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Droplet Motion on Sonically Excited Hydrophobic Meshes

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ABSTRACT

The sonic excitation of the liquid droplet on a hydrophobic mesh surface gives rise to a different oscillation behavior than that of the flat hydrophobic surface having the same contact angle. To assess the droplet oscillatory behavior over the hydrophobic mesh, the droplet motion is examined under the external sonic excitations for various mesh screen aperture ratios. An experiment is carried out and the droplet motion is recorded by a high-speed facility. The findings revealed that increasing sonic excitation frequencies enhance the droplet maximum displacement in vertical and horizontal planes; however, the vertical displacements remain larger than those of the horizontal displacements. The resonance frequency measured agrees well with the predictions and the excitation frequency at 105 Hz results in a droplet oscillation mode (n) of 4. The maximum displacement of the droplet surface remains larger for the flat hydrophobic surface than that of the mesh surface with the same contact angle. In addition, the damping factor is considerably influenced by the sonic excitation frequencies; hence, increasing sonic frequency enhances the damping factor, which becomes more apparent for the large mesh screen aperture ratios. The small-amplitude surface tension waves create ripples on the droplet surface.

Keywords: Sonic excitation, droplet oscillation, hydrophobic mesh, damping

INTRODUCTION

Liquid droplets and their behavior on surfaces are of interest in various applications such as biomedicine,¹ combustion,² and self-cleaning.³ In general, the balance among the external, surface tension, gravity, and viscous forces can govern liquid droplet motion on the surfaces. Force due to surface tension is related to the stiffness of the droplet⁴ while viscous force is associated with the damping of the motion under viscous dissipation.⁵ The gravitational force causes droplet puddle, which is related to the droplet size and the contact angle, provided that the puddling becomes negligible for the droplets having sizes comparable or less than the capillary length.⁶ The external force created by an acoustic excitation gives rise to a droplet wobbling while creating a fluid motion.⁷ Hence, the sessile droplet behavior can be manipulated by the acoustic waves, which causes droplet oscillatory motion. The acoustic power level of the excitation, surface tension, and viscosity of the droplet fluid remain important for the lateral and vertical motions of the droplet on the hydrophobic plane. The harmonic, subharmonic, and superharmonic modes of oscillations can occur at sonic excitation frequencies within the range of the Rayleigh-Lamb inertia-capillary frequencies;⁸ however, for low-frequency oscillations, the droplet behavior is mainly governed by the droplet size and the tension between the fluid-solid interface.⁹ Moreover, the droplets demonstrate different behavior on the oscillating liquid films and a permanent bouncing can result over the oscillating liquid film. Based on the excitation frequency and the amplitude of the excitation, mainly the Rayleigh frequencies influence the droplet bouncing mechanism.¹⁰ The nonlinear hydrodynamic effects can be created in the droplet fluid by the Rayleigh surface acoustic waves and the assumption of Stokes model for fluid motion fails to predict the fluid velocities at high oscillation frequencies because of the nonlinear hydrodynamic effects created inside the droplet fluid.¹¹ Hence, rocking, and ratcheting of droplets can occur over the surface depending on the non-linear hydrostatic effect created within the droplet. The vertical and horizontal motions of the droplet motion are limited with the droplet pinning forces due to the contact angle hysteresis and interfacial resistance. This situation is usually observed at low amplitude and frequency oscillations. However, as the excitation frequency increases the droplets can overcome the pinning forces and move into a ratcheting mode. Furthermore, as the excitation frequency increases further, the droplet can jump and break

into newborn droplets while ejected from the surface.¹² As the surface wetting changes to a superhydrophobic state, then, the sonic excitation can cause jumping of the droplets at a ratcheting mode. The impacting droplet on the oscillating surface undergoes a complicated behavior such that increasing Weber number significantly affects the retraction forces and the droplet rebound height can be attenuated because of the instability of the droplet rim.¹³ However, for the hydrophilic surfaces, the droplet behavior differs considerably under the sonic excitation. The droplet remains pinned on the surface and it shows rather sliding and climbing behavior than the rebounding; hence, depending on the sonic frequencies, the droplet shape change and the climbing height varies considerably.¹⁴

The hydrodynamic interference of droplets with the external sonic excitation can create a jetting effect on the droplet motion. The combination of increasing surface hydrophobicity, reducing droplet fluid viscosity, and increasing fluid surface tension enhances the velocity of the droplet during the jetting motion.¹⁵ The droplet jetting behavior can be modified as the droplet motion is arranged over the thin liquid film, which is excited by the sonic waves. The thin film oscillation under the surface (acoustic) waves can result in an irregular droplet wobbling behavior, which causes the complicated acousto-fluidics-phenomena while creating internal streaming in the droplet fluid and changing the droplet jetting behavior.¹⁶ In some cases, the droplet can adhere under the influence of periodic oscillations, and droplet motion becomes droplet size and oscillation frequency dependant. The transversal motion can occur predominantly within the range of the droplet's first natural frequency at which the asymmetric shape deformations are encountered. However, as the frequency increases, the adhering droplet breaks into smaller droplets.¹⁷ From the application point of view, the sonic excitation of droplets over surfaces can find solutions for some engineering problems such as surface cleaning and corrosion prevention of electronic devices¹⁸ and microfluidics of droplet displacement in micromachining processes.¹⁹ In such practical applications, the flow field developed within and around the sonically excited droplets remains critical for droplet mobility over the surfaces. Since the precise experimental investigation for internal fluidity and external flow around the excited droplets is extremely challenging, the numerical predictions of the flow field remain fruitful.²⁰ Nevertheless, accurate flow predictions can shed light on the droplet behavior over the vibrating surfaces and provides useful guidance for experimental investigations.

The sonic excitation of a droplet over hydrophobic surfaces can give rise to alteration of interfacial contact and resistance that influences the pinning force over the surface. The creation and evolution of surface tension and gravity waves and hydrostatic pressure variation in the droplet fluid modify droplet shape dynamically during the acoustic excitations. Depending on the acoustic excitation frequencies and amplitudes, the droplet can undergo various modes of oscillations. In some modes, droplet jumping and breaking into newborn small droplets become unavoidable. Although droplet behavior on hydrophilic and hydrophobic surfaces under acoustic excitations has been studied,^{6,21-23} the sonic wave direct interaction with a droplet fluid and resulting droplet motion on hydrophobic mesh surfaces were left for future study. As a liquid droplet is dispensed over the mesh surface, the interfacial area of the droplet over the mesh reduces significantly because of the open screen area of the meshes. The droplet fluid remains exposed to surrounding air over the open screen of the meshes and the sonic excitations from the droplet bottom result in pressure waves directly imposed to the droplet exposed surfaces. This alters the droplet behavior from those exposed to the acoustic excitations, such as Lamb waves, over the hydrophobic surfaces. Consequently, investigation of the dynamic response of the droplet under direct sonic excitations becomes necessary to evaluate the modes of droplet oscillation, the resonance frequency, and the time evolution of the maximum height. Hence, the droplet behavior over the hydrophobic mesh surface is studied and the influence of the sonic excitation frequencies on the droplet characteristics is examined. The metallic meshes with different screen areas are hydrophobized and a high-speed recording facility is utilized to evaluate the droplet response to the sonic excitations.

