

Renal Oxygenation in male Metabolic Syndrome as evaluated by Blood Oxygen Level-Dependent Magnetic Resonance Imaging

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Research

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Abstract

Background- Blood Oxygen Level-Dependent Magnetic Resonance Imaging (BOLD-MRI) provide regional measurements of oxygen content using deoxyhemoglobin paramagnetic characteristics. Metabolic Syndrome (MS) could affect renal oxygenation, which have an impact on the clinical course of the disease. The goal of this study was to evaluate BOLD-MRI findings in kidneys of male patients with MS.

Materials and Methods- A total of 24 males patients with MS were collected in the hospital and 24 male volunteers were selected as the control group. All volunteers underwent a renal scan using 3.0T magnet (Philips, Achieva). R_2^* of the renal cortex and medulla was measured on BOLD images.

Results- Medullary R_2^* (MR_2^*) and Medulla/Cortex R_2^* ratio [MCR] were significantly lower in MS patients ($MR_2^*=24.39\pm 2.18\text{ s}^{-1}$, $MCR=1.29\pm 0.14$) than in controls ($MR_2^*=28.21\pm 4.70\text{ s}^{-1}$, $MCR=1.53\pm 0.28$) ($P<0.01$), and cortical R_2^* (CR_2^*) values were not significantly different between the two group.

Conclusions- The MR_2^* and MCR were lower in male patients with MS compared to controls. MR_2^* and MCR were potential imaging biomarkers for prediction of early renal impairment in male MS.

Background

Metabolic Syndrome (MS) and chronic kidney diseases [CKD] have become global health problems and increasing worldwide. Data from National Health and Nutrition Examination Survey (NHANES) showed that overall prevalence of the metabolic syndrome in the United States was 33% from 2003 to 2012^[1] and the prevalence of CKD was 13.1% in the United States from 1999 to 2004^[2]. MS was a significant risk factor for CKD [but the pathogenesis is not yet well understood^[3-5].

There are increasing evidences suggesting an association between CKD and chronic renal hypoxia^[6,7]. In order to understand the renal oxygenation status in MS, it is necessary to monitor renal oxygenation in these patients noninvasively.

BOLD-MRI is currently the only noninvasive technique that evaluate oxygenation in vivo tissue. BOLD-MRI is sensitive to magnetic field inhomogeneity induced by deoxyhemoglobin. As field inhomogeneity makes water molecules de-phase faster, the acquired gradient-echo signals decay faster with echo time. With different echo time values, we apply an exponential decay function to calculate parameter R_2^* ($R_2^* = 1/T_2^*$). BOLD-MRI is based on the assumption that blood oxygen level is in equilibrium with that in tissue. In the interest of simplicity, we ascribed the changes in R_2^* values to changes in oxygenation, suggesting that an increase in R_2^* values implies reduced oxygenation^[8-10]. BOLD-MRI has been used to provide regional measurements of oxygen content in experimental models and human kidney diseases^[11-15]. However, none of the published studies examined renal oxygenation in MS patients. The purpose of the study was to evaluate BOLD-MRI findings in male patients with MS.

Materials And Method

The protocol of this study was discussed, approved and recorded by the ethics committee of the hospital. 24 male patients with MS were enrolled in the study and 24 male volunteers were selected as the control group. Informed consent was obtained from all participants involved in this study.

2.1 Determination of MS

According to the definition of 2013 Chinese diabetes society (CDS 2013) MS was defined as three or more of the following abnormalities: (1) waist circumference ≥ 90 cm for men, (2) Fasting Triglyceride (TG) ≥ 1.70 mmol/L, (3) Fasting High density lipoprotein cholesterol (HDL-C) < 1.04 mmol/L, (4) Blood pressure $\geq 130/85$ mmHg and/or receiving treatment for previously diagnosed hypertension, (5) Fasting blood glucose (FBG) ≥ 6.1 mmol/L or oral glucose tolerance test (OGTT) 2h blood glucose (BG) ≥ 7.8 mmol/L and/or confirmed diabetes that is under treatment^[16].

