

# Visual Feedback Improves Bimanual Force Control Performances at Planning and Execution Levels

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## Research Article

**Keywords:** force, variability, bimanual, control, coordination, patterns, across, trials

**Posted Date:** July 12th, 2021

**DOI:** <https://doi.org/10.21203/rs.3.rs-677666/v1>

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3 **Planning and Execution Levels**

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15 **Running Title:** Visual effects on bilateral motor synergies and force control

16 **Abstract Words:** 200

17 **Text Words:** 3,701

18 **Number of Figures:** 4  
19  
20

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### **Abstract**

The purpose of this study was to determine whether altered interlimb coordination patterns across trials improved bimanual force control capabilities within a trial. Fourteen healthy young participants completed bimanual force control tasks at 5%, 25%, and 50% of maximum voluntary contraction with and without visual feedback. To estimate synergetic coordination patterns between hands across multiple trials, we analyzed our primary outcome measure by performing an uncontrolled manifold analysis. In addition, we calculated force accuracy, variability, and regularity within a trial to quantify task stabilization. Using Pearson's correlation analyses, we determined the relation between the changes in bilateral motor synergies (i.e., a proportion of good variability relative to bad variability) and bimanual force control performance from no-vision to vision conditions. The findings revealed that the presence of visual feedback significantly increased bilateral motor synergies with a reduction of bad variability components across multiple trials, and decreased force error, variability, and regularity within a trial. Further, we observed significant positive correlations between higher bilateral motor synergies and increased improvements in force control capabilities. These findings suggested that bimanual synergetic coordination behaviors at the planning level modulated by external sensory feedback may be related to advanced task stabilization patterns at the execution level.

## Introduction

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Bimanual force control is frequently involved in conducting various activities of daily living<sup>1</sup>. Moreover, successful interlimb force coordination contributes to accomplishing the goals of bimanual movements<sup>2</sup>. Conventional perspectives on bimanual force coordination assume that force outputs from each hand need to be coupled such as a single unit so that these coupling patterns improve bimanual force control performance<sup>3</sup>. However, recent studies raised a proposition that two hands consistently interact and compensate each other in motor synergies to stabilize task performance. The reason being that the central nervous system tends to select the synergetic movements in numerous options (i.e., motor abundance) rather than attempting to find a specific method (i.e., motor redundancy)<sup>4,5</sup>.

The uncontrolled manifold (UCM) analysis is frequently used for estimating individual's motor synergetic patterns between two limbs<sup>4,6</sup>. Given that the UCM findings mainly focus on changes in motor control patterns across multiple trials, this approach provides an elegant way to explore movement variability and compensatory behaviors in the motor system at the planning levels<sup>7,8</sup>. The UCM analysis quantifies the proportion between the variance of fundamental elements projected to the UCM line (i.e., good variability that has no effect on task performance) and those projected to the orthogonal (ORT) line (i.e., bad variability that interferes with task performance). Thus, a higher proportion of good variability relative to bad variability indicates greater synergic force outputs produced by the two hands across different trials. Importantly, the increased synergic forces may contribute to the stabilization of overall task performances.

Several UCM studies examined changes in interlimb force coordination patterns (i.e., bilateral motor synergies) across multiple bimanual force control trials according to specific constraints (i.e., organism, task, and environment constraints) that may influence an individual's coordination functions<sup>9-11</sup>. For example, findings from studies on elderly people

85 and individuals post stroke revealed less bilateral motor synergies with higher task error and  
86 variability within a trial as compared with age-matched controls because of their potential  
87 organism constraints such as impaired sensorimotor processing<sup>10,12,13</sup>. Moreover, the  
88 asymmetrical task goals during bimanual force control increased bilateral motor synergies  
89 with more precise force control in healthy young adults in comparison to the symmetrical  
90 force production tasks<sup>6,9,11</sup>. Although these findings indicated that certain constraints may  
91 simultaneously influence levels of bilateral motor synergies across multiple trials and force  
92 control capabilities within a trial, whether specific changes in motor synergic patterns are  
93 directly related to an altered state of overall task stabilization in the motor system is still  
94 unclear.

95 To determine the relationship between bilateral motor synergies and task  
96 stabilization, we modulated visual information during bimanual force control tasks. Previous  
97 findings reported that the presence of visual information improved force accuracy, variability,  
98 and regularity with better force coordination function (e.g., more negative correlation  
99 between two hands) within a trial, whereas the absence of visual information impaired the  
100 force control capabilities and facilitated more positive correlation patterns<sup>14,15</sup>. Further, some  
101 studies reported that the modulation of visual information strongly affected individual's  
102 motor control strategies using higher cognitive functions as indicated by altered motor  
103 synergic patterns across multiple trials<sup>16,17</sup>.

104 Thus, the purpose of this study was to examine altered bilateral motor synergies  
105 across multiple trials and force control capabilities within a trial for healthy young adults  
106 while manipulating vision and no-vision conditions. Further, we determined whether changes  
107 in bilateral motor synergies were related to task stabilization during bimanual force control  
108 tasks. Participants executed movements associated with three different targeted force levels  
109 (i.e., 5%, 25%, and 50% of maximum voluntary contraction: MVC) because an individual's

110 motor control strategies across trials and within a trial may be influenced by different task  
111 difficulty<sup>18-20</sup>. Given that the positive effects of visual information on motor control  
112 capabilities<sup>21</sup>, we hypothesized that from no-vision to vision conditions the participants  
113 would increase bilateral motor synergies and improve force control capabilities, and further  
114 the increase in bilateral motor synergies would be related to more improvements in task  
115 stabilization.