EXPERIMENTAL

The metallic meshes formed from Steel (AISI 304) wires having 400 μm diameter were used in the experiments. Figs. 1a to 1d show the schematic presentation of the water droplet over the hydrophobized mesh. The mesh has square screen spacings and the width size (a) changes for different mesh screen configurations; hence, different sizes of the screens were used in the experiments, which include the open aperture ratio of 61.17%, 62.34%, and 64.51%. The mesh screen open aperture ratio was defined through the mesh open screen area ($a \times b$, where $a = b$)

and the pitch area ($p_1 \times p_2$, where $p_1 = p_2$), $A_s = \frac{a \times b}{p_1 \times p_2} \times 100\%$ (Fig. 1c). The functionalized silica particles were used to hydrophobize the mesh wire surfaces. The solution was prepared with a mixture of 14.4 mL of ethanol, 1 mL of de-ionized water, and 25 mL of ammonium hydroxide, and later 3:4 molar ratio of silane was added.²⁴ The solution was placed in coating equipment (Biolin Scientific) and the samples were coated, and later the coated samples were placed in the laboratory fume hood for 2 hours allowing volatile compounds to evaporate. The coated surface was assessed using the scanning electron microscope (SEM, JEOL 6460) and atomic force microscope (AFM, Flex-Axiom, Nanosurf). The wetting characteristics of the coated mesh surfaces were evaluated by using a Goniometer (Kyowa, model DM 501). To create sonic excitations under the mesh, a fixture was designed and manufactured. Fig.2 shows a schematic view of the experiments. The loudspeaker (Edifier Inc.), which was operated at 9 V (DC) and 0.44 A, was used to create the adjustable sonic excitation frequencies under the hydrophobized mesh. The accelerometer was used to ensure the frequency and amplitude of the excitation sonic waves. Several tests were conducted initially to assess the droplet response to the excitation frequencies and powers. The excitation frequencies within the range of 40 Hz to 150 Hz were selected. The selection was based on the magnitude and frequencies of the oscillations created on the droplet. It is worth mentioning that by lowering the excitation frequency beyond 40 Hz, the droplet did not demonstrate notable oscillations, and the droplet mitigation from the hydrophobic mesh either by rolling or expelling (jumping) occurred as the excitation frequency was increased beyond 150 Hz. A speed-camera system was used recording the droplet behavior during the sonic excitations. The camera was operated at 5000 fps having a resolution of 1280×800 pixels with a pixel size of $14 \mu\text{m} \times 14 \mu\text{m}$. The tracker program was utilized to extract and analyze the recorded data. Uncertainty analysis was carried out evaluating the experimental uncertainty. The experimental uncertainty was determined through the method adopted earlier,²⁵ i.e. the uncertainty is: $\sigma_u = \sqrt{\int_{x_o}^{x_n} (x - x_e)^2 f(x) dx}$, where, x is the variable obtained from the data set, x_e is the mean value of the variable, n being the number of data points in the data set, and $f(x)$ is the probability function, which is in a Gaussian form. The probability distribution was used to determine the function diameter. The bias error was estimated as 0.5 pixels because of the small peaks in the distribution spectrum, which were difficult to evaluate with accuracy. The uncertainty was estimated in the order of 3.5%.

RESULTS AND DISCUSSION

A droplet behavior on a hydrophobic mesh, which is externally excited by sonic waves, is investigated. The metallic meshes are hydrophobized by depositing functionalized nano-silica particles. The influence of the sonic excitation frequency and mesh screen open area on the droplet motion in terms of natural and resonant frequencies, mode of oscillation, and droplet maximum displacement are analyzed.

Surface Characteristics of Meshes:

The optical image of the hydrophobized metallic mesh is shown in Fig 3a while the SEM micro-image of the coated surface is shown in Fig. 3b. The line scan of the surface obtained from the atomic force microscope is also shown in Fig. 3c. The meshes consist of uniformly extended square open screens and hydrophobized wires (Fig. 3a). The hydrophobized wire surface composes of agglomerated nano-silica particles forming nanosize webs-like structures (Fig. 3b). Since the particle agglomeration appears to be non-uniform over the surface, it creates nanosize cavities and pillars like topology forming the texture. This can be seen from Fig. 3c (surface line scan). The presence of nano-peaks and nano-valleys are the result of the agglomeration of the nano-particles during deposition. The maximum peak height is about 140 nm and the average surface roughness is 94 nm while the roughness parameter is almost 0.52. It should be noted that the roughness parameter is the same as the ratio of pillar area over the projected surface area. The roughness parameter partly resembles the texture morphology of the surface and as the roughness parameter approaches unity, the surface becomes highly rough, and roughness parameter zero yields no-pillars over the surface, i.e. perfectly smooth surface. The contact angle on the mesh surface is measured by a Goniometer. However, establishing the droplet contact line on the surface can differ from that of the smooth hydrophobic surface. This is because the droplet partially inflects into the mesh through the mesh screens. The apparent contact angle is considered for the measurements, which can change with the mesh size.²⁵ After considering the

mesh geometry composes of isotropic structures and the fluid inflection in the mesh screens is small, then the apparent contact angle can be written as:²⁶

$$\cos \theta_{app} = \frac{1}{D_n} (\pi - \theta_c) \cos \theta_c + \frac{1}{D_n} \sin \theta_c - 1 \quad (1)$$

where $D_n = \frac{(d+w_{avg})}{d}$ is the pitch length of the mesh normalized by the wire diameter (d), w_{avg} represents the aperture width of the mesh screen open area (spacing of two adjacent warp/weft – wrap is the wires run lengthwise of the mesh and weft is that wires run across the mesh – corresponding to the center-plane of the open mesh screen), and θ_c is the contact angle over the mesh material (steel). Fig. 4 depicts the contact angle predicted and measured with open screening area ratios. It is worth mentioning that the open screen aperture ratio represents the ratio of aperture area to the pitch area, i.e. $A_s = \frac{a \times b}{p_1 \times p_2} \times 100\%$, here a and b are the horizontal and vertical gaps in the mesh screen while p_1 and p_2 are the gaps of the centroid of two adjacent mesh wires in horizontal and vertical directions (Fig. 1c).²⁷ The deviation between the predictions and the result of Eq. 1 occurs and it is associated with the considerations incorporated in formulating Eq. 1, i.e. mesh sizes are not precisely the same and they are not exactly distributed uniformly over the entire mesh. In addition, droplet fluid inflection in the mesh screen open area may not be small for the meshes used in the experiments. The mesh size and the apparent contact angle measured for different mesh screen open areas are provided in Table 1. Increasing the screen aperture ratio incorporated in the current study lowers the contact angle. The contact angles are measured by adopting the precision measurement method.²⁸ In this case, the circumference of the droplet image obtained from the Goniometer is fitted in a mathematical function. The horizontal line is introduced to account for the contact line of the droplet. In some cases, the horizontal line may not exactly correspond to the droplet contact line; hence, a correction angle (α_{BL}) is introduced to fix the exact contact line over the surface. The droplet contact angle is evaluated from the function fitted via:

$$\theta = 90^\circ + \arcsin\left(\frac{\Delta y}{R}\right) \mp \alpha_{BL} \quad (2)$$

where Δy is the vertical distance between the contact line and the fitted curve center, and R is the equivalent radius of the mathematical function fitted. The correction angle (α_{BL}) due to the inclination of the droplet contact line varies within 0° to 3° . The error estimated in the droplet contact angle measurement basing on the several repeats is within 3%.

