

Elevated circulating stem cells level is observed one month after implantation of Carmat bioprosthetic total artificial heart

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Short Report

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Abstract

The Aeson® total artificial heart (A-TAH) has been developed as a total heart replacement for patients at risk of death from biventricular failure. We previously described endothelialization of the hybrid membrane inside A-TAH probably at the origin of acquired hemocompatibility. We aimed to quantify vasculogenic stem cells in peripheral blood of patients with long-term A-TAH implantation. Four male adult patients were included in this study. Peripheral blood mononuclear cells were collected before A-TAH implantation (T0) and after implantation at one month (T1), between two and five months (T2), and then between six and twelve months (T3). Supervised analysis of flow cytometry data confirmed the presence of the previously identified $\text{Lin}^- \text{CD133}^+ \text{CD45}^-$ and $\text{Lin}^- \text{CD34}^+$ with different CD45 level intensities. $\text{Lin}^- \text{CD133}^+ \text{CD45}^-$, $\text{Lin}^- \text{CD34}^+ \text{CD45}^-$ and $\text{Lin}^- \text{CD34}^+ \text{CD45}^+$ were not modulated after A-TAH implantation. However, we demonstrated a significant mobilization of $\text{Lin}^- \text{CD34}^+ \text{CD45}^{\text{dim}}$ ($p = 0.01$) one month after A-TAH implantation regardless of the expression of CD133 or c-Kit. We then visualized data for the resulting clusters on a uniform manifold approximation and projection (UMAP) plot showing all single cells of the live Lin^- and CD34^+ events selected from down sampled files concatenated at T0 and T1. The three clusters upregulated in T1 are CD45^{dim} clusters, confirming our results. In conclusion, using a flow cytometry approach, we demonstrated in A-TAH-transplanted patients a significant mobilization of $\text{Lin}^- \text{CD34}^+ \text{CD45}^{\text{dim}}$ in peripheral blood one month after A-TAH implantation.

Introduction

The Aeson® total artificial heart (A-TAH, Carmat, Velisy Villacoublay, France) has been developed as a total heart replacement for patients at risk of death from biventricular failure (1). The A-TAH is a biventricular, autoregulated, pulsatile, electro-hydraulically actuated heart replacement device with all components embodied in a single device, implanted in the pericardial sac (2). The surfaces in contact with the patient's blood are formed from expanded polytetrafluorethylene and bovine pericardial tissue membrane processed in glutaraldehyde (3). These types of material have demonstrated a high level of biocompatibility in various applications such as bioprosthetic cardiac valve replacement (4). A-TAH efficacy has been proven in a feasibility study and then in a pivotal study, mainly in the indication of bridge-to-transplantation, leading to recent CE market approval (5, 6).

We previously described, in the first three implanted patients, the histological characteristics of explanted devices (7). In electron microscopy, we found a homogeneous adherent fibrin cellular network with endothelial cell deposition on this fibrin cap (7). The endothelial phenotype was confirmed with vascular endothelial (VE)-cadherin expression and the presence of tight junctional structures observed by electron microscopy (7). The origin of these endothelial cells remains unknown. Indeed, these cells shall originate from the circulating blood, since there is no physical connection between the endothelialized hybrid membrane and the patient's blood vessels. This could be linked to circulating endothelial progenitor cells (EPCs) or very small embryonic-like stem cells (VSELs) (1). EPCs and, in particular, endothelial colony-forming cells (ECFCs) obtained in culture are vasculogenic cells in adult humans (8, 9). However, the

phenotype of circulating EPCs is classically described as a subpopulation of circulating CD34⁺ and/or CD133⁺ stem cells expressing mainly VEGFR-2 receptor (KDR in human)(10). A multidimensional proteomic approach of circulating cells allowed us to fully characterize stem and progenitor cells in peripheral blood that could be at the origin of the endothelial cells. This extensive phenotyping enabled us to demonstrate that non-KDR cells with immaturity markers can be mobilized and confirmed the absence of KDR on circulating stem/progenitor cells (11). These mobilized progenitor cells could come from VSELs. These latter's are defined in human as lineage-negative (Lin⁻), CD133⁺ and/or CD34⁺ and CD45⁻ cells of small size (12–14). VSELs are able to give rise to endothelial cells and promote post-ischemic revascularization (15, 16).