## 116 **Results**

### 117 ***UCM findings: bilateral motor synergies, good variability, and bad variability***

118 Repeated measures ANOVA on the Visual Condition  $\times$  Force Level ( $2 \times 3$ ) design for  
119 the  $V_{\text{Index}}$  showed a significant Vision Condition main effect [ $F(1, 13) = 211.585; P < 0.001$ ;  
120 partial  $\eta^2 = 0.942$ ; Fig. 1A]. Post-hoc analysis revealed that the values of  $V_{\text{Index}}$  were  
121 significantly greater in the vision condition than those in the no-vision condition collapsed  
122 across three targeted force levels. Two-way repeated measures ANOVA on the  $V_{\text{UCM}}$   
123 demonstrated a significant Force Level main effects [ $F(1.042, 13.549) = 19.045; P = 0.001$ ;  
124 partial  $\eta^2 = 0.594$ ; Fig. 1B]. The post-hoc analysis showed higher values of the  $V_{\text{UCM}}$  at 5%  
125 of MVC than those at 25% of MVC ( $P = 0.002$ ) and 50% of MVC ( $P = 0.002$ ).

126 The analysis on the  $V_{\text{ORT}}$  revealed a significant Vision  $\times$  Force level interaction [ $F(2,$   
127  $26) = 4.078; P = 0.029$ ; partial  $\eta^2 = 0.239$ ; Fig. 1C]. The post-hoc analyses indicated that the  
128 values of  $V_{\text{ORT}}$  were significantly less in the vision condition than those in the no-vision  
129 condition at 5% of MVC ( $P < 0.001$ ) and 50% of MVC ( $P < 0.001$ ). At 25% of MVC, the  
130 analysis similarly showed different trends in the  $V_{\text{ORT}}$  between vision and no-vision  
131 conditions ( $P = 0.051$ ). These findings indicate that interlimb coordination across multiple  
132 trials as indicated by bilateral motor synergies was improved when visual feedback was  
133 available, and further the presence of visual feedback reduced bad variability components in  
134 bilateral motor synergies. These patterns were observed across all targeted force levels.

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Insert Figure 1 about here

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135 ***Bimanual motor performance findings: force accuracy, variability, and regularity***

136 Repeated measures ANOVA on the two-way Visual Condition  $\times$  Force Level ( $2 \times 3$ )  
137 for the RMSE revealed a significant Vision  $\times$  Force level interaction [ $F(1.328, 17.261) =$   
138  $27.193; P < 0.001$ ; partial  $\eta^2 = 0.677$ ; Fig. 2A]. The post-hoc analyses revealed that the  
139 values of RMSE were significantly less in the vision condition than those in the no-vision  
140 condition across the three targeted force levels ( $P < 0.001$ ). Further, in the no-vision  
141 condition, the values of RMSE significantly increased as the force level elevated ( $P < 0.001$ ).

142 A two-way repeated ANOVA on the CV showed two significant main effects: (a)  
143 Vision Condition [ $F(1, 13) = 61.273; P < 0.001$ ; partial  $\eta^2 = 0.825$ ; Fig. 2B] and (b) Force  
144 Level [ $F(1.157, 15.045) = 5.594; P = 0.028$ ; partial  $\eta^2 = 0.301$ ]. The post-hoc analysis on the  
145 Vision Condition main effect revealed less CV in the vision condition than those in the no-  
146 vision condition. Additional post-hoc analysis on the Force Level main effect showed higher  
147 CV at the 5% of MVC ( $M \pm SE = 5.61 \pm 0.65\%$ ) than those at the 25% of MVC ( $M \pm SE =$   
148  $3.54 \pm 0.28\%$ ;  $P = 0.020$ ).

149 Analysis of the SampEn revealed a significant Vision  $\times$  Force Level interaction [ $F(2,$   
150  $26) = 5.162; P = 0.013$ ; partial  $\eta^2 = 0.284$ ; Fig. 2C]. The follow-up tests showed higher  
151 SampEn in the vision condition than those in the no-vision conditions across the three  
152 targeted force levels ( $P < 0.001$ ). Further, for both visual conditions SampEn decreased as the  
153 targeted force level increased ( $P < 0.001$ ). Taken together, these findings indicate that the  
154 presence of visual feedback efficiently improved bimanual force control performances within  
155 a trial, as indicated by less force error, variability, and regularity regardless of different  
156 targeted force levels.

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Insert Figure 2 about here

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157 ***Correlation findings: bilateral synergies versus force control performance***

158 To determine whether changes in interlimb coordination patterns across multiple  
159 trials (i.e., bilateral motor synergies) were related to changes in bimanual force control  
160 performances (i.e., force accuracy, variability, and regularity) within a trial from the no-vision  
161 to vision conditions, we performed Pearson's correlation analyses. Given that the positive  
162 effects of visual feedback on bilateral motor synergies and force control performances  
163 similarly appeared across different targeted force levels, we analyzed the correlation patterns  
164 including the findings from the three targeted force levels. The correlation findings showed  
165 that greater changes in the  $V_{\text{Index}}$  from the no-vision to vision conditions were significantly  
166 related to an increased reduction in the CV collapsed across the three targeted force levels  
167 (Fig. 3A). Moreover, increased values of the  $V_{\text{Index}}$  with visual feedback were significantly  
168 related to higher values of SampEn collapsed across the three targeted force levels (Fig. 3B).  
169 However, the analysis failed to show a significant correlation between the  $V_{\text{Index}}$  and RMSE  
170 ( $r = -0.138$ ;  $P = 0.385$ ). These findings indicate that advanced interlimb coordination patterns  
171 across multiple trials were related to increased improvements in bimanual force control  
172 performances within a trial.

