

Endogenous N-oleoylethanolamine Crystals loaded Liposomes with Enhanced Hydrophobic Drug Loading Capacity for Efficient Stroke Therapy

Shichao Wu

Xiangya Hospital Central South University

Di Liao

Xiangya Hospital Central South University

Xi Li

Xiangya Hospital Central South University

Zeyu Liu

Xiangya Hospital Central South University

Lin Zhang

Xiangya Hospital Central South University

Fanny Mo

Xiangya Hospital Central South University

Shuo Hu

Xiangya Hospital Central South University

Jian Xia

Xiangya Hospital Central South University

Xiangrui Yang (✉ yangxr@xmu.edu.cn)

Xiamen University <https://orcid.org/0000-0002-6238-7904>

Research Article

Keywords: Stroke, N-oleoylethanolamine (OEA), Liposomes, Neuroprotective, Positron emission tomography (PET)

Posted Date: July 27th, 2021

DOI: <https://doi.org/10.21203/rs.3.rs-732565/v1>

License:   This work is licensed under a Creative Commons Attribution 4.0 International License.

[Read Full License](#)

Abstract

Background. Although the preparation of liposomes achieves great success and many have received regulatory approval, their retention of highly hydrophobic drugs is still problematic.

Results. Herein we report a novel strategy for efficiently loading hydrophobic drug to liposomes for stroke therapy. N-oleoylethanolamine (OEA), an endogenous highly hydrophobic molecule with outstanding neuroprotective effect, was successfully loaded to OEA-SPC&DSPE-PEG liposomes (OSDP LNPs) with a drug loading of 15.9 ± 1.2 wt%, four times higher than those prepared via traditional methods. Efficient retention in OSDP LNPs greatly improved the pharmaceutical property and therefore enhanced the neuroprotective effect of OEA. Through the data of positron emission tomography (PET) and TTC-stained brain slices, it could be clearly visualized that the acute ischemic brain tissues were preserved as penumbral tissues and bounced back with reperfusion. The in vivo experiments stated that OSDP LNPs could significantly improve the survival rate, the behavioral score, the spatial learning and memory ability of the MCAO (middle cerebral artery occlusion) rats. Meanwhile, the cerebral infarct volume, the edema degree, the apoptosis of the neurons and the inflammation within the brain were also greatly decreased.

Conclusions. These results suggest that the OSDP LNPs have a great chance to develop hydrophobic OEA into a potential anti-stroke formulation.

Background

The integration of drug and amphipathic molecules into nano-assembly achieves great success on optimizing the pharmaceutical properties of insoluble drug [1–4]. There are two primary procedures in an integration process: the crystallization of the drug and the self-assembly of the amphipathic molecules [5, 6].

When the drug is the chief component, its crystallization would be the main process [7, 8]. Serving as the crystallization inhibitor and stabilizer, the amphipathic molecules would co-precipitate on the drug crystals, terminating their growth and stabilizing them [9]. As a result, micro- or nanocrystals would obtain instead of bulk crystals. For instance, 10-hydroxycamptothecin could assemble into nanofibers, which would grow into comet-shaped nanocrystalline assemblies under the guidance of a block copolymer additive- PLGA [5]. The main advantage of the drug nanocrystals is the high drug loading, which might come up to more than 50% [10, 11]. However, the high drug loading brings out the long-term instability and severe burst release. To address the problem, high amounts of amphipathic molecules are involved in nanodrug. In this case, the self-assembly of the amphipathic molecules became the main process, accompany with the co-precipitate of the drug into the assemblies [12]. The liposomes, with the drug uniformly dispersed, were prepared via this strategy [13–16]. Compared with the nanocrystals, the liposomes possessed significantly enhanced stability and controlled drug release property. Until now, a number of liposomes have received regulatory approval, and many more are in the pipeline [17, 18]. The therapeutic benefits of the liposome technology rely on the ability of long-circulation to increase the

efficiency of chemotherapeutic agents by delivering high concentrations of the drug to tumor sites, while reducing their accumulation in normal tissues to minimize the side-effect [19]. Hence, the drug loading property of the liposome is one of the key factors which influence their efficiency. However, the retention properties of drugs in liposomes are largely drug dependent [20]. Loading the drug in response to transmembrane pH gradients would further increase the drug loading and the stability [21]. Via the technology, weak-base drugs, originally difficult to retain in liposome, could receive a relatively high retention property [22, 23]. However, retention of highly hydrophobic drugs in liposomes is still problematic [24–26]. For instance, the loading efficiency of paclitaxel by different methods varies from 1.5–4% by weight [27, 28]. This extremely low drug loading is due to the highly hydrophobic property of paclitaxel [29]. Current strategies to develop liposome-based formulations of highly hydrophobic drugs have focused on incorporation of these drugs in the lipid bilayer of liposomes [20]. However, these formulations could not possess a high drug loading, and drug rapidly exchanges from the liposome bilayer, leading to their instability in the blood circulation [24].

To enhance the drug loading and the stability of liposomes, our group developed hydrogen bond based liposomes of various drugs [30–33]. Through forming hydrogen bond between the drug and soybean lecithin, the drug could be efficiently and firmly loaded in liposomes, possessing a high drug loading and enhanced controlled release property. Based on this method, we report a novel strategy here which could cleverly combine the self-assembly of the amphipathic molecules with the crystallization of the drug. With the crystallization of hydrophobic OEA inside the OSDP LNPs, the drug loading increased by four times compared to those of traditional methods. In the *in vivo* experiments, the OSDP LNPs possessed an outstanding neuroprotective effect and achieved enhanced therapeutic efficiency in the treatment of the cerebral injury caused by MCAO.

