

Simple Multiplication in the Brain: A MEG Study Comparing Fast and Slow Responses

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Abstract

Despite decades of studies, it is still an open question on how and where simple multiplication is solved by the brain. This fragmented picture is mostly related to the different tasks employed. Although in neuropsychological studies patients are asked to perform and report simple oral calculations, neuroimaging and neurophysiological studies often use verification tasks, in which the result is shown, and the participant must verify the correctness. This MEG study aims to unify the sources of evidence, investigating how brain activation unfolds in time using a single-digit multiplication production task. We compared the participants' brain activity – focusing on the parietal lobes - based on response efficiency, dividing their responses in fast and slow. Results showed a higher activation for fast, as compared to slow, responses in the left angular gyrus starting after the first operand, and in the right supramarginal gyrus only after the second operand. A whole-brain analysis showed that fast responses had higher activation in the right dorsolateral prefrontal cortex. We show a timing difference of both hemispheres during simple multiplications. Results suggest that while the left parietal lobe may allow an initial retrieval of several possible solutions, the right one may be engaged later, helping to identify the solution based on magnitude checking.

Introduction

Several sources of evidence seem to suggest that a simple arithmetic task - as one-digit multiplication - entails a relatively complex process, bilaterally located in the brain^{1–3}. This is in contrast with traditional explanations of multiplication deficits in the neuropsychological literature. Dehaene and Cohen's review⁴ of traditional accounts concluded that only the left hemisphere, in the lower parietal lobe, stores a repertory of tables (i.e., over-learned single-digit multiplications (e.g.,7x3=21; 6x7= 42), referred to, in math psychology, as "arithmetical facts"). A lesion to this system would lead to mistakes in the retrieval of such "facts". A closer inspection of neuropsychological evidence, however, shows that in mental multiplication there is also a crucial contribution by the right hemisphere, insofar as right brain damaged patients commit a significant number of mistakes. This fact, however, was not noticed and commented upon before recent studies⁵.

Nowadays, the notion that both hemispheres are involved in simple multiplication is supported by evidence from different techniques (fMRI 1,6 , TMS 7 , EEG 8 , MEG 3 , and PET 9). An interesting hint on the relative role of left and right hemisphere (especially of parietal lobes) comes from studies with Direct Current Electrocortical stimulation (DCE) during neurosurgery 10,11 . Results in these studies showed errors associated with the inhibition of either left or right parietal sites. Crucially, the errors were qualitatively different according to the hemisphere that was stimulated. Inhibition of left sites, resulting in a greater role for the right hemisphere, was associated with a prevalence of approximation errors (e.g., 7x3=20). In contrast, inhibition of the right sites, with the left hemisphere taking a relatively greater burden, showed a prevalence of retrieval errors 10 , namely the solution was erroneously chosen from stored solutions (e.g., 7x3=28). Thus, each hemisphere would potentially contribute to obtaining the solution of the operation:

the left hemisphere would act by retrieving a possible solution and the right hemisphere by indicating the approximate numerical interval where such a solution should be sought. A particular strength of these latter results was related to the high spatial specificity of technique employed (i.e., DCE), which allowed for direct interference with specific brain areas. However, only specific sites were stimulated, and it was not possible to investigate more complex networks or track the involvement over time of specific areas. The knowledge of the time-course of brain activation during simple mental multiplication and the lateralization of these processes mostly comes from electroencephalography (EEG) studies on healthy participants.

One of the first studies that investigated the time-course activity and hemispheric involvement during onedigit multiplication was performed with ERPs (event-related potentials), using a verification task (e.g., 6x4=24: "yes or no?";8). They found a distinction between simple and difficult problems – while the former involved a short-lived activation in the left parietal electrodes, the latter rose more slowly in the electrodes over the same areas. Additionally, with increasing processing times, effects were found on electrodes of both hemispheres. In another study, Jost and collaborators 12 found that the effects depended on the problem size, with operations classified as "larger problems" (e.g., 7 x 8) showing a larger slow negativity in fronto-central and right temporal electrodes, as compared to "smaller problems" (e.g., 2 x 3). While EEG studies on mental multiplication mostly employed ERP analyses, several studies on other aspects of mental arithmetic (i.e., addition or subtractions) exploited time-frequency analysis to investigate modulations on specific oscillatory responses 13-18. Even if none of these time-frequency studies focused specifically on the lateralization of areas, results suggest that modulation in certain frequencies is associated with specific strategies, with theta increase associated with fact retrieval 14 and alpha decrease associated with the use of procedural strategies 17,19. Thus, the study of the oscillatory responses can provide useful complementary information on mental processing²⁰. Importantly, even if many of these EEG studies explicitly suggested the potential involvement of either the left or the right hemisphere, these claims were based on an electrode level. Given the low spatial resolution of the EEG, any conclusion on the brain areas involved (without appropriate analysis, such as source estimation) may be potentially misleading²¹ and should be taken cautiously. This limitation has been recently overcome by Salillas and colleagues³ with magnetoencephalography (MEG), which warrants a very good spatial resolution when source estimation methods are used. In the study of Salillas and colleagues³, which also used a verification task, results confirmed an involvement of both hemispheres and at least three brain networks involved, which included the bilateral inferior frontal areas, mainly activated in response to correct solutions, a left-lateralized frontoparietal network, which is activated in response to incorrect table-related solutions, and a right lateralized frontoparietal network, activated in response to unrelated solutions.