2.2 The inclusion and exclusion criteria

The inclusion criteria of MS were as follows: (1) age between 18-75 years old, (2) without contraindications of MRI examination, (3) eGFR is not less than 60 ml/min/1.73 m². (4) in accordance with the MS definition of CDS 2013. Exclusion criteria of MS were as follows: (1) combined with other kidney diseases such as polycystic kidney disease, glomerular nephritis, etc. (2) difficult to analyze because of poor image quality (3) nephrotoxic and vascular drugs were used within 8 weeks before the examination. The inclusion criteria of volunteers were as follows: (1) age between 18-75 years old. (2) without contraindications of MRI examination. (3) eGFR is normal. Exclusion criteria of volunteers were as follows: (1) difficult to analyze because of poor image quality. (2) Nephrotoxic and vascular drugs were used within 8 weeks before the examination.

2.3 Physical measures

Anthropometric indices including height, blood pressure, waist circumference and weight was measured by trained physicians and nurses. All subjects wear light clothing without shoes and height and weight were measured by an automated height and weight machine. Participants were in a standing position with arms on side, legs straight, and knees together, with feet flat pointed outward. Waist circumference was measured in a horizontal plane, midway between the inferior margin of the last rib and the superior margin of the iliac crest. Blood pressure was measured twice by trained nurse, and the average value of these 2 measuring points was recorded (before the blood pressure was measured, all participants need at least 5 minutes to rest).

2.4 Laboratory Assays

For all Participants, venous blood were collected after an overnight fast. Serum creatinine (Scr) was measured with an enzymatic method on an autoanalyzer (Hitachi 7170, Hitachi, Tokyo, Japan). The eGFR was obtained from the Modification of Diet in Renal Disease (MDRD) equations. $eGFR (ml/min/1.73 m^2) = 175 \times (Scr)^{-1.234} \times (Age)^{-0.179}$ [17]. Determination of High density lipoprotein (HDL) concentration was performed by commercially available reagents (Shanghai Gensource Co., Ltd, Shanghai, China). Total cholesterol (TC) and triglyceride (TG) levels were determined enzymatically with commercially available reagents (Roche Diagnostics, Mannheim, Germany). SUA level was measured with a colorimetric method (Roche Diagnostics, Mannheim, Germany). HOMA-IR was calculated according to the formula: $HOMA-IR = [fasting plasma glucose (mmol/L) \times fasting insulin (mU/L)/22.5]$ [18].

2.5 BOLD-MRI: Acquisition

BOLD-MRI examinations were performed on a 3.0 T magnet (Philips, Achieva). The data were acquired by a breath-hold (15 second) multiple gradient echo sequences. Parameters were as followed: 16 echoes, echo time (TE): 1.20 ms; repetition time (TR):16 ms; spacing: 0 mm; thickness: 5 mm; bandwidth: 1753.5 Hz; flip angle: 25 degrees; field of view (FOV): 350 x 350 mm; matrix: 176 x 173. All the subjects were fasting 4 hours before MRI scan.

2.6 BOLD-MRI: Analysis and data measurement

The data were analyzed by ITK-SNAP software and R_2^* values were measured and generated by the software automatically by regions of interest (ROI). Two coronal slices were acquired as measurement plane through the middle of the kidneys . ROI with fixed size were placed in the upper, middle and lower pole of both kidneys in cortex and medulla . Five ROIs were placed in cortex and medulla , respectively, avoiding the renal collection system, yielding a total of 20 ROIs in both kidneys per slice. R_2^* value were measured twice by two experienced radiologists and the final mean R_2^* value was obtained by averaging values from two measurements. Because R_2^* values are easily affected by several external effects such as magnetic field inhomogeneity, coil positions, etc [19] , we also calculated the Medulla/Cortex R_2^* ratio $\frac{MR_2^*}{CR_2^*}$ for each subject besides cortical R_2^* (CR_2^*) and Medullary R_2^* (MR_2^*). Assuming that CR_2^* and MR_2^* are similarly influenced by the same external effects, the MCR will be less impacted by external effects.

2.7 Statistical analyses

All statistical analysis were performed by SPSS (IBM, Armonk, NY; statistics 20.0). Continuous variables were shown as mean \pm one standard deviation if data had normal distribution. Intraclass correlation coefficient (ICC) of two measurement data was calculated to evaluate interobserver consistency. If ICC values is more than 0.75, a high reliability was considered and the data were used. To detect the different

renal oxygenation between cortex and medulla, R_2^* value was compared in each group by paired t test. To test the difference between MS group and control group, CR_2^* , MR_2^* and MCR were compared respectively (Independent samples t test). Besides, the relationship between R_2^* values and eGFR was assessed by Pearson correlation analysis. $P < 0.05$ was considered as significant.