Results And Discussion

Preparation and characterization of OSDP LNPs

A key feature of the research is the precursor mediated, controlled drug crystallization inside the liposomes. In order to obtain nanosized crystals in the liposomes, the traditional nanoprecipitation technique were optimized. The hydrogen bond were formed between OEA and lecithin (SPC) via our previous method [18, 20], which was confirmed by H^1 NMR and XRD. In the H^1 NMR spectra (Fig. 1A), the peak at 7.76 ppm (ascribed to the $-NH-$ of OEA), the peak at 4.63 ppm (ascribed to the $-OH$ of OEA), and the peak at 3.47 ppm (ascribed to phosphatidylcholine of SPC) appeared to obviously weakened in the OEA–SPC complex, illustrating the formation of hydrogen bonds. The disappear of the sharp peaks of bulk OEA in the XRD pattern of OEA-SPC also confirm that the hydrogen bonds might have formed between OEA and SPC molecules (Fig. 1B).

Afterwards, extra OEA and OEA–SPC were dissolved in dichloromethane, which was then dispersed in DI water containing DSPE-PEG under ultrasonic conditions. After stirring for one hour, the system turned into a stable, white O/W suspension with the dispersion of the organic droplets in the continuous phase. In

this stage, there was an arrangement of DSPE-PEG molecules with the hydrophobic groups of DSPE around the organic droplets and the PEG groups in the continuous phase. The droplets could be seen as precursors, which might proceed via non-classical crystallization routes. Lastly, with dichloromethane rapidly removed by rotary evaporation, the multistage crystallization process proceeded. Due to the evaporation of the organic phase, water molecules entered the droplets, resulting in the precipitation and arrangement of SPC-OEA complex. Hence, phospholipid bilayers were prepared according with the arranged DSPE-PEG molecules. The bond of OEA to SPC molecules would serve many nucleation sites, leading to a number of OEA crystal nucleus. The rapid evaporation of the organic phase would induce a high supersaturation, under which the OEA crystal nucleus grew into OEA nanocrystals and rapidly reached the thermodynamically stable crystalline form. Since the phospholipid bilayers were flexible, their shapes might be changed by OEA nanocrystals. Followed by extrusion through polycarbonate membranes (0.22 μm pore diameter), irregularly non-spherical shaped liposomes, with drug crystal inside and phospholipid bilayers outside, were successfully prepared. The representative structure illustration of the OSDP LNPs is depicted in Fig. 1D.

As illustrated in Fig. 1C and Figure S1, the OSDP LNPs were around 100 nm with an irregularly non-spherical shape. It could be noticed that the black fields inside of the liposomes appear darker than the fields forming the contour of the liposomes, which appear to be a paler shade of grey (Fig. 1C-b and c). The inside dark field might owe to the existence of OEA crystals, whose molecules arranged well-ordered and closely. Since the electrons could not easily pass through the closely packed crystals, the inside field of the liposomes showed a deep color. On the contrary, the phospholipid bilayers were loosely arranged, leading to a higher electron transmittance and hence a light shade. The two different colored sections also illustrated the delicate hierarchical architectures of the OSDP LNPs.

X-ray diffraction was also employed to detect the form of OSDP LNPs. As shown in Fig. 1B, the sharp peaks of bulk OEA would disappear with the formation of hydrogen bonds in the OEA-SPC complex. Nevertheless, a majority of sharp peaks of OSDP LNPs belongs to OEA, suggesting its high crystallinity. Although, the OEA within OSDP LNPs shows the same polymorphic form as their bulk counterparts, the width of the peaks have reduced a lot, which might attribute to the nanoscaled crystal size of OEA within OSDP LNPs. Meanwhile, the coverage of lipid bilayer on the OEA nanocrystals led to the weakness of OEA.

Stability test and in vitro drug release study

The biggest advantage of the OSDP LNPs lies in the sustained drug release property with a high drug loading. The drug loading of OSDP LNPs could reach up to 15.9 ± 1.2 wt%, while that of the OEA-SPC LNPs collected from the traditional method ranged from about 0.5 wt% to 3.0 wt%. With the formation of hydrogen bonds, the drug loading increased to about 8.0 wt%. When the nanoscaled OEA crystal appeared within the liposomes, the drug loading was redoubled to 15.9 ± 1.2 wt%. Although the drug loading of many liposomes might come up to more than 50 wt%, the retention of highly hydrophobic

drugs is still a critical bottleneck.²⁰ The drug loading of many liposomes was less than 10 wt%, or even less. In this research, the formation of hydrogen bonds, plus the crystallization within the liposomes, greatly enhanced the retention of OEA with highly hydrophobic property. A well-established study showed that drug release could be controlled by the drug-loading content of the particles. High drug loading means severe burst release, while poor drug loading brings well controlled drug release [21]. As to OSDP LNPs (Figure S2), higher drug loading also led to a little burst release within the first 8 h, which might come from the exposed OEA crystals and the OEA on the surface of the liposomes. Compared to the OEA crystals without the coverage of lipid bilayer, this slight burst release could be neglected. Just like the OEA-SPC NPs with a drug loading of 8.2 wt%, the OSDP LNPs exhibited a remarkably prolonged and controlled drug release in the next 40 h, which could almost be seen as zero-order release. That is to say, the enhanced drug loading did not reduce the controlled release property of the liposomes. This was owing to the unique construction of the liposomes. Unlike other drug crystals, the OEA crystals was located in the center of the OSDP LNPs, covered with lipid bilayers and bonding with the SPC molecules, which would largely limit the diffusion of the drug. Hence, the OSDP LNPs possessed a steady sustained release pattern throughout the release period. Moreover, the lipid bilayers, the PEG chains, the monodisperse, the high Zeta potential (-16.1 mV, Figure S3) and the small particle size contributed to the stability of the OSDP LNPs. With minor size changes, the OSDP LNPs could preserve stability in an aqueous environment for 48 hours (Figure S4). On the contrary, the OEA-SPC NPs (d = 213 nm) without coating of PEG chains would aggregate within 6 hours. And the lyophilized OSDP LNPs redissolved easier than OEA-SPC NPs. The redissolved dispersion of lyophilized OSDP LNPs possessed a size of about 180 nm and was still applicable for intravenous injection within 1 month, while the OEA-SPC NPs couldn't (Figure S5). The reason was the strong hydrophilicity of PEG, which could stabilize the liposomes and make them more soluble in water.