Despite this vast literature, there are still many open questions on the relative role of specific brain areas during simple single-digit multiplications. One open question concerns the choice of the task design. While in neuropsychological²² and DCE^{10,11} studies, patients are actually asked to orally retrieve the result (in this way the experimental task corresponds closely to the behavior of interest), most of the

evidence on the time-course of single-digit multiplication in neuroimaging (e.g., PET, fMRI) and neurophysiology (e.g., EEG, MEG) is based on verification tasks^{3,8,23-28}. Indeed, the experimental design based on verification has some advantages, as it avoids the problem of oral response artifacts and allows for a finer control of the experimental setting. However, verification is a less frequent task in everyday life. Moreover, it introduces some potential confounding effects. Besides encoding both operands, verification tasks could strongly induce plausibility checking strategies, also requiring the evaluation of the proposed answer and its mathematical relation with the operands. Instead of performing a calculation, a participant could wait for the proposed response, first use some plausibility checks, and then come up with a decision (correct or not). This is particularly relevant for incorrect responses. In theory, one could accurately classify an incorrect response (e.g., 5 x 4 = 21) as "wrong" without accessing the actual correct response, but just retrieving from memory general information that in single digit multiplication involving 5 and 21 is not a possible result. Although this potential problem has been taken into account by classifying incorrect responses between "table related" or "not table related"23, it is not possible to fully exclude that the participant relies on strategies to perform the task, rather than reflecting the investigated behavior of performing calculations. Other studies employed alternative methods to tackle these limitations, for example using tasks in which several operations were concatenated and ERP between the operations were analyzed (e.g., $2 \times 3 + 7$)¹². In that task, participants must implicitly produce the interim result of the concatenated operation before they can go on with the next calculation step. Even if this task limits the possibility of plausibility checking, it still relies on verification and cannot completely rule out the possibility that approximate calculations were performed, and that the final answer was based on plausibility.

In the present study, we tried to overcome these limitations by designing a task that specifically tackles these issues and provides additional hints on how multiplication occurs in the brain and on how the involvement of specific areas (focusing on left and right parietal lobes) unfolds in time. To this aim, we used MEG recordings, exploiting its excellent temporal and good spatial resolution. We used a simple production task, in which participants were asked to say aloud the response as fast as possible. This allows a direct comparison with the paradigms used in the neuropsychological and DCE literature on one side, and with neuroimaging and neurophysiological data obtained with healthy participants, on the other side. To compare response efficiency, we adopted an individual-based approach to classify the problems into two groups. In our case, efficient (i.e., correct and fast, Fast Responses) and inefficient (i.e., correct and slow, Slow Responses), responses were compared on an individual basis (for an analogous strategy, see for example²⁹⁻³¹). This allowed us to compare not fast and slow responders, but fast and slow responses, within the same individual, comparing two activities in which the processing is likely to be very similar, but with different efficient outcomes. Similarly to previous verification studies^{3,14}, we focused our analysis on both Event Related Fields (ERF, which is the MEG correspondent of ERP) and time-frequency analyses. Based on previous clinical findings, with production tasks in neuropsychological populations and in DCE¹⁰, we focused on the left and right parietal lobes, hypothesizing a sequential activation of the left followed by activation of the right hemisphere, especially prominent in *Fast* compared to *Slow Responses.* We expected that in the case of *Fast Responses*, the averaging procedure used to determine

brain activation would likely lead to higher values in the areas involved in fact retrieval, as compared to the *Slow Responses*²⁸. This is because the average of signals across different trials highlights the activations that are consistent across all trials and more variable brain responses (i.e., in timing) are likely to be canceled out in the averaging. We expected a higher consistency for *Fast Responses*, as compared to the more variable *Slow Responses*, and that this would lead to higher brain activation detected for the *Fast Responses*.

Material And Methods

Participants

A sample of 21 healthy participants voluntarily took part in the study (11 female and 10 male). We excluded participants with any neurological or psychiatric disease that could affect cognitive performance or who had a history of developmental dyslexia or dyscalculia. The mean age of participants was 25.8 years (SD = 3.01, range = 20-32) and their mean education was 17.09 years (SD = 2.18, range = 13-22). All participants were right-handed. Details on participants are reported in the Supplementary Materials.

Ethics Statement

The study was approved by the local ethics committee (Comitato Etico per la Sperimentazione Clinica della provincia di Venezia e IRCCS San Camillo) and conducted following the guidelines of the Declaration of Helsinki.

Recording Procedure

Before entering the magnetically shielded room, participants underwent initial preparation, which consisted of the placement of three head coils, to monitor head position during MEG recording, and eight external electrodes. These electrodes were used to record VEOG, HEOG, ECG (bipolar montage) and the muscular activity of mouth, with two electrodes placed on the orbicularis oris (upper left and lower right corners of the mouth).

Continuous MEG signal was acquired using a whole head 275-channel system (CTF-MEG). Data were sampled at 1200 Hz, with a hardware anti-aliasing low pass filter at 300 Hz. Before the experimental session, participants underwent a five-minute resting state session (not analyzed in the present work) and then undertook the experimental task that consisted of three runs of five minutes each. The total duration of the experiment was approximately 30 minutes. After the MEG recording session, three Vitamin-E capsules were placed exactly on the coil positions and the participants completed an MRI scan (Philips Achieva, 1.5T). This procedure allowed the co-registration of MEG data and MRI data. The MRI scan was always performed on the same day of the MEG recording. In all recordings, head movements never exceeded the threshold of 5 mm on any axis.

Task procedure

Upon signing the informed consent form, participants were instructed that they would be required to perform simple calculations during a MEG recording. Before the beginning of the experiment, and after the instructions were given, the participants had the possibility to rehearse the multiplication tables, to limit the potential effect of anxiety on the task performance. In a pilot study, several participants asked if it was possible to rehearse the multiplication tables before performing the task and reported to be distressed not to have this opportunity. This possibility was only given before the experimental trials.

The task recording session was divided in three runs of five minutes each, with small breaks between each run. The experiment was programmed with the free software Psychopy⁴⁹ (version 1.82), running on a PC. The task was a mental multiplication with two one-digit numbers. Participants were required to say aloud the result of the multiplication of the two numbers.

Each trial was organized as follows: first a fixation symbol (#) was presented for 800 ms, followed by the first number (henceforth, *First Number*) presented for 400 ms, a blank screen for 300 ms, and then a second number (henceforth, *Second Number*) lasting for 3000 ms. Participants were instructed to respond as quickly and as accurately as possible, saying aloud the response before the *SecondNumber* disappeared (See Figure 4), which was up to 3000 ms after the *Second Number*. They were explicitly instructed to avoid hesitations and mouth movements before the response. Prior to the beginning of the experimental task, participants underwent a familiarization session with five stimuli. All stimuli subtended about 1.5° of visual angle on the horizontal plane. Stimuli were presented using white Courier font on a black background screen. We recorded the latency of the oral response after the *Second Number* and divided the correct responses into *Fast* or *Slow* on an individual basis.