Table 1. Specification for wire mesh size adopted. a and b are horizontal and vertical wire spacings in a single mesh cell, and d is mesh wire diameter. $A_s = \frac{a \times b}{p_1 \times p_2}$, ($A_s = \frac{a \times b}{p_1 \times p_2} \times 100\%$, p_1 and p_2 are the gap of the centroid of two adjacent mesh wires.

a	b	d	A_s	θ_a
(mm)	(mm)	(mm)	(%)	
1.5	1.5	0.42	61.17	155
1.57	1.57	0.42	62.24	153
1.72	1.72	0.42	64.54	150

Droplet Dynamic Behavior:

The external sonic excitation of the droplet results in the formation of capillary and gravity oscillations in the droplet fluid. Depending on the wavelength of the external oscillations, the capillary wave or the gravitational oscillations become dominant in the droplet fluid. Earlier, the natural oscillation of an inviscid droplet is related to:²⁹

$$\left(\frac{f_R(n)}{f_c}\right)^2 = \frac{1}{3\pi} n(n-1)(n+2) \quad (3)$$

where f_c is the capillary frequency ($f_c = \sqrt{\frac{\gamma}{m}}$, where m is the drop mass), f_R being the natural Rayleigh frequency and n is the mode of oscillation. As the external oscillation wavelength becomes shorter than the fluid capillary length $\sqrt{\frac{\gamma}{g\Delta\rho}}$, where γ is surface tension, g is gravity, and $\Delta\rho$ is the difference of fluid and air densities, then the effect of the capillary wave on droplet

fluid oscillation becomes dominant.³⁰ Consequently, the natural frequency of the droplet oscillation can be deduced from the equation of motion (second-order linear homogenous ODE) in the form of:³¹

$$f_n = \frac{\omega_n}{2\pi} = \sqrt{\frac{n(n-1)(n+2)\gamma}{4\pi^2 \rho R^3}} \quad (4)$$

Here, ρ is the density of the droplet fluid and R is the droplet equivalent diameter. The natural frequency of the droplet oscillations varies depending on the modes (n) of oscillations. The natural frequencies predicted from Eq. 4 and measured for the droplet oscillation mode $n = 3$ are 67 Hz (prediction) and 63 ± 5 Hz (experiment) while the droplet oscillation mode of $n = 4$ is 101 Hz (prediction) and 98 ± 5 Hz (experiment). Moreover, the contact angle of the droplet changes during droplet fluid oscillations. The dependence of droplet contact angle on the oscillation frequency is formulated earlier,³² and the condition satisfying the resonant oscillation of the droplet surface gives rise to the relations:³³ $l_c = 2R\theta$ and $l_c = \frac{n\lambda}{2}$ or $\theta = \frac{n\lambda}{4R}$, here l_c is the circumferential length of the droplet over the surface, θ is the contact angle, R being the equivalent radius droplet curvature, λ is the oscillation wavelength. For the capillary waves, the frequency of the droplet surface oscillation (f_c) takes the form:³⁰ $f_c = \sqrt{\frac{2\pi\gamma}{\rho\lambda^3}}$. Since the droplet with a small volume on the hydrophobic surface demonstrates an almost spherical cap shape, the droplet volume is associated with the contact angle and the drop mass (m). The resonant oscillation frequency, then, becomes:³³

$$f = \frac{\pi}{2} \sqrt{\frac{\pi^3 \gamma (\cos^3 \theta - 3\cos \theta + 2)}{24m \theta^3}} \quad (5)$$

Eq. 5 demonstrates that as the frequency of the oscillation changes, the contact angle of the droplet on the mesh surface changes. Nevertheless, the change of the contact angle for the external sonic excitation frequencies is small and as observed from the experiments, it is within the order of $\pm 3^\circ$ at 105 Hz. The small variation of the contact angle with the frequency can be associated with the interfacial contact length over the mesh, which is greater than that of the

droplet on the hydrophobic plain substrates. It is worth noting that the droplet on the mesh has interior and exterior contact lines because of the mesh screen open area. In addition, the pinning of the sessile droplet, which is associated with the surface tension at the interface, is related to $\sim \pi D_c \gamma \cos \theta_c$, where D_c is the droplet contact length over the mesh, θ_c apparent contact angle. The gravitational and the pinning forces oppose the excitation force generated at the droplet bottom because of the pressure force created by the sonic excitation over the droplet exposed areas. Since the droplet apparent contact angle change is small, the effect of contact angle variation on the droplet oscillation frequency becomes small during the sonic excitations. This can be seen from Figs. 5a and 5b, in which the experimental data for the maximum vertical (Fig. 5a) and horizontal (Fig. 5b) displacement of the droplet surface are shown with time for different excitation frequencies and the mesh screen open aperture ratios (A_s). The hydrophobic plain surface having the same droplet contact angle is also accommodated in Fig. 5 for comparison. The maximum displacement of the droplet surface represents the difference of displacement between the droplet under sonic excitations and without sonic excitation (sessile droplet) on the mesh surface. The vertical and horizontal displacements have almost the same peak values with time for all oscillation frequencies. Increasing frequency enhances the vertical and horizontal displacement of the droplet surface, i.e. droplet surface maximum height increases. The frequencies selected enable to keep the droplet over the mesh surface through the experiments, i.e. the droplet repelling because of detachment from the surface is avoided. Since the sonic excitation is applied from the droplet bottom side, the vertical displacement of the droplet surface is larger than the horizontal displacement. Droplet oscillation creates wobbling of the droplet over the mesh surface and the frequencies incorporated does not result in the droplet rolling or sliding motions over the surface. Moreover, the influence of the mesh screen open aperture ratio (A_s) on the maximum vertical displacement is not significant (Fig. 5a). However, a small increase in the horizontal displacements is observed (Fig. 5b) such that increasing the mesh screen open aperture ratio enhances the vertical displacement of the droplet. This becomes more apparent for the mesh screen open aperture ratio of $A_s = 64.5\%$. This indicates that the extended exposure area of the droplet bottom surface results in the larger horizontal wobbling. The plain hydrophobic surface results in a larger contact surface than the meshes; however, the three-phase contact line remains smaller than that of the mesh because of the droplet fluid interface with the wire surfaces. This lowers the pinning force of the droplet over the surface. The sonic

excitations, therefore, can create a larger vertical and horizontal displacement of the droplet surface, which can be observed when comparing the horizontal and vertical displacements of the droplet at various frequencies. Hence, the droplet stability under large wobbling over the sonic excitations becomes questionable for the plain hydrophobic surface. The experimental observations demonstrate that the droplet tends to roll over the hydrophobized plain surface as the excitation frequency increases beyond 105 Hz.

Fig. 6 shows the optical views of the droplet obtained from the high-speed recording at various excitation frequencies at three different times. The vertical displacement of the droplet and mode of oscillation change as the frequency increases. However, the distinct behavior of the droplet can be observed for mesh and plain hydrophobic surfaces. The maximum droplet surface vertical displacement remains higher than that of the droplet on the mesh surface. On the other hand, the dispersion relation of the hydroelastic waves in the droplet fluid located on the hydrophobic surface plays an important role in categorizing the waves in terms of their wavelengths. In general, the dispersion relation of the hydroelastic waves in the liquid over the surface of a plate takes the form:³⁴

$$f^2 = \left(gk + \frac{\gamma}{\rho} k^3 + \frac{D}{\rho} k^5 \right) \tanh(kh) \quad (6)$$