The aim of the present study was to identify the distribution and phenotype of potential circulating vasculogenic stem cells in four patients after long-term A-TAH implantation.

Materials And Methods

Aeson® bioprosthetic total artificial heart (A-TAH) study design and population

The four patients presented in this study were derived from an ongoing single-arm prospective non-blinded and non-randomized study (NCT02962973) (6). The first patient was a 66-year-old who had the device implanted for 599 days and died. The second one was a 57-year-old who had the device implanted for 304 days before receiving a heart transplant. The third patient was 70 years old and had the device implanted for 271 days and was heart transplanted. The last patient was a 43-year-old who had the device implanted for 308 days before heart transplant. All patients were classified in Interagency Registry for Mechanically Assisted Circulatory Support (INTERMACS) 3 or 4 and clinical characteristics are presented in **Table 1**.

Sampling

Peripheral blood samples were collected on EDTA respectively before (T0), after one month (T1), between two and five months (T2), and between six and twelve months after A-TAH implantation (T3). Ficoll-isolated peripheral blood mononuclear cells (PB-MNCs) were isolated, aliquoted, frozen, and stored to assess the distribution of stem cells by spectral flow cytometry.

Flow cytometry

PB-MNCs samples from patients were slowly thawed and resuspended in PBS-SVF-EDTA buffer for counting in first step and resuspended at a concentration of 10 millions of cells per mL. Cells were incubated with an anti-human antibodies cocktail of lineage (α-CD3, α-CD14, α-CD16, α-CD11b, α-CD11c, α-CD19, α-CD56), CD45-BV650 (BioLegend), CD34-PeCy7 (BioLegend), c-Kit (CD117)-PeDazzle594 (BioLegend), CD133-VioBright667 (Miltenyi Biotec) and Zombie NIR (Biolegend) for viability during 30 minutes in the dark. Cells were washed by adding PBS-SVF-EDTA buffer and centrifuged two times.

Before acquisition, cells were fixed during 45 minutes in the dark at 4°C. Acquisitions were performed with a three lasers Aurora spectral flow cytometer (Cytek). Unmixing was calculated and applied to samples based on reference single stained PB-MNCs controls. Data were first analyzed in a supervised way with FlowJo (FlowJo, LLC) to identify immature cells. Down sampling of CD34⁺ population was done for every sample. Featured on CD45, CD34, CD133 and c-Kit expressions, consecutive dimension reduction was performed by Uniform Manifold Approximation and Projection (UMAP) algorithm (17) and meta-clustering was assessed by FlowSOM enabled identification of 7 clusters among the CD34⁺ cells using the cloud-based platform OMIQ (<https://www.omiq.ai/>).

Statistical analysis

Continuous data were expressed as mean of cells ± standard error of the mean. In the univariate analysis, we determined the differences within repeated measures by a non-parametric test. A p-value of 0.05 was considered statistically significant. Statistical analysis was performed using with GraphPad Prism 9 software (GraphPad Software Inc., San Diego, USA).