Result

3.1 Clinical characteristics

Baseline clinical characteristics of two groups were shown in Table 1. Participants of two groups were well matched for age, height, serum creatinine (Scr), serum uric acid (SUA), total cholesterol (TC), low density lipoprotein (LDL) and hemoglobin (HGB). The weight, body mass index (BMI), blood pressure (BP), waist circumference (WC), fasting insulin (FIN), fasting blood glucose (FBG), triglyceride (TG), alanine aminotransferase (ALT), aspartate aminotransferase (AST) in MS group were significantly higher than those in control group and high density lipoprotein (HDL) and eGFR were significantly lower than those of control groups, respectively.

3.2 BOLD-MRI image and Intraclass correlation coefficient (ICC)

On the BOLD-MRI image, the demarcation of the renal cortex and medulla is clear. Intraclass correlation coefficient of two measurement data was calculated to evaluate interobserver consistency and ICC value of R_2^* was 78.7% for cortex and 88.6% for medulla (both ICC > 0.75).

3.3 Comparison of BOLD Parameters in MS and controls groups

Paired t test showed that the R_2^* value was lower in cortex than that in medulla. (Table 2). Independent sample t test showed that the cortical R_2^* values were not significantly different between the two groups. Both MR_2^* and MCR values were significantly lower in patients with MS compared with controls (Table 3 and Fig. 2).

3.4 ROC curve analysis of BOLD Parameters

The ROC analysis showed that the area under the curve (AUC) was 0.814 for MR_2^* , and 0.835 for MCR which were both higher than that of eGFR. By calculating the Youden index, optimal diagnostic threshold of MR_2^* was 25.104 Hz, and the sensitivity and specificity were 66.7% and 87.5%, respectively. Similarly,

optimal diagnostic threshold of MCR was 1.380 and the sensitivity and specificity were 75% and 83.3% (Table 4 and Fig. 3).

3.4 The correlation of BOLD Parameters with eGFR

The relationship of BOLD parameters and eGFR was analyzed by the Pearson correlation analysis. It showed that there was no statistical correlation between CR_2^* and eGFR. However, MR_2^* showed statistical positive correlation with eGFR ($r = 0.417$, $P = 0.003$). Similarly, MCR also showed statistical positive correlation with eGFR ($r = 0.466$, $P < 0.001$) (Fig. 4)

Discussion

In this study, BOLD-MRI was used to evaluate the renal oxygenation in two groups noninvasively. Intra-class correlation coefficient showed that there was favorable interobserver consistency of R_2^* . As shown in table 1, average eGFR in MS group was significantly lower than that of control groups (88.35 ± 20.19 vs 100.26 ± 17.36), suggesting that MS group was in early renal impairment. The result also showed that MR_2^* and MCR of MS group were significantly decreased when compared with those of the control groups. The area under the curve yielded a cut-off value of 0.814, with sensitivity of 66.7% and specificity of 87.5% for MR_2^* . Similarly, the area under the curve yielded a cut-off value of 0.835, with sensitivity of 75% and specificity of 83.3% for MCR. Above results showed that MR_2^* and MCR, which were both better than eGFR, were potential imaging biomarkers for prediction of early renal impairment.

The MR_2^* was significantly higher than CR_2^* in both MS group and control groups, which was consistent with previous reports^[20]. We considered the result was an effect of different renal regional blood distribution. It is known that human kidneys receive approximately 25% of the cardiac output and renal blood flow reaches about 400 ml/100g. The medulla accounts for about 10% blood flow perfusion, which is markedly less than that of cortex. Thus, R_2^* in the medulla is significantly higher than that of the cortex, suggesting that medullary region is relative hypoxia under physiological steady state conditions^[21-23].

The CR_2^* was not significantly different between MS group and control group. The results showed that oxygenation in cortex was not obviously affected by MS in the early stage of renal impairment, which may be a result of the compensatory effect of kidney. Renal oxygenation is based on a balance between oxygen supply and consumption. The oxygen supply to the cortex is well in excess of the oxygen demand under physiological steady state conditions^[24]. Therefore, we speculated that oxygen was oversupplied to cortex and cortex was not in a state of hypoxia in the early stage of renal impairment. Besides, oxygen dissociation curve may be another factor accounting for the result. As it known to all, the partial pressure of oxygen is approximately 50 mmHg in renal cortex, and approximately 10 mmHg in renal medulla under physiological steady state conditions. The oxygen dissociation curve becomes steeper when the partial

pressure of oxygen is less than 26.6mmHg and becomes flat when the partial pressure of oxygen is more than 60mmHg^[25]. This indicated that small changes of oxygen partial pressure in renal cortex do not lead to evident changes of oxygenation in cortex.