Assessment of the neuroprotective effect of the OSDP LNPs *in vivo*.

To assess the *in vivo* neuroprotective effects of the OSDP LNPs on ischemic cerebral injury, systematic experiments were performed on rats. According to our previous study [30, 35], OEA could obviously reduce the cerebral infarct volume of the brains from the MCAO rats. Hence, it could be speculated that a lot of ischemic tissues were preserved to be ischemic penumbra with the administration of OEA, which could be salvaged by timely reperfusion. To visualize the ischemic penumbra and its recovery, positron emission tomography (PET) of [¹⁸F]fluoro-2-deoxy-D-glucose ([¹⁸F]FDG) was employed to assess the cerebral glucose metabolism [36, 37]. PET data were acquired for 20 minutes at 0 h, 1 h, and 2 h after reperfusion. Since the inflammation-related high-[¹⁸F]FDG uptake might appear around 3 d post-reperfusion [38], PET data were collected within 2 h post-reperfusion to eliminate the effect of inflammation. As shown in Fig. 2a, the right cerebral hemisphere of all the operated rats exhibited significantly reduced glucose metabolism compared with the left cerebral hemisphere at 0 h. The reason was that the blood supply of the right cerebral hemisphere was cut off and [¹⁸F]FDG could not arrive. Then, with 1 h of reperfusion, the

hypoperfused area began to recover in all the operated rats, and their uptake of [^{18}F]FDG began to increase. Interestingly, about 41.7% of the right cerebral hemisphere from the rats administrated with OSDP LNPs exhibited significantly elevated signals compared with the normal tissues (the blue dashed outline in Fig. 2a). And the enhancement extended to 83.6% of the right cerebral hemisphere at 2 h post-reperfusion. The PET intensity of these regions was about 63.24 ± 2.43 kbp/mL, which was much higher than that of the left cerebral hemisphere (51.76 ± 2.58 kbp/mL). In these regions, the cutting-off blood flow and thereby glucose supply is compensated by an increase of glucose uptake and phosphorylation rate to maintain cellular energy consumption [39], which might be used for repairing the cell damage caused by hypoperfusion. The enhanced glucose metabolism also stated the good cell viability in the region, and the region was called “the ischemic penumbra” in clinic. The ischemic penumbra would recover and functioned well afterwards, which could be verified via the TTC-stained brain slices (Fig. 2b). It could be observed that almost all the hypoperfused brain tissues, whose blood supply had been cut off for 90 min, were not infarcted via the administration of the OSDP LNPs. The results indicated that the hypoperfused brain tissues with elevated PET signals after reperfusion were mostly likely to recover. On the contrary, the other MCAO rats did not exhibited enhanced glucose metabolism in the ischemic brain tissues. Although the brains were recovering with reperfusion, the low-level glucose metabolism stated their terrible cell viability at 1 h post-reperfusion. What’s worse, an obvious infarction core appeared at 2 h post-reperfusion (The red dashed outline in Fig. 2a). While the other hypoperfused brain tissues possessed similar glucose metabolism to that of the left cerebral hemisphere, they had suffered from irreparable damage owing the acute ischemia and might ultimately die. Many hypoperfused brain tissues with certain PET signals at 2 h post-reperfusion were infarcted as shown in the TTC-stained brain slices of 24 h post-reperfusion (Fig. 2b). Then the cerebral infarct volume and the cerebral edema degree of all the rats were calculated (Fig. 2c-d). With a cerebral infarct volume of about 372.2 ± 26.9 mm³ and a cerebral edema degree of $13.6 \pm 1.0\%$, the operated rats without treatment had a severe brain damage, which would lead to a serious neurological deficit. With the treatment of free OEA, the cerebral infarct volume of the rats was reduced to 332.2 ± 35.3 mm³ and the cerebral edema degree to $11.3 \pm 1.1\%$. However, there was no significant difference between the OEA and MCAO groups ($P > 0.05$), which was in according with our previous studies [30]. Nevertheless, the cerebral infarct volume was decreased to 78.2 ± 18.4 mm³, and the cerebral edema degree was also decreased to a slight level. The data stated that the rats treated with OSDP LNPs suffered from much less brain damage than the rats of the other groups. What’s more, the photos of the TTC-stained brain slices, plus the PET data, forcefully demonstrated that the acute ischemic brain tissues could be preserved as penumbral tissues to a great extent via the administration of OSDP LNPs. And the preserved penumbral tissue would bounce back with reperfusion and possess an increased glucose metabolism within hours to compensate the reduced supply, leading to a better and more rapid recovery.