Results And Discussion

PB-MNCs from four male patients were collected before A-TAH implantation (T0) and after implantation at one month (T1), between two and five months (T2), and then between six and twelve months (T3). As the A-TAH hybrid membrane has been described as being endothelialized after several months of implantation (7), we decided to explore the phenotype of circulating stem cells after implantation in order to hypothesize the cell origin of these newly formed endothelial tissues. Supervised analysis of flow cytometry data confirmed the presence of the previously identified Lin⁻CD133⁺CD45⁻ and Lin⁻CD34⁺ with different CD45 level intensities. Lin⁻CD133⁺CD45⁻ and Lin⁻CD34⁺CD45⁻ were assumed to contain VSELs and were not modulated during the period studied here. The statistical analysis showed that, among the three populations of CD34⁺ only the Lin⁻CD34⁺CD45^{dim} was significantly increased one month after A-TAH implantation in contrast to pre-implantation level ($p = 0.01$), regardless of the expression of CD133 or c-Kit. Indeed, Lin⁻CD34⁺CD45^{dim} population could be sub-divided into four categories according to the positivity of CD133 and c-Kit. When CD133 or c-Kit were positive, we always observed a significant increase in stem cells after implantation, whereas there was no significant difference after A-TAH implantation in the Lin⁻CD34⁺CD45^{dim}CD133⁻c-Kit⁻ population. The data for the resulting clusters are visualized on a UMAP plot in **Figure 1** showing all single cells of the live Lin⁻ and CD34⁺ events selected from down sampled files concatenated at T0 and T1. The algorithm proposed seven clusters. As demonstrated in **Figure 1A**, three of the seven clusters evidenced are upregulated in T1, in contrast to T0: clusters 7, 4, and 2. In **Figure 1B**, analysis demonstrated that the increase concerned the three CD45^{dim} clusters, confirming our results presented in **Table 2**. Thus, using a flow cytometry approach, we showed a significant mobilization of Lin⁻CD34⁺CD45^{dim} in peripheral blood one month after A-TAH implantation. We recently described a progressive endothelialization of the bioprosthetic hybrid membrane of the A-TAH that could be at the origin of its acquired hemocompatibility (7). As there is no physical connection

between the internal membrane of the device and the patient's blood vessels, the source of these neo-endothelial cells in the A-TAH shall come from the circulating blood. Thus, the aim of this study was to identify by conventional flow cytometry approaches stem cells in blood that could be mobilized and could give rise to newly formed endothelial cells on the hybrid membrane of the A-TAH.

In the past years, CD34⁺ cells emerged as the most convincing cell type among those that have been evaluated for their use in cell-therapy trials and as biomarker of cardiac disease (10). CD34⁺ hematopoietic stem cells with the CD45^{dim} phenotype have been proposed as a source of extra hematopoietic cells like cardiomyocytes for example (18), although this has been controversial (19). However, in human adults, we don't know with certitude the stem cell at the origin of ECFCs. Indeed, it is now admitted that ECFCs are the main human post-natal vasculogenic cells (8). ECFCs have been described to grow from circulating CD34⁺ cells present in adult peripheral blood, but during *in vitro* expansion part of the cells lose CD34. CD34⁺ and CD34⁻ ECFCs have different angiogenic properties and CD34 expression in ECFCs could be related to a specific state of endothelial phenotype (20). Their origin has been proposed in CD45 negative cells (21) but subtype of CD34 involved in ECFC differentiation is unclear (22). CD34⁺ cell sub-populations may be derived from VSELs. VSELs were first identified as CD45 negative cells and characterized by their very small size (3-5 μm in diameter) in murine and human bone marrow (5-6 μm in diameter) (14). VSELs are mobilized into peripheral blood in response to injury following acute myocardial infarction (23) or critical leg ischemia (15) and we previously demonstrated that these cells trigger post-ischemic revascularization (15). Others and we have also shown VSELs ability to differentiate into endothelial cells (15, 24-26). Human VSELs have been described expressing CD133, but some description of human CD34⁺VSELs have been done and their vascular differentiation ability confirmed (27). CD34⁺VSELs can regenerate damaged organs and may solve the problems inherent in the use of controversial embryonic stem cells or induced pluripotent stem cells indeed. In our study, we did not include any size beads. However, when back gating our populations, we can assume that Lin⁻CD133⁺CD45⁻ cells are only small sized cells compatible with VSELs phenotype. In contrast, Lin⁻CD34⁺CD45⁻ and Lin⁻CD34⁺CD45^{dim} are a mix of small and large sized CD34⁺ cells. Lin⁻CD34⁺CD45^{dim} of small size has never been specifically studied in terms of multipotent differentiation ability. Thus, we observed the mobilization of a CD34⁺ population with CD45^{dim} expression while the CD45^{neg} population was not mobilized. This CD45^{dim} population contained various-sized cells. Further study needs to evaluate the ability of CD45^{dim}CD34⁺ cells of small and "normal size" to give rise to endothelial cells *in vitro* and *in vivo* and validate the origin of newly formed endothelial cells on top of A-TAH hybrid membrane.