Stimuli

All combinations between one digit numbers were used in each session, excluding same number multiplication (e.g., 5 x 5, 2 x 2) and multiplication including 1 or 0 as an operand (as in Niedeggen & Rösler, 1999). This led to 54 different operations that were repeated three times in the three sessions, which constituted the whole experiment. Within each session, the presentation of each possible combination was randomized.

Behavioral data pre-processing and trial categorization

Behavioral data were analyzed to categorize responses given by participants as *Fast* or *Slow*, on an individual basis. This methodology has been previously applied in several domains. Van den Berg and colleagues, for example, analyzed the EEG activity associated with fast and slow RTs within the same individual in a task of visual-search²⁹. In another choice-response task, trials of correct responses were ordered by RTs in quartiles and the EEG activity analyzed separately⁵⁰. Again, a similar methodology was also applied by Novikov and colleagues³⁰ who performed within-subject EEG analysis with distinction between fast and slow behavioral responses (based on the individual medians), to investigate the two

different mechanisms that underlie response-speed during a sustained attention task. Similar to above-mentioned strategies, in our study, efficient (i.e., correct and fast) and inefficient (i.e., correct and slow) responses were compared on an individual basis³¹. In our case, for *Fast Responses*, the brain is likely to follow a practiced, quick, and efficient route to retrieve the correct response, whereas in *Slow Responses* it is likely that less efficient (and more variable) strategies are utilized (LeFevre *et al.*, 1996). Notably, participants provided correct answers also in the trials with a *Slow Response* (ensuring that the stimuli were actually processed), but the slower response time indicates that the processing was less optimal.

Vocal responses were recorded as .wav files with Psychopy used to define the onset of the response from the Second Number, using custom code and the CheckVocal free software⁵¹. After defining the vocal response times, correct responses from each subject were divided in three equal groups. Fast Responses were operationally defined as the 18 fastest correct responses within a run, calculated separately for each participant. Slow Responses were operationally defined as the 18 slowest correct responses within a run, calculated separately for each participant. The remaining 18 intermediate responses were not used for further analyses. Using this procedure, the FastResponses corresponded approximately to scores below the 33rd percentile, and the Slow Responses correspond approximately to the scores above the 66th percentile. Previous studies have already applied analogous strategies of stratifications in several domains to create different quantiles of the response-time distribution 37,50,52. The separation we adopted was chosen to ensure the highest possible number of stimuli and the highest possible separation between *Fast* and *Slow Responses*. As the experiment included three runs, this led to a total of 54 trials (18 x 3), prior to trial rejection, for each subject, for each condition (Fast vs Slow). This strategy yielded a reasonable number of trials to have a satisfactory signal-to-noise ratio, as qualitatively determined in pilot studies. The Fast vs Slow categorization allowed us to rely on well-known statistical analyses for MEG data at source level (i.e., cluster-based permutation). To investigate whether our hypothesis (of increased variability for *SlowResponses*) was supported by the data, we conducted an ANOVA, using standard deviation of RT of responses for each participant within *Fast* as opposed to *Slow* Responses (see Supplementary Materials, Figure S.1.2). Details on changes of reaction times over runs, as well as other additional details, are reported in the Supplementary Material.

MEG Preprocessing

MEG data pre-processing followed a standard pipeline that included filtering of continuous data (high pass: 0.1 Hz, notch filter 50 Hz and harmonics), artifacts removal with Signal-Space Projection algorithm (SSP), data segmentation (epochs starting from -2 seconds from the *First Number* to 3.7 seconds after the *Second Number*), trial rejection of epochs to check for residual artifacts. For extensive details on MEG preprocessing see Supplementary Material.

Source estimation

For the source analysis, individual T1 MRI scans were used. The MEG forward model was calculated with the overlapping spheres method and the source reconstruction was performed with the wMNE (weighted

Minimum Norm) algorithm, calculated on cortex. The noise covariance was calculated from 3 minutes of empty room recording. Details on source estimation procedure can be found in the Supplementary Material.

Event Related Fields (ERF) analyses at source level

To calculate ERFs from each initial epoch, a smaller set of epochs was then extracted. This set of epochs was time locked to the *First Number* (with -200 ms before the *First Number* used for baseline correction) and lasted from -200 to 1300 ms after the stimulus, Thus the epoch included the presentation of the *First Number* from 0 to 400, a blank from 400 to 700, and the presentation of the *Second Number* from 700 to 1300. We limited the analysis to 600 ms after the *Second Number* (that is 1300 ms after the *First Number*) because it was before the fastest response time across all participants, which was at 608.5 ms. Sensor data were from trials where averaged to obtain the ERF and filtered with a low-pass filter at 40 Hz. Averages were made separately for Response Type (*Fast* vs *Slow*). ERF analyses were divided into two main groups: ROI (Regions of Interest) analyses and Whole-brain analyses.

In the ROI analysis, MEG data were analyzed on *a priori* selected ROIs, chosen according to the hypotheses and from the existing literature. For this analysis we focused on the following ROIs: Left Angular Gyrus, Right Angular Gyrus, Left Supramarginal Gyrus, and Right Supramarginal Gyrus from the Destrieux atlas⁵⁶. ROIs were defined according to the FreeSurfer automatic parcellation of cortex surface. For both ROI and whole brain-analysis, average sensor data were projected to the cortex using the common kernel (see 2.8 Source estimation), then transformed in z-scores, computed using the same baseline employed for the baseline correction (i.e., -200-0 ms before the *First Number*). For the ROI analysis, we extracted z-scored time series from each ROI using the mean values of all vertices contained in that ROI.

For the whole-brain analysis, z-scores at individual level were first projected on a common template (MNI, Colin27), made by 15000 vertices, using the FreeSurfer registration method implemented in Brainstorm, and then spatially smoothed with a Gaussian kernel with Full Width Half Maximum (FWHM) of 3 mm.

