low and high myopia

There were no significant differences in age, CCT, BIOP, SP, ambrosio relational thickness horizontal (ARTh), and CBI between the low and high myopia groups. There was a significant difference in SSI ( $t=8.960$ ,  $p=0.01$ ) and integrated radius (IR) ( $t=-3.509$ ,  $p=0.01$ ) (Figure 3, Table 4).

Table 4: Comparison of the parameters in low and high myopia

Group	Number	Age (years)	CCT (microns)	biOP	SP-A1	DAmax (mm)	IR (mm)	ARTh	CBI	SSI
Low myopia	161	23.2±6.12	553±32.9	16±2.07	108.520±15.699	4.272±0.448	7.663±1.071	589.402±114.500	0.214±0.184	0.920±0.138
High myopia	506	24.0±5.56	551±29.3	16±1.98	107.787±14.884	4.360±0.413	7.953±0.991	577.718±106.814	0.224±0.183	0.813±0.129
t		-1.616	0.770	-1.354	0.538	-2.328	-3.509	1.190	-0.609	8.960
p		0.107	0.441	0.176	0.590	0.020	0.01	0.234	0.543	0.01

CCT: central corneal thickness; biOP: biomechanically corrected intraocular pressure; SP-A1: stiffness parameter; DAmax: maximum deformation amplitude; IR: integrated radius; ARTh: ambrosio relational thickness horizontal; CBI: Corvis biomechanical index; SSI: stress-strain index

Statistical significance has been defined as  $p < 0.05$ .

### 3.3.3 Regression analysis of SSI and baseline characteristics

Multiple linear stepwise regression analysis was performed with SSI as the dependent variable and SE, Km, CCT, biOP, and age as independent variables (Table 5). The following regression equation was obtained:

$$SSI = 0.768 + 0.021SE + 0.02biOP + 0.006AGE - 0.013KM + 0.001CCT$$

Table 5: Multiple linear stepwise regression analysis with SSI as the dependent variable

	$\beta$	t	$p$	95% CI
Constant	0.768	6.429	$\leq 0.01$	0.534,1.002
MRSE (D)	0.021	14.114	$\leq 0.01$	0.018,0.024
biOP	0.020	12.752	$\leq 0.01$	0.017,0.023
Age (year)	0.006	11.352	$\leq 0.01$	0.005,0.007
Km (D)	-0.013	-5.680	$\leq 0.01$	-0.018,-0.009
CCT ( $\mu\text{m}$ )	0.001	5.558	$\leq 0.01$	0.000,0.001

CI: confidence interval; MRSE: manifest refraction spherical equivalent; biOP: biomechanically corrected intraocular pressure; Km: mean keratometry CCT: central corneal thickness; SSI: stress-strain index

Values are presented 95% confidence intervals, and statistical significance has been defined as  $p < 0.05$ .

### 3.3.4 Correlation between corneal biomechanical parameters and SSI

A1-time, HC-time, A2DefA, WEM, SP-A1, ARTh, CBI, IR, and biOP were weak positively correlated with SSI. DAmx, A2-time, and A2DefA were weakly negatively correlated with SSI. HCDefA, HCDefArea, PD, IR, and DefAmx were strongly negatively correlated with SSI. No significant correlation was found between A1DefA and SSI (Table 6, Figure 4).

Table 6: Correlations between SSI and Corvis ST parameters

Parameters	SSI	
	r	$p$
A1-time (ms)	0.272	$\leq 0.01$
A2-time (ms)	-0.323	$\leq 0.01$
HC-time (ms)	0.218	$\leq 0.01$
A1DefA (mm)	-0.007	0.798
A2DefA (mm)	0.081	$\leq 0.01$
HCDefA (mm)	-0.721	$\leq 0.01$
HCDefArea ( $\text{mm}^2$ )	-0.665	$\leq 0.01$
DefAmx (mm)	-0.564	$\leq 0.01$
DAmx (mm)	-0.388	$\leq 0.01$
PD (mm)	-0.597	$\leq 0.01$
WEM (mm)	0.288	$\leq 0.01$
SP-A1	0.316	$\leq 0.01$
ARTh	0.113	$\leq 0.01$
IR	-0.555	$\leq 0.01$
CBI	0.199	$\leq 0.01$
biOP	0.230	$\leq 0.01$