All in all, bioprosthetic A-TAH implantation allowed us to evidence the mobilization in peripheral blood of Lin⁻CD34⁺CD45^{dim} stem cells that could be at the origin of the endothelial recovery. In order to organize new cell-therapy trials or determine the cells at the origin of endothelial lineage *in vivo* further studies need to appreciate the size of stem cells that are mobilized and able to build vessels. This topic of adult stem cells at the top of the hierarchy of endothelial lineage requires research on stem cells in peripheral

blood in other cardiovascular mobilization situations, especially organ replacement requiring cell recolonization. New multidimensional proteomic approach by flow, imaging, or mass cytometry associated with bioinformatic analysis may help to ameliorate the screening of stem cells involved in the vasculogenic process.

Declarations

Acknowledgments:

We would like to acknowledge all nurses, technicians and physicians involved in the cardiac Surgery department involved in A-TAH implantation. The central illustration figure was created with BioRender.com

Ethical Approval

Samples from the four patients in the C-TAH CE Mark clinical trial (Identifier: NCT02962973)

Consent to Participate:

All patients signed informed consent to participate to research and authorized their data publication.

Consent to Publish:

All co-authors agree to publish these data.

Authors Contributions:

LG, CG and GD analyzed the data and wrote the paper. NG, AP, LS, CP, TM performed and/or analyzed the data. CL, PI, ACarpentier and IN included patients and reviewed the paper. ACapel and PJ organized clinical trials. A Carpentier is inventor of C-TAH and reviewed the paper. DMS supervised the work, analyzed the data and wrote the paper.

Fundings:

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Competing Interests:

A Carpentier is cofounder and shareholder of CARMAT SA. DM Smadja received consulting fees from CARMAT. C Latremouille, A Capel and P. Jansen are employed by CARMAT-SAS.

Availability of data and materials:

All data are available upon request.

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Tables

Table 1: Pre-Implantation characteristics of patients implanted with A-TAH

Patients	1	2	3	4
Age (years)	66	57	70	43
Gender	Male	Male	Male	Male
BSA (m ²)	2.13	1.89	2.06	2.36
Cardiac index (L/min/m ²)	1.24	1.66	1.60	1.65
INTERMACS class	4	3	3	3
Indication	DT	BTT	DT	BTT
Support duration (days)	599	304	271	308

BSA: body surface area; INTERMACS: Interagency registry for mechanically assisted circulatory support
DT: Destination therapy, BTT: bridge-to-transplantation.

Due to technical limitations, Table 2 is only available as a download in the Supplemental Files section.