Time-frequency analysis

To provide a more complete picture of the MEG activations, we also used time-frequency analysis. For the time-frequency (TF) analysis, starting from the initial trials (-2 to 3.7 seconds), we extracted at single-trial level MEG time series, separately for each ROI. These time series were calculated as the first components of a fast PCA on the time series of all vertices belonging to the ROI (based on built-in Brainstorm function). We then performed a Morlet Wavelet time-frequency decomposition of this extracted signal on a broad range of frequencies, ranging from 1 to 45 Hz (with step of 1 Hz). Wavelets were built starting from mother wavelet with 1 Hz and 3 sec of Full Width Half Maximum (FWHM), and generating all remaining wavelets from this initial one, keeping constant the number of cycles across frequencies.

With the time-frequency decomposition, we extracted the Magnitude values separately for each frequency at single-trial level. These values were averaged across runs, separately for each condition, such that two averages were obtained for each participant – one for *Fast* and one for *Slow Responses* (with values for each ROI). We finally calculated the Event Related Synchronization/Desynchronization (ERS/ERD), using as baseline the -300 ms -200 ms time window prior to the *First Number*, by applying the formula [(Epoch_Signal - Baseline_mean)/(Baseline_mean)]*100.

Statistical analyses

For the ERF analysis at ROI level, preliminary visual inspection showed that data were normally distributed. Therefore, parametric analyses, including ANOVA and t-tests, were used. All analyses, that is, ERF ROI analysis, ERF Whole Brain, and Time-frequency, were performed on the same epoch interval, that is from the presentation of the *First Number* to 600 ms after the presentation of the *Second Number* (so from 0 to 1300 ms after the *First Number*).

ROI analyses were performed by means of repeated measures ANOVAs, separately for each ROI. The analysis included the following variables: *Time Interval* (thirteen levels: 0-100 ms, 100-200 ms, 200-300 ms, 300-400 ms, 400-500 ms, 500-600 ms, 600-700 ms, 700-800 ms, 800-900 ms, 900-1000 ms, 1000-1100 ms, 1100-1200 ms, 1200-1300 ms) and Response (two levels: Fast, Slow). Data for each time interval were calculated as arithmetic means of all values within the interval. Due to relatively small number of participants, there was no possibility to include more factors in the ANOVAs. Given the potential differences in responses and signal range across ROIs, we used four separate ANOVAs, one for each ROI. For the sake of completeness, we also completed an additional ANOVA analysis (reported in the Supplementary Materials) using type 1 sum of squares. Although type 1 ANOVA is typically not recommended, it allowed us to also include the ROI factor in a single analysis. Interestingly, this additional ANOVA including the ROI factor, confirmed the results, showing an additional interaction of ROI, Response, and Interval, with analogous pattern to the one reported in the manuscript. To compensate for inflated type 1 error, we corrected all p-values obtained across all ANOVAs with False Discovery Rate correction for multiple comparisons (FDR) (Benjamini and Hochberg 1995). Post-hoc comparisons for significant ANOVA effects were calculated as paired t-tests, with FDR correction applied within each ANOVA. Effect size for each effect in the ANOVA was calculated as global eta squared ⁵⁸.

To analyze ERF data at whole brain level, a cluster-based permutation approach was used, using data of all 15,000 vertices of source-reconstructed activations. We performed a single cluster-based permutation analysis, encompassing the overall epoch considered in all analyses, starting from the presentation of the *First number* (0 ms) to 1300 ms afterwards (that is 600 ms after the *Second Number*). To reduce the computational burden of this analysis, and following standard indications (Groppe et al. 2011), we downsampled the data to 150 Hz prior to performing the cluster-based permutation. In this analysis, the number of permutations was set to 1000, minimum number of neighbors was set to 2, and alpha level was set to 0.05.

To analyze time-frequency data, we performed a single cluster-based permutation on the 0-1300 ms time window (without downsampling), on all Frequencies and ROIs. In this analysis, number of permutations was set to 1000, minimum number of neighbors was set to 0 (because the topographic information was lost in the ROI time-series extraction procedure), and alpha level was set to 0.05.

Finally, to analyze the relationship between ERF data at source level and Response times, we calculated a series of Spearman correlations between the average reaction time of the participants for *Fast* and for *Slow Responses* (separately), with the average ERF value for each ROI, separately for each level of *Time Interval*. To account for the large number of comparisons, p-values were adjusted with FDR correction.

Results

Behavioral Results

Participants had a mean accuracy of 87% (range 70-98%) in the task. The results on only accurate responses were used to distinguish Fast or Slow Responses (see "Behavioral data pre-processing and trial categorization"). Fast Responses had an average response time of 927.35 ms (SD = 113.79), whereas Slow Responses had an average response time of 1576.641 ms (SD = 195.38). Fast Responses also showed significantly lower variability across participants as compared to Slow Responses [F(1,20) = 273.54, p < 0.001].

Details on the behavioral analysis of *Fast* and *Slow Responses* across participants and across runs are reported in the Supplementary Material. No participant reported discomfort during the task in the short debriefing performed at the end of the task.

MEG Results

ERF Analysis on ROI

Results on ERF analysis on a priori selected ROI are shown in Figure 1.

Left Angular Gyrus

The ANOVA investigating the difference in z-scores after the *First Number* on Left Angular Gyrus showed a main effect of *Response* [F(1,20) = 9.74, p = 0.03, ges = 0.03], and a significant effect of *Time Interval* [F(12,240) = 23.55, p < 0.001, ges = 0.30]. The main effect of *Response* was associated with higher z-scores for *Fast* as compared to *Slow Responses*. The effect of Time Interval indicated a gradual increase of z-scores after the presentation of the *First Number*, with a peak at around 900-1000 ms after the *First Number*, which is about 300 ms after the presentation of the *Second Number*.

Right Angular Gyrus

The ANOVA investigating the differences on Right Angular Gyrus showed only an effect of interval [F(6, 120) = 20.71, p < 0.001, ges = 0.31]. Corrected post-hoc t-tests investigating this effect showed that the

mean z-scores were different across different intervals, increasing almost monotonically and with the highest value in the last time window, 1200-1300 ms after the *First Number* (that is 500-600 ms after the *Second Number*).