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Insert Figure 3 about here

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173 **Discussions**

174 The purpose was to determine the effect of two visual conditions and three targeted  
175 force levels on bilateral motor synergies and force control performances during isometric  
176 force control tasks in healthy young adults. One of our leading questions involved whether  
177 altered interlimb coordination patterns across trials improved bimanual force control

178 capabilities within a trial. Additionally, we examined the correlation between changes in  
179 bilateral motor synergies and force control performances to specify whether selecting optimal  
180 bimanual coordinative motor solutions across multiple trials was related to successful task  
181 stabilization within a trial. The combined findings revealed that in the vision condition the  
182 performers significantly increased bilateral motor synergies while reducing bad variability  
183 across multiple trials. Moreover, the presence of visual feedback significantly improved  
184 bimanual force control performances within a single trial, as indicated by higher force  
185 accuracy, less force variability, and greater force irregularity. Importantly, we observed  
186 significant correlations between an increase in bilateral motor synergy and improvements in  
187 force control performances from no-vision to vision conditions collapsed across the three  
188 targeted force levels.

189         The UCM findings revealed that the values of bilateral motor synergies between two  
190 hands significantly increased from no-vision to vision condition with a reduction of bad  
191 variability components across the three targeted force levels. According to Newell's  
192 constraints theory<sup>34,35</sup>, cooperative bimanual movement patterns in the motor system were  
193 primarily dependent on three constraints within a single trial: (a) organism constraints (e.g., a  
194 performer's capability), (b) environmental constraints (e.g., extrinsic feedback), and (c) task  
195 constraints (e.g., task difficulty). In addition to the within-trial findings, previous UCM  
196 studies demonstrated the effects of three constraints on interlimb coordination patterns across  
197 multiple trials, as they observed decreased bilateral motor synergies in a specific population  
198 (e.g., older adults)<sup>10,12,36</sup> and easier task difficulty (e.g., symmetrical tasks)<sup>9,11</sup>. Similarly, the  
199 current findings confirmed the influence of an environmental constraint (i.e., visual  
200 information) on bilateral motor synergies consistent with prior results<sup>9,10</sup>. Moreover, the two  
201 targeted force levels below 50% of MVC did not alter bilateral motor synergies although the  
202 ratio of good and bad variability was affected by the task constraint<sup>13,23</sup>. These findings

203 indicated that the performers showed a tendency to maintain the level of bilateral motor  
204 synergies during various submaximal force modulations by interactively modulating the  
205 ratios of good variability and bad variability across multiple trials.

206         The presence of online visual feedback increased bilateral motor synergies  
207 implicating more cooperative motor actions between two hands with the reduction of bad  
208 variability components across multiple trials. Freitas and colleagues proposed the stability-  
209 optimality trade-off phenomenon in human behaviors<sup>37</sup>. Specifically, an optimality strategy  
210 represents that the central nervous system selects an optimal motor solution from numerous  
211 motor elements (i.e., motor redundancy) by minimizing the variance of force elements  
212 produced by two limbs along the UCM line. On the other hand, a stability strategy indicates  
213 the organization of numerous motor elements (i.e., motor abundance) for stabilizing task  
214 performance by decreasing the variance of force elements along the ORT line resulting in  
215 greater index of bilateral motor synergies (i.e., higher good variability relative to bad  
216 variability). These two motor control strategies may independently influence actions  
217 generating synergetic interlimb movements<sup>28,37-39</sup>. Taken together, our findings suggest that  
218 when the simultaneous task-related visual feedback is available, the performer may prefer the  
219 stability strategy for successful task performances across multiple trials via increasing  
220 bilateral motor synergies while minimizing bad variability components.

221         As we expected, bimanual force control capabilities within a trial were more  
222 improved in the vision condition, as indicated by decreased task error, variability, and  
223 regularity. Presumably, providing visual feedback facilitates activation of visuomotor  
224 networks contributing to online motor corrections and task stabilization during isometric  
225 force control<sup>9,14,25,40</sup>. In addition, the availability of online visual information may positively  
226 regulate firing rates on neuromuscular systems by decreasing the neural noise of synaptic  
227 input and motor neuron pools<sup>9,41</sup>. Moreover, the performers increased force irregularity in the

228 vision condition indicating more compensatory and adaptive force outputs between hands. A  
229 prior study reported increased values of approximate entropy (ApEn) on bimanual forces  
230 from no-vision to vision conditions<sup>14</sup>. Given that SampEn analysis may have higher  
231 independence of results according to different data lengths<sup>29</sup>, we additionally confirmed force  
232 regularity reduced by visual information with the advanced nonlinear approach. Perhaps, the  
233 presence of visual information decreases environmental entropy while simultaneously  
234 increasing motor entropy, referred to as compensatory trade-off effects<sup>42,43</sup>.