As an acute disease, ischemic stroke possesses a high mortality, and reducing death rates must be the primary task to a formulation for stroke. As shown in Fig. 2e, only 45.8% of the MCAO rats could survive for 14 d, and the administration of free OEA could not obviously change this data. In comparison, OSDP LNPs could effectively protect from MCAO and increase the survival rate to 83.3%. Furthermore, we

speculated that the rats administrated with OSDP LNPs were more likely died from the complications of MCAO, not from the cerebral injury. The small cerebral infarct volume illustrated that they suffered from a little cerebral injury (Fig. S6). The result indicated that the administration of OSDP LNPs might extend the time window for beneficial reperfusion.

Since the behavior of the stroke patients was one of the most important evaluation indicators in clinic, the behavior ability of the rats was evaluated via Garcia method. The Garcia scores of the rats were evaluated at 1, 3, 5, 7, and 14 d after operation. As shown in Fig. 2f, the sham-operated rats got full marks, while the operated rats only got about 10 points in the 1st assessment, illustrating the neurological function deficit of the models and the success of our operation. The rats administrated with OSDP LNPs performed much better than those of the other two operated groups throughout the assessment ($p < 0.01$). In addition to getting higher scores, the rats administrated with OSDP LNPs maintained enhanced recovery rate within the first week after operation, which might come from the preserved penumbral tissue. Under the protection of OSDP LNPs, more penumbral tissues were preserved and revived with reperfusion, leading to a better and more rapid recovery. On the contrary, OEA seemed to have no effect on improving neurological function deficit, owing to its extremely low bioavailability.

Morris water maze task.

Learning and memory are one of the most important computational strategies of the brain, which might be impaired by ischemia stroke. To examine the effects of OSDP LNPs on spatial learning and memory, rats were exposed to the water maze task. Between day 15 and 19 after operation, the rats were trained with five trials per day. Spatial learning ability was assessed by escape latency (the time required to find the platform in training). Compared with the sham group, the operated rats without treatment exerted much longer escape latency, illustrating their impaired spatial learning ability (Fig. 3A). Owing to their severe brain damage, two rats even could not find the platform within 120 seconds in the third training, while all the sham rats could reach the platform within 60 seconds in the first training. Compared with those of the MCAO group, the rats treated with OSDP LNPs needed less time to find the platform, stating their improved spatial learning ability. Moreover, the training seemed to be more effective to the rats of the nanodrug group, leading to a result that the escape latency was decreased from 75 s in the first training to 23 s in the fourth training (Fig. 3A). The result also illustrated their strong learning ability. At last, the data had no significant difference with that of the sham group, forcefully illustrating that the OSDP LNPs treatment effectively protected the spatial learning ability of the operated rats. Interestingly, the sham-operated rats exhibited significantly smarter than the operated rats after the first training. When entering water in the second training, many of them looked around to confirm the position of the platform, and straightly swam to it. Two rats treated with OSDP LNPs began to have the same performance in the fourth training, while the rats of the other groups just swam around to find the platform throughout the training.

When the platform was removed, the rats of the sham group and the nanodrug group exhibited markedly increased target crossing times (Fig. 3B), indicating their stronger potential memory for the removed platform. Moreover, it could be seen from the traces that the rats of the sham group and the nanodrug group always swam around the position of the removed platform (Fig. 3C). This strongly indicated that they had significant purpose and strong memory for the removed platform. On the contrary, the rats of the other groups possessed much less target crossing times and almost random traces, indicating their little memory for the platform. The results stated that the OSDP LNPs greatly ameliorated ischemia-induced spatial memory impairment.

Immunofluorescence staining and cell counting.

The intractable sequelae of stroke mostly resulted from the injury of neurons, which were really hard to recover. Here, TUNEL staining was employed to evaluate the apoptosis of the neurons in hippocampal CA1, which mainly involved in memory and cognition. As shown in Fig. 3D, none apoptotic cell was detected in the hippocampal CA1 of the sham-operated rats, while a significant increase in apoptotic cells could be found in those of the MCAO group and the OEA group. The results stated that the MCAO was likely to induce the apoptosis of the neurons, and this could not be improved by the administration of free OEA. In contrast, only one apoptotic cell was observed in the field of the nanodrug group. This significant decrease was likely related to the improved learning and memory ability of the rats of the nanodrug group. The result also indicated the nice neuroprotective effect of OSDP LNPs.

According to our previous studies [35, 40, 41], OEA could inhibit the inflammation of reperfusion, which was one of the most primary causes of the brain injury. Microglia and astrocyte play paramount roles in the brain inflammation, which could be specifically marked by Iba-1 and GFAP, respectively. Hence, the quantity of expressed Iba-1 and GFAP was used to evaluate the inflammation of reperfusion. As depicted in Fig. 4A and Fig. 4B, both markers suggested that the inflammation was slight in the sham-operated rats, while a significant increase could be observed in the cortex around the ischemic focus of the MCAO group and OEA group. With the administration of OSDP LNPs, the inflammation was decreased to a low level. The result indicated that the OSDP LNPs could greatly alleviate the inflammation induced by ischemic reperfusion, and therefore provide significant neuroprotective effects.

Conclusion

In summary, the study demonstrates a simple but novel method to fabricate internal crystallized liposomes to efficiently encapsulate highly hydrophobic OEA. The hydrogen bond within OEA-SPC totally changed the form of OEA and enhanced its solubility. Then, the crystallization of OEA inside the OSDP LNPs further enhanced the drug loading, and hence, the bioavailability of OEA would highly increase. With further studies focused on the assessment of the neuroprotective effect of the liposomes, the various indicators of the MCAO rats, including the survival rate, the behavioral score, the spatial learning and memory ability, the cerebral infarct volume, the edema degree, the apoptosis of the neurons and the

inflammation within the brain, were greatly improved via the administration of OSDP LNPs. What's more, it could be clearly visualized that almost all the acute ischemic brain tissues were preserved under the protection of OSDP LNPs and quickly recovered with reperfusion. These results suggest that the internal crystallized liposomes have potential applications in the field of hydrophobic drug delivery, and the OSDP LNPs may open new opportunities for the clinic use of hydrophobic OEA as a potential anti-stroke candidate.