Left Supramarginal Gyrus - First number

The ANOVA on the z-scores after the *First Number* on Left Supramarginal Gyrus showed a significant main effect of *Time Interval* [F(12, 240) = 33.73, p < 0.001, ges = 0.26]. Z-scores increased monotonically, with the highest value in the last time window (1200-1300 ms after the *First Number*, that is 500-600 ms after the Second Number).

Right Supramarginal Gyrus - First number

The ANOVA on the *First Number* on the Right Supramarginal Gyrus showed a significant effect of Interval [F(12, 240) = 26.17, p < 0.001, ges = 0.36], and a significant interaction between *Response* and *Time Interval* [F(12, 240) = 4.07, p = 0.006, ges = 0.02]. The post-hoc t-tests investigating the significant interactions showed that *Fast Responses* and *Slow Responses* were significantly different only in the last two time windows (1100-1200 ms and 1200-1300 ms), that is from 400 ms after the presentation of the *Second Number*.

ERF Whole-brain Cluster Based permutation analysis

The cluster-based permutation analysis showed significant differences between *Fast* and *Slow Responses*. In all cases, the analysis pointed to higher activations for *Fast* as compared to *Slow Responses*. In particular, two clusters were found, capturing the effects on the two hemispheres [Left cluster mass = 159993, cluster size = 59777

Right cluster mass = 159627, cluster size = 60849, *ps* = 0.009]. Results on the first cluster were started about 500 ms after the presentation of the *First Number* and were localized in the left hemisphere, especially in the Angular Gyrus. This higher activation was also visible in the rest of the analyzed time points until approximately 1000 ms. However, after the presentation of the *Second Number*, larger activations for fast responses were also found in the left frontal lobe, close to the Left Inferior Frontal Gyrus (see upper part of Figure 2).

The second cluster captured the effects localized in the right hemisphere, again with higher activation for *Fast Responses* as compared to *Slow responses*. This effect was evident from about 900 ms after the presentation of the *First Number* (that is about 200 ms after the presentation of the *Second Number*) and was localized initially in the right Dorsolateral Prefrontal Cortex (DLPFC). On later time points (at 1200 ms, approximately 500 ms after the *Second Number*), the effect was also localized in the Right Supramarginal Gyrus, in nearby areas of the right parietal cortex, together with the Right Insula and Right Frontopolar areas (see lower part of Figure 2).

Time-frequency ROI Analysis.

Results from the cluster-based permutation performed on time-frequency analysis showed a significant difference between *Fast* and *Slow* in three ROIs: Right Angular Gyrus [p = 0.01, cluster mass = 8180, cluster size = 2509], Left Supramarginal Gyrus [p = 0.008, cluster mass = 8783, cluster size = 3128], and Right Supramarginal Gyrus [p = 0.002, cluster mass = 13608, cluster size = 4677]. Significant differences were mostly observed in the delta frequency band (2-4 Hz), and, in the Right Supramarginal Gyrus, in the theta range (4-5 Hz). The effects in Delta were observable in all the analyzed epochs in Right Angular Gyrus, Left Supramarginal Gyrus, and Right Supramarginal Gyrus. The effect in Theta in the Right Supramarginal Gyrus was already observable after the presentation of the *First Number*. Results are reported in Figure 3.

Correlation Analysis between ERF and Response time

The correlation analysis investigating the relationship between ERF at source level (average in the time windows included in the ANOVA) and Response Time did not show any significant correlation after correction for multiple comparisons. Detailed results are reported in the Supplementary Material.

Discussion

The present MEG study investigated the temporal involvement of the left and right hemispheres (with a focus on the left and right parietal lobes) in performing simple multiplications. Participants were asked to say aloud the result of single-digit multiplication problems, with the two operands (*First Number* and *Second Number*) presented sequentially. We designed this experiment to overcome some limitations of the past literature of neuroimaging and neurophysiology studies on mental multiplication, which mostly relies on verification tasks (i.e., after the operation is showed, the results are presented, and the participants are asked to respond whether the proposed solution is correct or not) in which participants may use some sort of familiarity judgment instead of computing an answer. The present production task more closely reproduces the behavior of performing a simple multiplication. It is more similar to the tasks used in studies with neuropsychological patients or using DCE during neurosurgery, filling the gap between the different fields of literature. We compared *Fast* and *Slow Responses*, determined on an individual basis^{30,32}, using the rationale that the higher activation in the *Fast Responses* will unveil the more efficient (i.e., fast) route for accomplishing the task. MEG data were analyzed using ERF and time-frequency analysis, which provide strictly related, but complementary, information.

In the ROI analysis on ERF, focusing on the left and right parietal lobes, we found an initially higher activation of the Left Angular Gyrus for *Fast* as compared to *Slow Responses*, starting after the presentation of the *First Number* and lasting after the *Second Number*, up to few hundred milliseconds before providing the response. We also found a significantly higher activation for *Fast Responses* after the presentation of the *Second Number* (400-500 ms and 500-600 ms after its appearance) in the Right Supramarginal Gyrus (see Figure 1). The results were confirmed in the bottom-up analysis using cluster-based permutation, which again showed a higher activation in *Fast Responses*, first in left parietal areas,

then in right frontal areas, and finally also in left frontal areas and, in a more widespread fashion, in centro-parietal and frontal areas of the right hemisphere.