SSI: stress-strain index; Corvis ST: corneal visualization Scheimpflug technology; A1-and A2-times: time reaching the first and second applanation; HC-time: highest concavity-time; A1 and A2DefA: displacement of corneal apex at the first or second applanation or at the moment of highest concavity after whole eye motion is removed; HCDefA: amplitude at the highest concavity; HCDefArea: deflection area at the highest concavity; DefAmx: maximum deflection amplitude; DAmx: maximum deformation amplitude; PD: peak distance; WEM: whole eye movement; SP-A1: stiffness parameter; IR: integrated radius; ARTh: ambrosio relational thickness horizontal; CBI: Corvis biomechanical index; biOP: biomechanically corrected intraocular pressure

Statistical significance has been defined as  $p < 0.05$ .

## 4 Discussion

Myopia is a public health problem [9] with a high prevalence, especially in the Far East [10]. The onset and progression of myopia has been associated with genetic and environmental factors [11, 12]. Previous studies have noted that myopia is correlated with an increase in corneal curvature and a decrease in corneal thickness [13]. Animal studies have shown a change in the length of the eye and shape of the anterior cornea during the process of myopia modelling [14, 15]. It is also known that high myopes have lower corneal hysteresis than emmetropes [16]. However, it is difficult to detect the ocular biomechanical properties *in vivo* [17]. The Corvis ST provides information on corneal deformation parameters by visualising the dynamic reaction of the cornea to a single puff of air [18].

In our study, one of the new Corvis ST parameters—SSI, was evaluated in myopic eyes. We demonstrated that the SSI was positively correlated with SE ( $r=0.313$ ,  $p<0.01$ ) (Figure 1). When comparing eyes with low and high myopia, there were no significant differences in CCT, bIOP, SP, ARTh, and CBI, although there was a significant difference in  $SSI_{\text{t}}=8.960$ ,  $p<0.01$  and  $IR_{\text{t}}=-3.509$ ,  $p<0.01$  (Figure 2, Table 4) values. The results showed that the SSI of high myopia was lower than that of low myopia, suggesting that the biomechanical properties of the cornea changed and corneal hardness decreased with an increase in the SE.

Inmaculada Bueno-Gimeno et al. used ocular response analyser and suggested that corneal biomechanical properties appear to be compromised in myopia from an early age, especially in high myopia [19]. Another study showed a weak although significant correlation between corneal hysteresis (CH) and refractive error, with CH being lower in both moderate and high myopia than in emmetropia and low myopia [20]. Wu et al. [21] reported a difference in corneal biomechanical properties between 835 low myopic eyes and 1027 high myopic eyes. Low CH and corneal resistance factor and high cornea-compensated and Goldmann-correlated IOPs were suggested to be associated with high myopia. However, the correlation of the biomechanics of myopia is controversial. Some studies reported no significant correlation between myopia and CH [22, 23]. The results of our study showed a strong negative correlation of SSI with  $HCDefA_{\text{r}}=-0.721$ ,  $p<0.01$ ,  $HCDefArea_{\text{r}}=-0.665$ ,  $p<0.01$ ,  $PD_{\text{r}}=-0.597$ ,  $p<0.01$ ,  $IR_{\text{r}}=-0.555$ ,  $p<0.01$ , and  $DefA_{\text{max}}_{\text{r}}=-0.564$ ,  $p<0.01$  (Table 6, Figure 3). Wang et al. [24] found that eyes with high myopia had a larger corneal DA than eyes with mild-to-moderate myopia, and A2-time and HC-radius were positively correlated with SE. Eyes with high myopia also showed longer DA and smaller HC-radius. Similar results were reported by Miaohe et al. [5]. These findings are consistent with our results.