Our results showed that both MR_2^* and MCR measurements of MS group were significantly decreased when compared with those of control group, which was not consistent with another BOLD-MRI study of MS in animal models^[26]. We believe the results could be explained in part by the different stages of renal impairment that were investigated. In the pig BOLD-MRI study, the eGFR in MS group was significantly higher than that of control groups, suggesting kidney exhibited glomerular hyperfiltration after 16 weeks of diet-induced MS. As a result, mitochondria were overwhelmed by substrate excess, leading to inefficient energy production and thereby medulla hypoxia^[26]. Similarity, human kidney also exhibits glomerular hyperfiltration during early stage of MS^[27], which will theoretically lead to mitochondrial dysfunction and thereby medulla hypoxia. However, eGFR in MS group was significantly lower than that of control group in our study. Reduced glomerular filtration rate attenuated active absorption of NaCl in the medulla proximal tubule, which have an apparent contribution to the reduced oxygen consumption and obvious increase oxygenation in renal medulla^[25]. Similar results in medulla also has been documented by BOLD-MRI in the form of CKD. In a CKD study conducted by Yuelang Zhang showed that the MR_2^* in the control group, mild renal impairment group and moderate to severe renal impairment group gradually decreased, indicating less renal hypoxia with more severe renal damage^[21]. The results from this CKD study lends support to our findings of increase oxygenation in medullary with MS, possibly due to the reduced tubular sodium reabsorption and therefore lead to reduced oxygen consumption.

In addition to the alteration of tubular reabsorption, BOLD-MRI techniques may be another possible reason that account for the apparent increase oxygenation in renal medullary in MS group. BOLD-MRI technique indirectly measures medullary oxygenation by measuring changes of regional oxygen content in the adjacent capillaries. R_2^* value is a measurement of endogenous capillary deoxyhemoglobin concentration, which is thought to be in equilibrium with that of the surrounding tissue under normal circumstances. However, MS could induce tubulointerstitial injury^[28]. The renal tubulointerstitial fibrosis interfere with oxygen diffusion from the capillary to the surrounding medullary tissue, which lead to non-equilibrium between capillary and surrounding tissue oxygenation. Therefore, the MR_2^* value, which is a measurement of capillary deoxyhemoglobin concentration, may be decreased because of the reduced oxygen extraction from the capillaries and ultimately lead to “increase” in medullary oxygenation^[29].

In all participants, there was no correlation between CR_2^* and eGFR, while there was a significant positive correlation between the MR_2^* and eGFR. This might be the result of their different sensitivity to the change of oxygen status. As mentioned above, the oxygen dissociation curve becomes steeper when oxygen pressure is less than 26.6 mmHg and becomes flat when oxygen pressure is more than 60mmHg. This indicated that small changes in medullary oxygen partial pressure will lead to a huge change of MR_2^* .

The limitations of this study were as follows: (1) The sample size was relatively small and all participants were male. However, Despite the small number of subjects, there was a significant difference in the MR_2^* between MS group and control group; (2) Renal blood flow is affected by different phases of the cardiac cycle and no information was acquired on renal perfusion in our study. We therefore can not determine whether changes in renal oxygenation were the result of alterations in renal blood flow. Nevertheless, Textor has shown that renal oxygenation is largely independent of renal blood flow, suggesting that renal blood flow did not have a huge influence on the renal R_2^* value^[30].

Conclusion

In conclusion, decreased MR_2^* and MCR in male patients with MS were detected when compared with those in controls. The etiology for the increased oxygenation in MS is not clear. We speculate that it may be related to an alteration in oxygen consumption and possibly to factors inherent to BOLD-MRI techniques. Besides, MR_2^* and MCR were potential imaging biomarkers for prediction of early renal impairment in male MS.

Declarations

Ethics approval and consent to participate

The protocol of this study was discussed, approved and recorded by the ethics committee of The Third Affiliated Hospital of Southern Medical University.

Consent for publication and competing interests

Written informed consent for publication was obtained from all participants and the authors declare that they have no competing interests.