235         Importantly, our findings revealed that an increase in bilateral motor synergy across  
236 multiple trials from no-vision to vision conditions was positively correlated with the  
237 improvements in force control performances (i.e., a reduction of force variability and  
238 regularity) collapsed across the three targeted force levels. Ranganathan and Newell reported  
239 that the presence of visual information during bimanual finger force control tasks contributed  
240 to reducing disturbances on the variability in degrees of freedom (DOFs) at the execution  
241 level and facilitating the use of numerous motor solutions at the planning level<sup>7</sup>. Further, the  
242 findings suggested that synthesizing motor control processes between execution and planning  
243 levels may consequently stabilize task performances<sup>7</sup>. Accordingly, the current findings  
244 confirmed the potential relation between bilateral synergetic coordination strategies at the  
245 planning level (i.e., between multiple trials) and traditional and temporal structural of motor  
246 variability of DOFs produced by two hands at the execution level (i.e., within a single trial).

247         Moreover, our correlation findings supported a proposition that the motor system  
248 may prefer the stability strategy from no-vision to vision conditions because we observed  
249 greater bilateral motor synergies with reduced bad variability related to advanced task  
250 stabilization patterns such as less variable and regular bimanual force outputs<sup>37</sup>. As revealed  
251 in a neuroimaging study, force control improvements in the vision condition were  
252 significantly related to visuomotor processing with greater parietal cortical activations<sup>44</sup>.

253 Given that the parietal cortex was highly involved in both motor execution and planning<sup>44-46</sup>,  
254 the presence of online visual information may increase neural resources for the visuomotor  
255 integration contributing to more adaptive and corrective motor strategies at the execution  
256 level and updating motor control strategies at the planning level.

## 257 **Conclusions**

258 The current study revealed that visual feedback during bimanual isometric force  
259 control tasks significantly increased bilateral motor synergies across multiple trials while  
260 simultaneously reducing bad variability components. An apparent consequence of the  
261 improved force control capabilities within a single trial involves reduced force error,  
262 variability, and regularity. Importantly, we observed that a higher frequency of bilateral motor  
263 synergetic patterns was positively related with more improvements in force control  
264 performances from no-vision to vision conditions. These findings suggest that the presence of  
265 task-related visual information contributes to improved coordinative behaviors between  
266 hands at both planning and execution via potential facilitation of visuomotor cortical  
267 activations for task stabilization. Despite the positive effects of task-related visual  
268 information on task stabilization across multiple trials and within a trial, how the presence of  
269 visual feedback differently influences bimanual force control strategies is still unknown.  
270 Thus, future studies should investigate the effects of variations of visual feedback (e.g., visual  
271 gain or frequency) on bimanual force control strategies active during motor action planning  
272 and execution.

## 273 **Methods**

### 274 ***Participants***

275 Fourteen young adults (mean  $\pm$  standard deviation age = 21.6  $\pm$  2.3 years; eight  
276 females and six males) participated in this study. All participants were right-handed healthy  
277 individuals without musculoskeletal deficits in their upper extremities and cognitive

278 dysfunctions. The current study protocols were approved by the University of Florida's  
279 Institutional Review Board, and we confirmed that all methods were performed in accordance  
280 with the relevant guidelines and regulations. All participants read and signed an informed  
281 consent before starting the test.

### 282 *Experimental setup*

283 We used isometric force control paradigms during bimanual wrists and fingers  
284 extension movements consistent with the prior experimental designs<sup>10,13,22</sup>. Initially, the  
285 participants sat 78 cm away from a 43.2 cm LED monitor (1024 × 768 pixels; refresh rate =  
286 100 Hz) and placed their forearms on the desk in comfortable positions (i.e., 15–20° of  
287 shoulder flexion and 20–40° of elbow flexion). Next, the participants situated their hands and  
288 fingers under the customized platforms embedded with two force transducers (MLP-75,  
289 Transducer Techniques, 4.16 × 1.27 × 1.90 cm, range = 75 lbs., 0.1% sensitivity). During the  
290 tasks, the participants extended their hands and fingers upward against the platforms to  
291 produce isometric forces.

292 Initially, the participants conducted three maximal voluntary contraction (MVC)  
293 trials (trial interval = 6 s and rest time between trials = 60 s). Using a mean value of three  
294 peak force outputs across the MVC trials, we set three submaximal targeted force levels (i.e.,  
295 5%, 25%, and 50% of MVC) for each individual. These targeted force levels have been  
296 previously tested and the findings showed that people may produce different force control  
297 strategies depending on altered targeted force levels<sup>13,20,23,24</sup>.

298 The goal of each submaximal isometric force control trial was to match and maintain  
299 bimanual force production around a targeted force level for 20 s. Based on previous  
300 studies<sup>22,25,26</sup>, we administered two different visual conditions: (a) vision and (b) no-vision.  
301 Specifically, in the vision condition the LED monitor simultaneously displayed the  
302 performer's force outputs produced by both hands with a white line trajectory and a targeted

303 force level, a green line centered on the monitor during each 20 s trial. In the no-vision  
304 condition, we removed the white force trajectory after the first 5 s, and then the performer  
305 saw only a targeted force level for the remaining 15 s. Participants completed 12 trials for  
306 each experimental block (i.e., 6 experimental blocks = 2 visual conditions  $\times$  3 targeted force  
307 levels), for a total 72 submaximal force control trials. During these submaximal force control  
308 tasks, we randomly assigned the six experimental blocks to participants with each block set at  
309 a constant visual angle ( $= 1^\circ$ )<sup>27</sup>.