These results, obtained within a simple production task, are surprisingly similar to those employed recently with a more traditional verification task, also in MEG. Indeed, Salillas and colleagues³ found that in the case of a comparison of correct vs incorrect solutions in single-digit multiplication, a complex network of areas, encompassing both parietal and frontal areas of the left and right hemisphere, were involved, peaking about 600 ms after the solution was presented. We observed a similar pattern, especially in a late time window, about 500 ms after the Second Number. These similarities, as seen from one side, suggest that production and verification tasks engage similar areas in simple multiplication, and that results from a verification task are not actually excessively distorted by the design. However, production and verification tasks also showed some differences. In the production task we found an earlier involvement of the left parietal cortex, after the first operand was presented, which lasted during the presentation of the second operand. This resembles the results found with a verification task using ERP at electrode levels by Kiefer & Dehaene⁸, who also investigated responses after the second operand and who found an initial left lateralized response for a priori defined easy multiplications⁸. These results underline a similarity between verification and production tasks, also highlighting the importance of analyzing brain responses not only after the solution is presented^{3,33} but additionally after the second operand is presented. This initial involvement of the left hemisphere is in line with traditional accounts that state a role of left parietal areas for retrieving results in simple multiplications (i.e., fact retrieval).

Interestingly, significant differences between *Fast* and *Slow Responses* were already observed after the *First Number*. Since, at that stage, it was not possible to retrieve the result of the multiplication, this activation could reflect other generic processes, such as a higher allocation of attention. Alternatively, the activation in this stage could be related to a preliminary selection of some possible results. Concerning this last possibility, in the context of this experiment, each *First Number* could be followed only by 7 possible other numbers (same number multiplication, and multiplication with 1 and 0 were excluded), narrowing the actual potential results that should be retrieved. For example, if the *First Number* is 8, the potential results are 16, 24, 32, 40, 48, 56, and 72. Thus, it is possible that after seeing the *First Number*, a participant starts to select a candidate result (or several candidate results) and the higher activation of the Left Angular Gyrus for *Fast Reponses* captures this effect. This interpretation would be again in line with the DCE findings during awake surgery, which show table selection errors (e.g., 7 x 3 = 28) when the left parietal lobe takes over the task after inhibition of the right parietal lobe^{10,11}.

Within the right hemisphere, about 500 ms after the *Second Number*, a higher activation was found in right frontal areas, especially in the DLPFC and in the right insula. The activation of right DLPFC could be related to monitoring processes involved during the retrieval^{34,35} or to working memory demands¹. The activation of the right insula could suggest that *Fast Responses* are associated with a consistent involvement of attention in the same time windows³⁶. There was not a higher involvement of the frontal lobe in the *Slow* as compared to *Fast Responses*, in contrast with fMRI findings¹⁵. Given the methodology

employed, this result is not surprising. The temporal precision of MEG allowed us to track the relatively higher (and faster) activations of left and right areas during fact retrieval. However, if an activation of an area is inconsistent across trials, or across participants, the high temporal resolution of MEG is detrimental to the possibility of capturing the effect. In fact, the averaging procedure cancels out the activations that are not consistent over time. This is confirmed by analysis of RTs (see also Supplementary Materials) and is the case of an expected higher frontal activation in *Slower Responses*. Hence, these results do not imply that there is no involvement of frontal areas in *Slow Responses*, but that in *Fast Responses* there is a consistent activation of right frontal areas before providing the answer.

To shed further light on multiplication processing we used time-frequency analysis. In the existing literature on arithmetic processing, time-frequency analysis was used to unveil the neural correlates of different strategies used to accomplish the task¹⁷. We decided not to focus on specific a priori frequencies, and we opted for a bottom-up approach, investigating the frequencies from 1 to 45 Hz. Statistical analysis showed reliable differences between Fast and Slow Responses in both hemispheres, with effects restricted to lowest frequencies, in the range of delta (2-4 Hz) and theta (5-7 Hz). As compared to ERF results, time-frequency analysis showed significant differences between Fast and Slow Responses in slightly different areas, as no difference was found in the Left Angular Gyrus but in the Left Supramarginal Gyrus, and effects were also found for the Right Angular Gyrus. Although one can be tempted to conclude that time-frequency analysis captured qualitatively different processes as compared to ERF, as the two areas were very close, a more cautious interpretation is that this difference is related to the limits in the spatial resolution of the MEG. The results in the delta range resemble the effects obtained in the ERF analysis, and are likely to be related to the slow wave enhancement that generate the ERF components²¹. Importantly, these results confirm the role of both the Left and Right parietal lobes in fact retrieval. Given the low frequency range and the temporal smearing due to the Morlet deconvolution, we cannot speculate about the timing of effects on the delta range. Interestingly, within theta frequencies (about 5-7 Hz), we found slightly higher temporal resolution. Results showed higher magnitude changes in theta in the *Fast* rather than *Slow Responses*, already after the presentation of the *First Number*. We may hypothesize that this as a general orienting activity and cognitive control, which has been found with frontal and parietal distribution, for optimal target processing and decision making^{37–39}. The fact that the increased theta magnitude began soon after the presentation of the First Number, and continued during the presentation of the Second Number, can be associated with an orienting activity or with the role of theta oscillations in the successful recollection of memories and source retrieval 40,41. Of note, higher theta modulations have been previously associated with fact retrieval¹⁴. Thus, these results would be in line with the traditional account of the role of left hemisphere in mental multiplications⁴, supported and extended by the more recent development of DCE studies¹⁰.

A qualitative inspection of time-frequency results also showed other interesting aspects. For example, Slow Responses were associated, in the upper alpha band, with lower magnitude, as compared to Fast Responses in the last 200 ms of all ROIs (see Figures in the Supplementary Materials for larger versions of time-frequency results). In studies focused on additions¹⁹, the authors found that lower magnitude (i.e. desynchronization) in upper alpha (10-13 Hz), as compared to baseline, was associated with the use of a specific strategy to solve the problem, that is to rely on procedural rules^{17,19}. Importantly, because these differences in the alpha band were not statistically significant, we can only speculate that this pattern of time-frequency is also related with strategy differences between *Fast* and *Slow responses*. Future studies focusing on these frequency bands could explore this possibility. Importantly, we did not explicitly assess for the strategy used by the participants (see for example⁴²), neither did we suggest them to use specific strategies, but given the observed reaction times (see also Supplementary Materials), it is reasonable to conclude that in the case of *Fast Responses* a direct retrieval (i.e., a "fact retrieval") from memory occurred.