Availability of data and material

The data used or analyzed during the current study are available from the corresponding author on reasonable request.

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Authors' Contributions

YongQiang Li and XiaoDong Zhang conceived and designed the study. Chijian Li and Shisi Li performed the trial and wrote the paper. YiHao guo provided technical support. Shiyi Liang, Yuxiang Huang, Ge Qian and Wecheng Xv reviewed and edited the manuscript. All authors read and approved the manuscript.

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Trial registration

20170811. Registered 2 August 2017, Retrospectively registered, <http://www.nysy.com.cn/cn/xkrc/xsjl11/>

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Tables

Table 1. Baseline characteristics of MS and controls enrolled in the study.

	MS n=24	Controls n=24	P
Age years	37.38±9.05	34.42±7.75	0.230
Weight kg	89.44±13.58	65.93±8.75	<0.001
Height m	1.71±0.56	1.70±0.69	0.599
BMI kg/m ²	30.43±4.33	22.67±2.67	<0.001
SBP mmHg	141±11.10	124±9.19	<0.001
DBP mmHg	86.33±8.84	73.67±8.32	<0.001
Waist circumference cm	105.34±10.10	83.45±6.30	<0.001
Serum creatinine μmol/L	94.46±17.36	86.75±12.53	0.085
eGFR mL/min/1.73m ²	88.35±20.19	100.26±17.36	0.034
Fast insulin μU/ml	20.44±9.78	8.48±4.11	<0.001
HOMA-IR index	1.88±0.34	1.13±0.34	<0.01
Fast blood glucose mmol/L	6.11±1.39	4.90±0.46	<0.001
Serum uric acid μmol/L	420.75±102.51	390.96±92.17	0.295
Total cholesterol mmol/L	4.65±1.15	4.71±0.85	0.839
Triglyceride mmol/L	2.61±1.48	1.19±0.24	<0.001
Low density lipoprotein mmol/L	2.21±0.99	2.62±0.20	0.158
High density lipoprotein mmol/L	1.22±0.30	1.52±0.38	0.004
Aspartate aminotransferase(U/L)	43.00±25.65	23±16.34	0.002
Alanine aminotransferase(U/L)	28.50±13.33	21.83±8.79	0.047
Leukocyte(x10 ⁹ /L)	7.11±2.68	6.08±0.83	0.083
Hemoglobin g/L	154.25±11.23	150.83±11.79	0.309

Table 2. Comparison of R₂* between cortex and medulla.

	Cortex R ₂ *	Medulla R ₂ *	t	p
MS n=24	19.04±1.64	24.39±2.18	-9.750	<0.001
Controls n=24	18.54±1.75	28.21±4.70	-10.936	<0.001

Table 3. Comparison of BOLD Parameters in MS and Control group.

	MS (n=24)	Controls (n=24)	t	P
Cortex R_2^*	19.04±1.64	18.54±1.75	1.017	0.315
Medulla R_2^*	24.39±2.18	28.21±4.70	-3.612	0.001
MCR	1.29±0.14	1.53±0.28	-3.836	<0.001

Table 4: Diagnostic efficiency of BOLD parameters and clinical index of renal function

	AUC	Sensitivity	Specificity	Cut-off point	95%CI	P
Cortex R_2^*	0.392	1.000	0.042	22.180	0.229-0.556	0.201
Medulla R_2^*	0.814	0.667	0.875	25.104	0.690-0.938	<0.001
MCR	0.835	0.750	0.833	1.380	0.715-0.955	<0.001
SCR	0.360	0.125	1.00	70.500	0.198-0.522	0.097
eGFR	0.682	0.667	0.750	93.093	0.526-0.839	0.030