310 A custom LabVIEW Program (National Instruments, Austin, USA) conducted  
311 standardized testing procedures and data collection. All force signals were sampled at the rate  
312 of 100 Hz using a 16-bit analog-to-digital converter (A/D; NI cDAQ-9172 + NI 9215 and  
313 minimal force unit detection = 0.0016 N) and amplified using a 15LT Grass Technologies  
314 Physio-data Amplifier System (Astro-Med Inc.) with an excitation voltage of 10 V and a gain  
315 of 200.

### 316 *Data analyses*

317 For the following offline-data analyses, we initially filtered the raw force data using a  
318 bidirectional fourth-order Butterworth filter at 20 Hz of cut off frequency using a custom  
319 Matlab program (Math Works™ Inc., Natick, USA). The middle 10 s (i.e., 5–15 s; 1,000 data  
320 points) of force signals was most important for minimizing transient effects of early or later  
321 motor corrections in a trial.

322 To estimate bimanual force coordination across trials, we quantified bilateral motor  
323 synergies based on the UCM theory<sup>4,6,11,13</sup>. First, we calculated a mean force value for each  
324 hand within a trial and normalized the mean force value into fundamental elements pair using  
325 a targeted force level. For instance, when a targeted force level is 80 N, a performer may  
326 produce 70 N of mean force produced by two hands (i.e., 30 N from left hand and 40 N from  
327 right hand). Thus, a pair of normalized fundamental elements included: (a) left hand: (30 N /

328 80 N)  $\times 100 = 37.5\%$  and (b) right hand:  $(40 \text{ N} / 80 \text{ N}) \times 100 = 50\%$ . Finally, this calculation  
 329 was repeated across 12 trials for each experimental block, and the 12 pairs of normalized  
 330 fundamental elements were projected to two distinctive lines: (a) UCM line (Fig. 4A) and (b)  
 331 ORT line (Fig. 4B), respectively.

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Insert Figure 4 about here

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332 The variance components projected to the UCM line are associated with successful  
 333 motor control capabilities (good variability:  $V_{UCM}$ ). On the other hand, the variance  
 334 components projected to the ORT line interfere with motor control (bad variability:  $V_{ORT}$ )<sup>28</sup>.  
 335 The  $V_{Index}$  (i.e., a proportion of  $V_{UCM}$  relative to  $V_{ORT}$ ) indicates an index of bilateral motor  
 336 synergies ranging from -2 to 2 values (Formula 1). Note that higher values of  $V_{Index}$ , close to  
 337 2, represent better bimanual coordination patterns across multiple trials<sup>10</sup>.

338 For additional parametric statistical analyses, we performed Z-transformation on all  
 339  $V_{Index}$  values using Formula 2 consistent with prior findings<sup>11,13</sup>.

$$340 \quad V_{Index} = \frac{V_{UCM}/df_{UCM} - V_{ORT}/df_{ORT}}{V_{TOT}/df_{TOT}}$$

341 (1)

342 Where  $df_{UCM}$  shows degrees of freedom of  $V_{UCM}$  ( $df = 1$ ),  $df_{ORT}$  is degree of freedom of  $V_{ORT}$   
 343 ( $df = 1$ ),  $V_{TOT}$  indicates the sum of  $V_{UCM}$  and  $V_{ORT}$ , and  $df_{TOT}$  is degrees of freedom of  $V_{TOT}$   
 344 ( $df = 2$ ).

$$345 \quad V_{Index} (Z - transformed) = 0.5 \times \ln \frac{2+V_{Index}}{2-V_{Index}}$$

346 (2)

347 To assess bimanual force control performance within a trial, we calculated three  
 348 outcome measures: (a) force accuracy: root mean square error (RMSE), (b) force variability:  
 349 coefficient of variation (%CV) = SD of force / mean force  $\times 100$ , and (c) force regularity:

350 sample entropy (SampEn; Formula 3)<sup>29,30</sup>.

$$351 \text{ SampEn}(x, m, r, N) = \ln \left[ \frac{C_m(r)}{C_{m+1}(r)} \right] \quad (3)$$

352 where  $m$  is specific pattern length,  $r$  is a criterion of similarity in the time series, and  
 353  $C_m(r)$  indicates occurrence of repetitive patterns of length  $m$  in time series  $x$  (i.e., force  
 354 data in the time samples) excluding the self-match<sup>30</sup>. Consistent with a previous study, we  
 355 used a value of 2 for  $m$  and  $r = 0.2 \times$  standard deviation (SD) of force data<sup>29</sup>.

### 356 *Statistical analyses*

357 All outcome measures (i.e.,  $V_{\text{Index}}$ ,  $V_{\text{UCM}}$ ,  $V_{\text{ORT}}$ , RMSE, CV, and SampEn) were  
 358 analyzed with two-way repeated measure ANOVAs (Visual Condition  $\times$  Force Level;  $2 \times 3$ ).  
 359 We confirmed the normality of all dependent variables across vision and force level  
 360 conditions using the Shapiro-Wilk's  $W$  test<sup>31</sup> and Levene's test<sup>32</sup>. When the sphericity  
 361 assumption was violated, we reported the degrees of freedom adjustments using Greenhouse-  
 362 Geisser<sup>33</sup>. For conducting post hoc analysis, we used Bonferroni's pairwise comparisons.  
 363 Finally, Pearson's correlation analysis was used to identify potential relationships between  
 364 changes in bilateral motor synergy and changes in force control performances including force  
 365 accuracy, variability, and regularity from no-vision to vision conditions. All statistical analyses  
 366 were performed using the IBM SPSS Statistics 22 (SPSS Inc., Chicago, IL, USA) and we set  
 367 an alpha level at 0.05.