Previous studies have shown that the biomechanical properties of the cornea are correlated with CCT. Eyes with thick CCT exhibited strong corneal resistance to external force and are less prone to deformation [25]. Higher intraocular pressure may mask abnormal corneal biomechanical properties, resulting in apparently normal HCDA measurements [26]. The introduction of SSI resolved this issue because it estimates the material stiffness [27]. Eliasy et al. [7] used the numerical models in the SSI parametric study that covered wide variations in IOP, CCT, geometry and material parameters, which covered and slightly extended beyond the ranges reported in clinical studies. Through the consideration of a Corvis parameter—SP-HC, which is more strongly correlated with corneal stiffness than IOP, SSI is intended to be independent of intraocular pressure and corneal geometry. As a new index, it could help in the detection in patients with higher risk or susceptibility for ectasia development or progression after refractive surgery and could aid in surgery planning.

In this study, we observed a weak correlation among BIOP ( $r=0.23$ ,  $p<0.01$ ), CCT ( $r=0.125$ ,  $p<0.01$ ), and SSI (Table 3). It indicated that despite correction, the effect of corneal biomechanics cannot be completely independent of IOP and thickness, which is consistent with our clinical experience and previous studies. Effects of IOP and corneal biomechanics on eye behaviour are difficult to separate; IOP also affects the immediate corneal stiffness. It is generally believed that sex has no significant effect on corneal biomechanics [28]. Our study also suggested that the corneal biomechanical properties of myopia may have nothing to do with sex. Correlation between stress-strain behaviour and age was reported [8, 29], although this study found that there was no strong significant correlation between age ( $r=0.198$ ,  $p<0.01$ ) and SSI, which may be correlated with the concentration of the individual age included.

It is noteworthy that the mean CCT value measured by Corvis ST ( $553\pm 29.96$   $\mu\text{m}$ ) was slightly lower than that measured by Pentacam corneal topography ( $554\pm 31.04$   $\mu\text{m}$ ) ( $t=4.970$   $p<0.01$ ). However, it has been shown that Corvis-ST CCT measurements have good repeatability [30].

The main limitation of the current study is lack of eye axis parameters and a control group with emmetropia, despite a large sample size with myopic participants, which will be improved and supplemented in future studies.

## 5 Conclusions

In conclusion, our study showed that there was a positive correlation between SSI and SE. It may provide a new way to study the mechanism of myopia. In different grades of myopia, the SSI values were lower in eyes with higher SE. This indicates that the mechanical strength of the cornea may be compromised in high myopia. Future studies can corroborate the findings of our study. A longitudinal study in progressive and stable myopic participants is warranted.

## 6 Abbreviations

A1-time: the first and applanation time; A2-time: the second applanation time; ARTh: ambrosio relational thickness horizontal; bIOP: biomechanically corrected intraocular pressure; CBI: Corvis biomechanical index; CH; corneal hysteresis; Corvis ST: corneal visualisation Scheimpflug technology; CCT: central corneal thickness; CI: confidence interval; DA: deformation amplitude; DCR: dynamic corneal response; DefAmax: maximum deflection amplitude; HCDefArea: deflection area; IR: integrated radius; Km: mean keratometry; IOP: intraocular pressure; PD: peak distance; SE: spherical equivalent; SP-A1: stiffness parameter; SP-HC: stiffness parameter at highest concavity; SSI: stress-strain index; WEM: whole eye movement

## 7 Declarations

### 7.1 Ethics approval and consent to participate

The study adhered to the tenets of the Declaration of Helsinki and was approved by the ethics committee at Tianjin Eye Hospital.

### 7.2 Consent for publication

Not applicable.

### 7.3 Availability of data and materials

The datasets during and/or analysed during the current study are available from the corresponding author on reasonable request.

### 7.4 Competing interests

The authors declare that they have no competing interests.

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### 7.6 Authors' contributions

FH and YW contributed to the conception of the work. FH, PHW and MD.L performed data acquisition and analysis, as well as drafting of the manuscript. JN.M was also involved in data analysis. YW and Vishal Jhanji revised the manuscript and produced the final version. All authors reviewed and approved the final manuscript.