Figures

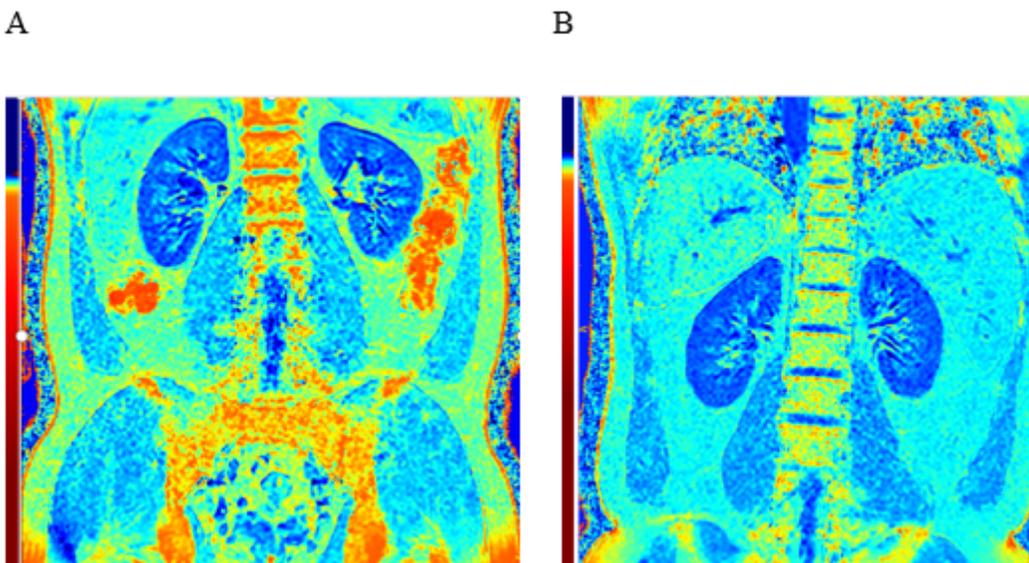


Figure 1

R2* map in coronal plane of the kidneys in a 36-year-old healthy volunteer. B:R2* map in coronal plane of the kidneys in a 37-year-old MS patient.

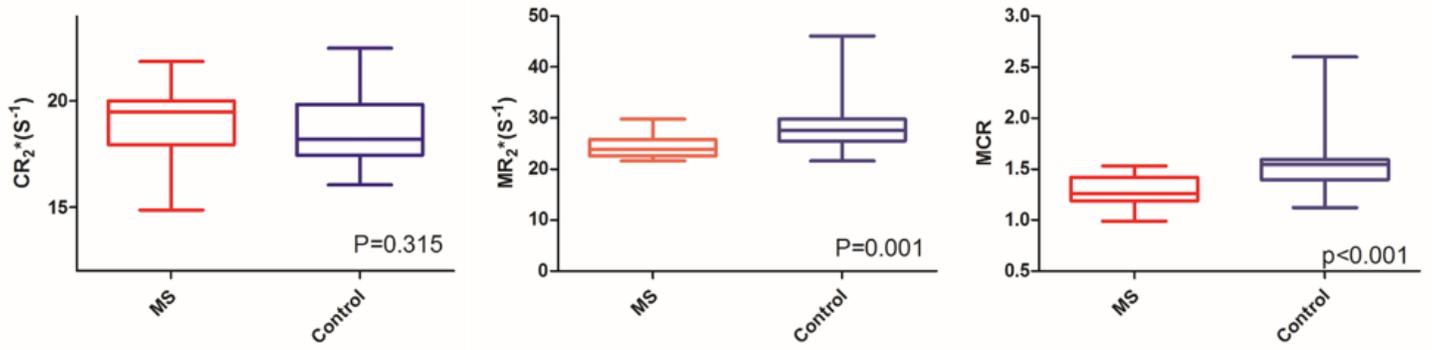
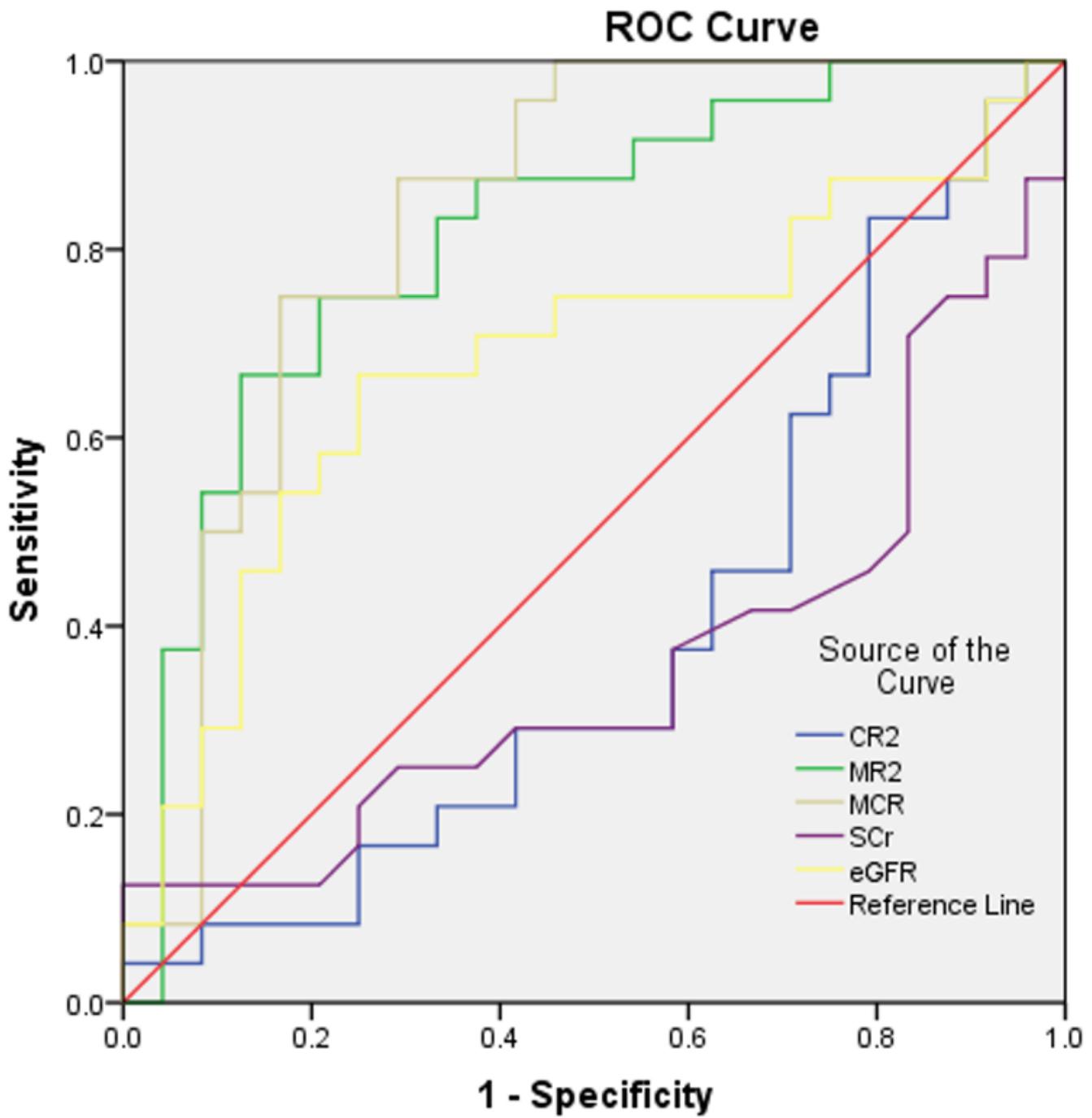