Materials And Methods

Materials

All chemical reagents were of analytical grade and used without further purification unless otherwise stated. OEA (purity grade > 90.0%), SPC (soybean phosphatidylcholine, purity grade > 90%) were obtained from Shanghai Macklin Biochemical Co., Ltd (Shanghai, China). DSPE-PEG (MWCO 2000) was purchased from Ponsure Biotechnology Co., Ltd (Shanghai, China). Dichloromethane (DCM), and tetrahydrofuran (THF) were provided by Sinopharm Chemical Reagent Co., Ltd. (Shanghai, China). 2, 3, 5-triphenyltetrazolium chloride (TTC) were obtained from Shanghai yuanye Bio-Technology Co., Ltd (Shanghai, China)

Preparation of OEA – SPC Complex (OEA-SPC)

3 mg of OEA powder and 15 mg of SPC were codissolved in a glass pressure vessel with 8 mL of THF, accompanied by vigorous agitation at 40°C for 8 h. Then, THF was removed via vacuum rotary evaporation with a rotary evaporator (RE-5299; YUHUA, Gongyi, China).

Preparation of OSDP LNPs

The OSDP LNPs was synthesized by a nanoprecipitation technique. In brief, OEA (5 mg), and OEA-SPC (3 mg of OEA) were codissolved in 10 mL of DCM, and then the clear homogeneous solution was then dropwise (0.2 mL/min) introduced into distilled water (40 mL) containing DSPE-PEG (20 mg) under magnetic stirring (200 rpm/min). After stirring for one hour, the system turned into a stable, white O/W suspension. Subsequently, the dichloromethane was rapidly removed by rotary evaporation, producing a clear suspension and resulting in the formation of the OSDP LNPs. The OEA-SPC NPs were prepared in the same way except no extra OEA was added in this procedure and DSPE-PEG was replaced by SPC.

Characterization

The OEA – SPC was analyzed using XRD (Phillips X'pert Pro Super), and ^1H NMR (AVANCE III 400 MHz). The bulk OEA powers and SPC were used as control.

The OSDP LNPs were also analyzed with XRD to examine the form of OEA in OSDP LNPs. Morphology of the OSDP LNPs was examined by TEM (Tecnai G2 F20, USA) at 200 kV. The Size and zeta-potential values were determined by a Malvern Zetasizer Nano-ZS machine (Malvern Instruments, Malvern). Three parallel measurements were carried out to determine the average values. The content of OEA in OEA-SPC NPs was determined by LC-MS (LCMS ORBITRAP VELOS PRO ETD, USA). The content efficiency was calculated by Equations (1):

$$\text{Drug loading content of OEA(\%)} = \frac{\text{weight of OEA in NPs}}{\text{weight of NPs}} \times 100\% \quad (1)$$

In vitro drug release study

The *in vitro* drug release studies of OSDP LNPs were performed via the dialysis technique. The bulk OEA powers, OEA-SPC NPs and OSDP LNPs were dispersed in PBS buffer solution (10 mL) and placed in dialysis bags (MWCO 3500 Da). Then, the dialysis bags were immersed in PBS (0.1 M, 150 mL, pH 7.4) and continuously oscillated in a shaker incubator (180 rpm, 37°C). All samples were assayed by LC-MS.

Drugs administration

The OSDP LNPs were dissolved in saline with ultrasonic breaking. OEA and Twain's 80 was dissolved in saline under strong shaking. Drugs (1.5 mg/kg, iv) were administered once in rats at the time of redispersion, and daily for 14 consecutive days after ischemia.

Preparation of the focal cerebral ischemia model

Focal cerebral ischemia was induced by middle cerebral artery occlusion (MCAO) in adult male Sprague-Dawley (SD) rats, as previously described. In brief, rats were anesthetized with chloral hydrate (400 mg/kg, ip). The 4 - 0 silicon rubber-coated nylon monofilament was inserted into the right internal carotid artery (ICA) of the rats through the external carotid stump, and past the ECA/ICA bifurcation to occlude the origin of the middle cerebral artery (MCA) at the junction of the circle of Willis. The monofilament was kept in place for 90 min then withdrawn. Sham-operated rats were treated with an identical surgery except that the intraluminal filament was not inserted. Rats were excluded if hemorrhage was found in the brain slices or at the base of the circle of Willis during postmortem examination.

Positron Emission Tomography

PET scans at various time points post-operation (0 h, 1 h, and 2 h), image reconstruction were performed using a nanoScan® PET/CT (Mediso, HUN). MCAO rats (n = 6) were injected with [¹⁸F]-2-fluoro-2-deoxy-D-

glucose (FDG) via the tail vein and 20 min PET scans were performed. Since the best imaging time of FDG was about 45 min after administration, FDG was injected 45 min before each detection time.