### 7.7 Acknowledgements

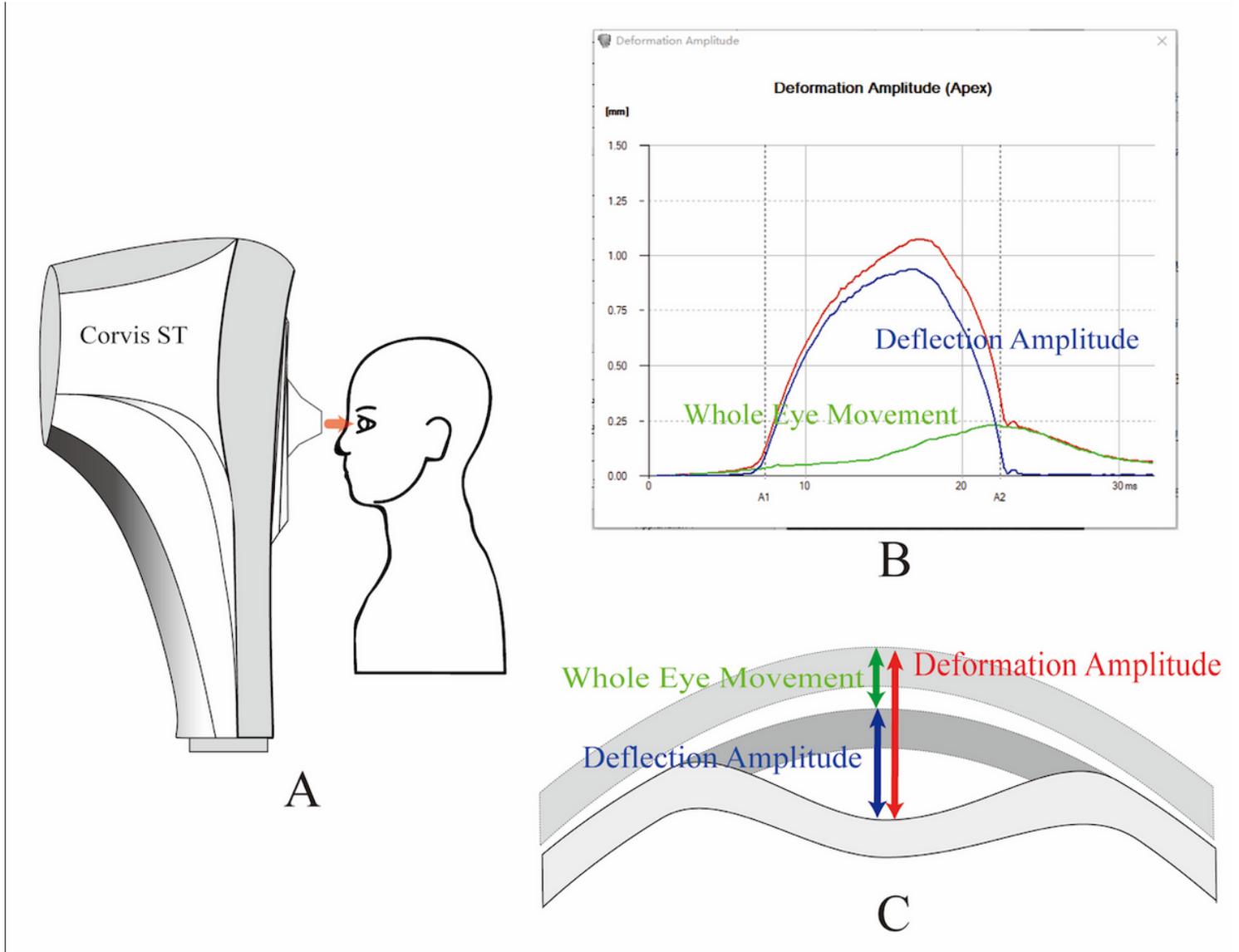
Not applicable.