Altogether, these results, integrated with both existing neuropsychological and DCE 10,11 and neuroimaging and neurophysiological literature, allow us to sketch a tentative explanation of the involvement of the left and right hemisphere in single digit multiplication. We speculate that this task could be related with the activation of left parietal cortex (in particular, the Left Angular Gyrus), reflecting the initial retrieval of potential candidates. This activation is followed by an activation of the Right Supramarginal Gyrus, which could reflect a process of checking the magnitude of the possible candidates retrieved by the left hemisphere. The left hemisphere plays a crucial role in the retrieval process but it is, at the same time, prone to errors, insofar as it may choose one table result that is next to the wanted one 10. By contrast, one of the putative functions of the right parietal lobe would thus be to help identify (and perhaps amend) these errors. Thus, the present data seem to be compatible with a view that the right hemisphere always enters, automatically, into this play, even when the process is fast and smooth. Interestingly, the proposal of a "quality check" role of the right supramarginal gyrus is also in agreement with findings from a variety of numerically-related tasks including quick decisions about the number of syllables in a word⁴³ and significant disruption of time judgments when rTMS was applied to this area 44. Finally, the activation of other more frontal areas could reflect the motor execution (Left Inferior Frontal Gyrus) and some additional monitoring processess to check if the selected result is correct (Right Dorsolateral Frontal Cortex). However, although consistent with the present findings, this interpretation needs to be confirmed by future research that could try to characterize whether the interference of the right parietal regions are detrimental only to mathematical processes or they generalize to other kinds of mental representations.

A potential criticism of this study is that the effects could reflect motor preparation. However, there are several arguments to refute this intepretation. First, if the observed activations were merely a consequence of articulatory preparation we would have expected a high correlation between response times and the brain activation (which was not the case, see Supplementary Materials). Second, if the effect was merely an effect related to motor preparation we would have expected similar (but) shifted, time courses of ERF data in *Slow* vs *Fast* responses, but this is not the case, as the time courses are mostly overlapping. Third, the different activations across conditions are not in the areas that are expected in tasks that include simple retrieval of a word (i.e., simple naming task). Indeed, a naming task in MEG shows typical activations in the classical areas of language production (mostly left lateralized),

but not in right frontal areas⁴⁵. Even if right parietal effects may be found, they are expected to be in earlier time windows^{45,46}. Finally, a motor preparation effect is expected to be associated with a decrease in beta frequencies, which should be higher and more consistent in the case of *Fast* as compared to *Slow Responses*. Time-frequency plots (as clearly showed by Figure 3) suggest that this is not the case. There was no significant difference in betas across conditions, but rather there is a qualitative difference in the opposite direction, with a larger beta decrease in the case of *Slow Responses*.

Limitations

The present study has some limitations that need to be underlined. First, given the correlational nature of MEG recordings and the type of contrast used (Fast vs Slow Responses), we cannot disentangle which area is "necessary" for a given operation or the areas that are always involved. Rather, the contrast between Fast and Slow Responses shows the activations that are more likely to be present before a Fast Response, that is, an efficient response. The actual importance of these activations should be corroborated by neuromodulation studies (e.g., TMS⁷). Secondly, the sample included in the current study was mostly composed of people with a degree in Psychology or Linguistics (see Supplementary Material for details, Table S1). Third, our distinction between Fast and Slow Responses is also just one of the possible methods to classify the responses, and finding the optimal method to study response efficiency (in terms of speed) is an issue that could be investigated in future studies. A final aspect to take into account is the potential overlap between response efficiency (as we classified in the present study) and problem size. There is a wide literature on the effects of problem size in mental multiplication 12,19,47,48. "Large problems", that is problems including multiplication with larger numbers (e.g., 7 x 9), require longer reaction times than "small problems" (e.g., 2 x 3). In the present study, it is not possible to tease apart the two effects because, often, fast responses were related to small problems (see Supplementary Materials, Table S2); however, this was not always the case. Future studies with a larger number of multiplications included in the experimental settings could have enough stimuli to better address this aspect and clarify (and distinguish) if specific and different routes depend on efficiency and on problem size, and/or their interaction.

Conclusions

In summary, the findings of the present study fill the gap between neuropsychological and studies with DCE, which uses mostly production tasks, and neuroimaging and neurophysiological studies, which used mostly verification tasks. We interpret the results as consistent with recent literature and compatible with the idea of a joint participation of the two hemispheres in single-digit multiplications¹⁰. Using an approach based on comparison of fast and slow responses, we showed how an early left hemisphere activation is followed by a right hemisphere activation before the answer is provided. The sequence of brain hemisphere involvement would be routinely adopted by literate people for problems that do not require extra effort, presumably the easiest and most practiced ones. The specific areas sub-serving these processes seem to be, consistent with most (permanent and temporary) lesion and neuroimaging studies,

the angular and the supramarginal gyrus in both the left and the right hemispheres. The results we presented open several new questions on the potential role of parietal lobes and other frontal areas during fact retrieval that could be addressed by further research on the field.

Declarations

AUTHOR CONTRIBUTIONS:

GA, RP, CS, and SB conceived the study. GA, RP, and CT collected the data. GA, RP, GR, and SF performed the pre-processing of the data. GA and SF performed the statistical analysis. FP supervised the data collection. All of the authors contributed to the writing of the manuscript and interpretation of the results.

DATA AND CODE AVAILABILITY STATEMENT:

All code will be made available, upon request. Data will be made available, upon permission from host institution, as data controller.

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COMPETING INTERSTS

The authors declare no competing financial interests.