Here, f is the frequency, k being the wavenumber, D is the plate flexural stiffness, and h is the liquid depth. The dominant fluid force can define the hydroelastic waves types. In this case, the first term on the right side of Eq. 6 resembles gravity, the second term is the surface force, and the third term is bending force; hence, the gravity and surface tension forces generally define the wave dynamics in the fluid as the drop is located on the stationary and stiff surface.³⁵ The Capillary waves are the results of the interaction due to the surface and inertial forces. The gravity waves are generated as the gravitational force (first term in Eq. 6) dominates over the surface tension and bending forces (second and third terms in Eq. 6). However, the hydroelastic forces can also be grouped in line with their wavelengths. In this case, three main scales could be introduced based on the force ratios. These are:³⁶

$$\lambda_{g\gamma} = 2\pi\sqrt{\frac{\gamma}{\rho g}} \quad : \quad \lambda_{\gamma k_D} = 2\pi\sqrt{\frac{k_D}{\gamma}} \quad : \quad \lambda_{gk_D} = 2\pi\sqrt{\frac{k_D}{\rho g}} \quad (7)$$

here, k_D is the flexural stiffness of the plate, $\lambda_{g\gamma}$ is the gravity-capillary wavelength, $\lambda_{\gamma k_D}$ is the flexural-capillary wavelength, and λ_{gk_D} is the flexural-gravity wavelength. As the wavelength becomes longer the influence of the forces creating the wave becomes dominant in the fluid 35. After knowing that the mesh has both vertical and horizontal displacements are small as compared to droplet fluid during the oscillations, the oscillation wavelengths, which are greater than the gravity-capillary wavelength ($\lambda_{g\gamma}$), governs the droplet oscillatory behavior during the excitation. Alternatively, for the droplet located on the hydrophobic mesh and flat plate surfaces, the resonant modes can occur on the surface and the nodal patterns are created on the droplet geometry, which can be observed from the optical images (Fig. 6). For the gravity-capillary dominant waves in the droplet, the resonant frequency can be further arranged to yield:³⁷

$$f^2 \approx \frac{2\pi n^3 \gamma}{\rho l_c^3} \quad (8)$$

where $l_c = 2\pi R$, R being the droplet radius and n is the integer number and takes the values 2, 3, 4, The first resonance frequency measured affecting the droplet shape is at about 67 Hz while its counterpart predicted from Eq. 8 is about 67.8 Hz for the excitation frequency of 105 Hz. Since R is in the order of 2.94 mm for the water droplet, the mode of oscillation yields about $n = 4$ 31 at the droplet resonance frequency of 67.8 Hz. It is worth mentioning that Eq. 8 is the simplified version of the equation proposed in the early study for the resonant frequency,³⁷ i.e. for Eq. 8, it is assumed that $n(n-1)(n+1) = n^3$, which results in 6.25 % of error, and the droplet perimeter $l_c = 2\pi R$, which may lead to an error because the droplet shape is not perfectly. The evaporation of the surface can also be neglected due to the short period, the total perimeter of the droplet surface (l_c) remains the same even though it deforms under the gravity-capillary forces.

Figs. 7a and 7b show the decay of the droplet maximum displacement along the x, and y-axis for various sonic excitation frequencies and different mesh screen open aperture ratios (A_s). It is

worth mentioning that the displacement is the difference between the maximum and minimum droplet vertical top height after the ending of the sonic excitations. In this case, the droplet maximum displacement is related to the oscillations after the sonic excitations being shot-off. The contact angle variation during droplet oscillation can affect the damping of the maximum displacement with time after the excitation is shot-off.³⁸ However, this influence is found to be small due to the large contact line on the hydrophobic mesh surface, which is similar to the bubbles on the hydrophobic surface. Hence, the droplet pinning force becomes larger while reducing the droplet contact angle variation with the excitation frequencies. Therefore, the dependence of the contact angle variation on the damping becomes weak and the peaks of the maximum displacement occur at the same time during shot-off period. Moreover, the decay rate of the maximum displacement amplitude provides the damping rate of the droplet oscillations. The decay rate of the droplet amplitude follows $e^{-\delta t}$, where δ is the damping factor. The damping factor reduces as the mesh screen open aperture ratio reduces. For the droplet excitation at 105 Hz and, after the shot-off, the damping factor for the vertical oscillation changes for the plain and mesh screen open aperture ratios, i.e. the damping factor takes the values of 15.6 s⁻¹, 17.5 s⁻¹, 19.04 s⁻¹, and 34.08 s⁻¹ for 61.2 %, 62,3%, and 64.5% of mesh screen open aperture ratios, and the plain surface, respectively. However, the damping factor differs for the horizontal oscillation of the droplet, i.e it takes the values 3.²⁷ s⁻¹, 5.12 s⁻¹, 9.76 s⁻¹, and 19.54 s⁻¹, for the plain and mesh screen open aperture ratios of 61.2 %, 62,3%, and 64.5%, respectively. The damping factor remains larger along with the vertical oscillation of the droplet than that of the horizontal motion. In addition, the damping factor for the plain hydrophobic surface remains lower than that corresponding to the droplet motion on the mesh surface for all excitation frequencies. Consequently, the mesh surface allows relatively gradual decay of the droplet oscillatory motion than that occurring on the plain surface. In general, the damping in the droplet occurs because of the viscous dissipation and surface tension effects. The influence of the viscosity and surface tension on the damping can be estimated, in relative terms, from the ratio of viscous to surface tension forces.⁴ This yields the expression $\sim \frac{\mu f D^2}{\gamma}$, where μ is droplet fluid viscosity, D is the droplet equivalent diameter, f is in the order of $2\pi\omega$. In this case, 60 μ L water droplet leads the force ratio in the order of 9×10^{-6} , which is considerably small. Hence, the influence of the viscous dissipation on the droplet damping is negligibly small. In addition, the

bulk viscous damping factor can be associated with the fluid viscosity, the wavenumber, and the density in the form of:³⁸ $\frac{2\mu}{\rho} k^2$, where k is the wavenumber $k = \frac{2\pi}{\lambda}$, here λ is the wavelength of the oscillation. The damping factor at 60 Hz of the droplet oscillation yields 0.14 s⁻¹, which is much smaller than that estimated from the experiments for 60 μ L droplet on a mesh screen open aperture ratio of $A_s = 61.2$, which is (7.8 s⁻¹). Hence, the damping factor is not significantly affected by the viscous dissipation in droplet fluid. The surface tension waves, which are created during the droplet oscillation, disturb the flow streaming and can cause streamline turbulence.³⁹ This, in turn, can cause turbulent kinetic energy dissipation and can contribute to the damping in the droplet oscillation. Since the excitation frequencies are low (60 Hz to 105 Hz range), the kinetic energy dissipation is considered to be small³⁷ and its contribution to the damping is expected to be very small. However, surface tension waves create small-sized spiky oscillations on the droplet surface, which is observed during the experiments.

CONCLUSION

The behavior of a water droplet on a hydrophobic mesh and subjected to the sonic excitation from the droplet bottom is considered and the influence of the mesh screen open area on the droplet oscillation is examined. The metallic meshes having square screen open areas are incorporated and the mesh surface is hydrophobized by depositing functionalized nanosize silica particles. The hydrophobized surface results in the contact angle of $150^\circ - 155^\circ \pm 3^\circ$ and hysteresis of $4^\circ \pm 2^\circ$. Increasing the mesh screen open area changes the droplet contact angle; however, the hysteresis remains almost the same. A high-speed recording system and a tracker program are used to quantify the natural and resonant frequencies of the droplet oscillations. Increasing sonic excitation frequency enhances the droplet maximum displacement in both horizontal and vertical plains, which is more pronounced for large mesh screen open aperture ratios (A_s); however, the vertical displacement remains larger than the horizontal displacement of the droplet. In addition, for a plain hydrophobic surface with the same contact angle, the vertical and horizontal displacements become larger than that corresponding to the mesh. Hence, droplet oscillation remains critical for droplet mobility over the plain hydrophobic surface, i.e. droplet can be rolled off over the hydrophobic plain surface for the frequency ranges at which the droplet remains sessile on the mesh surface. Hence, the droplet remains more stable on the mesh surface

than that on the flat substrate. For an excitation frequency of 105 Hz, the resonance frequency results in the droplet oscillation with $n = 4$ mode, which agrees well with the predictions. The damping factor for the droplet oscillation along the vertical and horizontal plains change; in which case, the damping factor attains larger values for the vertical plane than the horizontal plane. In addition, increasing sonic excitation frequency enhances the damping factor of the droplet. The contribution of the viscous damping on the droplet oscillation remains small for all sonic excitation frequencies considered in the experiments.