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## Figures



**Figure 1**

Schematic view of the Corvis ST test and cornea deformations. The air puff impinges (pink line) on the corneal surface, the cornea becomes concave and whole eye motion (green line) is simultaneously initiated in the backward direction. Deformation amplitude: deformation of the corneal apex (red line). Deflection amplitude (mm): displacement of corneal apex  $y$  after eye motion is removed (blue lines). Corvis ST: corneal visualisation Scheimpflug technology

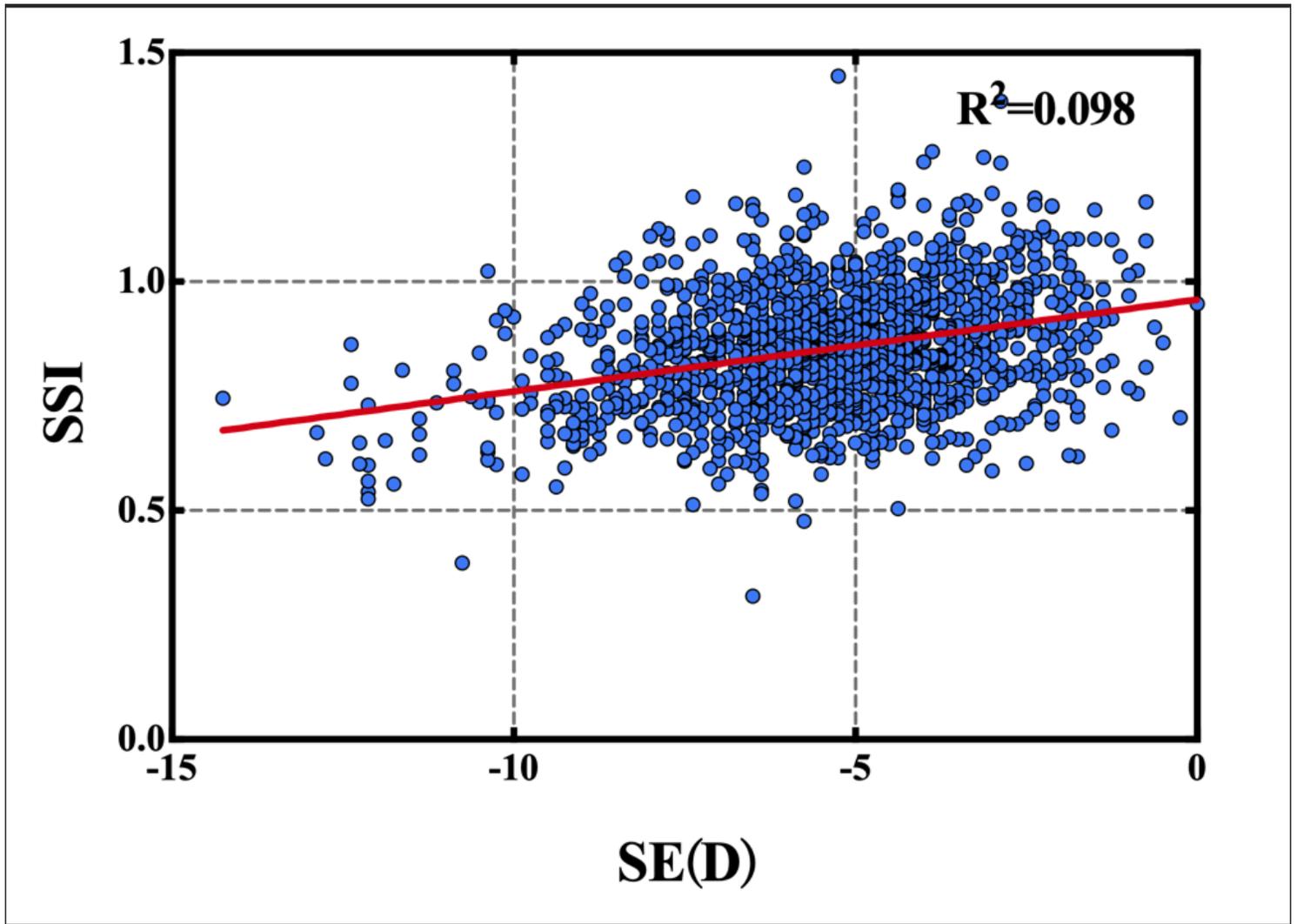


Figure 2

Scatter plots showing significant correlation between SSI and spherical SE ( $r=0.313$ ,  $p<0.01$ ) SSI: stress-strain index; SE: spherical equivalent