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Figures

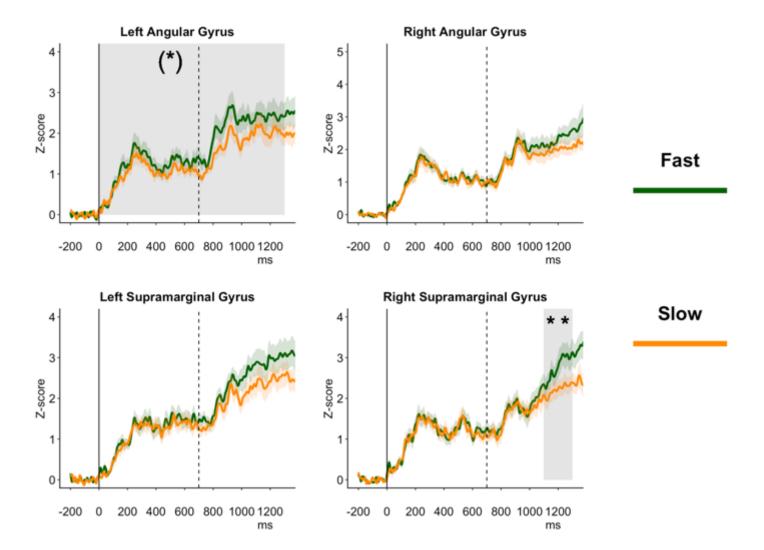


Figure 1

ROI analysis time-locked to the First Number. The figure shows the Event Related Fields (ERF) z-scores for each Region of Interest (ROI). Each ERF waveform represents the average time-series of z-scores of all participants within an ROI. Z-scores were calculated from source absolute values of activation. Shaded bands indicate standard errors around the mean. The gray areas and asterisks enclosed in round brackets ("(*)") highlight the time windows in which the ANOVA showed significant differences in a main effect. The asterisks without square brackets ("*") indicate the time windows in which there was a difference in the post-hoc analysis. The solid vertical lines indicate the appearance of the First Number, whereas the vertical dashed lines indicate the appearance of the Second Number.

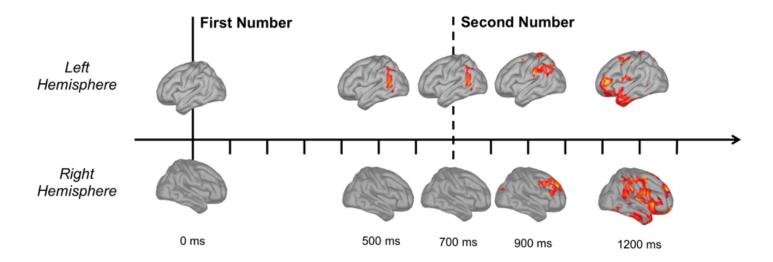


Figure 2

Results of cluster-based permutation analysis. The figure shows a schematic representation of results of cluster-based permutation analysis, comparing Fast Responses and Slow Responses (Fast >Slow). Colors highlight the areas in which the significant effects were mostly localized. In all cases, Fast Responses were associated with higher values (z-scores) compared to Slow Responses. The solid vertical line indicates the appearance of the First Number, whereas the vertical dashed line indicates the appearance of the Second Number. Differences were initially found in the left hemisphere (mostly in the Angular Gyrus), starting at about 500 ms after the First Number and lasting also after the second stimulus. Within the right hemisphere, significant differences were found about 200 ms after the presentation of the Second Number in the right frontal cortex, followed by a more widespread effect starting at encompassing also right parietal cortex.

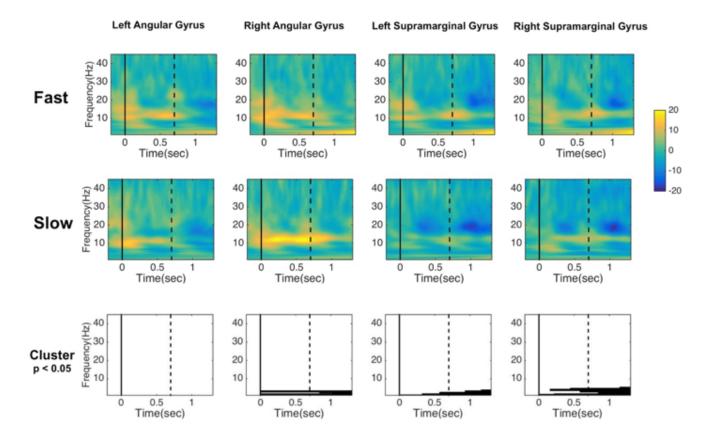


Figure 3

Results of time-frequency analysis on Fast and Slow responses. The figure shows the results of the time-frequency analysis based on Morlet deconvolution, comparing Fast Responses and Slow Responses. The two upper rows show the average response of the ERS/ERD change relative to a baseline window of -500 -200 ms. The first row depicts the average results in each ROI for Fast and Slow Responses. The bottom row shows the significant difference calculated with cluster-based permutation, with black areas denoting the time points and frequencies belonging to cluster with significant effects. In all significant effects, Fast Responses had higher magnitude values then Slow Responses. The significant differences were found for slow frequencies, mostly in the delta and partially in the theta range. The solid vertical line indicates the appearance of the First Number, whereas the vertical dashed line indicates the appearance of the Second Number. For a better inspection of the results, larger figures are reported in the Supplementary Material.

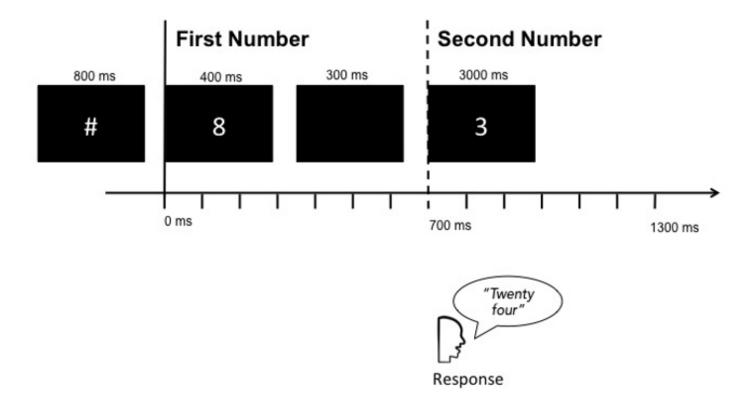


Figure 4

Schematic representation of the Task. The figure illustrates the task procedure. The participants were asked to answer after the Second Number, providing the results of the multiplication between the numbers. Analyses were conducted on ERF time-locked to the First Number (8 in the example, solid vertical line) and to the Second Number (3 in the example, dashed vertical line). The space between two ticks in the x-axis indicates a 100 ms interval.

Supplementary Files

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