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Author contributions

A.A. Abubakar did the experimental and analytical works, and contributed to the writing of the manuscript.

B. S. Yilbas did the research work with the collaboration of other co-authors and wrote the manuscript.

H. Al-Qahtani did some part of the experimental and analytical work, and contributed to the writing of the manuscript.

A. Alzaydi did some part of the experimental work and contributed to the writing of the manuscript.

Declaration of interest

We declare that the work carried out and presented in this manuscript does not involve in any Financial Interest.

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a (mm)	b (mm)	d (mm)	A_s (%)	θ_a
1.5	1.5	0.42	61.17	155
1.57	1.57	0.42	62.24	153
1.72	1.72	0.42	64.54	150

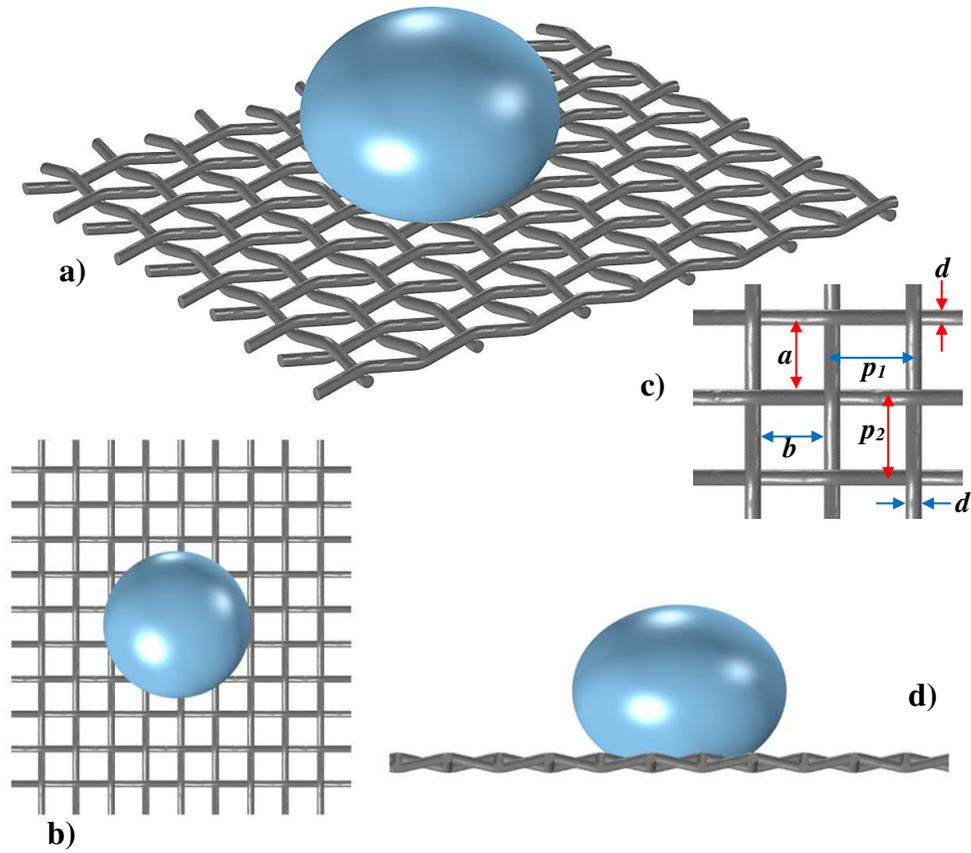


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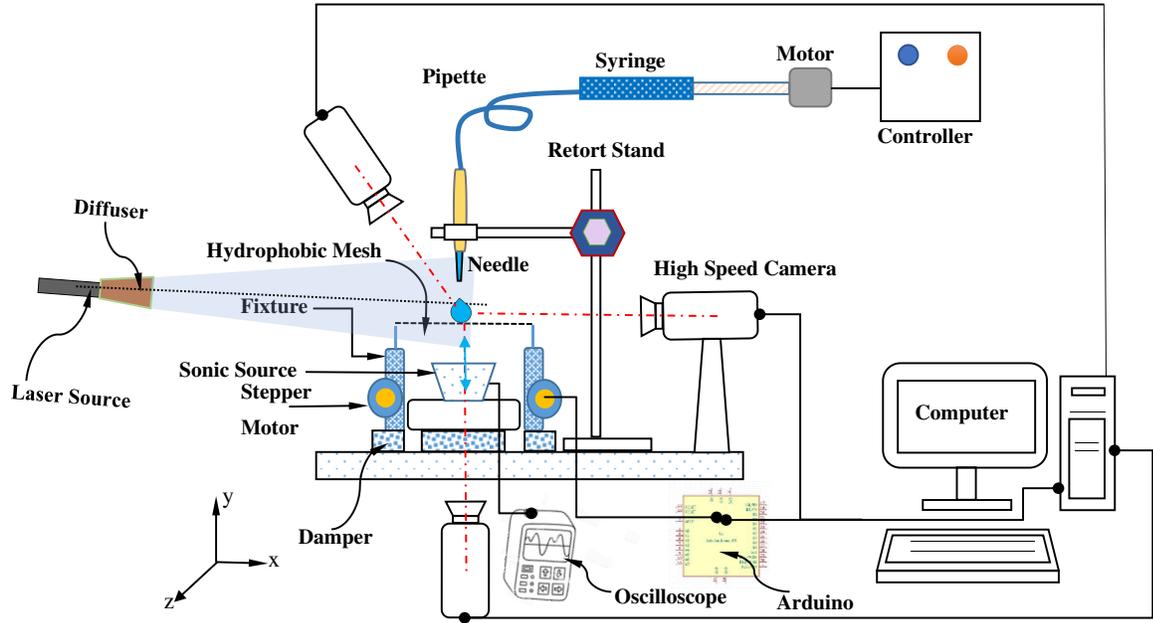