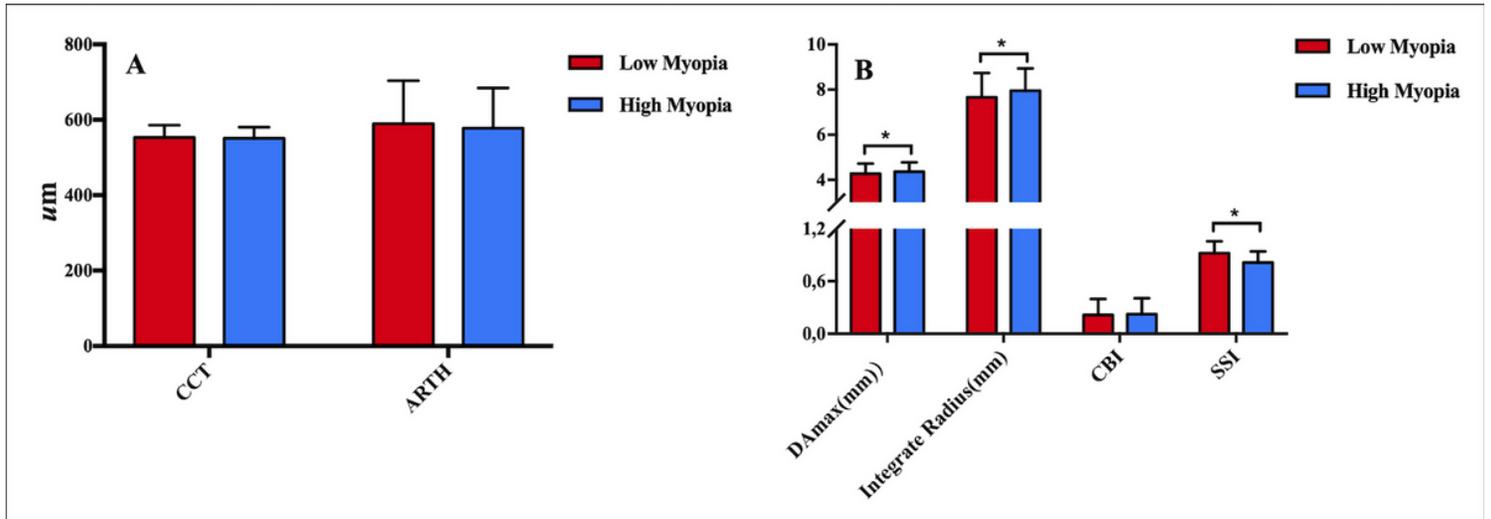
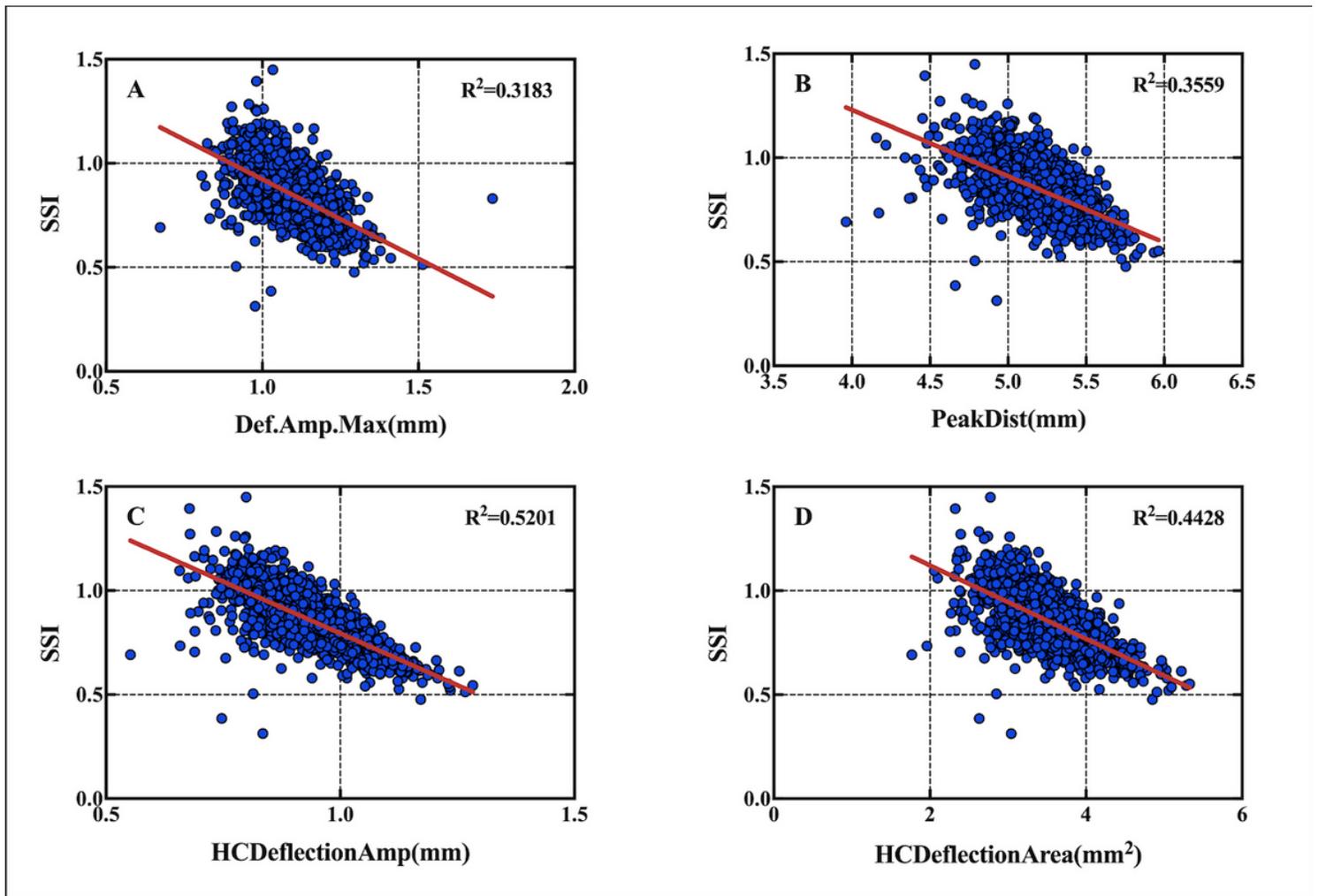


Figure 3

Histogram comparison of parameters in low and high myopia. The x axis represents the parameters for comparison between low and high myopia. The y axis represents the numerical value of the parameter CCT: central corneal thickness; ARTh: ambrosio relation thickness horizontal DAm<sub>max</sub>: maximum deformation amplitude; CBI: Corvis biomechanical index; SSI: stress-strain index



**Figure 4**

Scatter plots showing correlations of SSI with DefAmax ( $r=-0.564$ ,  $p \leq 0.01$ ), Peakdist ( $r=-0.597$ ,  $p \leq 0.01$ ), HCDefA ( $r=-0.721$ ,  $p \leq 0.01$ ), HCDefArea ( $r=-0.665$ ,  $p \leq 0.01$ ). SSI: stress-strain index ; DefAmax: maximum deflection amplitude; PD: Peak distance; HCDefA: highest concavity deflection amplitude; HCDefArea: highest concavity deflection area.