368

369

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- 473
- 474

475 **Author contributions**

476 HJL, JHL, NK, and JHC contributed to data collection, statistical analyses, data  
477 interpretation, and manuscript drafts. NK conceived and designed the study and conducted  
478 statistical analyses. All authors approved the final manuscripts.

479

480 **Funding**

481 This work was supported by Incheon National University Research Grant in 2020 (2020-  
482 0064).

483

484 **Competing interests**

485 The authors declare no competing interests.

486

487 **Data availability**

488 All data generated or analysed during this study are included in this published article.

489 **Figure Captions**

490

491 **Figure 1. Bimanual coordination across multiple trials using UCM approach ( $M \pm SE$ ).** (A)  
492 bilateral motor synergy ( $V_{\text{Index}}$ ) for visual conditions (vision versus no-vision) collapsed across  
493 the targeted force levels. (B) Good variability ( $V_{\text{UCM}}$ ) for the targeted force levels (5%, 25%,  
494 and 50% of MVC) collapsed across the visual conditions. (C) Bad variability ( $V_{\text{ORT}}$ ) for visual  
495 conditions (vision versus no-vision) as a function of targeted force levels (5%, 25%, and 50%  
496 of MVC).

497

498 **Figure 2. Bimanual force control performance within a trial ( $M \pm SE$ ).** (A) Force accuracy  
499 (RMSE) for visual conditions (vision versus no-vision) as a function of targeted force levels  
500 (5%, 25%, and 50% of MVC). (B) Force variability (CV) for the visual conditions (vision  
501 versus no-vision) collapsed across the targeted force levels. (C) Force regularity (SampEn) for  
502 visual conditions (vision versus no-vision) as a function of targeted force levels (5%, 25%, and  
503 50% of MVC).

504

505 **Figure 3. Correlation findings between changes in bilateral motor synergies and bimanual**  
506 **force control performances from no-vision to vision conditions.** (A) negative correlation  
507 between bilateral motor synergy ( $V_{\text{Index}}$ ) and force variability (CV) and (B) positive correlation  
508 between bilateral motor synergy ( $V_{\text{Index}}$ ) and force irregularity (SampEn).

509

510 **Figure 4. UCM analysis quantifying variances of fundamental elements projected to the**  
511 **UCM and ORT lines.** (A) The 12 pairs of normalized fundamental elements extracted from  
512 each trial (i.e., black circles) projected to both UCM line (i.e., blue line) and ORT line (i.e.,  
513 dotted red line) at 25% of MVC condition in the vision condition and (B) no-vision condition.

514

# Figures

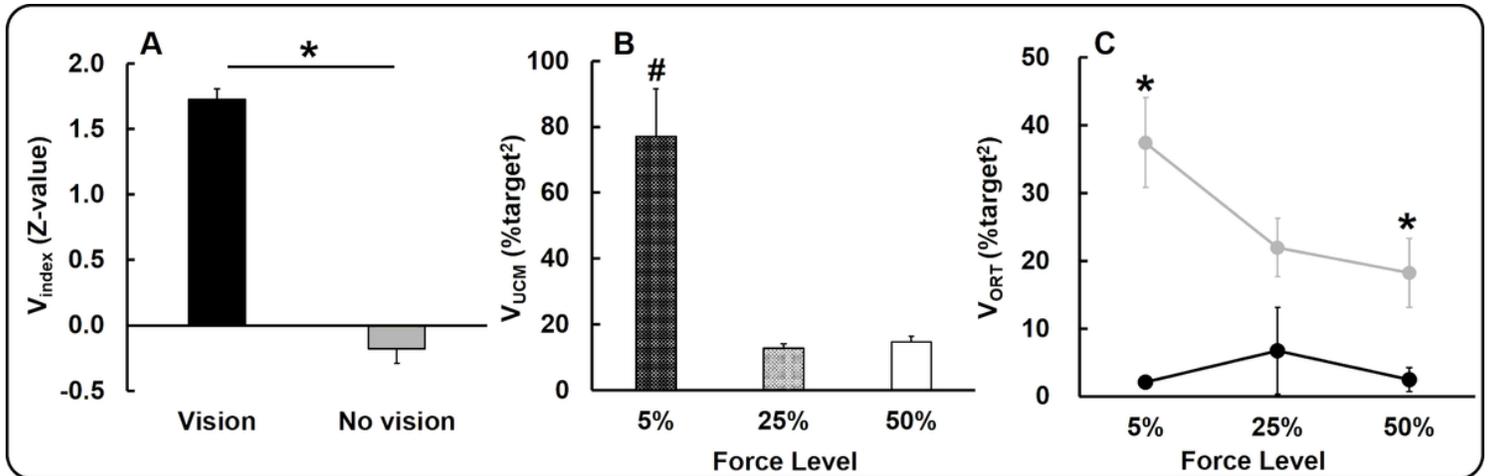


Figure 1

Bimanual coordination across multiple trials using UCM approach ( $M \pm SE$ ). (A) bilateral motor synergy ( $V_{index}$ ) for visual conditions (vision versus no-vision) collapsed across the targeted force levels. (B) Good variability ( $V_{UCM}$ ) for the targeted force levels (5%, 25%, and 50% of MVC) collapsed across the visual conditions. (C) Bad variability ( $V_{ORT}$ ) for visual conditions (vision versus no-vision) as a function of targeted force levels (5%, 25%, and 50% of MVC).