Measurement of infarct volume

After PET scans, the rats (n = 6) were decapitated at 24 h post-reperfusion, and the brains were removed rapidly and cut into six 2-mm thick coronal sections, which were then stained with standard 2% TTC at 37°C for 10 min followed by overnight immersion in 10% formalin. Images of the stained brain sections were captured using a digital camera. The infarct area on each TTC-stained section was measured with Image Tool 2.0 software and calculated as the infarct area thickness (2 mm). The summed infarct volume of all brain sections was calculated as the total infarct volume. To determine the extent of ipsilateral oedema, the percentage increase in the ischemic hemisphere volume was calculated by Equations (2):

$$\text{Ipsilateral oedema degree(\%)} = \frac{(\text{ipsilateral volume} - \text{contralateral volume})}{\text{contralateral volume}} \times 100\% \quad (2)$$

Measurement of the survival rate

The survival rate of the rats were recorded. (n = 12 rats for sham group and the nanodrug group, and n = 24 rats for the MCAO group and the OEA group)

Evaluation of neurological deficit:

At 1 d, 3 d, 5d, 7 d, and 14 d after reperfusion, rats (n = 10) were evaluated neurologically by a single examiner who was blinded to the animal groups using the Garcia score. Animals were given a score of 0 to 18 (higher scores indicate greater function).

Morris water maze task

Morris water maze (MWM) task was performed from day 15 to day 20 after reperfusion. The protocol followed the previous report. Acquisition training consisted of 5-days conditioning with five trails per day from day 15 to 19. For each trail, the rats (n = 8 for each group) were placed in water and allowed to swim for a maximum of 120 s. If the rats found the platform, they were allowed to remain on it for 15 s. If they cannot find the platform within 120 s, they would be guided to the platform. The escape latency of finding the platform were recorded. On day 20, the platform was removed and rats were given one 120-s retention probe test. We recoded the swimming traces of the rats by a video camera with a computer via

an image analyzer. The number of times each animal crossed the position where the platform had been previously located were measured by the analyzer.

Immunofluorescence staining and cell counting

Rats (21 d after reperfusion) were anesthetized with chloral hydrate and perfused transcardially with ice-cold saline followed by perfusion with 4% paraformaldehyde. The brains were extracted and dehydration with a 10%, 20%, 30% sucrose gradient and then coronal sectioned (30 μm) using a vibrating microtome (Leica, Wetzlar, Germany). The sections were incubated in PBS (0.5% Triton X-100 and 10% goat serum) for 1 h at room temperature, following by incubation with rabbit polyclonal, TUNEL (Elabscience, CHN), GFAP (CST, USA) or rabbit polyclonal Iba-1 (Abcam, UK) at 4°C overnight. After several PBS rinses, sections were incubated with Alexa Fluor 594 donkey anti-rabbit IgG (Abcam, UK) or Alexa Fluor 488 donkey anti-rabbit IgG (Abcam, UK). The number of TUNEL, GFAP or Iba1 positive cells was analysed by fluorescence confocal microscopy (EX61, Olympus, Tokyo, Japan). The positive cells were counted in three randomly chosen squares of identical size (460 \times 460 μm).

Statistical analysis

The statistical significance of treatment outcomes was assessed using one-way/two-way analysis of variance for the differences within treatments followed by Tukey's post hoc test (Prism 7 for windows, GraphPad Software Inc., USA); $P < 0.05$ was considered statistically significant in all analyses (95% confidence level).

Abbreviations

OEA: N-oleoylethanolamine; PET: Positron emission tomography; MCAO: middle cerebral artery occlusion; OSDP LNPs: OEA-SPC&DSPE-PEG liposomes; FDG: [^{18}F]-2-fluoro-2-deoxy-D-glucose.

Declarations

Ethics approval and consent to participate

All procedures were carried out in accordance with the National Institutes of Health Guide for the Care and Use of Laboratory Animals and were approved by the Animal Ethical and Welfare Committee of Central South University.

Availability of data and material

All data generated or analyzed during this study are included in this published article.

Competing interests

The authors declare that they have no competing interests.

Author Contributions

XY and JX designed the experiments. SW, DL, XL, ZL, and LZ conducted experiments. SW and XY analyzed the data. XY write the paper, SW and SH helped to revise the manuscript. F M supervised the study. All authors read and approved the final manuscript.

Funding

This work was supported by National Natural Science Foundation of China (81901221 and 82001273).

Authors' informations

The authors SW and DL contributed equally and should be considered as co-first authors.

Consent for publication

Not applicable.

Open Access

This article is distributed under the terms of the Creative Commons Attribution 4.0 International License (<http://creativecommons.org/licenses/by/4.0/>), which permits unrestricted use, distribution, and reproduction in any medium, provided you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made. The Creative Commons Public Domain Dedication waiver (<http://creativecommons.org/publicdomain/zero/1.0/>) applies to the data made available in this article, unless otherwise stated.

References

1. Yi X, Dai J, Han Y, Xu M, Zhang X, Zhen S, et al. A high therapeutic efficacy of polymeric prodrug nano-assembly for a combination of photodynamic therapy and chemotherapy. *Communications Biology*. 2018; 1.
2. Shamay Y, Shah J, Isik M, Mizrachi A, Leibold J, Tschaharganeh DF, et al. Quantitative self-assembly prediction yields targeted nanomedicines. *Nat Mater*. 2018;17:361+.