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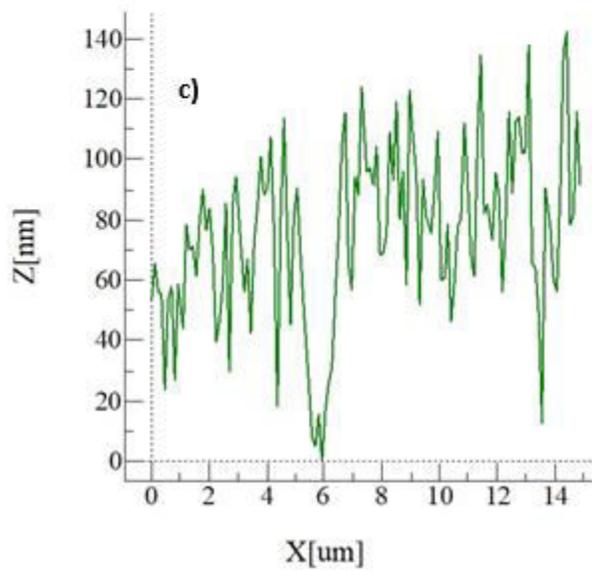
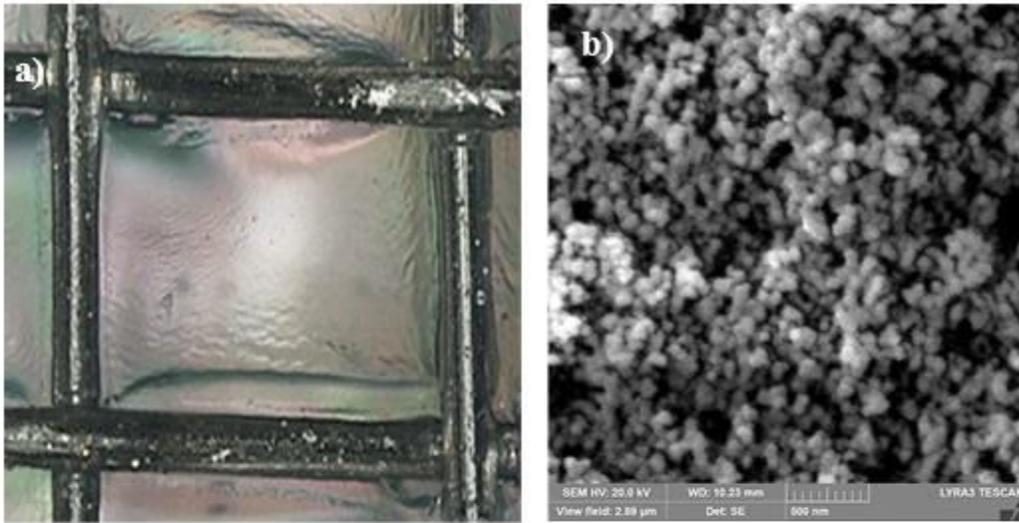


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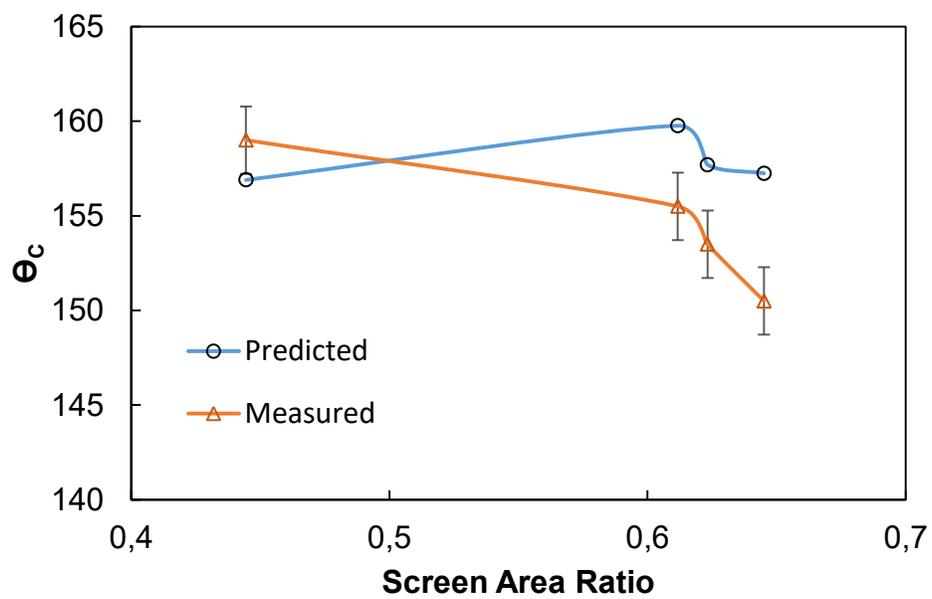


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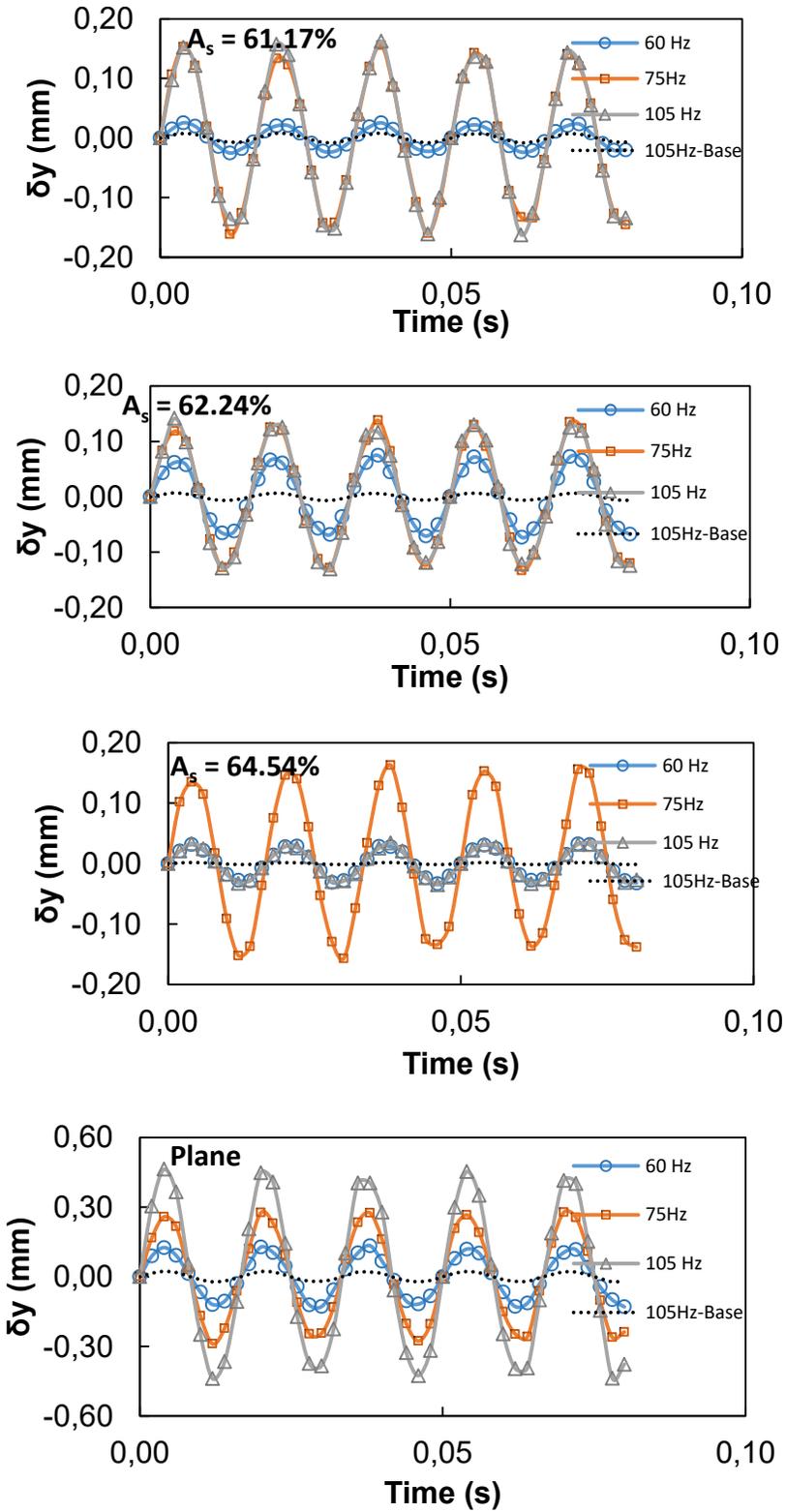