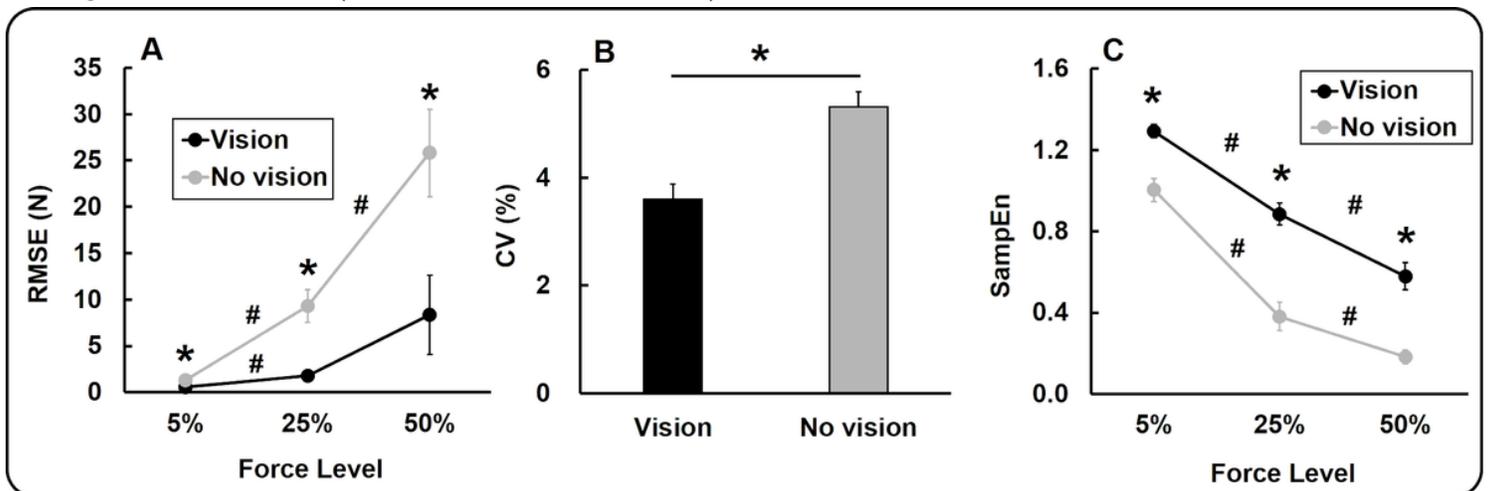


Figure 2

Bimanual force control performance within a trial ( $M \pm SE$ ). (A) Force accuracy (RMSE) for visual conditions (vision versus no-vision) as a function of targeted force levels (5%, 25%, and 50% of MVC). (B) Force variability (CV) for the visual conditions (vision versus no-vision) collapsed across the targeted force levels. (C) Force regularity (SampEn) for visual conditions (vision versus no-vision) as a function of targeted force levels (5%, 25%, and 50% of MVC).