Figure 2

Comparison of BOLD Parameters in MS and Control group.



Diagonal segments are produced by ties.

Figure 3

Diagnostic efficiency of BOLD Parameters and clinical index of renal function

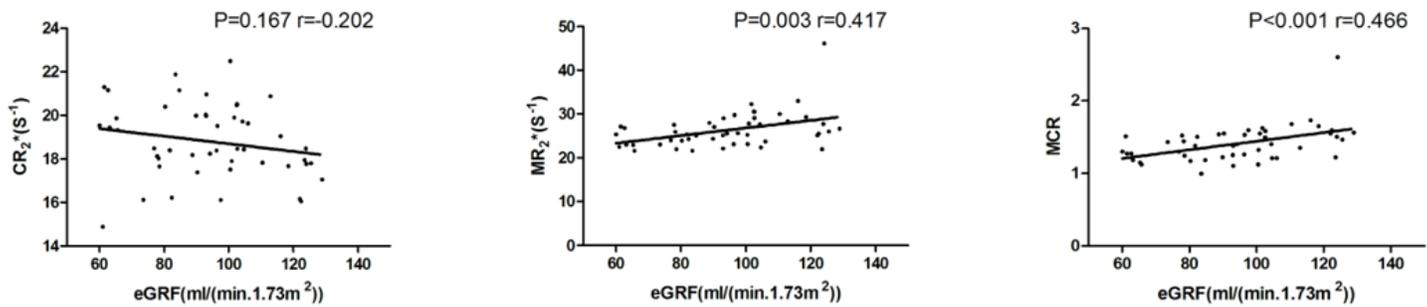


Figure 4

The correlation of BOLD Parameters with eGFR.