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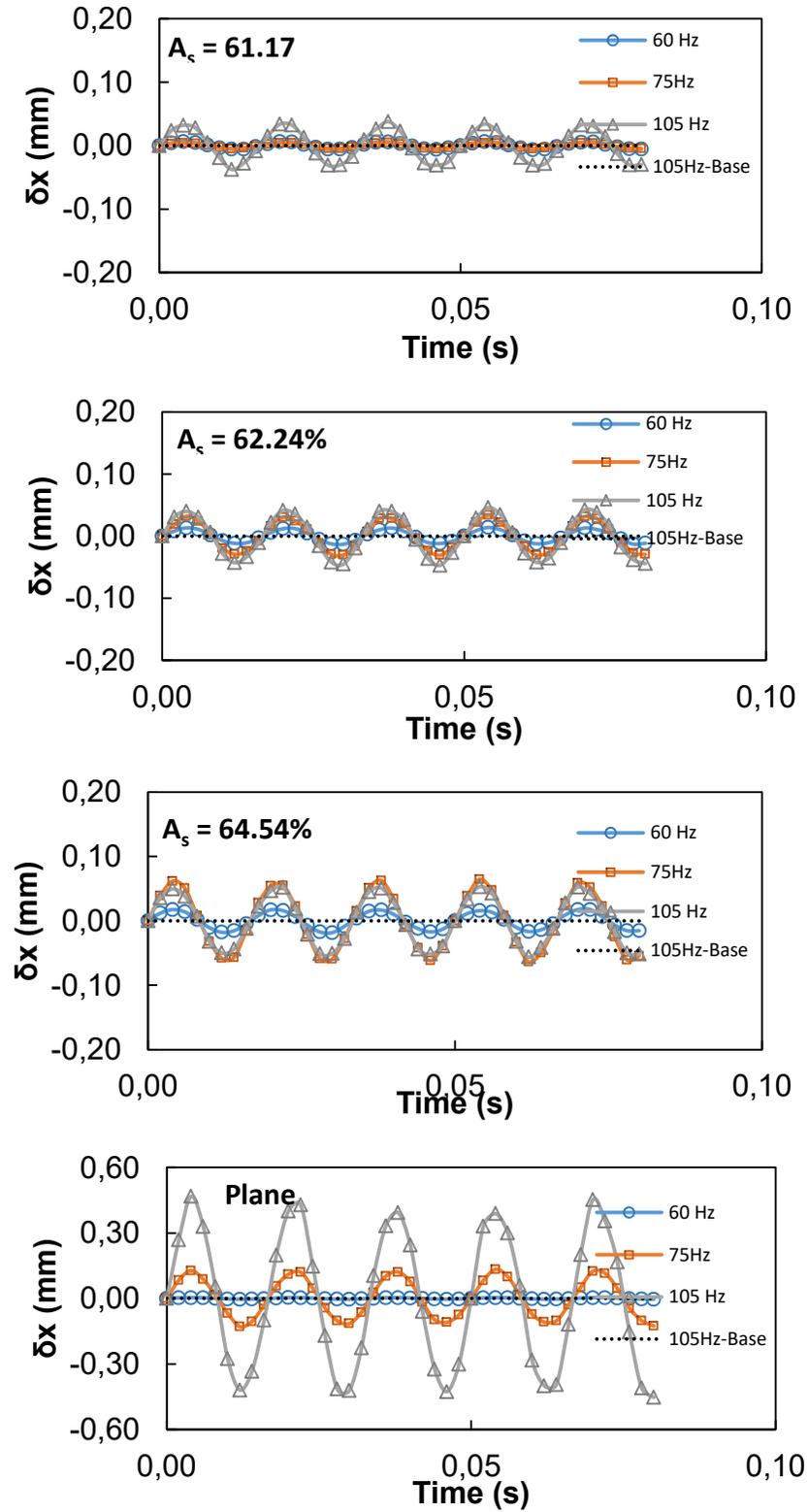


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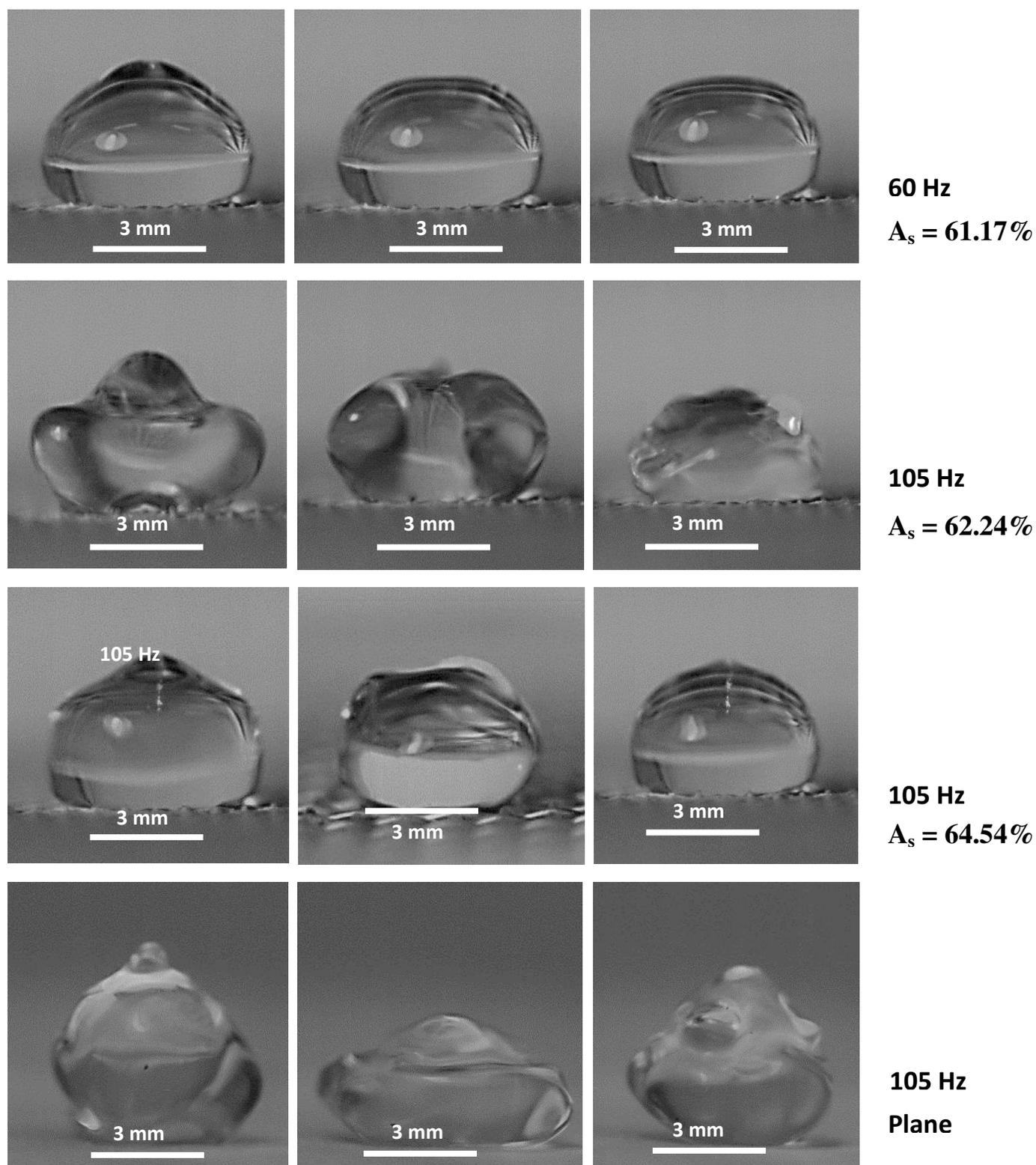