3. Shi J, Kantoff PW, Wooster R, Farokhzad OC. Cancer nanomedicine: progress, challenges and opportunities. *Nat Rev Cancer*. 2017;17:20–37.
4. Rosenblum D, Joshi N, Tao W, Karp JM, Peer D. Progress and challenges towards targeted delivery of cancer therapeutics. *Nature Communications*. 2018; 9.
5. Yang X, Wu S, Li Y, Huang Y, Lin J, Chang D, et al. Integration of an anti-tumor drug into nanocrystalline assemblies for sustained drug release. *Chem Sci*. 2015;6:1650–4.
6. Luo C, Sun B, Wang C, Zhang X, Chen Y, Chen Q, et al. Self-facilitated ROS-responsive nanoassembly of heterotypic dimer for synergistic chemo-photodynamic therapy. *Journal Of Controlled Release*. 2019;302:79–89.
7. Mann S. Self-assembly and transformation of hybrid nano-objects and nanostructures under equilibrium and non-equilibrium conditions. *Nat Mater*. 2009;8:781–92.
8. Keck CM, Muller RH. Drug nanocrystals of poorly soluble drugs produced by high pressure homogenisation. *European Journal Of Pharmaceutics Biopharmaceutics*. 2006;62:3–16.
9. Li FY, Qin Y, Lee J, Liao HW, Wang N, Davis TP, et al. Stimuli-responsive nano-assemblies for remotely controlled drug delivery. *Journal Of Controlled Release*. 2020;322:566–92.
10. Shen S, Wu Y, Liu Y, Wu D. High drug-loading nanomedicines: progress, current status, and prospects. *International Journal Of Nanomedicine*. 2017;12:4085–109.
11. Jermain SV, Brough C, Williams RO III. Amorphous solid dispersions and nanocrystal technologies for poorly water-soluble drug delivery - An update. *International Journal Of Pharmaceutics*. 2018;535:379–92.
12. Bodratti AM, Alexandridis P. Formulation of Poloxamers for Drug Delivery. *J Func Biomater*. 2018;9:24.
13. Somasundar A, Ghosh S, Mohajerani F, Massenburg LN, Yang T, Cremer PS, et al. Positive and negative chemotaxis of enzyme-coated liposome motors. *Nat Nanotechnol*. 2019;14:1129+.
14. Liu D, Chen B, Mo Y, Wang Z, Qi T, Zhang Q, et al. Redox-Activated Porphyrin-Based Liposome Remote-Loaded with Indoleamine 2,3-Dioxygenase (IDO) Inhibitor for Synergistic Photoimmunotherapy through Induction of Immunogenic Cell Death and Blockage of IDO Pathway. *Nano Lett*. 2019;19:6964–76.
15. Lakkadwala S, Rodrigues BdS, Sun C, Singh J. Dual functionalized liposomes for efficient co-delivery of anti-cancer chemotherapeutics for the treatment of glioblastoma. *Journal Of Controlled Release*. 2019;307:247–60.
16. Cheng MHY, Harmatys KM, Charron DM, Chen J, Zheng G. Stable. J-Aggregation of an aza-BODIPY-Lipid in a Liposome for Optical Cancer Imaging. *Angew Chem-Int Edit*. 2019;58:13394–9.
17. Crommelin DJA, van Hoogevest P, Storm G. The role of liposomes in clinical nanomedicine development. What now? Now what? *Journal Of Controlled Release*. 2020;318:256–63.
18. Bulbake U, Doppalapudi S, Kommineni N, Khan W. Liposomal Formulations in Clinical Use: An Updated Review. *Pharmaceutics*. 2017; 9.

19. Kwon GS, Kataoka K. Block copolymer micelles as long-circulating drug vehicles. *Adv Drug Deliv Rev.* 2012;64:237–45.
20. Allen TM, Cullis PR. Liposomal drug delivery systems: From concept to clinical applications. *Adv Drug Deliv Rev.* 2013;65:36–48.
21. Drummond DC, Noble CO, Guo ZX, Hong K, Park JW, Kirpotin DB. Development of a highly active nanoliposomal irinotecan using a novel intraliposomal stabilization strategy. *Cancer Res.* 2006;66:3271–7.
22. Tang W-L, Tang W-H, Szeitz A, Kulkarni J, Cullis P, Li S-D. Systemic study of solvent-assisted active loading of gambogic acid into liposomes and its formulation optimization for improved delivery. *Biomaterials.* 2018;166:13–26.
23. Liang J, Fang C, Wu W, Yu P, Gao J, Li J. Preparation and properties evaluation of a novel pH-sensitive liposomes based on imidazole-modified cholesterol derivatives. *International Journal Of Pharmaceutics.* 2017;518:213–9.
24. Yingchoncharoen P, Kalinowski DS, Richardson DR. Lipid-Based Drug Delivery Systems in Cancer Therapy: What Is Available and What Is Yet to Come. *Pharmacol Rev.* 2016;68:701–87.
25. Liang X, Gao C, Cui L, Wang S, Wang J, Dai Z. Self-Assembly of an Amphiphilic Janus Camptothecin-Floxuridine Conjugate into Liposome-Like Nanocapsules for More Efficacious Combination Chemotherapy in Cancer. *Advanced Materials.* 2017; 29.
26. Karim R, Palazzo C, Evrard B, Piel G. Nanocarriers for the treatment of glioblastoma multiforme: Current state-of-the-art. *Journal Of Controlled Release.* 2016;227:23–37.
27. Yang T, Cui FD, Choi MK, Cho JW, Chung SJ, Shim CK, et al. Enhanced solubility and stability of PEGylated liposomal paclitaxel: In vitro and in vivo evaluation. *International Journal Of Pharmaceutics.* 2007;338:317–26.
28. Zhang JA, Anyarambhatla G, Ma L, Ugwu S, Xuan T, Sardone T, et al. Development and characterization of a novel Cremophor (R) EL free liposome-based paclitaxel (LEP-ETU) formulation. *European Journal Of Pharmaceutics Biopharmaceutics.* 2005;59:177–87.
29. Singla AK, Garg A, Aggarwal D. Paclitaxel and its formulations. *International Journal Of Pharmaceutics.* 2002;235:179–92.
30. Yang X, Xu L, Zhou J, Ge Y, Wu S, Huang J, et al. Integration of phospholipid-complex nanocarrier assembly with endogenous N-oleoylethanolamine for efficient stroke therapy. *Journal of Nanobiotechnology.* 2019;17:8.
31. Li Y, Wu HJ, Jia MM, Cui F, Lin JY, Yang XR, et al. Therapeutic Effect of Folate-Targeted and PEGylated Phytosomes Loaded with a Mitomycin C-Soybean Phosphatidylcholine Complex. *Mol Pharm.* 2014;11:3017–26.
32. Li Y, Lin J, Yang X, Li Y, Wu S, Huang Y, et al. Self-Assembled Nanoparticles Based on Amphiphilic Anticancer Drug-Phospholipid Complex for Targeted Drug Delivery and Intracellular Dual-Controlled Release. *ACS Appl Mater Interfaces.* 2015;7:17573–81.