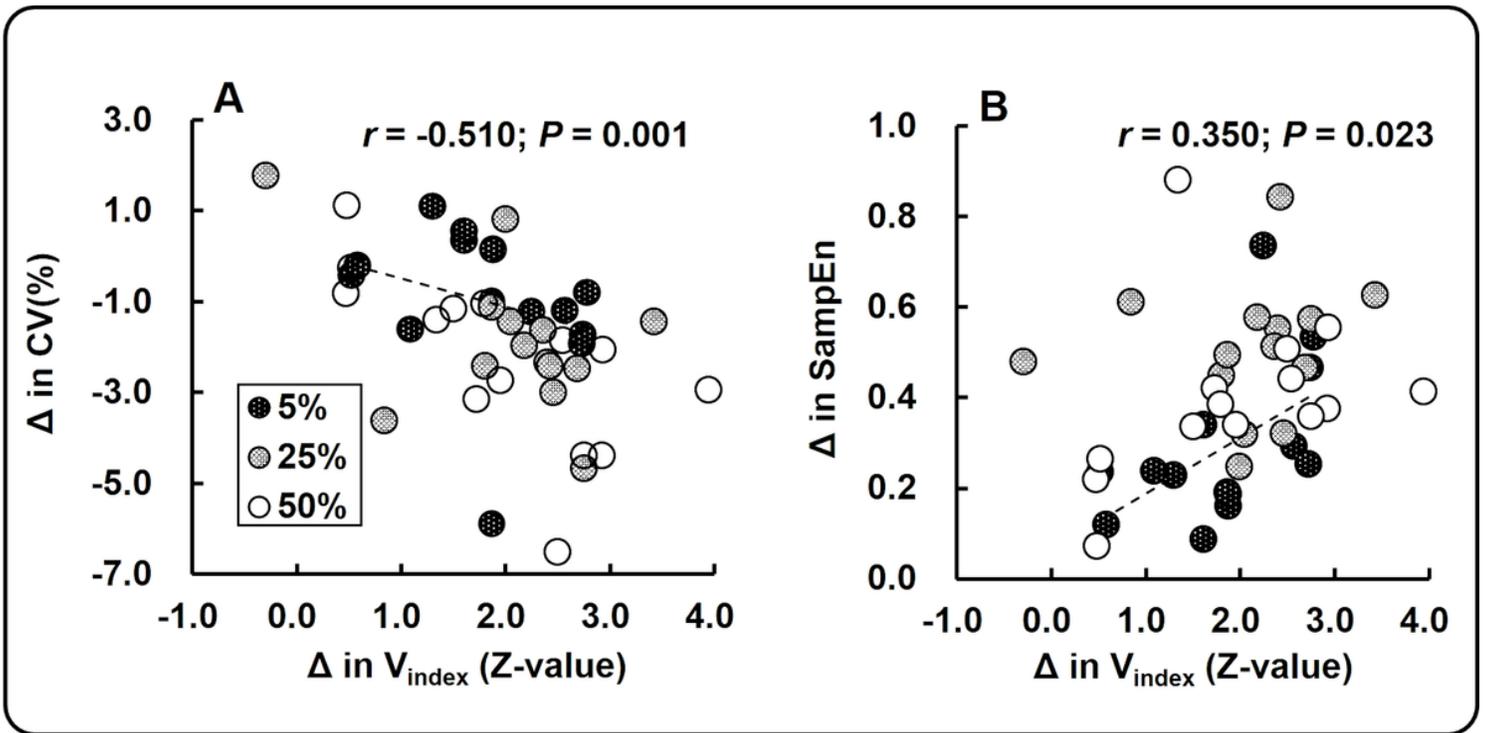


Figure 3

Correlation findings between changes in bilateral motor synergies and bimanual force control performances from no-vision to vision conditions. (A) negative correlation between bilateral motor synergy (VIndex) and force variability (CV) and (B) positive correlation between bilateral motor synergy (VIndex) and force irregularity (SampEn).

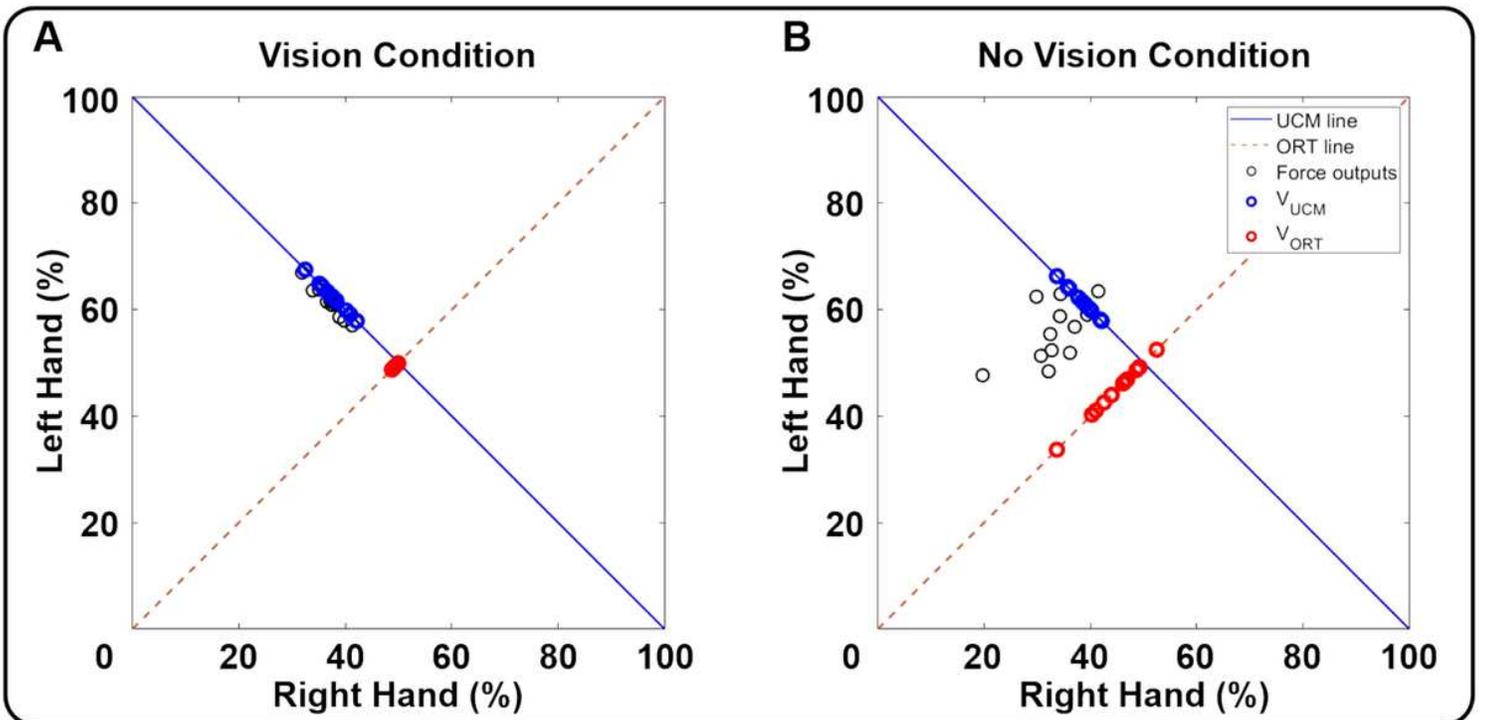


Figure 4

UCM analysis quantifying variances of fundamental elements projected to the UCM and ORT lines. (A) The 12 pairs of normalized fundamental elements extracted from each trial (i.e., black circles) projected to both UCM line (i.e., blue line) and ORT line (i.e., dotted red line) at 25% of MVC condition in the vision condition and (B) no-vision condition.