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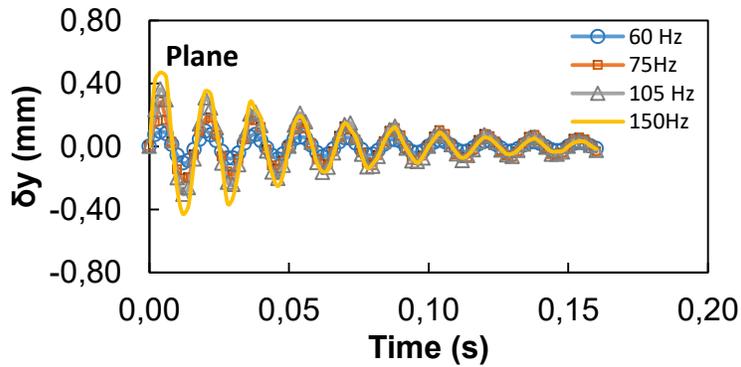
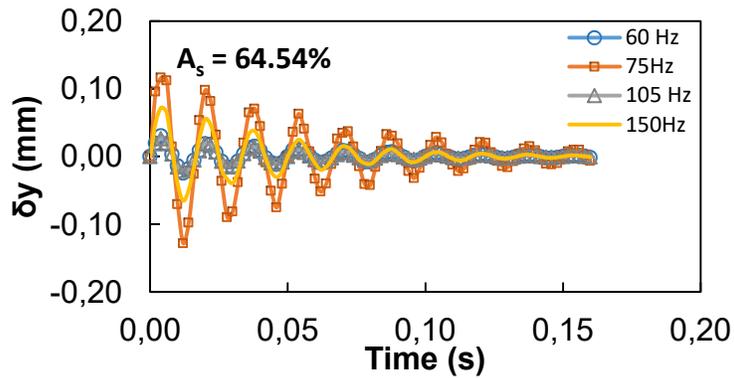
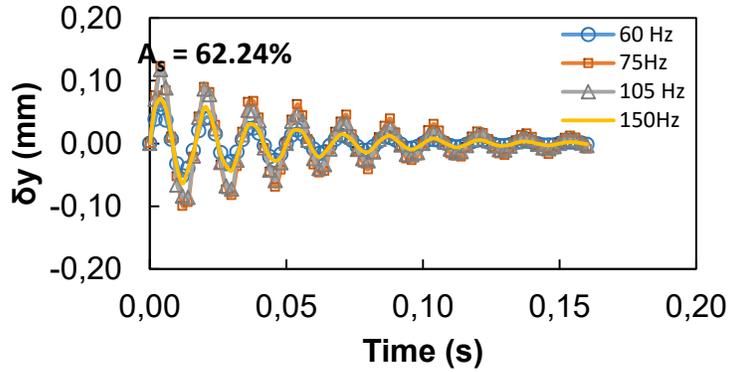
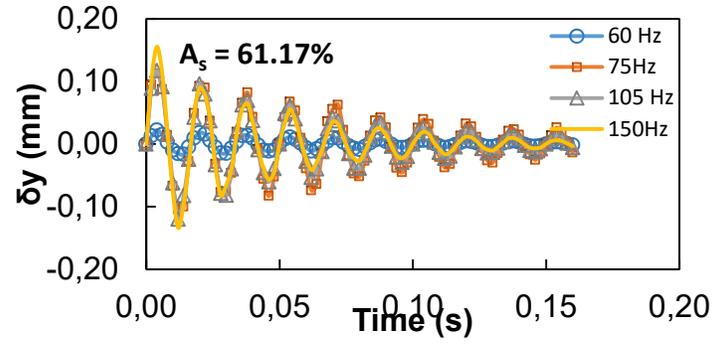


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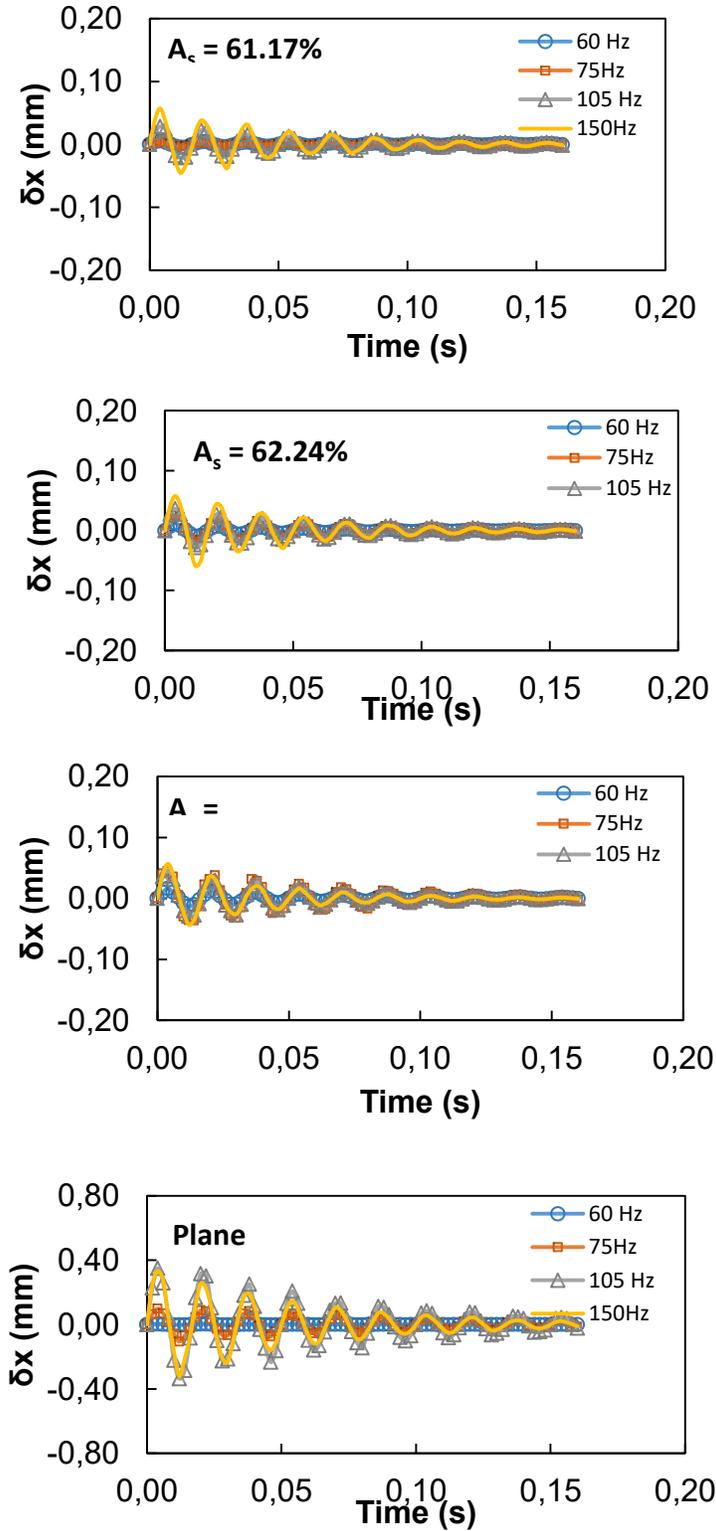


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