33. Li Y, Wu HJ, Yang XR, Jia MM, Li YX, Huang Y, et al. Mitomycin C-Soybean Phosphatidylcholine Complex-Loaded Self-Assembled PEG-Lipid-PLA Hybrid Nanoparticles for Targeted Drug Delivery and Dual-Controlled Drug Release. *Mol Pharm*. 2014;11:2915–27.
34. Pang JM, Luan YX, Li FF, Cai XQ, Du JM, Li ZH. Ibuprofen-loaded poly(lactic-co-glycolic acid) films for controlled drug release. *Int J Nanomed*. 2011;6:659–65.
35. Zhou Y, Yang L, Ma A, Zhang X, Li W, Yang W, et al. Orally administered oleoylethanolamide protects mice from focal cerebral ischemic injury by activating peroxisome proliferator-activated receptor alpha. *Neuropharmacology*. 2012;63:242–9.
36. Kelly PJ, Camps-Renom P, Giannotti N, Marti-Fabregas J, Murphy S, McNulty J, et al. Carotid Plaque Inflammation Imaged by F-18-Fluorodeoxyglucose Positron Emission Tomography and Risk of Early Recurrent Stroke. *Stroke*. 2019;50:1766–73.
37. Deng L, Wan H, Zhou H, Yu L, He Y. Protective effect of hydroxysafflor yellow A alone or in combination with acetylglutamine on cerebral ischemia reperfusion injury in rat: A PET study using F-18-fluorodeoxyglucose. *European Journal Of Pharmacology*. 2018;825:119–32.
38. Fukumoto D, Hosoya T, Nishiyama S, Harada N, Iwata H, Yamamoto S, et al. Multiparametric Assessment of Acute and Subacute Ischemic Neuronal Damage: A Small Animal Positron Emission Tomography Study with Rat Photochemically Induced Thrombosis Model. *Synapse*. 2011;65:207–14.
39. Walberer M, Backes H, Rueger MA, Neumaier B, Endepols H, Hoehn M, et al. Potential of Early F-18 -2-Fluoro-2-Deoxy-D-Glucose Positron Emission Tomography for Identifying Hypoperfusion and Predicting Fate of Tissue in a Rat Embolic Stroke Model. *Stroke*. 2012;43:193–359.
40. Yang L, Guo H, Li Y, Meng X, Yan L, Zhang D, et al. Oleoylethanolamide exerts anti-inflammatory effects on LPS-induced THP-1 cells by enhancing PPAR alpha signaling and inhibiting the NF-kappa B and ERK1/2/AP-1/STAT3 pathways. *Scientific Reports*. 2016; 6.
41. Zhou H, Yang W-s, Li Y, Ren T, Peng L, Guo H, et al. Oleoylethanolamide attenuates apoptosis by inhibiting the TLR4/NF-kappa B and ERK1/2 signaling pathways in mice with acute ischemic stroke. *Naunyn-Schmiedebergs Archives Of Pharmacology*. 2017;390:77–84.

Figures

Image not available with this version

Figure 1

¹H NMR spectra (A) and XRD patterns (B) of OEA, SPC, OEA–SPC NPs and OSDP LNPs. (C) TEM images of OSDP LNPs. (D) Illustration of the formation and the structure of the OSDP LNPs.

Image not available with this version

Figure 2

Therapeutic effects of the indicated formulations (0.9% NaCl (Sham), OEA and OSDP LNPs, ([OEA]=1.5 mg/kg) on cerebral damage after MCAO in rats. (A) PET images of [¹⁸F]FDG in rat brain at 0 h, 1 h, and 2 h after MCAO. Red dashed outline represent the infarct core and the blue dashed outline represent the acute viable tissue. The infarct volume (B, C), the edema degree (D), the survival curves (E), and the behavioral scores (F) were detected. Data are expressed as mean±SEM. n=24 rats per group. Right middle cerebral artery was occluded. (****=P<0.0001, compared to MCAO group.)

Image not available with this version

Figure 3

The effect of the formulations on MCAO-induced spatial cognitive deficits. The escape latency (A), the target crossings (B) and swimming traces (D) in the Morris water maze task were recorded. (C, E) Representative pictures of the hippocampal CA1 stained with TUNEL (scale bars: 125 μ m). Data are expressed as mean \pm SEM. n=10–12 rats per group. (**=P<0.01, ***=P<0.001, ****=P<0.0001, compared to MCAO group)

Image not available with this version

Figure 4

Quantification of the area of GFAP positive stain (A-B) and the area of IBA-1 positive stain (C-D) from the cortex around the ischemic focus. scale bars: 125 μ m. (****=P<0.0001, compared to MCAO group)

Supplementary Files

This is a list of supplementary files associated with this preprint. Click to download.

- [renamed06c1f.png](#)
- [Sl.docx](#)