Figures

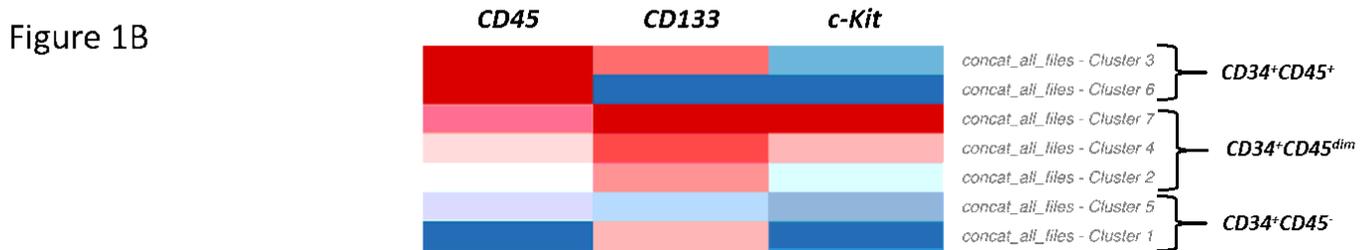
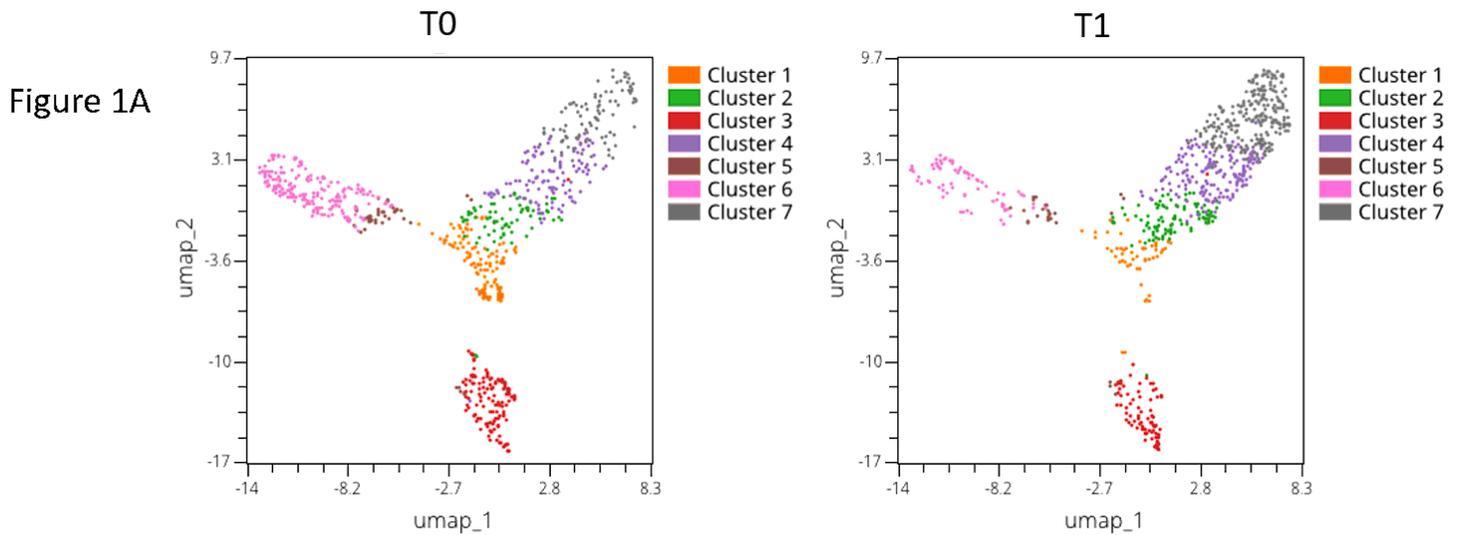


Figure 1

A- Patients concatenated CD34⁺ cells meta-clustering with UMAP visualization per condition, i.e. T0 before A-TAH implantation and T1 one month after implantation. B- Heatmap of CD45, CD133 and CD117 relative expression levels per cluster of CD34⁺ patients and time points concatenated. Central illustration figure: Using a flow cytometry approach, we demonstrated in A-TAH transplanted patients a significant mobilization of Lin-CD34⁺CD45^{dim} in peripheral blood one month after A-TAH implantation. This cell population could be at the origin of newly formed endothelial cells on top of hybrid membrane in Carmat bioprosthesis total artificial heart.

Supplementary Files

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- [Table2.docx](#)